

THE STEP TEST FOR BIOMECHANICAL ASSESSMENT  
OF HUMAN LOCOMOTION FUNCTION

by

MARIO DONATO D'ANGELO

MD(Brazil), MSc.

Thesis submitted for the Degree of Ph.D. in  
Bioengineering, University of Strathclyde

August, 1980

University of Strathclyde

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## ABSTRACT

## ABSTRACT

Locomotion analysis and lower limb action exploration in general has reached remarkable levels of sophistication in recent years. Such sophisticated developments have been accompanied by an apparently unavoidable and increasing complexity of apparatus and equipment. This has made installation of such facilities for routine clinical use expensive and complex and in consequence there are relatively few centres which such assessments have become available for disability diagnosis and treatment monitoring.

Concurrently there has been increasing attention directed to the possibility of developing a simple technique useable in the restricted space normally available in routine clinics. Grieve et al(1978)highlighted in their exploration of movement patterns of the lower limb the potential applicability for this purpose of a "step" test. In such a test the subject raises himself from a standing position on to a step of pre-determined height leading with either the right or left leg. The full cycle consists of a step up and a step down.

The aim of the investigation undertaken has been a definitive exploration of the step test in which in addition to kinematic characteristics, dynamic assessment of the variations involved was also to be included. It was found as work progressed that the full kinetic analysis required the development of an increasingly complex computer program suitable for the generalised variability of displacements and of the force actions involved in the step specified. As things have now developed the program presented in the thesis is a format of analysis that is able to handle walking on the flat, walking up and down ramps, walking up and down stairs, jumping etc, in fact any action in which the lower limbs are involved. The development of these analyses took up a far greater proportion of the total project time than was initially anticipated. Nevertheless this being the first time that such an all embracing program was attempted, it was felt worthwhile to reallocate the effort available in favour of the program design and specification.

Inescapably the actual applied investigation involving normal subjects and patients had then to be reduced to a pilot investigation. Even this pilot programme covering 5 normal subjects and 5 patients involved the detailed analysis of some 25,000 frames of film.

The results of these tests highlight the fact that the step test in this simple form will not produce the definitive clinical data hoped for. One of the conclusions of the investigation therefore amounts to a recommendation not to continue exploration of the simple step test. On the other hand data and experience gained points clearly to the significant potential of a test consisting of the subject moving up a step by graded and varying step heights in which monitoring the kinetic changes from step to step is likely to produce data of value in diagnosis and therapy monitoring. There was no time to undertake experimental work on this step concept apart from mooting its feasibility.

The thesis consists of six chapters:-

Chapter 1 is an introduction giving an appreciation of the background presenting the clinical requirements and the clearly demonstrated need for a simple means of patient assessment.

Chapter 2 puts forward a critical review of the literature and explores in outline the classic studies of human locomotion, the clinical applications of gait analysis and the biomechanical assessment of the stepping function.

In Chapter 3 the experimental investigations are outlined in the conventional manner providing the definition and planning of the project, the development of the relevant methodology, devices and apparatus. The chapter culminates in putting forward the experimental results in sample form in the text and in full in the relevant appendices.

Chapter 4 concerns the analysis of the data collected. It is in this chapter that the formulation of a pioneer system of analysis is put forward that permits the handling of generalised human motion involving the lower limb.

Chapter 5 discusses the applicability of the step test as explored to clinical requirements as defined. It highlights the significance of the techniques evolved and suggests that the step test in its simplest form is unlikely to be capable of development into an effective clinical tool.

The conclusions in Chapter 6 summarise the findings in direct statements.

The thesis concludes with the appropriate bibliography and 2 appendices which give an outline of all the work undertaken and completed.

## ACKNOWLEDGEMENTS

This thesis could not have been written without the assistance which I have received from many people. Firstly, I am grateful to Professor R. M. Kenedi without whom this work would have never been accomplished. He also deserves my gratitude for his friendly supervision and understanding throughout the course of this project.

I am indebted to Dr. D. W. Grieve for allowing part of the analysis to be conducted in his department at the Royal Free Hospital School of Medicine in London. I am also indebted to Dr. D. G. Peacock and his staff at the Computer Terminal in the School of Pharmacy of the University of London, for their help during the long stage of data processing.

I am grateful to the British Council and the Ministry of Overseas Development whose Technical Cooperation Training Scheme supported me during the work.

My thanks to Miss Alexis Ross for the great help with the photocopying of the thesis and to Mrs. Maria Lynch for the long and arduous hours in typing this project.

I would also like to thank my colleagues of the Bioengineering Unit for their stimulating company during my time at Strathclyde.

My wife, Dagmar, deserves my special thanks for her patience and understanding which has made the accomplishment of the work possible.

The continuous help and encouragement from my father is also recorded with my deepest gratitude.

Lastly, I would like to dedicate this work to my friend and supervisor Stephan Solomonidis, who made me part of his family and I know of no words to describe my gratitude.



CHAPTER 1

INTRODUCTION

## 1. INTRODUCTION

The need to develop a simple technique for clinical assessment of the locomotor function of the lower limb has increased considerably in recent years. More recently there has been increased interest in the study of activities other than level walking, such as stair and ramp ascending and descending.

It has been suggested by D'Angelo and Grieve (1977) that stepping could be employed as a suitable test to be used in a clinical environment. In 1978 Grieve et al have provided data on the kinematics of non-pathological subjects stepping on and off a platform. By interpolating the experimental results predictions have been made for the movements in the form of angular displacement of the limb segments which would be expected on a step of rise equal to 10% of a persons height.

The present project is, in fact, an attempt to test this hypothesis viz that the step test could be used as a clinical tool. A more sophisticated technique has been used in order to obtain a complete biomechanical description of the task. It was the author's view that the forces and moments had to be included in the analysis and to give a better understanding of biomechanics involved in the proposed test. Additionally it was felt that the data from both limbs should be collected simultaneously.

The step can be negotiated forward or backwards, upwards or downwards, so that for each side of the subjects (patients) there were four manoeuvres to be analysed. In order to accomplish such analysis a comprehensive computer programme had to be developed. Priority had to be given to the development of such a programme which could form the basis for further work in this area. Considering the pioneer aspect of the research, the time available for the development of the techniques and experimental procedure it was possible to only test five normals and five patients. Nevertheless it was found that certain preliminary conclusions could be arrived at. Modifications and suggestions for further work are included.

All possible exploration of the step test as suggested were investigated within the limitations of project time and laboratory facilities.

## CHAPTER 2

### CRITICAL REVIEW OF THE LITERATURE

- 2.1 The Classical Studies of Human Locomotion
- 2.2 Clinical Applications of Gait
- 2.3 Biomechanical Assessment of Stepping

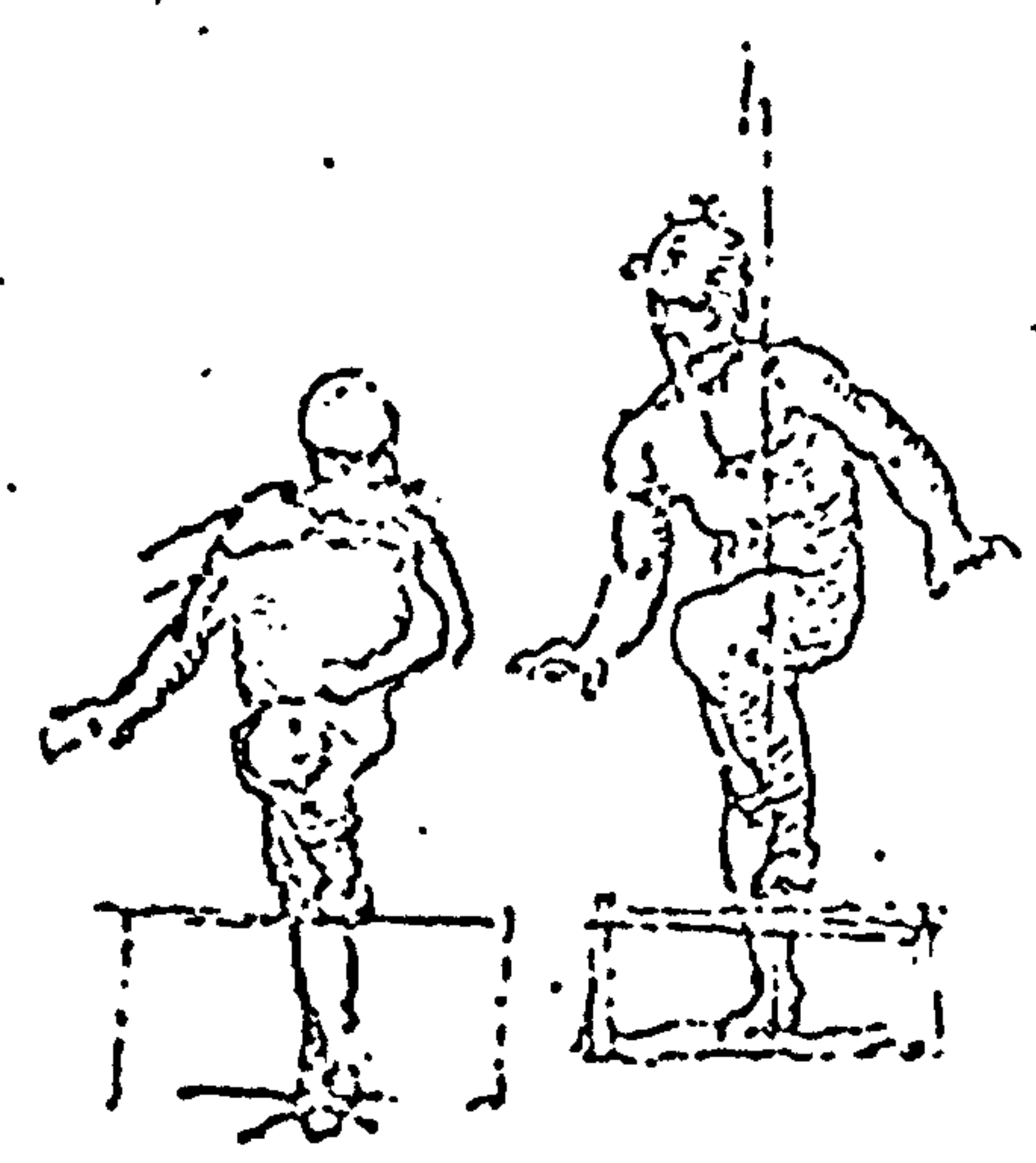
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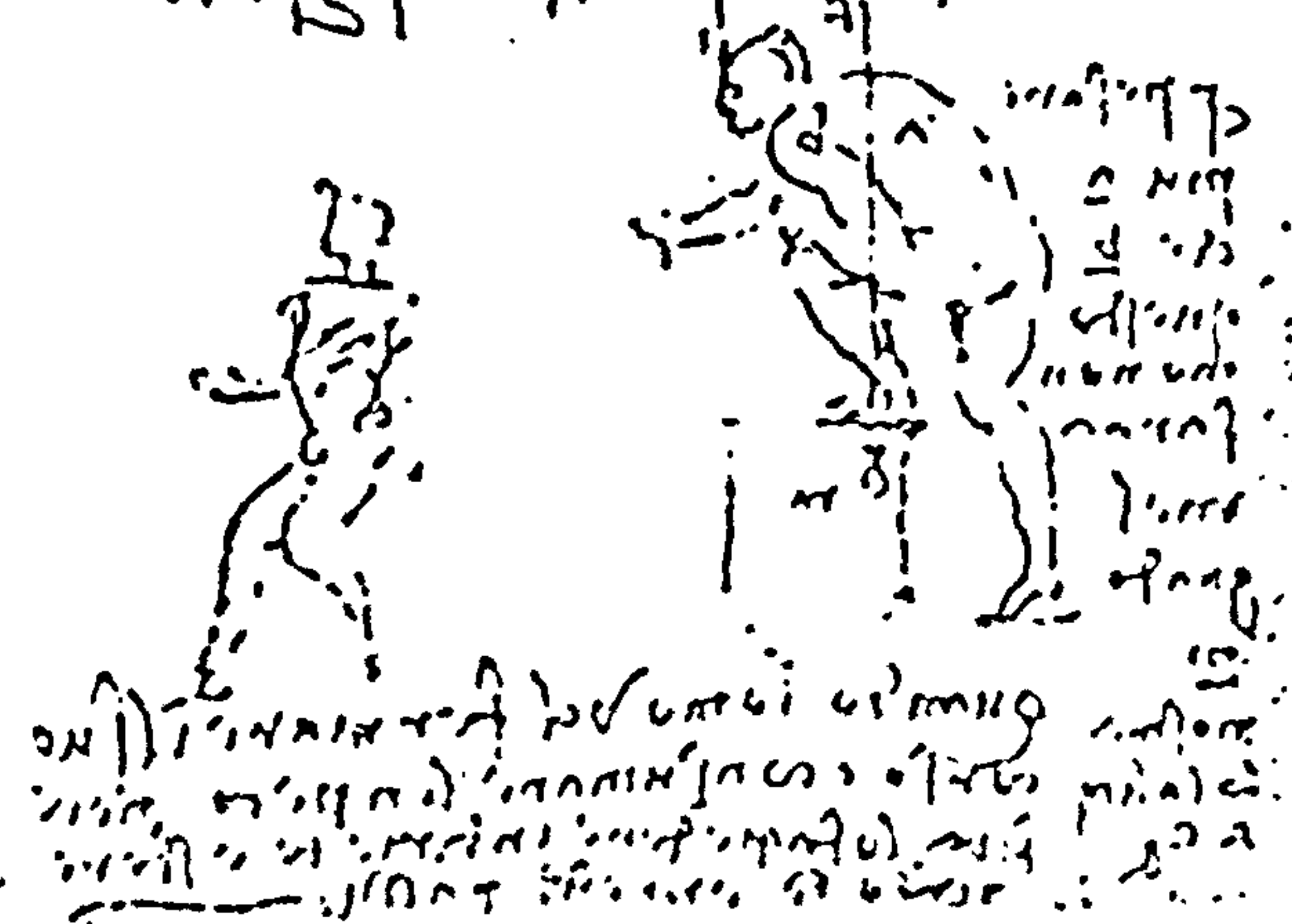


Fig 2.1

## 2. CRITICAL REVIEW OF THE LITERATURE

### 2.1 The Classical Studies of Human Locomotion

Locomotion is a phenomenon that has interested many investigators since the earliest days of our history. Walking is one of the few motor acts in which we all require a similar level of skill, since our working, domestic and social environments are designed to accommodate the walking man. Thus all possible modes of locomotion have attracted the interest of philosophers, mathematicians, anatomists, physiologists, surgeons, and recently bioengineers.

The motion of the human body in space has been investigated centuries before techniques were available for the accurate recording of the tasks. The title "Father of Kinesiology" is attributed to Aristotle (384 - 322 BC) whose treatise "Part of Animals, Movement of Animals, and Progression of Animals", has described for the first time the action of muscles and subjected them to geometrical analysis. He was the first to describe that in the process of walking rotatory motion is transformed into translatory motion.

Galen (131 - 201 AD) in his work "De Motu Musculorum" distinguished between motor and sensory nerves and between agonist and antagonist muscles groups.

Leonardo da Vinci (1452 - 1519) in his studies of anatomy was particularly interested in the structure and related performance of the human body. He has described the mechanics of the body in walking, stepping and jumping. (Fig. 2.1)

Galileo Galilei (1564 - 1643) who was a student of medicine before his searching for laws underlying certain physical phenomena, has also studied the motion of the human body. Alfonso Borelli (1608 - 1679) in his treatise "De Motu Animalium" among several things explained that bones serve as levers and that muscles function according to mathematical principles.

Direct experimentation on the movement of the body during locomotion has its foundations centuries later in the work of the Weber brothers (1836). They also initiated a series of experimental determinations of the whole body centre of gravity. The Webers observed the motions of the trunk through a telescope at a distance of 100 metres from the walkway, and in this way estimated the

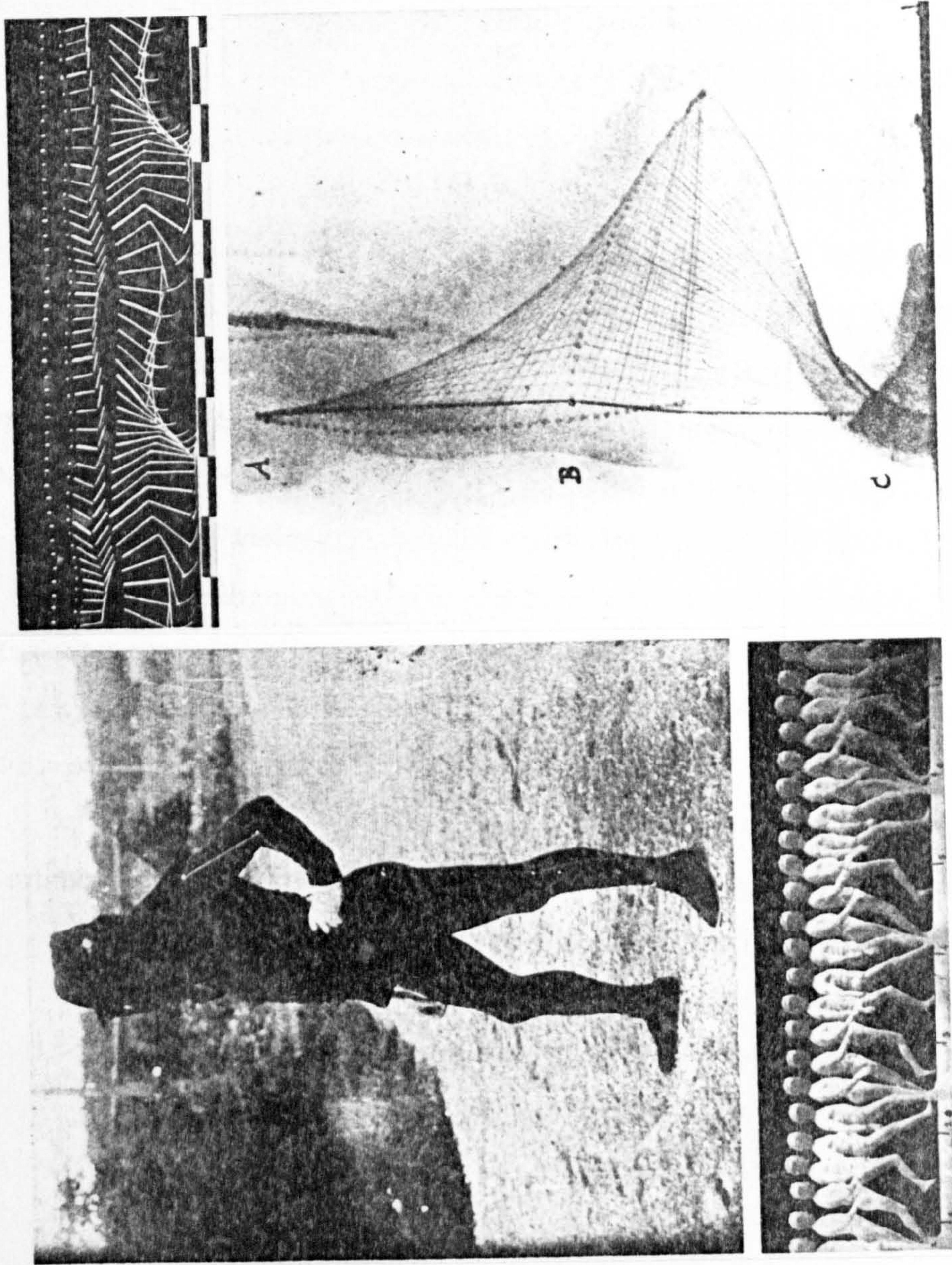


Fig 2.2

amplitude of the vertical oscillations and the inclination of the trunk to the vertical.

The first transducers attached to the body during locomotion were probably of the 'tabours' variety used by Marey (1885). His work is characterized by originality and inventiveness. He was quick to judge the importance of the work of Muybridge in 1882 which consisted of a series of photographs during the stepping of the trotting horse, by sequential exposures on 24 cameras mounted side by side. Marey however, devised a more elegant solution for field use in photographing birds and developed a photographic gun on which twelve exposures could be made in one second. The photographic plate was circular, and between each exposure ( $1/720$ th sec.) the plate was rotated 30 degrees. For the recording of human motion he invented an instrument called "chronocyclograph" which produced multiple exposures in a single photographic plate. (Fig. 2.2). A slotted disc rotated in front of the fixed plate making from  $1/10$ th exposures to  $1/5000$ th of a second. Experiments were carried out with the subjects dressed in many ways in order to produce better chronocyclographs. The precision offered by the new method allowed gait to be studied on a scientific basis.

Braune and Fisher (1890) used four chronocyclographs recording movements on the sagittal and coronal plane of walking. Incandescent tubes were attached to the limbs of a subject dressed in black. With this technique available these authors made laborious and detailed analysis of the human locomotion. From the kinematic descriptions of eleven points on the body Fisher (1898) by means of graphical differentiation, calculated the forces acting on the whole body centre of gravity. A notable aspect of the work of Braune and Fisher is the careful investigation in the area of anthropometry. Their investigation of the static and dynamic constants of human body segments provided data which was used by investigators for more than 50 years.

In 1916, Amar described an instrument that he had devised in order to evaluate artificial limbs. The apparatus which he called the "Trottoir Dynamographique" was the first force platform and consisted of two wooden beams, mounted on a cantilevered system of iron girders. In the region of each articulation a pneumatic chamber recorded pressure changes proportional to the applied force.

Amar reports the use of the force plate as an aid to the evaluation of pathological gait.

Elftman, in 1934 contributed to the study of gait with the design of a barograph which gave information on the distribution of pressure over the sole of the foot more accurately than had been previously possible. In 1939, he reported the design of a force plate which allowed him to calculate the instantaneous point of application of the force at the feet. Thus, by construction 'free body' diagrams for each segment of the lower limb and knowing the assumed centres of rotation of the joints Elftman calculates the net torque acting about the joints of the lower limbs, and from that an approximation for the net flexor and extensor muscles tensions throughout the walking cycle. In this classical paper, Elftman investigated the transfer of energy between the segments of the body in locomotion. An important concept introduced was that energy is being both supplied and absorbed by the muscles. These concepts had profound influence on future investigators in this area. Elftman, undertook further exploration on the principles of muscle action during locomotion (1941) with regard to the intrinsic property of the mechanics of muscle fibre.

Little advance was made until the work of Bresler and Frankel (1950) published, as an account of work done as part of the University of California programme. These studies basically repeated Elftman's own experiments using more sophisticated equipment. Bresler and Frankel used a platform instrumented with strain gauges to measure the vertical and horizontal components of applied forces, the torques, and to locate the instantaneous centre of pressure.

## 2.2 Clinical Applications of Gait

The majority of the work that has been done in the field of gait analysis has been undoubtedly oriented towards its possible applications in the clinical areas where locomotor assessment may be used either diagnostically or for noting progress as result of treatment. However, some of them are even more clinically oriented than the others, such as the work of Pauwells (1935). He calculated the magnitude and direction of the resultant force transmitted between the femoral head and the acetabulum for an individual standing on one leg. The value of this force he



suggested was 2.92 times body weight. The object of this work was to improve a technique for osteotomy of the hip joint.

The College of Engineering in collaboration with the Medical School of the University of California (1947) carried out an extensive locomotion study in normal and amputated subjects. The purpose of the research was to achieve improvements in the design of artificial limbs. The most significant development of the California Group was the design and construction of an accurate force-platform, which measured the components of the resultant force in three dimensions at the centre of the top plate and the component moments about these axes. They have used two force-plates (Klopsteg and Wilson 1954) avoiding the assumption of absolute symmetry in the forces developed by the two lower limbs. As part of the same project, Bresler and Berry (1951) had expanded the classical work of Fenn's calculations of energy and power input-output relationships during normal and amputee gait (Bressler, Radcliffe and Berry, 1958). They characterized gait as a "push-pull" mechanism involving the expenditure of energy by the posterior limb and the absorption of energy by the anterior limb. They also emphasised the value of the "lock-unlock-lock" sequence of events at the normal knee joint in maintaining the energy level of the head, arms and trunk (HAT) relatively constant. The positive moment immediately following heel strike indicated the resultant force passing anteriorly with respect to the knee joint giving the stability that the authors called "locking". The reaction moves to a line of action which falls posterior to the knee joint, referred to by the authors as "unlocking".

Marks and Hirschberg (1958) attempted to use a force platform on the analysis of hemiplegic gait, and were able to show significant differences in the vertical force and knee moment curves obtained from normals and hemiplegic subjects. Drillis in 1958 suggested that measurement of the time period between the two peaks of the vertical force, in relation to the total stance force may be a useful indicator of pathological gait.

The work of the Californian group was extended by Paul (1965). The line of actions and moment arms of the ilio-psoas, rectus femoris, gluteus maximus, biceps femoris, gluteus medius and adductor magnus muscles were approximated

to by measurements related to elastic threads appropriately attached to a skeleton. The period of activity of these muscles was detected by surface electromyography. With the use of photography and force-plate the net force and moment at the hip were calculated throughout the complete walking cycle. Furthermore by making certain assumptions Paul was able to estimate the three components of force between the head of the femur and the acetabulum. His results showed peak joint forces of approximately six times body weight to occur during the first 20% of the walking cycle.

Rydell (1966) made direct measurements of these forces *in vivo*, using a strain gauge instrumented head of an Austin-Moore hip prosthesis. The forces have been recorded during locomotion and other activities post operatively of a subject. The results showed peak forces of approximately two time body weight in one subject and over three times body weight in a second subject. Some dependance on the speed of walking was shown.

Most of the investigations concerned with pathological locomotion have been limited primarily to kinematic studies. As a typical example, Saunders (1952) postulated six determinants that may be used to assess gait patterns, they are: Pelvic rotation, pelvic tilt, knee flexion in stance phase, foot mechanisms, knee mechanisms and lateral displacements of the pelvis. All these determinants act to produce a sinusoidal displacement of the centre of gravity of the body of low magnitude, since this requires the minimal expenditure of energy.

Murray (1964) carried out a comprehensive study on the kinematics of human locomotion, obtained from photographic techniques producing "stick diagrams". This study was carried out in order to provide normal standards with which measurements of abnormal gait may be compared. The data was obtained by interrupted-light photography and the subjects were appropriately marked with reflective targets. Speed and timing of gait, stride dimensions, angular and linear displacements of the trunk and the limbs were measured and analysed.

While many workers have derived important conclusions from information concerning the linear and angular displacements of parts of the body in space as a function of time, others have tried to make use of the angular displacements of the lower limbs by producing means for the presentation of this basic information

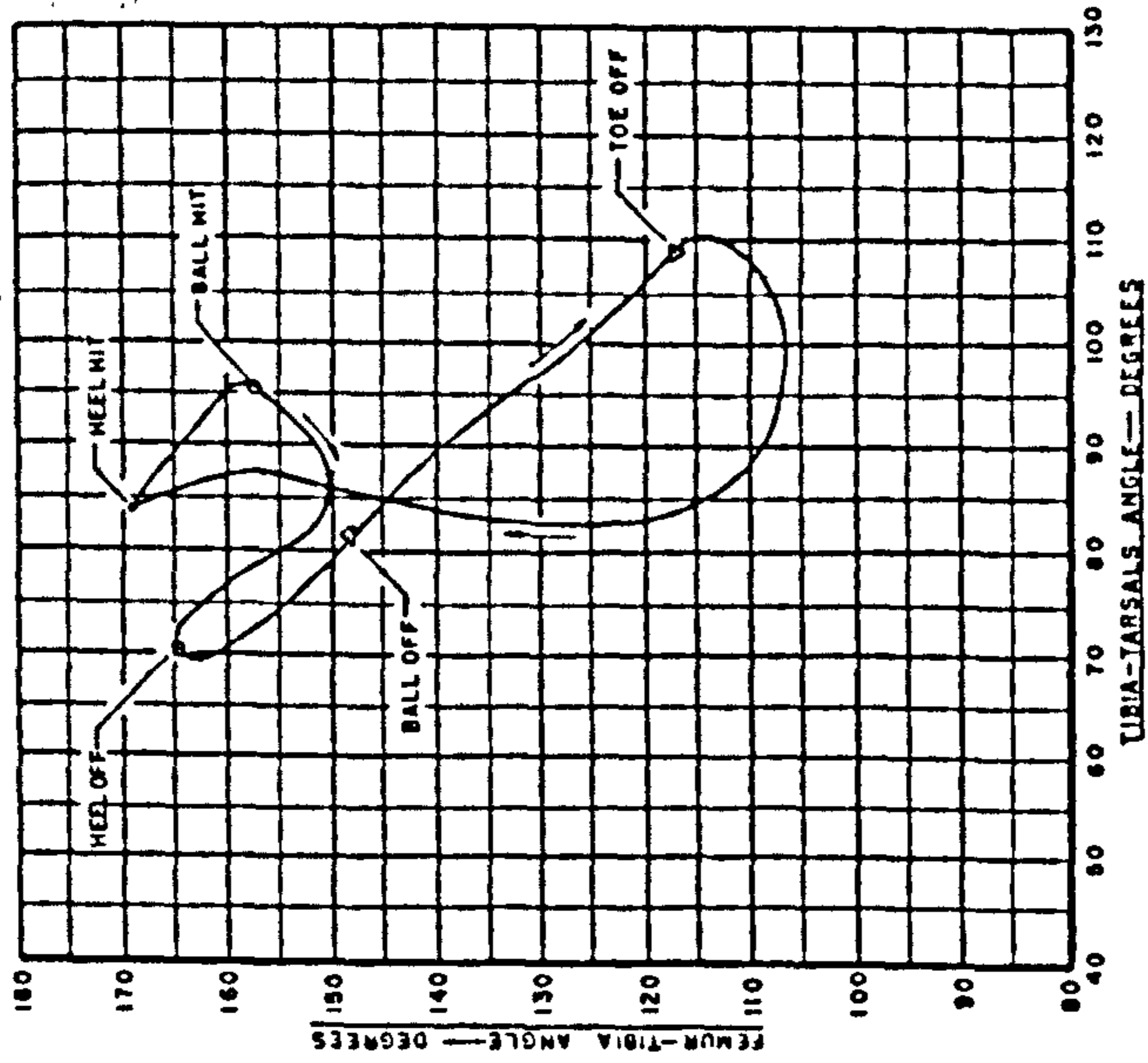


Fig 2.3

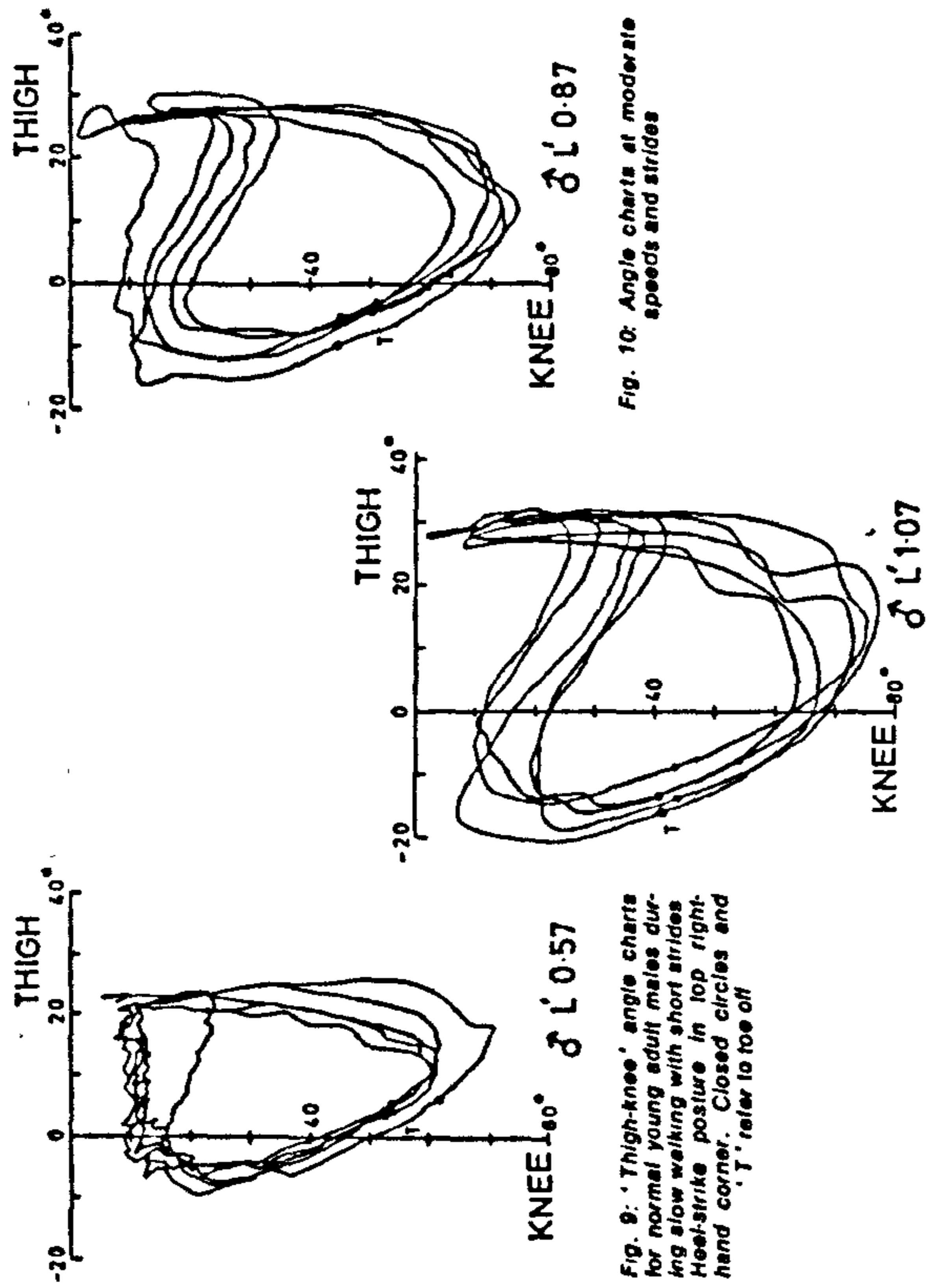


Fig 9: 'Thigh-knee' angle charts for normal young adult males during slow walking with short strides. Heel-strike posture in top right-hand corner. Closed circles and 'H' refer to toe off

Fig 10: Angle charts at moderate speeds and strides

Fig 11: Angle charts at fast speed and stride greater than stature

Fig 2.4

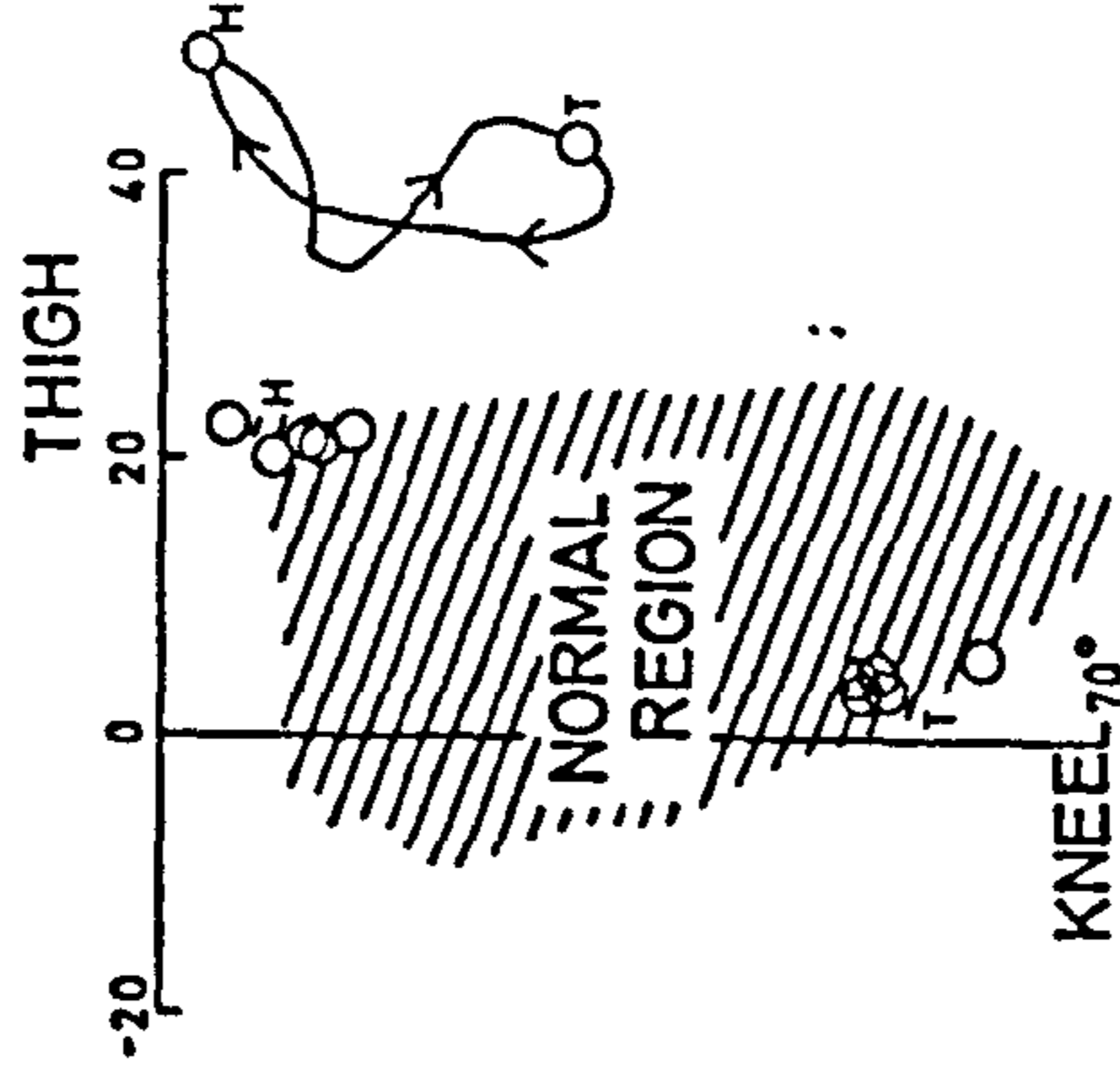


Fig 2.5

Fig 12: Thigh-knee angle chart for patient with painful hip (on right) together with region of normal charts for slow walking. 'H' and 'T' refer to heel-strike and toe-off respectively

in a meaningful way, enabling a pattern of movement to be characterized by a shape which is easily recognizable. This is achieved by producing a plot of one angle as a function of another angle. Wagner and Catranis (1954) (Fig.2.3) and Grieve (1968) (Fig. 2.4). Grieve called these charts "angle-angle diagrams" and he explored the idea of studying families of similar shapes in order to identify pathological conditions. According to Grieve's philosophy these shapes would be easily recognizable by a mathematically untrained person (clinician, paramedic, etc) just by looking at the shapes of the diagrams (Fig.2.5).

### 2.3 Biomechanical Assessment of Stepping

Although there is literature of a substantial amount of research on the biomechanics of human locomotion in level walking, very little is to be found for other activities such as the 'step' action. (Refer to section 3.1).

Cappozzo and Leo (1974) have used Fourier series to obtain a mathematical description of the kinematics of normal subjects walking upstairs, and devised a mechanical model in order to calculate the muscular moments around the major points of the lower limbs. The object of the exercise was to produce a descriptive technique which would facilitate the collection of reliable data in order to detect the important features of such manoeuvres so that the design of actual prostheses could be improved, and to be able to develop sophisticated walking machines. The authors described a characteristic pattern for all gait with a stride period from 1 to 1.50 seconds. No correlation could be made between the stride period and the anthropometric measurements, as the number of subjects tested was small. They suggested that when the stride period is outside of these above range some variations are evident, which could be correlated to a change of gait. The authors have presented an elegant technique to overcome the problem of handling kinematic data.

Grieve et al (1978) studied the kinematics of 21 normal subjects stepping at three different step heights. The sagittal plane rotations of the thigh and shank were recorded using a polarized light goniometer (Polgon). The purpose of this research was to attempt to establish a clinical test of the locomotor function of the lower limb. They have correlated the data between the heights of the step with the subjects stature and predicted norms for a step equal to 10% of the

stature. Only one leg was monitored at a time, no attempt having been made to measure both limbs simultaneously and only angular displacements were recorded. They expect that idiosyncratic differences could easily be detected by comparing the angle-angle diagram between subjects.

## CHAPTER 3

### EXPERIMENTAL INVESTIGATIONS

#### 3.1 Definition and Planning of Project

#### 3.2 Devices and Apparatus

#### 3.3 Methodology and Data Collection

##### 3.3.1 General

##### 3.3.2 Laboratory Procedure

##### 3.3.3 The Tests

#### 3.4 Experimental Results

##### 3.4.1 General

##### 3.4.2 Film Analysis

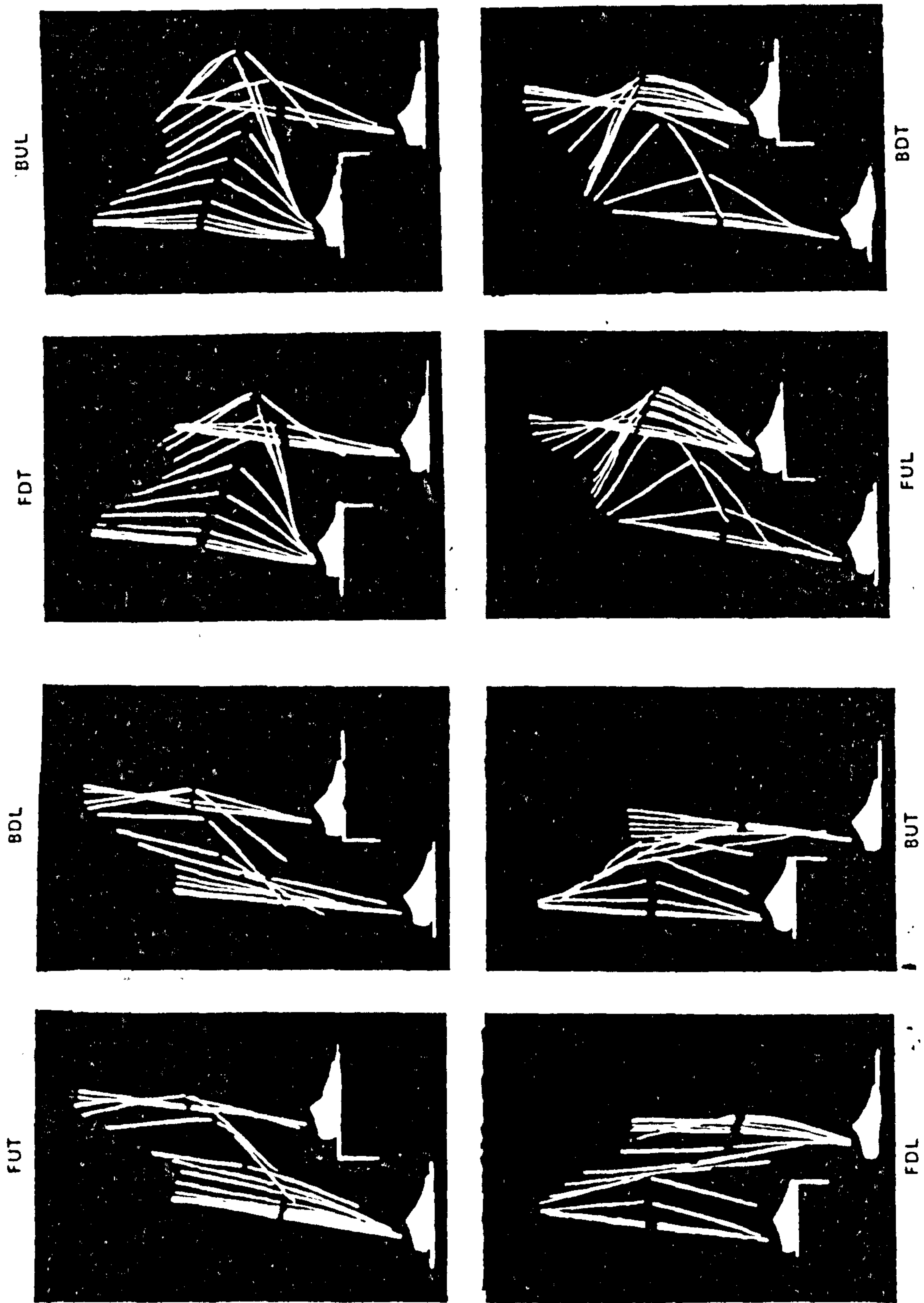


Fig 3.1 Strobe-flash photographs (re-touched) of marker tapes on the right limb of a normal adult male performing the four pairs of manoeuvres described on the text.

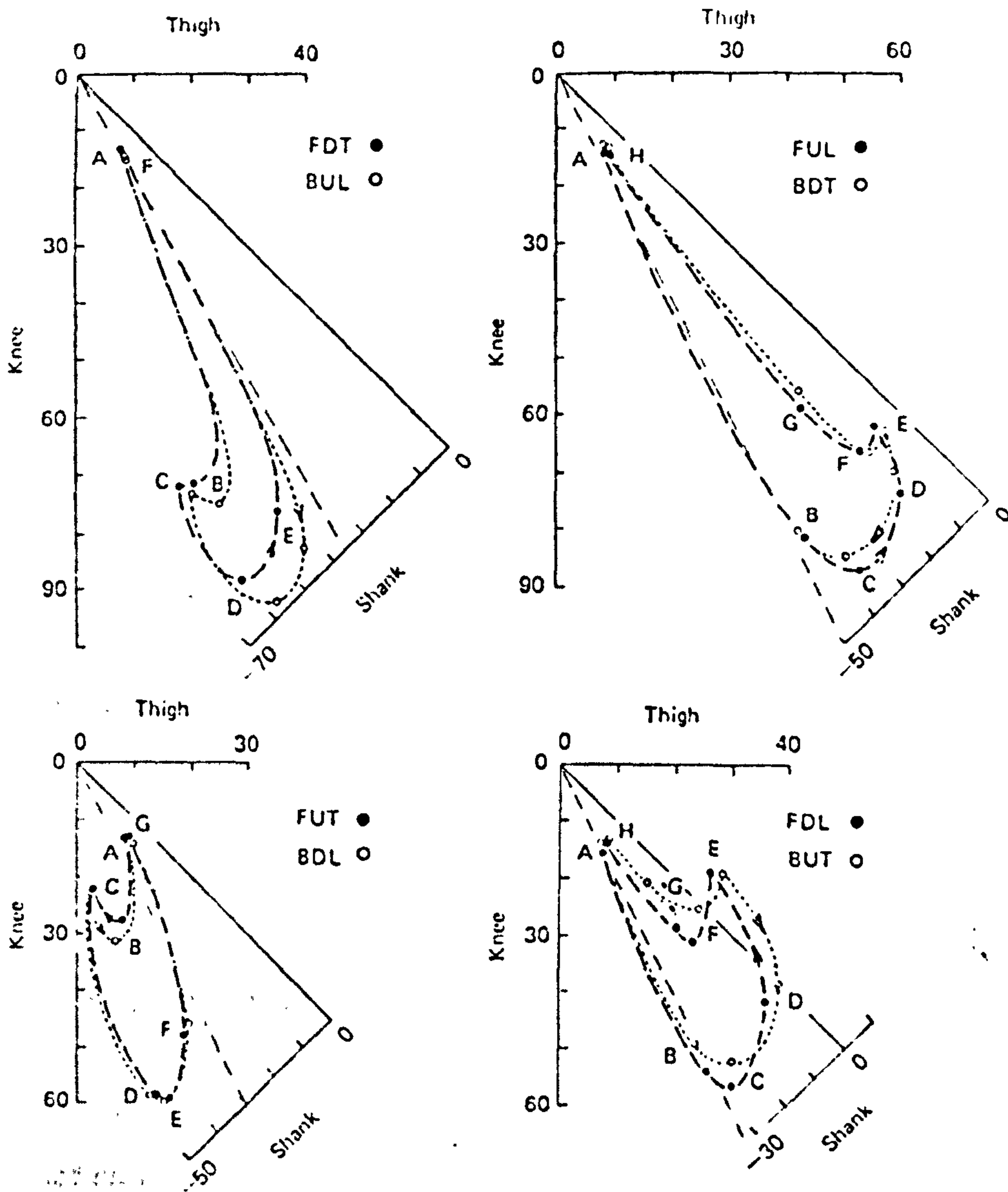
### 3. EXPERIMENTAL INVESTIGATIONS

#### 3.1 Definition and Planning of Project

Many aspects of gait have been widely studied both in experimental and clinical contexts. These include the assessment of the kinematics of the body segments as well as the ground to foot reactions and intersegmental loads transmitted by the major joints of the lower limbs. Although some different activities such as stair and ramp ascent and descent have been reported by and large the most widely studied activity has been the steady state walking on level surfaces. It has been suggested (D'Angelo and Grieve, 1977) and (Grieve et al 1978) that stepping could be employed as a test to be used for clinical assessment of the locomotor function in the lower limb from considerations of standardization, accuracy, convenience and minimal demand on space. The stepping movements can be performed in either a forward (F) or backwards (B) direction and in relation to the level surface, it can be either upwards (U) or downwards (D). When a limb leads (L) upwards and forwards in a stepping action, anti-gravity movements are performed which are in reverse time sequence of those it executes as a trailing (T) limb in the gravity-assisted movements backwards and downwards. Such conjugate pair of movement exhibit remarkable similarities in normal subjects (Fig. 3.1) although flexions in one case are extensions in the other, movements that are assisted by gravity in one are opposed by it in the other, and the muscle that is acting concentrically in one case will be acting eccentrically in the other.

Grieve et al (1978) provided data on the kinematics of non-pathological subjects stepping on and off a platform of various height. Predictions have been made of movements which would be expected on a step equal to 10% of a persons height. The biomechanical interpretation of such a task suggests that there would probably be less similarity in the conjugated manoeuvre in the presence of neuromuscular and articular disorders: thus it might be possible to assess performance by making within-subject comparisons. Considerations based on these studies show that more extreme positions of the joints are involved (using the letters above) in the FUL-BDT and FDT-BUL manoeuvres. This is due to the fact that the body passes through a position in which one limb is in contact with the step at the





Predicted forms of thigh-knee diagrams to be expected at a relative step height equal to 10% of stature.

Fig 3.2

same time as the contralateral one is acting as a support on the ground. This is a closely linked manoeuvre in which the position of the leading limb must closely reflect the difference of the height of the step and the ground (Fig. 3.2).

The present work reports a comprehensive three dimensional biomechanical analysis of "stepping" both for normals and for patients suffering from knee disorders. The activities analysed included taking a single step on level and on a step equal to 10% of the subjects height, both including their inverse manoeuvres. From all the possible combination of postures, the FUL-BDT has been chosen, because it represents the most natural task, i.e. the one that the subjects would have more confidence in performing as well as the one which is more likely to show variations.

### 3.2 Devices and Apparatus

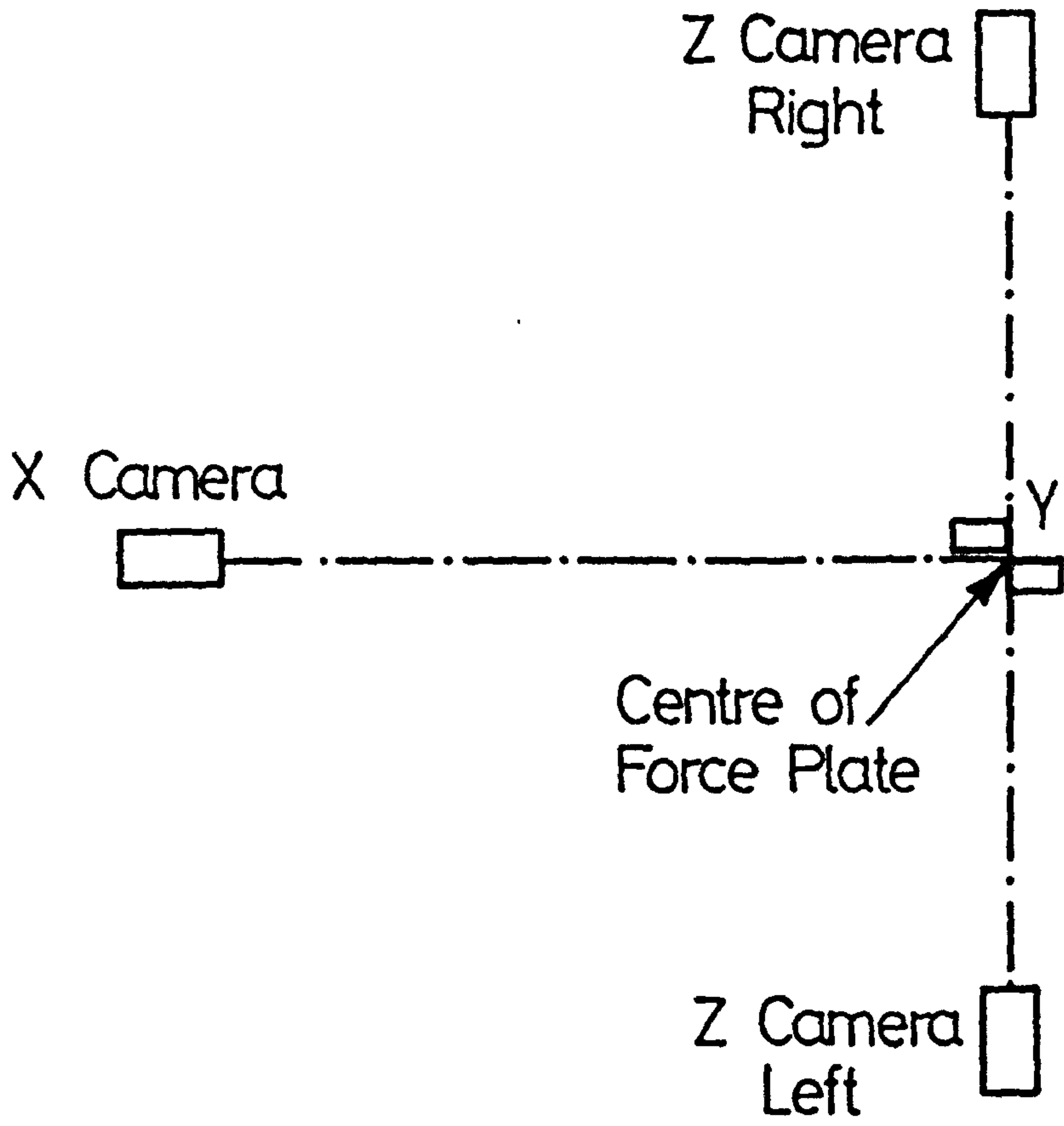
The tests were conducted using a walkpath incorporating two force sensitive platforms and three 16 mm cine-cameras. The forceplates are those supplied by the Kistler Instrument Company, and consist of two rigid steel plates supported on four transducers. The transducers which are of piezo-electric type, are mounted in such a way that it is possible to measure any force applied in terms of three orthogonal components (cartesian system) together with the three moments about the axes of the plate.

The platforms are mounted on concrete foundation blocks and are housed in a recess in the floor, so as the top of the plates are on the same level as the floor.

A set of nesting wooden platforms each of one cm thick were placed on top of the plate in order to create a step relative to 10% of the subject's height.

The twelve channels containing the force and the moment signals generated by the two force plates transducers are recorded and stored in magnetic tape at a sampling frequency of 50 Hz. This is achieved by means of a PDP-12 digital computer (Digital Equipment Co.). The analogue signals are later converted into digital form through a standard program (editor).

The kinematic data are obtained through photographic techniques and are recorded by three Paillard Bollex H. 16 (16 mm film) cine-cameras mounted



WALKPATH VIEWED FROM ABOVE

Fig. 3.3

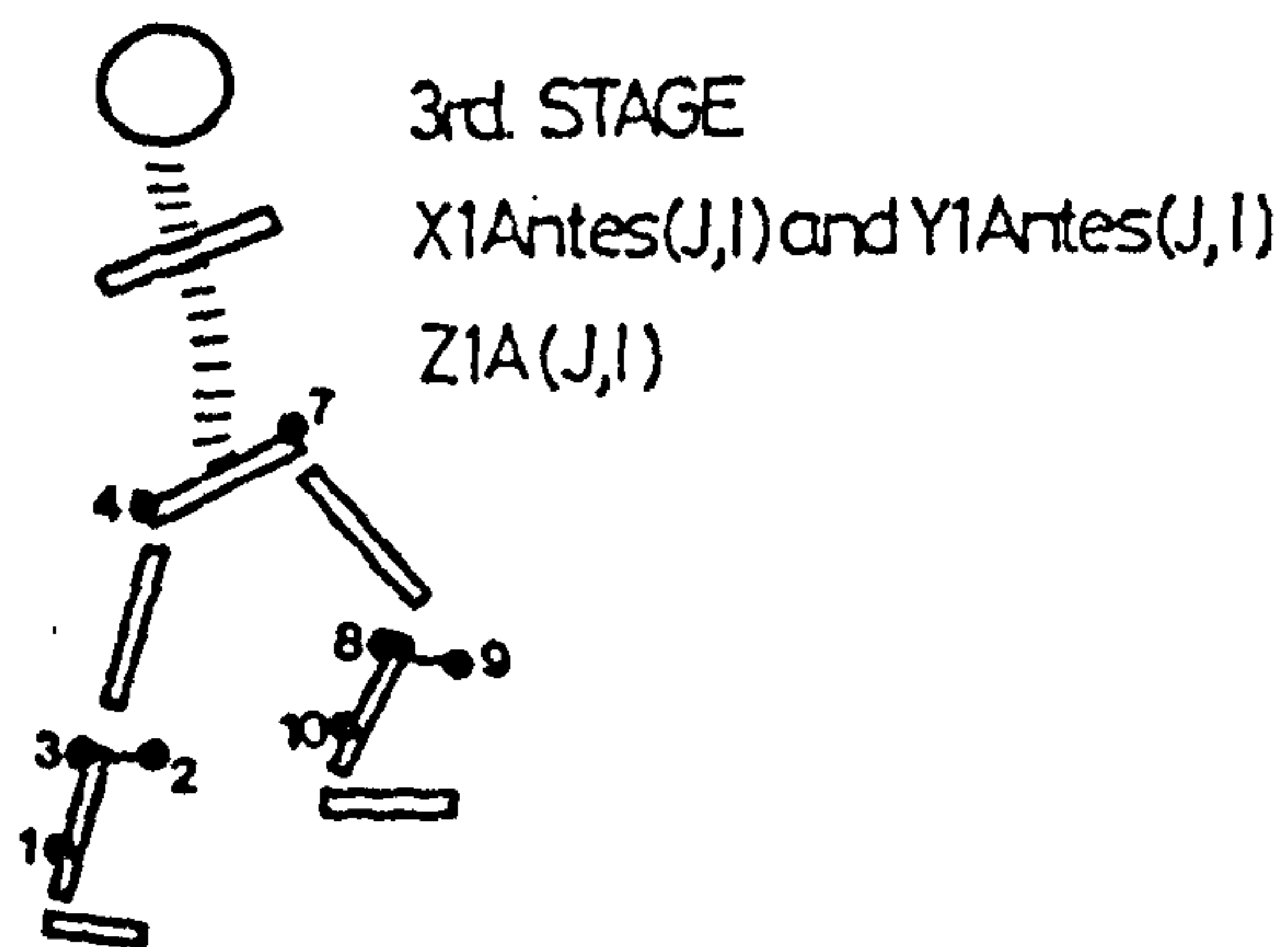
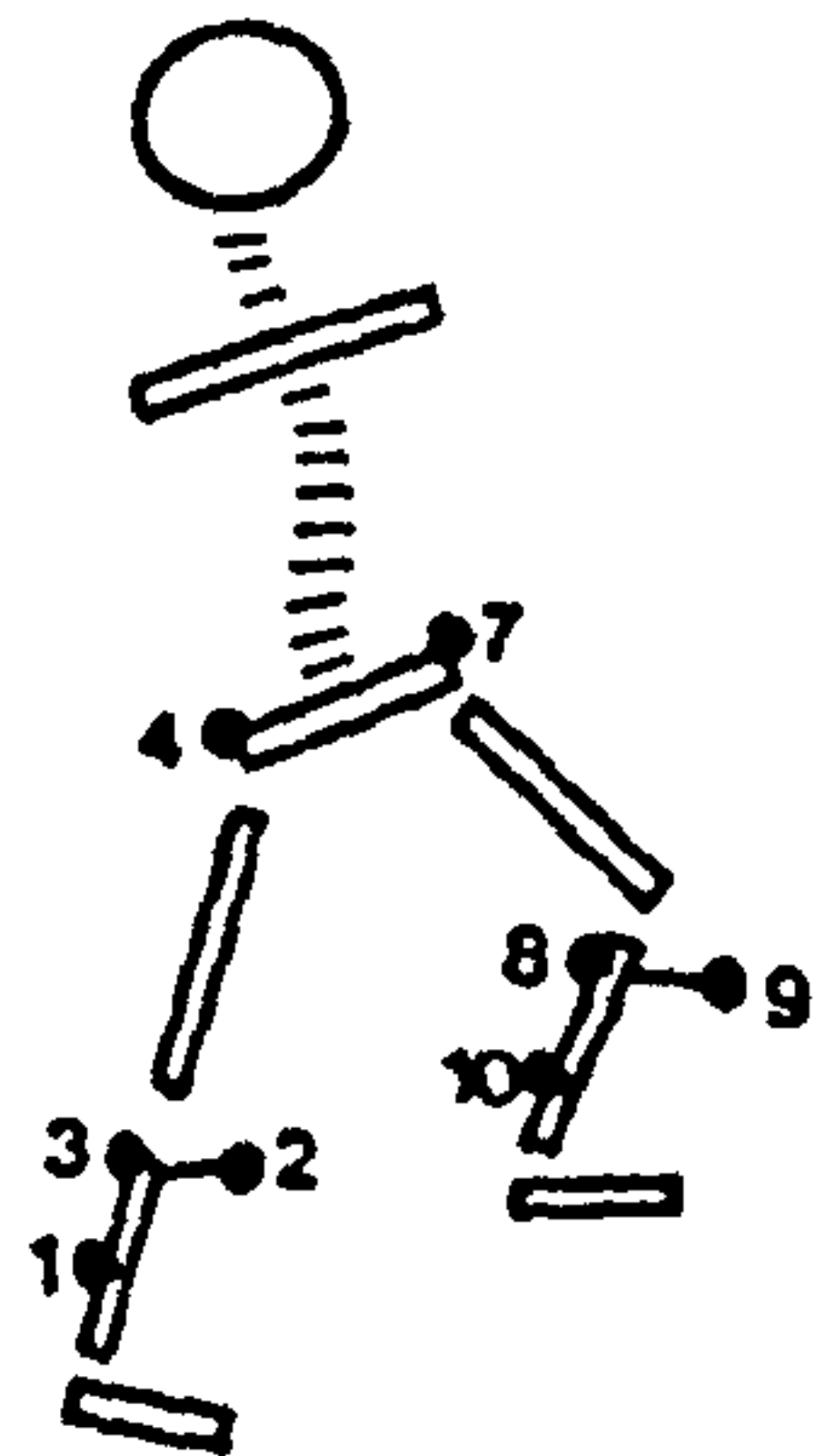
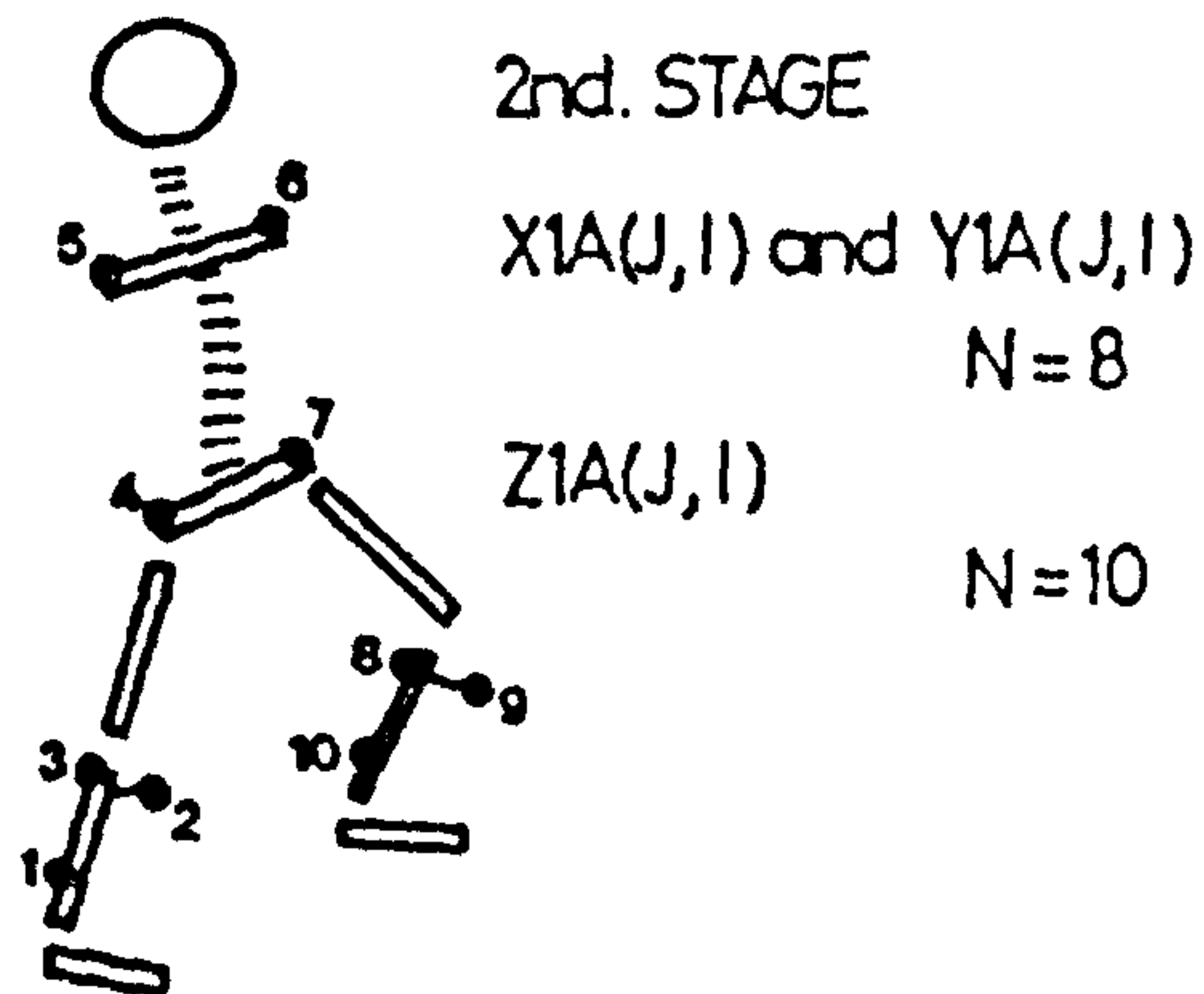
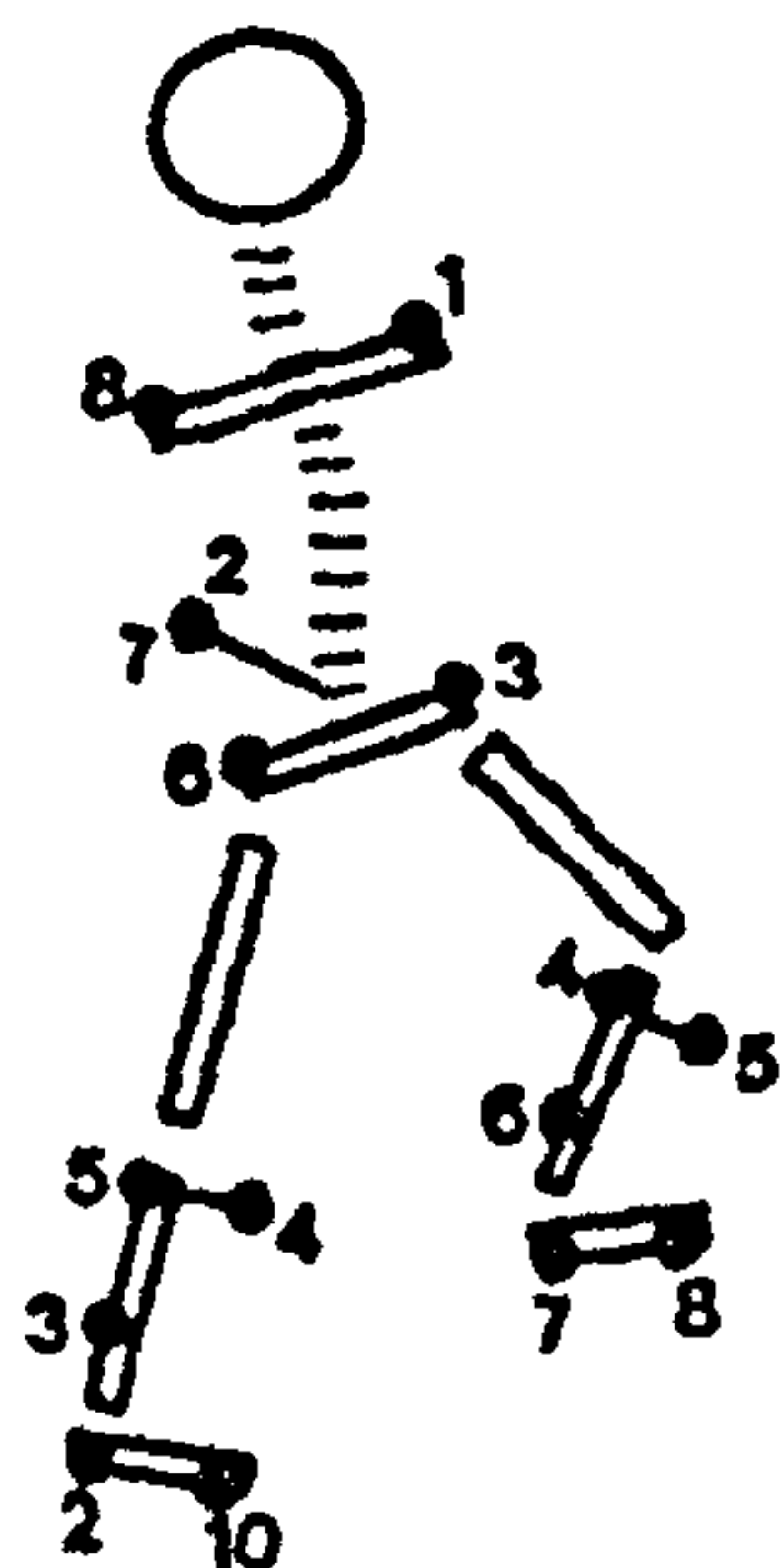
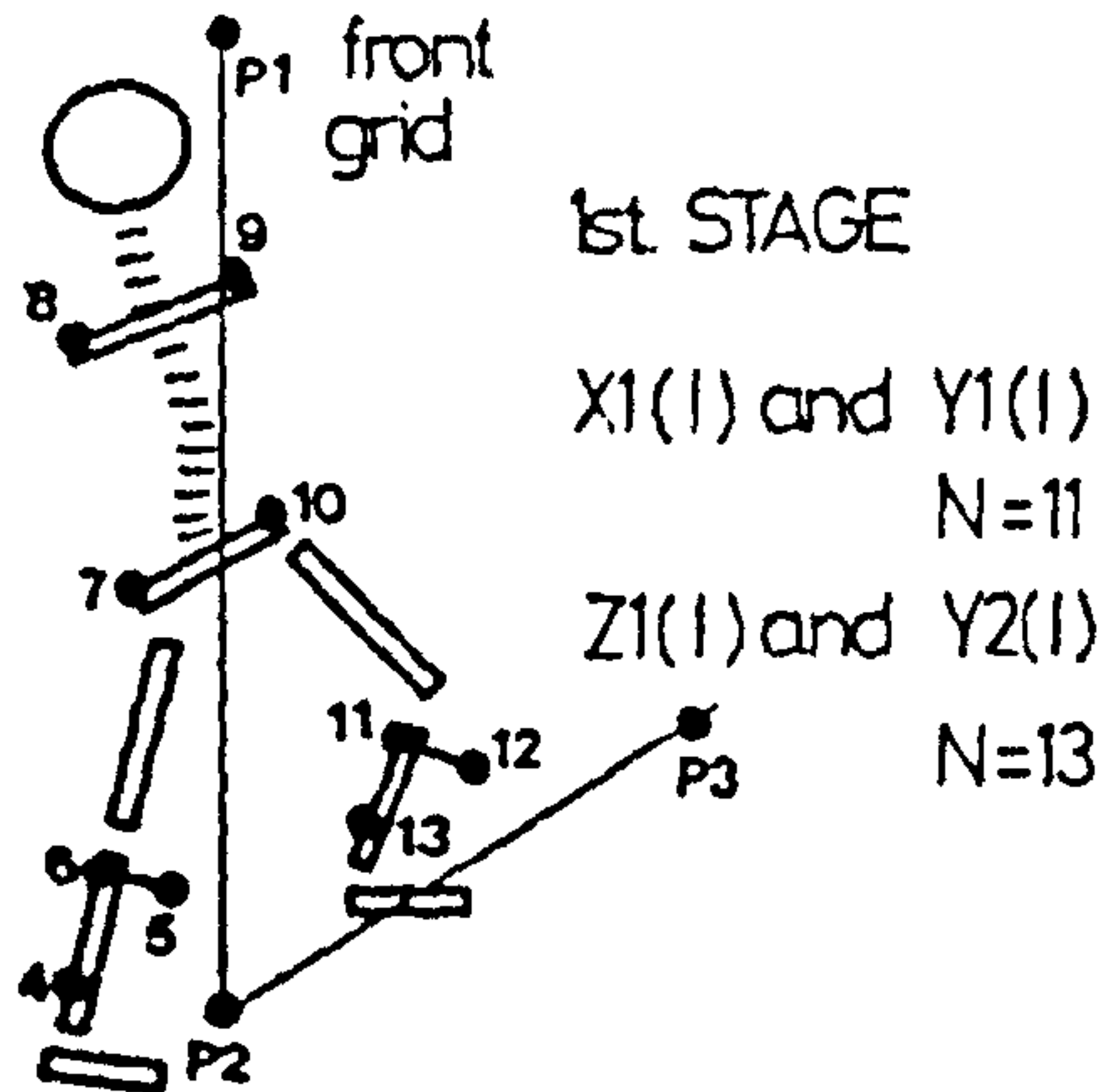
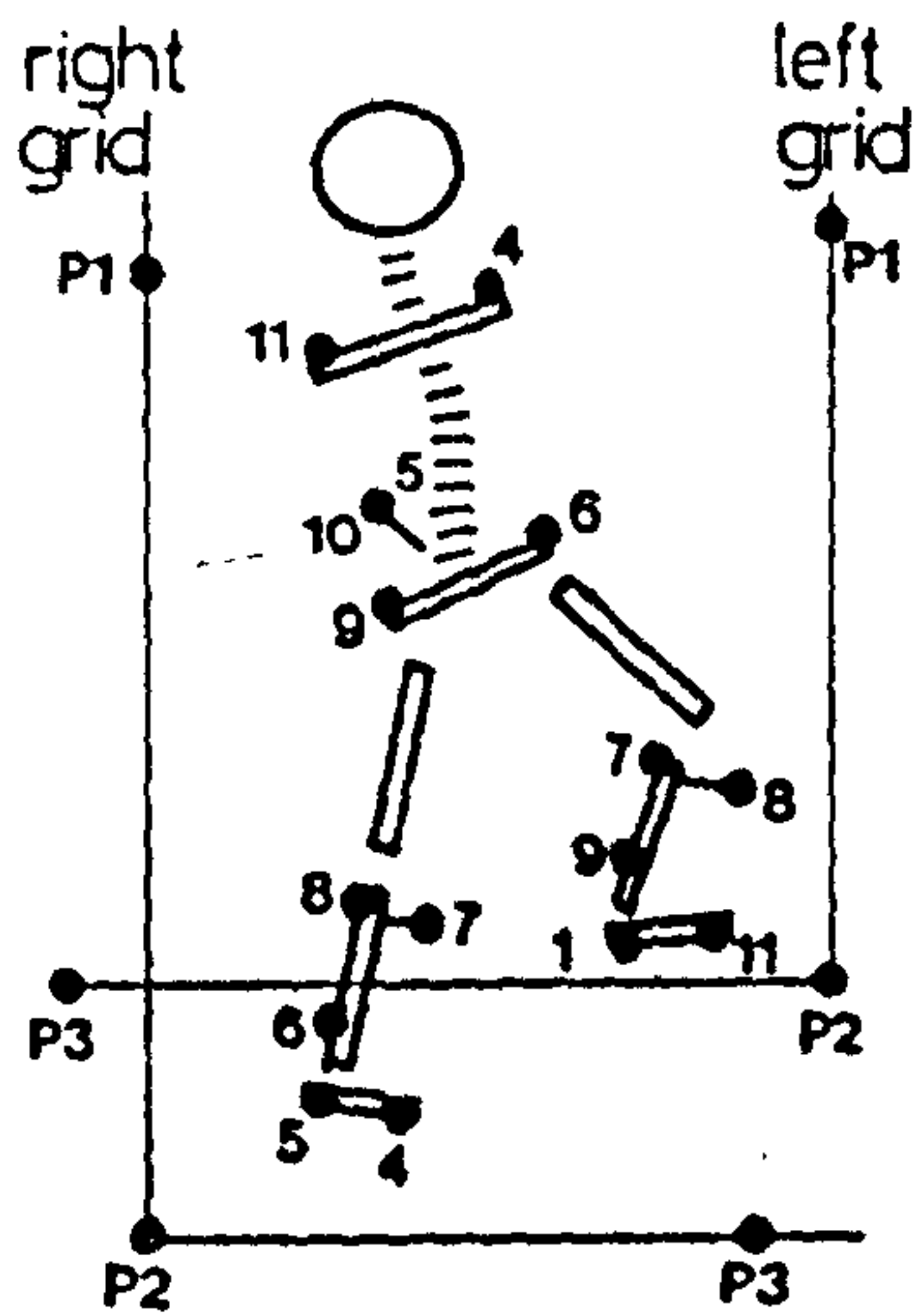


Fig. 3.4

in the X-Y and Z-Y grid planes (Fig.3.3). The shutter speed of the cameras is synchronized at 50 frames per second and colour film is used in each camera. Appropriate illumination is provided by overhead flood-lighting.

The force plate and cinematographic signals are related by firing a flash bulb in the fields of view of each camera. Additionally, firing of the flash bulb produces a transient voltage which triggers an event marker which is recorded on the magnetic tape containing the force plate data. Thus the film and the force data are related on line.

After each test the film is rewound in each camera and then re-exposed with the grid placed on the ground at the geometrical centre of the two force plates. The grid board consists of a black background with 5 inches (127 mm) square network of white lines.

### 3.3 Methodology and Data Collection

#### 3.3.1 General

To obtain spatial co-ordinates from the limb displacements on the cine-films records, skin markers are required. The markers are constructed of wooden spheres of one cm diameter and painted a fluorescent yellow colour. The markers are attached to the subject's body by means of double-sided adhesive tape placed between the marker backing and the skin. The markers are placed on the surface of the following joints: achromio clavicular joint, anterior superior iliac spines (ASIS), a tail marker on the lombo sacral joint region, on the tibial tuberosity, on the fibula head region, on the lateral aspect of the shank, midway between the fibula head and the ankle lateral malleolus, and on the heel and head of the fifth metatarsal joint. All the markers have been given initial identification numbers which will then be changed according to the requirements at different stages on the main programme developed to calculate the co-ordinates of the joints centre (Fig. 3.4 ).

The pelvis has been considered as a rigid body, three markers (six quantities) are required to define its position in space. The same approach has been used for the shank. Once these segments are defined, the co-ordinates of the hip, knee and ankle joint centres are then derived. This procedure has been

adopted to overcome a very common problem in defining the joint centres with markers placed on the skin surface of such joints; the difficulty due to the amount of movement of the skin around the joints during locomotion. The calculations are possible by stabilising the relating of patients anthropometric measurements with the marker system (this will be fully described in the chapter giving the mathematical analysis). To achieve this relationship it is necessary to take a static film shot (one frame of the film would be enough) of the subjects before the tests. This relates the joints' centre with the marker system relative to the grid for all the three cameras.

The hip joint centre is calculated relative to the position in space of the anterior superior iliac spines, this being based on a derived scaling factor for hip co-ordinate based in turn on the distance between the right and left iliac spines. These measurements were derived from skeletal and X-Ray measurements (in selected subjects) in order to obtain the scaling factor for each patients, where:

$$\text{SCALING FACTOR} = \text{PATIENT MEASUREMENT} / \text{SKELETAL MEASUREMENT}$$

The cine film recorded from the subject stepping on the sagittal (X,Y) plane is used to determine the X and Y co-ordinates of the joint centres, while the film recorded from the frontal (Z,Y) plane is used to measure the Z co-ordinate of the joint centred.

### 3.3.2 Laboratory procedure

Approximately one hour before the beginning of the test all the equipment is switched on and allowed to warm up. The cine cameras are loaded with 50 feet spools of Kodachrome 40 ASA 16 mm. film. This procedure is done with the cameras switched to "local mode" where they can be operated independently of each other. Illumination is provided by overhead floodlighting. The camera focus is adjusted and the lens apertures are set accordingly to readings of the photometer. It was found that best settings for the apertures were: f2.8 for the side cameras and f2 for the front one. The cameras are then switched to "remote mode" so that they can be operated synchronously from the control panel.

The charge amplifiers for the two force plates are divided into two sets for each plate: the top one which controls  $F_x$ ,  $M_y$ , and  $F_z$ , is set to operate at 100 mechanical units per volt. While the lower one which controls  $M_x$ ,  $F_y$  and

NAME	DATE
AGE	SEX
PATIENT	PATHOLOGY
TEST	
HEIGHT	
WEIGHT	
Distance between R and L ASIS	
Left ASIS to tail	Right ASIS to tail
ASIS to Gt. Troch. (Right)	ASIS to Gt. Troch. (Left)
Right thigh	Right shank
Left thigh	Left shank
Between shoulders	
Shoulder to ASIS (R)	Shoulder to ASIS (L)
Knee width (Right)	(Left)
Knee depth (Right)	(Left)
Ankle width (Right)	(Left)
Ankle depth (Right)	(Left)
COMMENTS	

Fig. 3.5

Mz is set to operate at 20 mechanical units per volt. The buffer amplifiers for each channel is set to give the desired attenuation. At this stage the computer is already loaded with two tapes: one containing a standard programme called SAM12 (Jordan 1978) and the data tape. The programme has instructions for the total number of analogue and multiplexed channels to be used.

A flash bulb is positioned in the flash light tripod, which is mounted on the run number block. The tripod is then positioned so that it is visible to all cameras without obscuring the subject as the manoeuvres are performed. The flash switch is placed on the control planner to be operated together with the cameras and force plates switches.

The test subjects were subjected to a close medical examination and were asked to wear briefs. They were tested barefoot. Questions relating to the history of their locomotor disturbance were asked, anthropometric measurements were taken and the markers were placed on their anatomical landmarks. This procedure takes on average 25 minutes and all the measurements as well as the relevant clinical aspects were recorded in a standard form (Fig.3:5 ).

### 3.3.3 The Tests

The subject is asked to stand on the top of force-plate 1 (Fig. 3.6) and is allowed to perform as many manoeuvres as possible in order to feel confident with the test. These manoeuvres consisted of stepping forwards starting with the right leg on the top of force plate 2. Secondly stepping (Fig. 3.6) backwards on the top of force plate 1 this time starting with the left leg. The manoeuvres were then repeated with a step equal to 10% of the patients height on the top of force plate 2.

The flash light was prepared, the computer reset and the force plates charge amplifiers inputs discharged. The cine cameras were started and then the subject was asked to perform the first manoeuvre. Each of the computer channels of stored load information was checked and if satisfactory and the spatial data appeared to be satisfactory (this includes the flash operation, cameras operation, and all markers being visible) the force plate data was written to the data tape. If the test was not satisfactory, then it was repeated, otherwise the same procedure was repeated for the next manoeuvres. On the test form all the details were noted, such as run number, block number on the computer tape etc. All the transducers



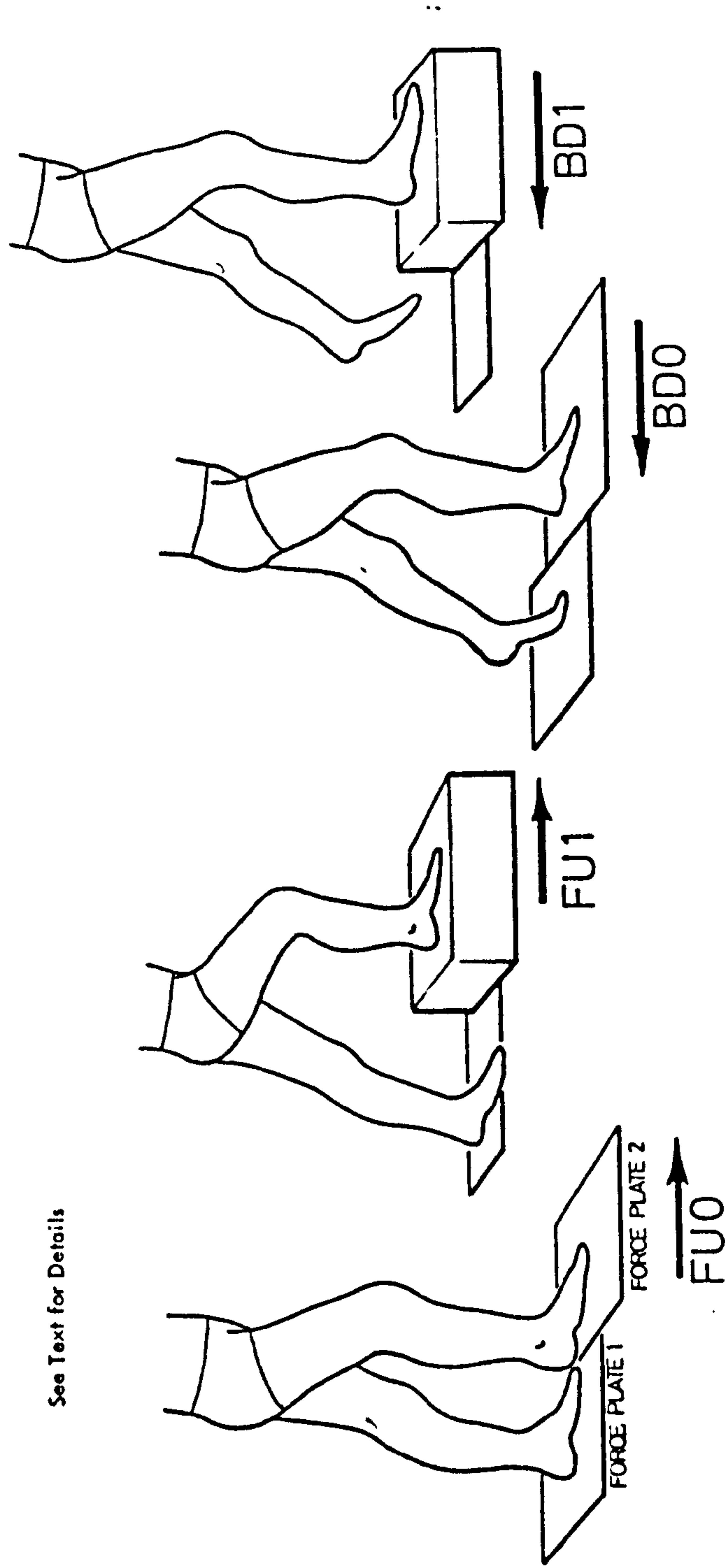


Fig. 3.6

Fig. 3.7

and force plate amplifier gain settings were also recorded.

Once the tests were finished all the cameras were set to "local mode", lenses covered and the film rewound. A grid board consisting of a black background with 5 inches (127 cm) square network of white lines was placed on the ground at the geometrical optical axes of the three cine cameras. The lenses were uncovered and each camera was so re-exposed, superimposing the white square network on the film image.

### 3.4 Experimental Results

#### 3.4.1 General

Force and moment data was stored on magnetic tape, while kinematic data was stored on cine film, both with sample intervals of 0.002 sec. and related on line through a flash bulb being fired in the field of view of the cameras and a transient voltage of the same event marking the force plate data. The method available to convey the data to CDC7600 computer to be processed is in the form of punched paper tape. (PPT)

Force and moment data was transferred from magnetic tape to PPT by means of the PDP12 computer, and this was achieved by means of a programme Editor (Jordan 1978). The data tape and the programme tape were loaded into the PDP12 and the desired block number selected. The events of the manoeuvres can be much more clearly seen using the Fy force plate data and with this channel displayed on the computer visual display unit (VDU) the first cursor was positioned on the beginning of the manoeuvre, while the second cursor was placed at the end of the event on the level of the base line. These positions were then checked for the other channels. All the values between and including the cursor values for each channel were then transferred to paper tape. The frame numbers of the cursors were recorded together with the frame where the flash event occurred.

#### 3.4.2 Film analysis

The analysis of the cine-film records was performed in a semi-automated mode using a vanguard-PCD Spectro Digital Trace Reader. The film was projected by a Vanguard projector head onto a PCD reader glass screen. A gantry moved across the screen, carrying a cursor which could be moved vertically over the

length of the gantry. Wire linkages on both gantry and cursor were connected to potentiometers, the output of which depend upon the X and Y co-ordinates of the cursors centre viewing sight. When a point on the body was located on the cursor sight, the depression of a switch caused the X and Y co-ordinates of the point to be punched onto paper tape.

Unfortunately, no printed output was available from the particular machine used, and human errors, eg. recording too few or too many co-ordinates per frame, were not detectable until a later stage of processing. As an aid to detecting errors of this nature, three fixed grid points were always recorded as the first data points in each frame enabling the co-ordinates at these points to be used as a basis for editing. Moreover, these three grid points are used to transfer the PCD reference system to the laboratory inertial frame system. The film is stepped through frame by frame until the frame in which the flash occurred is found, corresponding to the event marker on the force tape data. This event marker is related (as no. of points) to the point on the force data where the beginning of the movement occurs. This value was used on the film to identify the beginning of the manoeuvre. Both sides and front film were processed by following the same steps.

The paper tapes obtained by this procedure were read onto a magnetic tape in the CDC-7600 system at the University of London Computer Centre. Following editing subsequent processing of the co-ordinate data was carried out using FORTRAN IV programmes.

Control data such as subject and manoeuvre identification, camera specification etc, were typed directly onto paper tape in the correct sequence and spliced onto the beginning of each tape.

## CHAPTER 4

### ANALYSIS

- 4.1 Introduction
- 4.2 Cine Film Analysis
- 4.3 Parallax Corrections
- 4.4 Calculation of the Unknown Co-ordinate
- 4.5 Defining the Static Co-ordinate System
- 4.6 Defining the Dynamic Co-ordinate System
- 4.7 Intersegmental Force Actions
  - 4.7.1 Mass and Centre of Mass
  - 4.7.2 Moment of Inertia
  - 4.7.3 Accelerations of Limb Segments
- 4.8 Calculation of the Intersegmental Moments

## 4. ANALYSIS

### 4.1 Introduction

This chapter describes the theoretical analysis used to reduce the kinematics and force plate data recorded during the experimental sessions. The analysis converts the spatial data obtained from the cine films to real distance units and the force plate data into units of force, and thus loading information on the lower limb structures are obtained. A computer programme has been developed for this analysis (Appendix 1) and it is carried out in the following steps:

- (a) Real distances and loads are obtained by applying parallax and scaling corrections to the spatial data and force calibration factors to the force plate data.
- (b) From a kinematic static shot (the static test) recorded at the time of the experiment on the film, direction cosines are determined in order to define the co-ordinate system of the three markers mounted on the shank with respect to the ground reference system (GRS), and relate the shank system to the ankle and knee joints centre. The positional relationships between the shank markers and the joint centres remain the same during a test on a subject, but change from test to test and from subject to subject, thus requiring their positions to be redefined in the beginning of each test.
- (c) During the dynamic test, the shank and pelvic co-ordinate systems of the structure is moving relative to the laboratory reference system for each frame of the film. At the instant of a particular frame, the moving structure and the reference system are fixed relative to one another, thereby permitting the direction cosines in the GRS of each of the co-ordinate system to be defined.
- (d) Determinations of the loading between body segments at the anatomical joint centres, using both dynamic load and spatial data is obtained using Newtons' law.
- (e) The direction cosines of the co-ordinate systems are relative to the GRS, thus a vector in any of the co-ordinate systems when multiplied by the direction cosine matrix, transfer the vector in the GRS.

The assumptions made for this analysis are as follows:

- (i) Each structure, for which a co-ordinate system is defined is considered a rigid body; that is, the distance between the markers on the body is invariable.

The marker positions are chosen so that there is minimum skin movement relative to the respective bony prominences; therefore the marker is considered to be rigidly attached to the underlying skeletal structure.

#### 4.2 Cine Film Analysis

The output data from the Vanguard-PCD film analyser is given with respect to the bottom left hand corner of the screen, and in order to refer all co-ordinates to the geometrical camera axes, which correspond to a centre line between the two force plates, calculations must be performed. For each frame analysed, three known fixed points of the grid were taken in order to account not only for the transfer of the origin of the co-ordinate system, but also to eliminate any small displacements of the film frame due to imperfections on the sprocket holes on the film. REF determines the laboratory reference axes system using the co-ordinate of the 3 auxiliary points marked on the grid. CHANGE transforms the co-ordinates of each marker on the frame from the vanguard system to the laboratory system.

The output is in arbitrary units representing voltages output from the Vanguard-PCD potentiometres. The values differ from the true physical co-ordinates, the difference depending on the magnification of the projected image. As all the calculations are performed using true co-ordinates, the image co-ordinate values have to be multiplied by a scaling factor (SCALING, in metres) derived from a known dimension on the film. For this particular analysis the scaling factor was calculated using 0.127 m.squares drawn on the grid as follows:

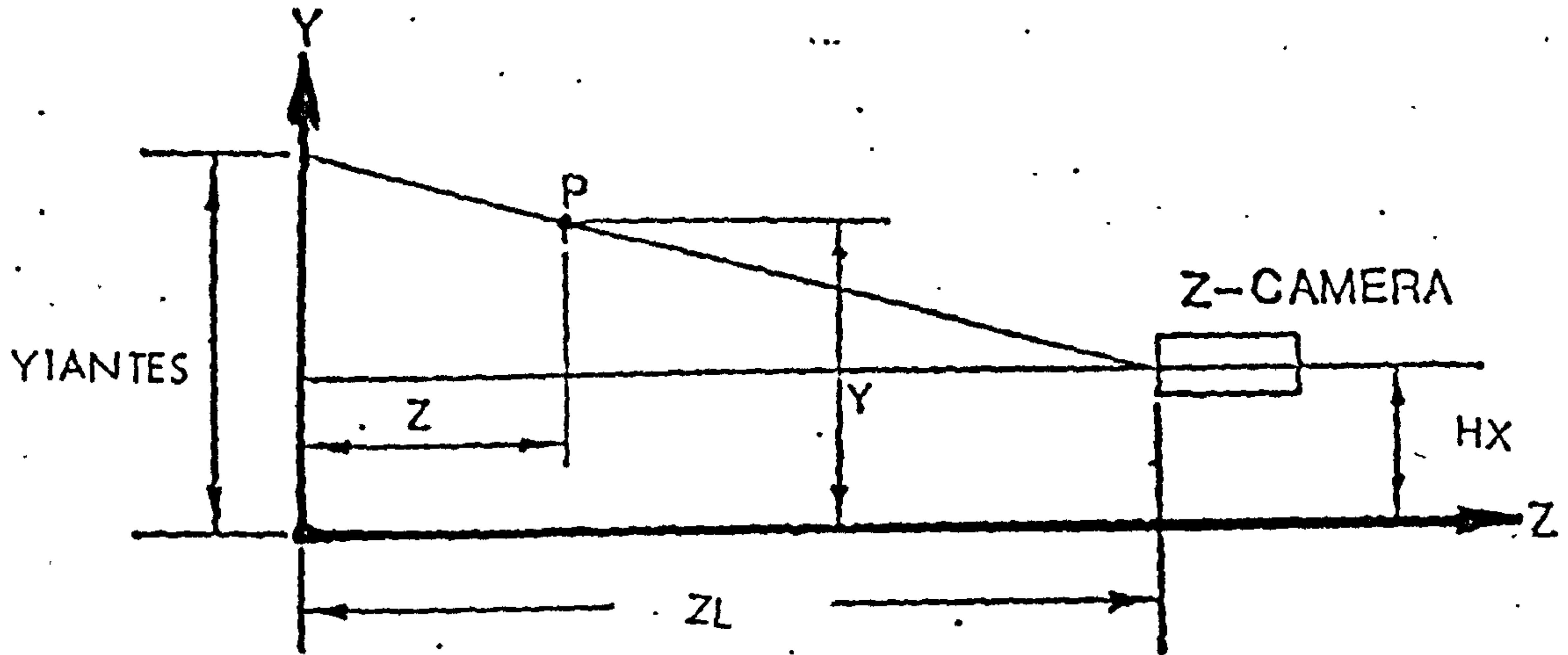
$$\text{SCALING} = \frac{0.127}{\text{The corresponding readings in Vanguard units}}$$

The force plate data on magnetic tape on the PDP 12 computer is in integer form between values of -512 to +512, where 512 represents an input voltage from the transducer amplifiers of 1 volt. To utilize this data in later calculations the stored information must be converted to the actual load units

$$\text{Force} = \text{FP data} \times \text{buffer const.} \times \text{amplif. set.} / 512 \text{ (in Newtons)}$$

$$\text{Moment} = \text{FP data} \times \text{buffer const.} \times \text{amplif. set.} \times 0.264 \text{ (in Newton meters)}$$

ELEVATION



-PARALLAX CORRECTION

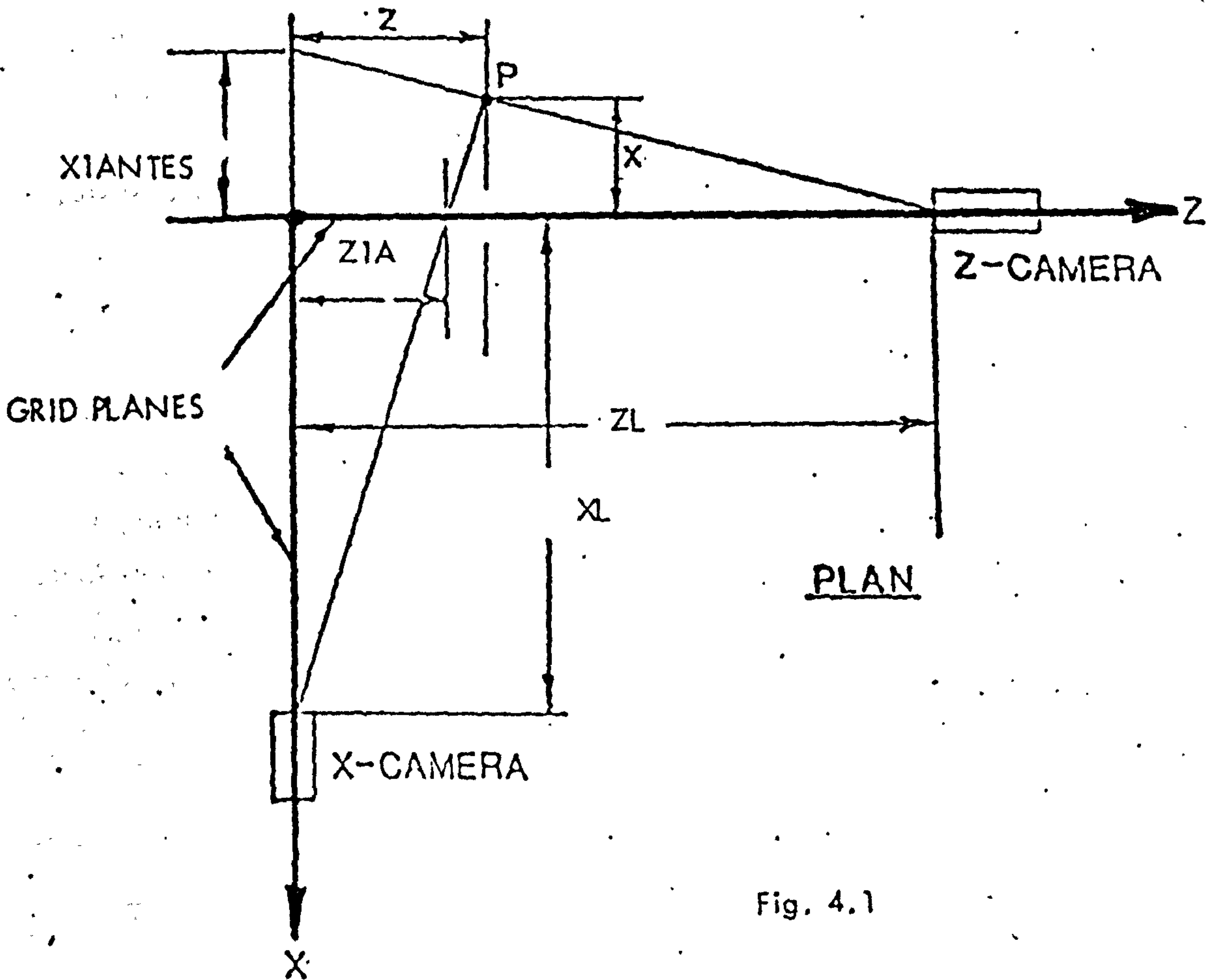


Fig. 4.1

### 4.3 Parallax Corrections

The co-ordinates obtained by reading directly from the film grid are apparent and a parallax equation must be developed to determine the true X, Y and Z co-ordinates of the marker. This is achieved by simple geometrical analysis

From (Fig. 4.1) it can be seen that (see Paul (1967) for full derivation of the equations):

$$Y = Y_{IANTES} - (Y_{IANTES} - HX) \frac{Z}{XL} \quad (1)$$

$$X = X_{IANTES} - X_{IANTES} \cdot \frac{Z}{ZL} \quad (2)$$

$$Z = Z_{IA} - Z_{IA} \cdot \frac{X}{XL} \quad (3)$$

$X_{IANTES}$ ,  $Y_{IANTES}$  and  $Z_{IA}$  are the apparent grid co-ordinates, and  $X$ ,  $Y$ , and  $Z$  are the true co-ordinates.  $HX$  and  $HZ$  are the distances of the X and Z cameras from the origin of the system and  $HX$  is the height of the cameras above the floor.

From equations (2) and (3):

$$X = X_{IANTES} \frac{(1 - Z_{IA}/ZL)}{(1 - X_{IANTES} \cdot Z_{IA}/ZL \cdot XL)} \quad (4)$$

$$Z = Z_{IA} \frac{(1 - X_{IANTES}/XL)}{(1 - X_{IANTES} \cdot Z_{IA}/ZL \cdot XL)} \quad (5)$$

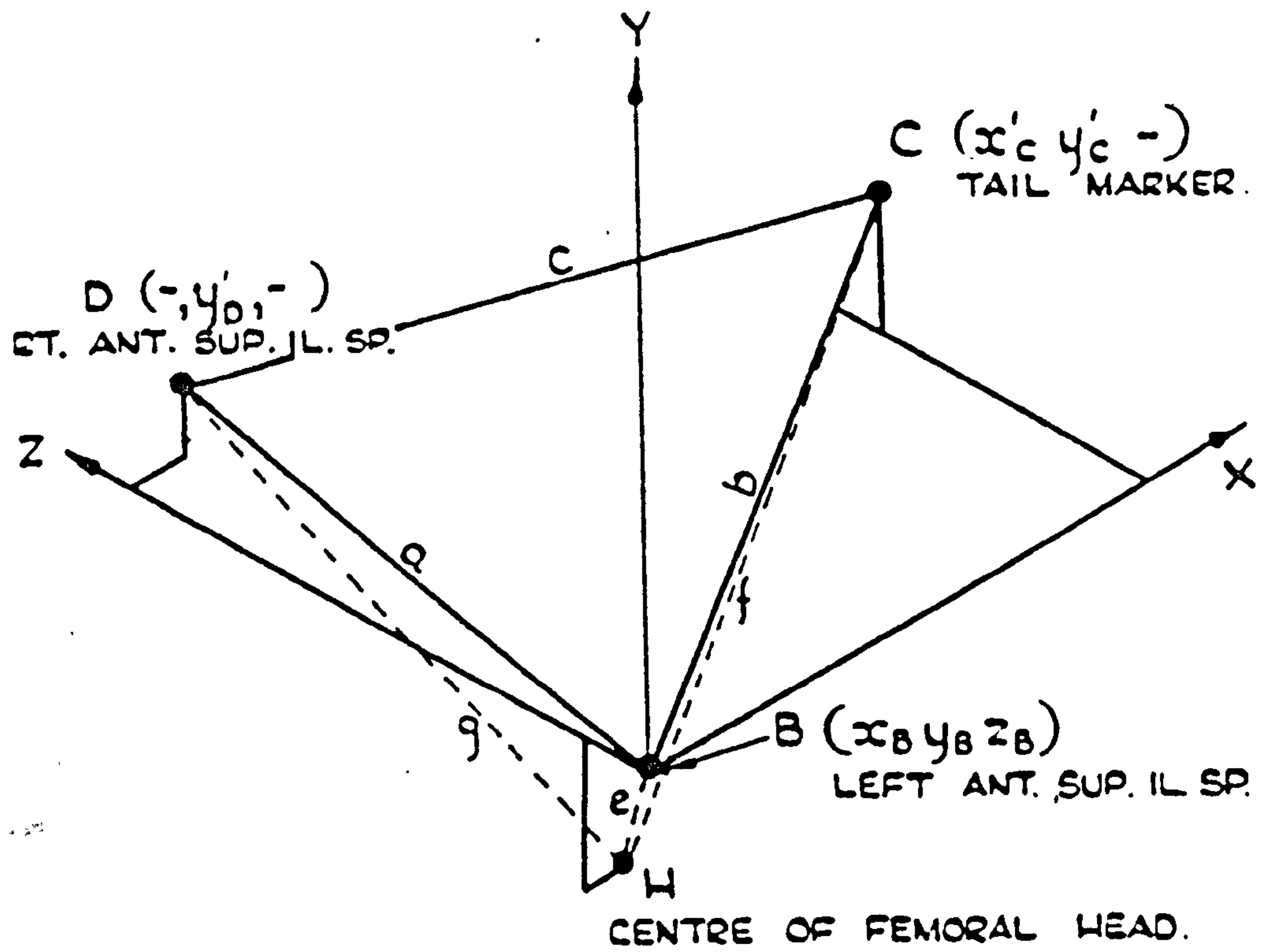
The true X, Y and Z co-ordinates of the markers are derived and the Ankle, knee and hip joint centres are calculated.

### 4.4 Calculation of the Unknown Co-ordinate

All the markers used in this analysis could be seen at least by two of the three cine-cameras so that the requirements for parallax correction were obtained. However, one exception was the tail marker placed on the Lombo-sacral region, this marker could only be seen by both side cameras. Thus the Z grid co-ordinate of this marker had to be calculated based upon the distances between the anterior superior iliac spine (ASIS) marker and the tail marker, (see fig.4.2) from the following equation:

$$(X_c - X_b)^2 + (Y_c - Y_b)^2 + (Z_c - Z_b)^2 = B^2 \quad (6)$$





REFERENCE POINTS ON PELVIS.

Fig. 4.2 (From Paul 1967)

$$\begin{aligned}
& Z_c^2 \left[ (X_{IANTESc} / ZL)^2 + (Y_{IANTESc} - HX)^2 / ZL^2 + 1 \right] + \\
& (2Z_c / ZL) \left[ X_{IANTES} (X_b - X_{IANTESc}) + (Y_{IANTESc} - HX) \right. \\
& \left. (Y_b - Y_{IANTESc}) - Z_b ZL \right] + (X_{IANTESc} - X_b)^2 + (Y_{IANTESc} - Y_b)^2 + \\
& Z_b^2 - B^2 = 0
\end{aligned} \tag{7}$$

In this quadratic equation only the smaller root is the solution required.

See Paul (1967) for full derivation of the method.

#### 4.5 Defining the Static Co-ordinate Systems

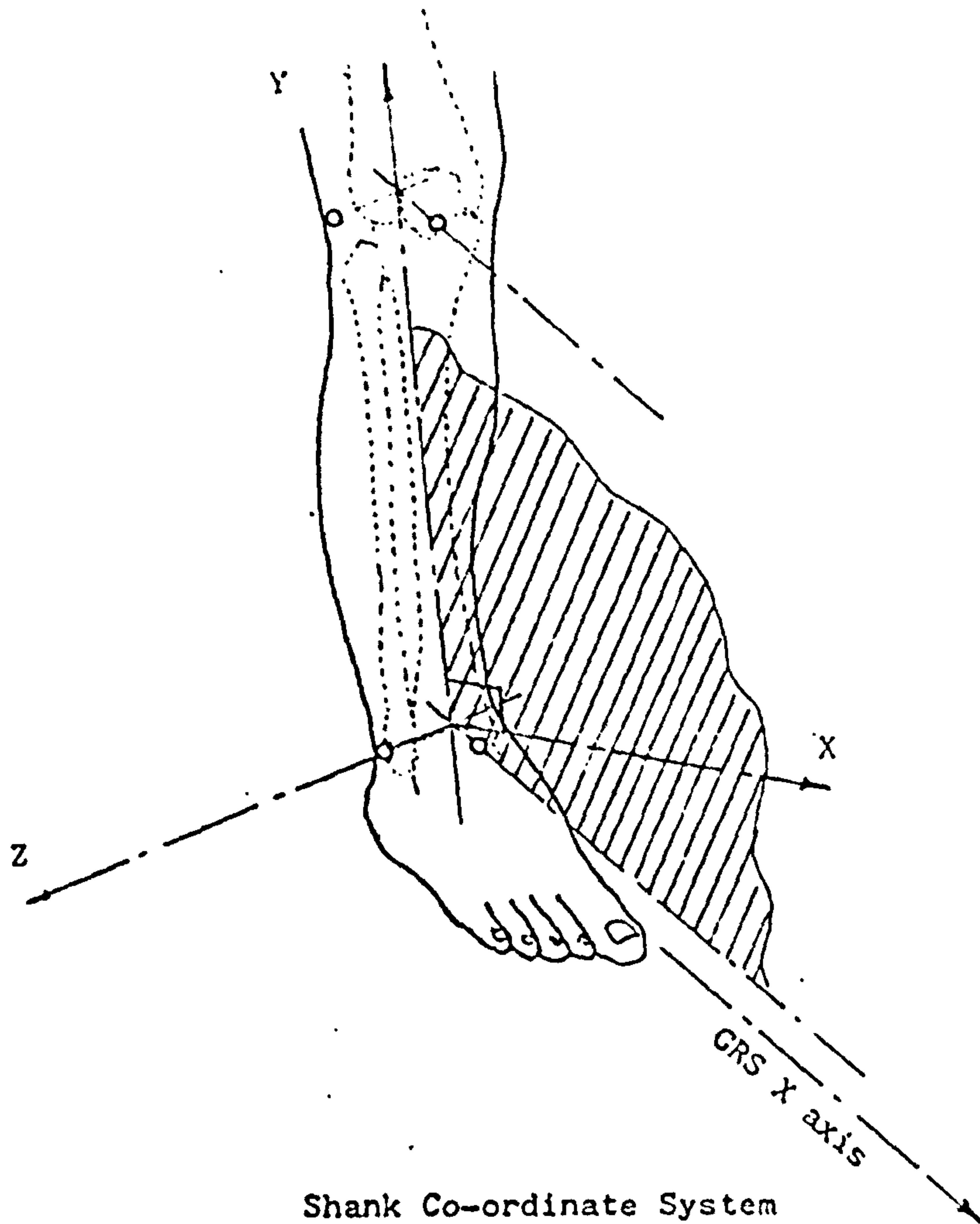
Static analysis employs a cine film frame from both the side and front cameras, with images of the patient's shank only, such that all calibration markers shown in Fig. 4.3 can be seen by both cameras. Three markers arranged in a triangle have been used to define a co-ordinate system. These markers are positioned such that a line joining two selected markers A and B in Fig. 4.3 lies on the Y axis. The Z axis is normal to the plane in which all the three markers lie and the X axis is perpendicular to both the Y and Z axes.

The shank co-ordinate system (see Fig.4.3) makes use of markers placed anterior and lateral to the knee and ankle joint centres such that the side camera will obtain from the lateral markers the X and Y co-ordinates, while the front camera obtains the Z co-ordinates from the joint front markers. A line joining the joint centres lies along the Y axis of the shank co-ordinate system. The normal to the plane in which the Y axis of this system and the X axis of the GRS lie, defines the Z axis and a line perpendicular to the Z and Y axis of this system defines the X axis.

Also from the static test, the direction cosines of the vector between the medial and the lateral knee markers and the medial and the lateral ankle markers are found. These direction cosines are applied in determining the medial knee and ankle marker co-ordinates in the dynamic tests.

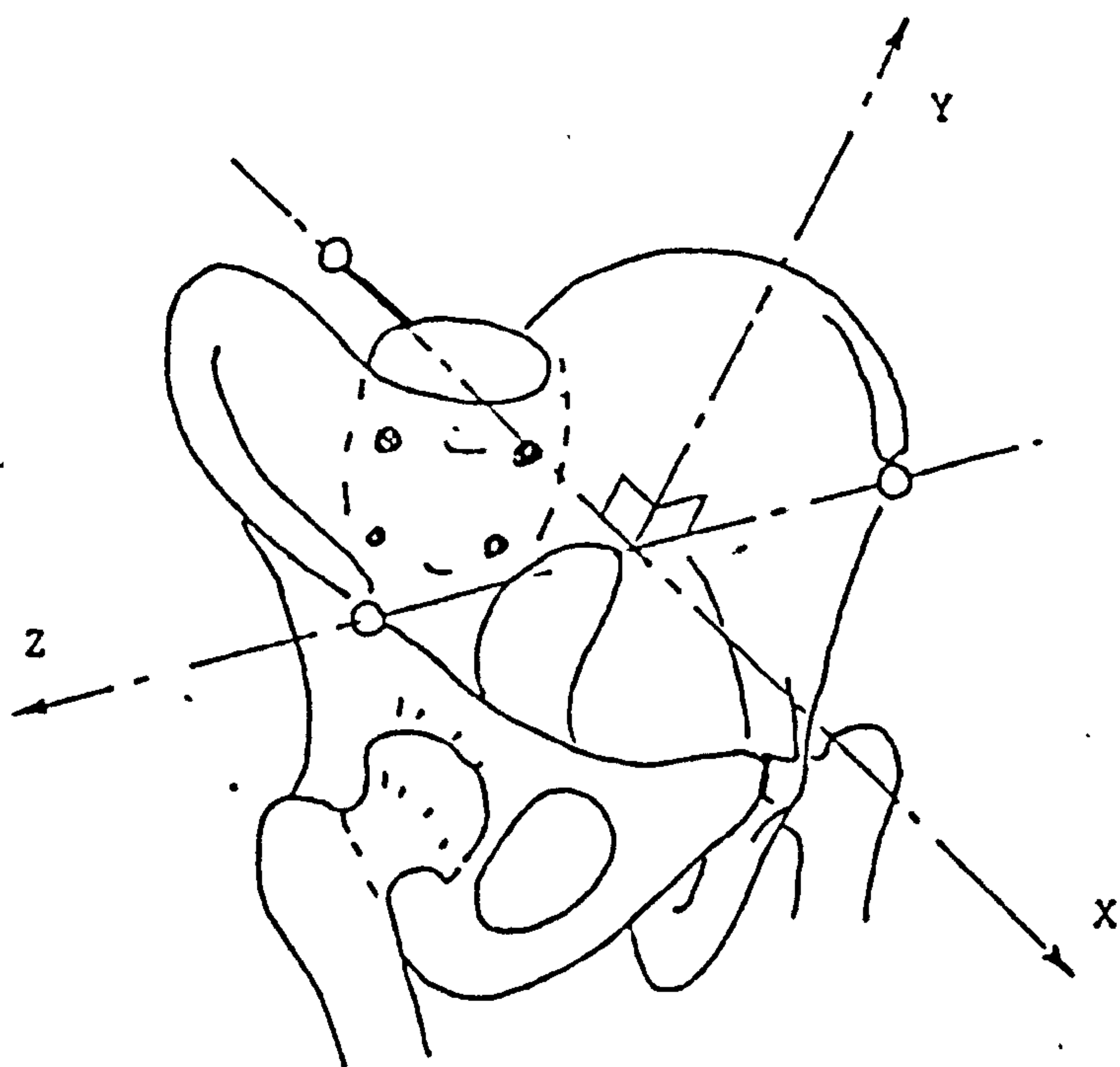
#### 4.6 Defining the Dynamic Co-ordinate System

Using the markers shown in Fig 4.3, the shank segment, the pelvis and the



Shank Co-ordinate System

Fig. 4.3



Pelvis Co-ordinate System

Fig. 4.4

thigh are obtained for successive frames of cine film. Once the marker co-ordinates have been found, the method used for obtaining the co-ordinate system in the dynamic situation is the same as that for the static situation.

The pelvis marker triangle co-ordinates (Fig.4.4) are obtained after parallax corrections. The Y axis is normal to the plane in which the three markers lie, while the Z axis is defined by the line between the two anterior superior iliac spines. The X axis is perpendicular to both Z and Y axes.

The sense of these axes are:

Y is positive from inferior to superior

X is positive from posterior to anterior

Z is positive from medial to right lateral.

From measurements performed on a skeleton and a number of normal subjects, the vector from the anterior superior iliac spine to the hip joint centre (HJC) of the same side in the pelvis co-ordinate system has the following components:

$$x = 0.183^* D86$$

$$y = 0.305^* D86$$

$$z = 0.122^* D86$$

Where D86 is the distance between the two ASIS. (Harrington 1974).

The thigh co-ordinate system takes the line between the hip and the knee joint centres to define its Y axis, as neither the hip nor the knee centres is defined by markers, position is obtained by taking a known vector from one marker (on the shank for the knee and ankle and on the ASIS for the hip) to the respective joint centre. From the static shot a vector is defined from the marker 1 (if left side marker 10) to both the knee and the ankle joint centre. This vector is then transferred to the GRS and added to the position vector of the respective camera to the marker.

## 4.7 Intersegmental Force Actions

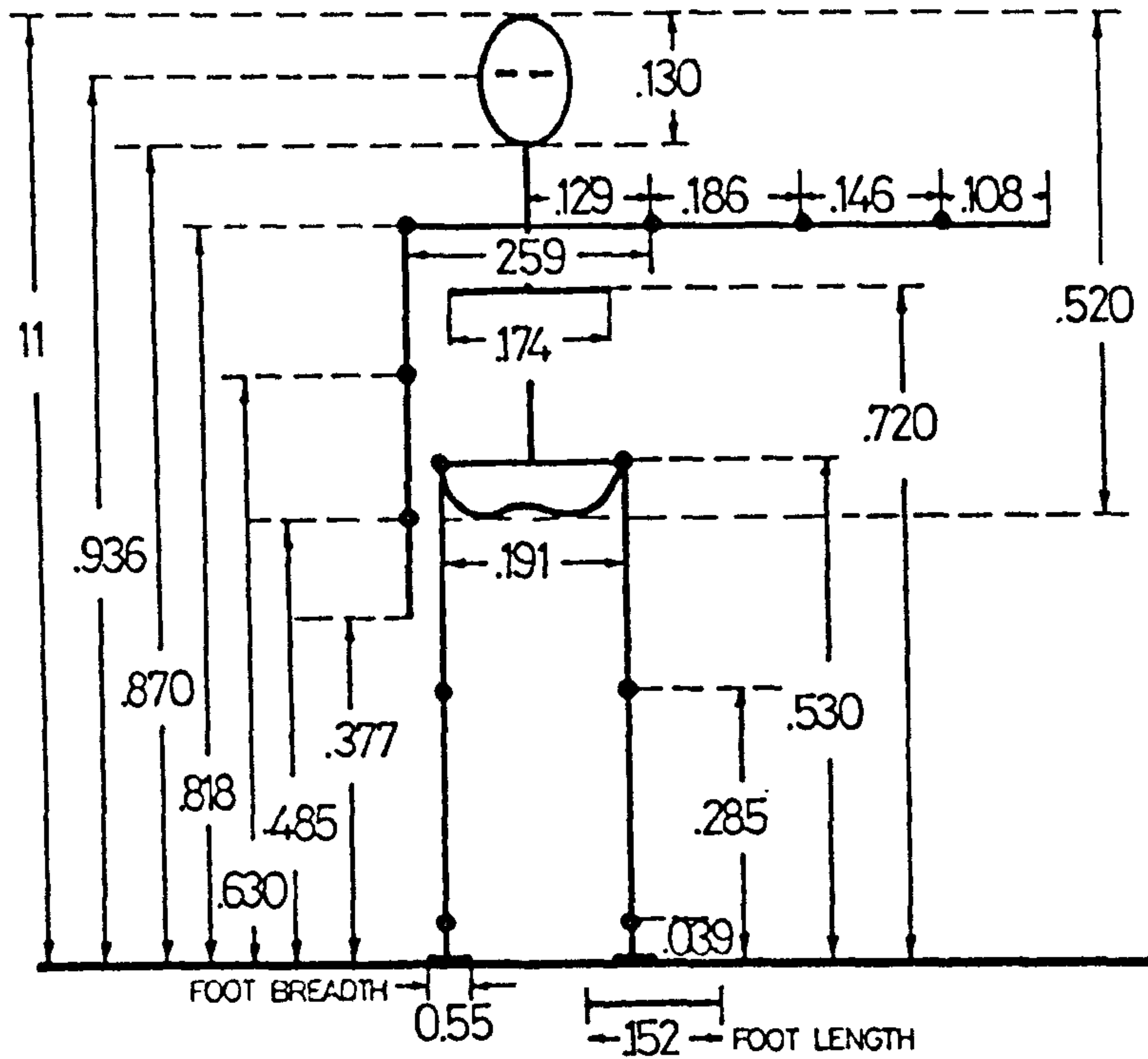
### 4.7.1 Mass and centre of mass

To calculate the force and moments acting on a joint during locomotion it is necessary to know the mass and the positions of the centre of mass of the limb segments. This is achieved by means of tables, for this particular work the information published by Drillis and Contini (1966) has been used (Fig. 4.5).

Fig. 4.5

BODY SEGMENT MASS PROPERTIES

(as reported by Contine and Drillis (1966) - Technical Report No. 1166.03 of New York University)



SEGMENT LENGTH EXPRESSED AS RATIO OF BODY HEIGHT

Segment Mass in Percent of the Total Body Mass (Mean Values)

Investigator:	Harless	Meeh	Braune and Fischer	Bernstein	Dempster	N.Y.U
Segment						
Head, Neck and trunk	53.42	59.08	49.68	52.98	56.50	58.04
Upper Arms	6.48	6.19	6.72	5.31	5.30	7.14
Forearms	3.62	3.38	4.56	3.64	3.10	3.60
Hands	1.68	1.48	1.68	1.41	1.20	1.20
Thighs	22.36	17.36	23.16	24.43	19.30	18.92
Shanks	8.78	9.35	10.54	9.31	9.00	8.40

TABLE XIII: Location of Mass Centres from Proximal Joint in Percent of Segment Length

Segments	Harless	Investigators			N.Y.U
		Braune and Fischer	Bernstein	Dempster	
Entire Arm	-	42.6	-	43.6	43.1
Upper Arm	48.5	47.0	46.6	43.6	44.2
Forearm and Hand	-	45.8	-	67.7*	38.2
Forearm	44.0	42.1	41.2	43.0	42.3
Hand	47.4	-	-	-	39.2
Entire leg	-	41.5	-	43.4	39.7
Thigh	46.7	44.0	38.6	43.3	41.0
Shank and foot	-	51.9	-	43.3	45.0
Shank	36.0	42.0	41.3	43.3	39.3
Foot (from heel)	46.0	43.4	-	43.3	44.5

\*Distance from elbow to ulnar styloid is assumed to be 100 percent.

TABLE XVIII: Ratio ( $\bar{C}_3$ ) of Radius of Gyration ( $p$ ) to Segment Length ( $l$ )

Segment	Braune and Fischer				N.Y.U and Live Subjects	Weighted Average
	I Cadaver	I Test	I Cadaver	II Test		
Entire Upper Extremity	-	-	0.30	0.31	0.24	0.252
Upper Arm	0.27	0.27	0.29	0.31	0.26	0.268
Forearm and Hand	0.26	0.28	0.29	0.32	0.25	0.263
Entire Lower Extremity	-	-	0.32	0.32	0.24	0.256
Thigh	0.26	0.27	0.31	0.31	0.23	0.250
Shank and foot	0.32	0.32	0.33	0.35	0.29	0.303
Shank	0.25	0.26	0.24	0.26	0.27	0.264
Average	0.27	0.28	0.30	0.31	0.25	0.265

It is assumed that these tests based on eight subjects provide better coefficients for the different segments.

For the purpose of determining the centre of mass, the foot and the shank are considered as one body.

#### 4.7.2 Moment of inertia

As in the case of mass and centre of mass the moment of inertia was also estimated using the information given by tables. (Fig. 4.5) Drillis and Contini.

The analysis ignores the torques due to moments of inertia about the long axis of the limb segments.

#### 4.7.3 Accelerations of limb segments.

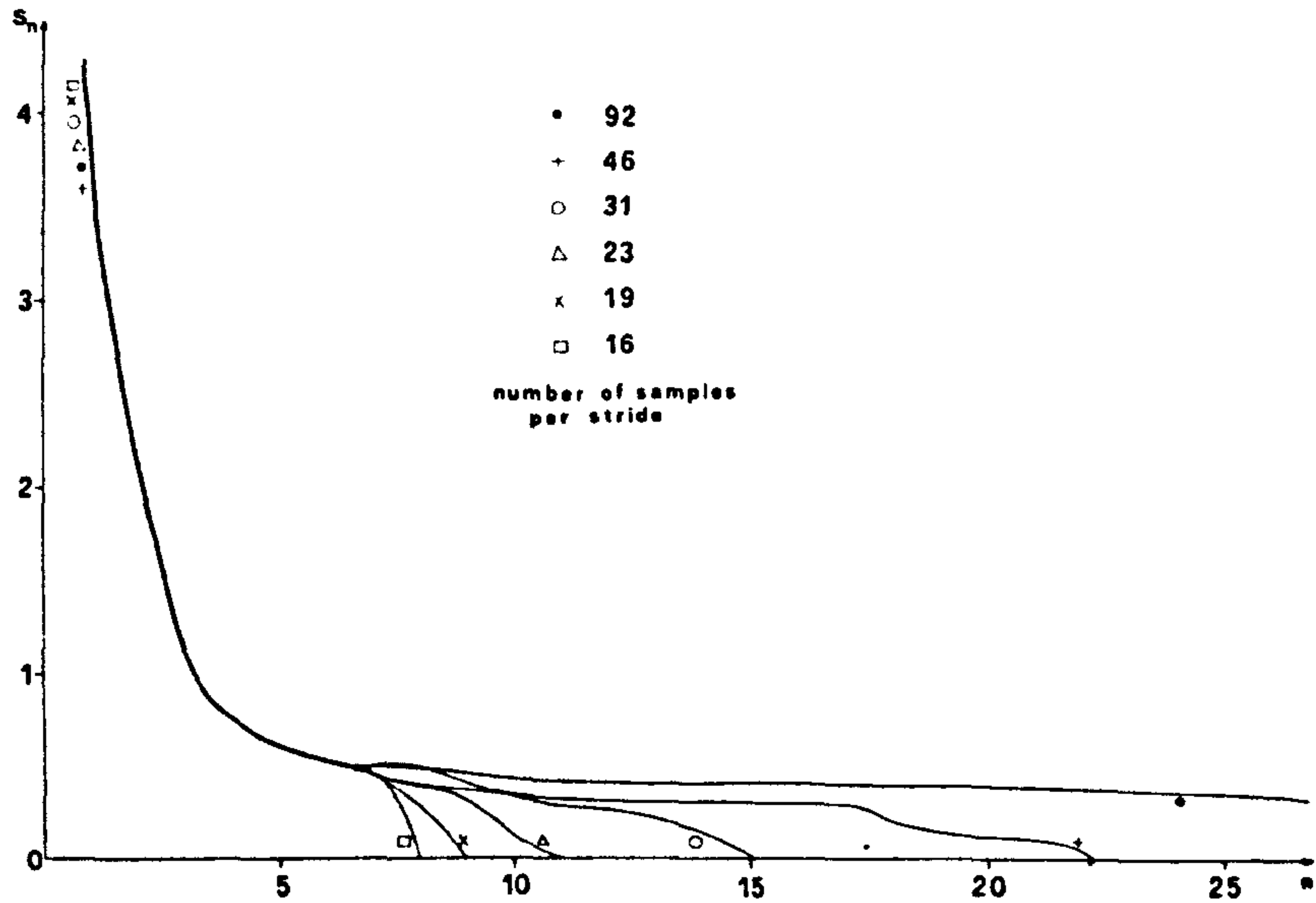
Velocity and accerlations are obtained by differentiation of the displacement data.

To reduce error due to noise in the signal some authors (see Winter et al 1974) have passed the displacement data through a low pass digital filter in order to reduce noise. Thus to achieve this the cut off frequency should be stated ad priori (usually up to 8 or 10 H.Z).

For the present analysis, the algorithm used has been described by Cappozzo et al (1975) which has been designed to obtain the time functions of the variables in an analytical form. Since all biomechanical functions can be represented as periodic functions, and have the properties of "well behaved" functions, they can be represented by trigonometric functions:

$$R\bar{n} = R\bar{n}(t) = A_0 + \sum_{i=1}^{\bar{n}} (A_i \sin \omega_i t + B_i \cos \omega_i t) \quad (8)$$

The technique comprises two steps: First, the determination of a function which fits the data accurately. Assuming that the sampled data are subject to a random error whose statistical characteristics do not change with time, each sample can be seen as an observation from a normal population having a mean value and variance. Under this assumption a method of least square is used for the estimation of the parameters  $A_0$ ,  $A_j$ ,  $B_j$ , and of the variance (for details see



Example of plot of the square root of the variance estimate  $[s(n)]$ , vs order  $n$  of the regression curve  $R_n$  for different sampling rates.

Best fitting parameters

GAIT	HARMONICS ORDER	$\eta_1$			$\eta_2$			$\eta_3$			$\bar{x}_H$			$Z_H$		
		Mod [°]	Phase [rad]	E [σ]	Mod [°]	Phase [rad]	E [σ]	Mod [°]	Phase [rad]	E [σ]	Mod [mm]	Phase [rad]	E [σ]	Mod [mm]	Phase [rad]	E [σ]
WALKING UPSTAIRS	0	17.6	—	—	133.8	—	—	88.7	—	—	20.8	—	—	817.7	—	—
	1	36.7	0.00	3.0	36.3	0.00	6.2	9.1	0.00	4.9	11.8	0.00	10.6	19.7	0.00	16.6
	2	3.8	1.16	1.0	7.8	2.08	2.9	3.8	1.04	4.1	11.8	-0.96	6.3	21.9	-3.03	4.1
	3	0.6	0.43	0.9	3.0	-3.08	1.7	3.1	-2.73	3.5	4.0	-1.26	6.6	4.5	-1.68	2.4
	4	0.8	0.28	0.8	0.9	-2.68	1.6	2.6	-0.87	2.9	4.2	-1.28	4.7	1.7	2.71	2.1
	5	0.3	1.19	0.8	1.2	3.14	1.3	1.4	1.73	2.8	2.3	-1.34	4.4	0.7	0.80	2.0
	6	0.6	0.14	0.4	0.7	-1.82	1.2	1.9	-1.98	2.4	3.3	-2.14	3.6	0.6	2.49	2.0
	7	0.4	0.74	0.3	0.4	-2.02	1.2	1.3	0.00	2.2	1.6	-2.32	3.4	0.6	2.79	1.9
	8	0.2	0.84	0.3	0.7	-1.23	1.1	1.2	2.63	2.0	1.8	-2.96	3.2	1.6	3.09	1.4
	9	0.1	0.48	0.3	0.7	-1.78	1.0	1.0	-0.98	1.8	0.7	-2.68	3.3	0.9	-0.03	1.2
	10	0.2	2.70	0.3	0.8	-1.47	0.8	1.0	0.90	1.6	0.3	-2.11	3.3	0.6	2.33	1.2
	11	0.2	2.40	0.2	0.3	-0.42	0.8	1.0	-3.07	1.4	2.1	-3.94	2.8	0.6	-2.43	1.1
	12	0.1	1.96	0.2	0.4	-0.89	0.8	0.6	-0.37	1.4	1.8	2.98	2.4	0.9	0.63	0.8
	13	0.2	2.31	0.1	0.6	0.03	0.4	1.3	1.71	0.8	2.1	1.88	1.3	0.8	1.82	0.4
	14	0.0	0.01	0.0	0.6	0.24	0.0	0.7	-2.00	0.0	1.8	1.46	0.0	0.4	0.83	0.0
LEVEL WALKING	0	11.7	—	—	181.1	—	—	100.6	—	—	494.4	—	—	870.4	—	—
	1	26.1	0.00	4.68	21.8	0.00	15.7	6.3	0.00	6.2	8.9	0.00	14.8	11.7	0.00	24.9
	2	8.7	0.68	2.14	20.8	-0.38	3.7	7.6	0.89	2.9	19.1	1.89	4.9	32.8	2.14	6.3
	3	2.3	-0.36	1.29	3.7	4.68	2.4	2.1	0.32	2.8	3.2	1.29	4.4	6.3	1.87	4.3
	4	1.2	1.17	0.9	1.9	1.11	1.9	2.9	1.58	1.2	2.4	-2.83	4.0	3.3	5.06	3.6
	5	0.2	-2.10	0.9	1.8	2.81	1.6	0.8	1.11	1.1	1.8	0.30	3.9	2.2	-2.30	3.2
	6	0.4	-0.37	0.9	0.8	-2.18	1.4	0.3	1.62	1.1	0.7	-2.82	4.0	1.6	-1.89	3.0
	7	0.5	0.74	0.8	0.7	-1.98	1.3	0.6	2.90	1.0	1.9	-1.20	3.8	1.4	-2.14	2.8
	8	0.2	0.88	0.8	0.3	-1.66	1.3	0.2	1.70	1.0	1.2	-2.89	3.7	1.2	-0.78	2.7
	9	0.1	0.88	0.8	0.3	-1.52	1.3	0.5	2.64	1.0	1.9	-2.43	3.4	0.8	1.67	2.7
	10	0.1	0.13	0.8	0.6	-1.44	1.3	0.7	3.11	0.8	0.8	-1.84	3.4	1.7	-0.32	2.4
	11	0.4	0.19	0.8	0.7	-1.38	1.1	0.3	2.11	0.8	2.6	-1.96	2.8	1.6	1.90	1.9

Fig 4.6



Carnahan et al 1969). Secondly, a minimization of the mean square error with respect to the parameters  $A_0, A_j, B_j$  is performed once the optimal parameters of the functions have been estimated, the problem of determining the more convenient number of harmonics, can be done by inspection of the plot of the square root of the variance versus the number of samples (Fig.4.6) from Cappozzo et al 1975). Once the analytical form of the displacement curve is known the velocities and accelerations can be found by analytical differentiation.

#### 4.8 Calculation of the Intersegmental Moments

The externally applied moments relative to the grid axis, acting at the centre of the joints are calculated from the ground to foot force actions and the joints spatial co-ordinates.

The sign convention adopted in this programme is in accordance with the proposed international standard (C.P.R.D.1975). This can be seen on Fig.4.7 which shows the positive directions for forces and moments.

For the calculation of the instantaneous centre of pressure at the foot allowance have to be made for the height of the step, placed on force plate two.

The general form of the moment equation is as follows: (see fig. 4.8 for orientation).

$$M_zK = M_zA - mg \bar{r}_1 \sin \theta_1 - I\ddot{\theta} - IF_x \bar{r}_1 \cos \theta_1 - IF_y \bar{r}_1 \sin \theta_1 + F_xA \bar{r}_2 \cos \theta_2 + F_yA \bar{r}_2 \sin \theta_2 \quad (8)$$

$F_xA$	=	$F_x$ component at the ankle joint.
$F_yA$	=	$F_y$ " " " " "
$IF_x$	=	x component of Inertia force acting at the CG
$IF_y$	=	y " " " " " "
$I\ddot{\theta}$	=	Inertia torque at the CG
$mg$	=	Weight of the limb
$M_zA$	=	Moment at the ankle

A computer programme has been developed to accept the force plate and kinematic film. A block diagram showing the operational sequence of the computer programme is given in Fig. 4.9

## CO-ORDINATE SYSTEM ADOPTED

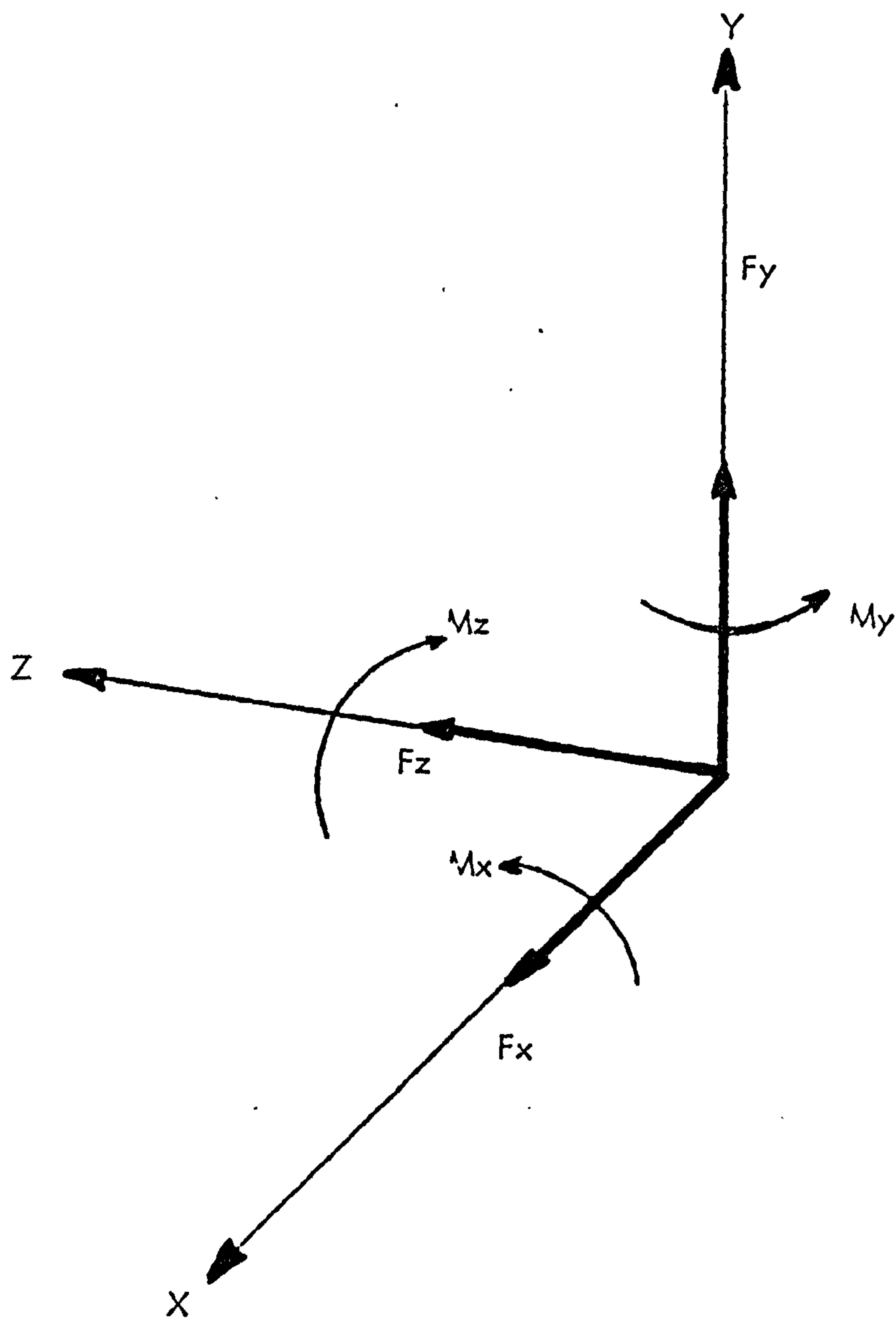


Fig. 4.7

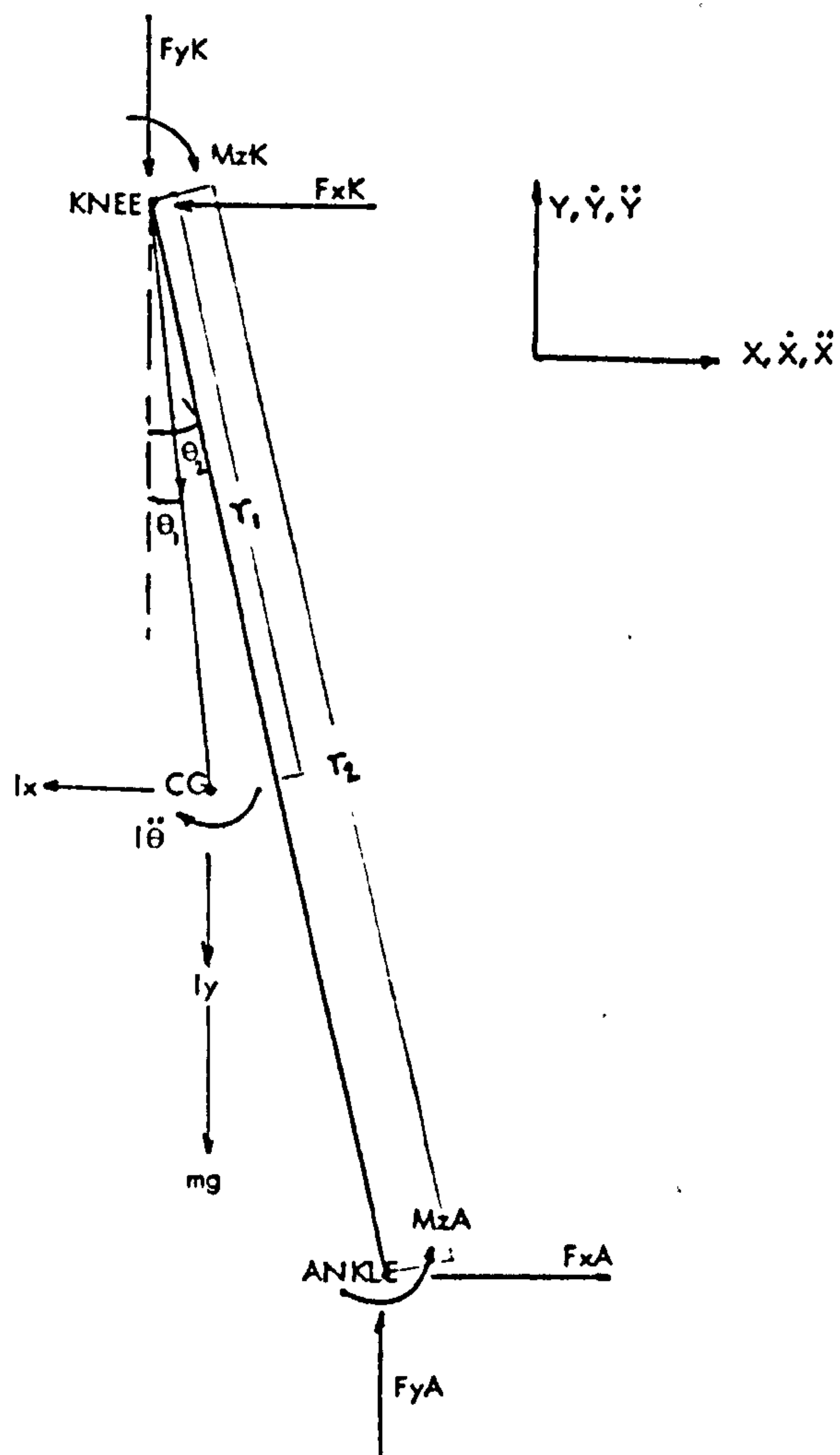


Fig. 4.8

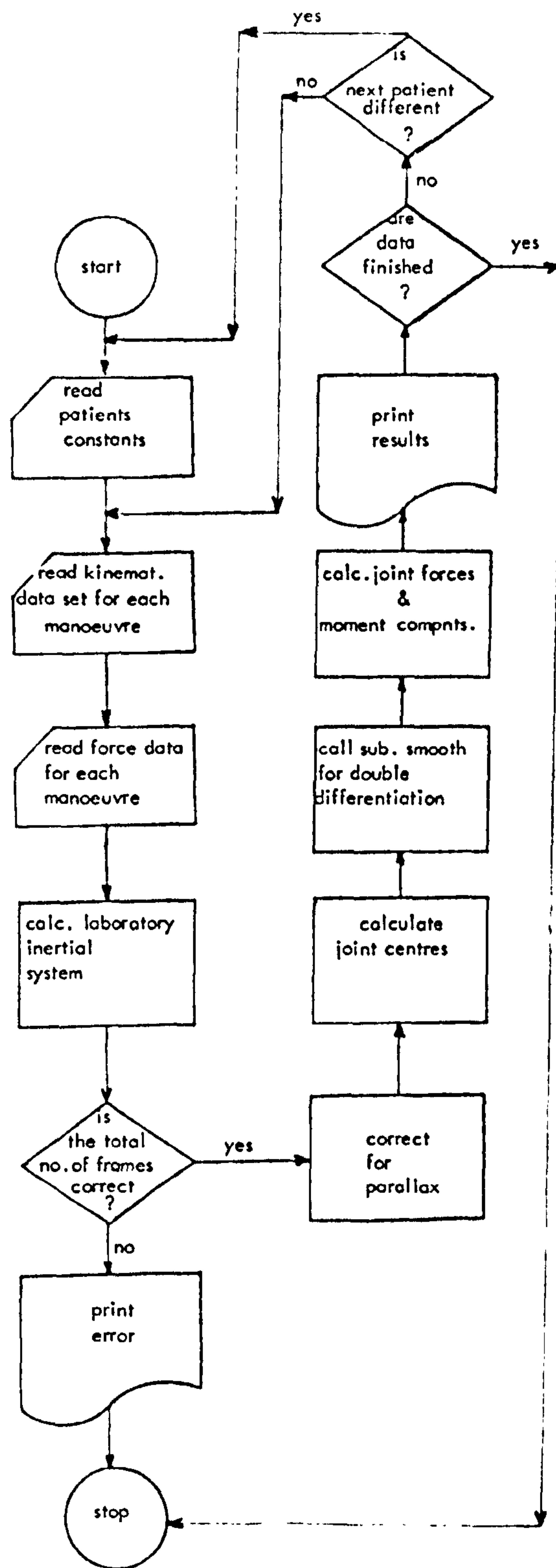


Fig. 4.9

## CHAPTER 5

### RESULTS AND DISCUSSION

#### 5.1 Introduction

#### 5.2 Raw Data and Calculation of Moment

#### 5.3 Moments in the Sagittal Plane

##### 5.3.1 Moments at the ankle joint

##### 5.3.2 Moments at the knee joint

##### 5.3.3 Moments at the hip joint

#### 5.4 Moments in the Coronal Plane

##### 5.4.1 Moments at the ankle joint

##### 5.4.2 Moments at the knee joint

##### 5.4.3 Moments at the hip joint

#### 5.5 Moments in the Transverse Plane

#### 5.6 The angle-angle Diagrams

#### 5.7 Angle-Velocity Diagrams

#### 5.8 Analysis of Result for One Particular Patient, P2 ("within-patient" comparisons)

##### 5.8.1 Introduction

##### 5.8.2 Moments in the sagittal plane

##### 5.8.3 The angle-angle diagrams

## CHAPTER 5 DISCUSSION OF RESULTS

### 5.1 Introduction

The step test described by Grieve et al (1978) included four basic pairs of manoeuvres (FUL-BDT, FDT-BUL, FDL-BUT and FUT-BDL). However, as outlined in the methodology only one pair of the four has been investigated in this project.

This is the first of the manoeuvres referred to as FUL-BDT. Grieve's nomenclature was designed to describe the manoeuvre and to correspond to the location of the Polgon sensors on the subjects leg. Thus, FUL means forward (F) upwards (U) with polgon sensors mounted on the leading (L) leg. FUT describes the same manoeuvre but this time with the polgon sensors mounted on the trailing (T) leg.

In this study the two manoeuvres carried out were described as follows:

- (i) with the subject (S) or patient (P) stepping forward (F) and upwards (U) always with the right leg leading. This manoeuvre is then referred to simply as FU 0 (or FU 1); zero to indicate zero height step and one to indicate 10% height step respectively. The results for the right leg are then referred to as R/FU 0 (or R/FU 1) and for the left leg as L/FU 0 (or L/FU 1).
- (ii) with the subject (S) or patient (P) stepping backwards (B) downwards (D) always with the left leg leading. This manoeuvre is referred to simply as BD 0 (or BD 1) zero to indicate zero height step and one to indicate 10% height step respectively. The results for the right leg are then referred to as R/BD 0 (or R/BD 1) and for the left leg as L/BD 0 (or L/BD 1).

It should be emphasised that, considerable amount of work was necessary in order to reduce the cine-film data using a Vanguard-PCD film analyser. Each manoeuvre was seen by three cameras (both limbs analysed simultaneously) for zero stepping height and 10% stepping height for each patient and subject. The number of frames analysed for each manoeuvre was about 300 (100 for each camera giving a total for all subjects and patients of the order of 25,000). On average, the film analysis for a patient (subject) carrying out all the manoeuvres was 12 hours. Furthermore, additional time had to be spent in editing the film data so as to ensure elimination of human errors.

- Fig. 5.1 FP data for normal subject 1, FU 1 manoeuvre  
Fig. 5.2 FP data for normal subject 1, BD 1 manoeuvre  
Fig. 5.3 FP data for patient 1, FU 1 manoeuvre  
Fig. 5.4 FP data for patient 1, BD 1 manoeuvre  
Fig. 5.5 Y displacements for subject 1, FU 1 manoeuvre  
Fig. 5.6 Y displacements for subject 1, FU 1 manoeuvre  
Fig. 5.7 Y displacements for patient 1, FU 1 manoeuvre  
Fig. 5.8 Y displacements for patient 1, BD 1 manoeuvre  
Fig. 5.9 Moments in sagittal plane for subject 1, FU 1 manoeuvre  
Fig. 5.10 Moments in sagittal plane for subject 1, BD 1 manoeuvre  
Fig. 5.11 Moments in sagittal plane for patient 1, FU 1 manoeuvre  
Fig. 5.12 Moments in sagittal plane for patient 1, BD 1 manoeuvre  
Fig. 5.13 Moments in coronal plane for subject 1, FU 1 manoeuvre  
Fig. 5.14 Moments in coronal plane for subject 1, BD 1 manoeuvre  
Fig. 5.15 Moments in coronal plane for patient 1, FU 1 manoeuvre  
Fig. 5.16 Moments in coronal plane for patient 1, BD 1 manoeuvre  
Fig. 5.17 Moments in transverse plane for subject 1, FU 1 manoeuvre  
Fig. 5.18 Moments in transverse plane for subject 1, BD 1 manoeuvre  
Fig. 5.19 Moments in transverse plane for patient 1, FU 1 manoeuvre  
Fig. 5.20 Moments in transverse plane for patient 1, BD 1 manoeuvre  
Fig. 5.21 Typical ground forces in normal level walking  
Fig. 5.22 Typical intersegmental moments for normal level walking  
Fig. 5.23 Angle-angle diagrams for normal level walking  
Fig. 5.24 Angle-angle diagrams for 10% step test

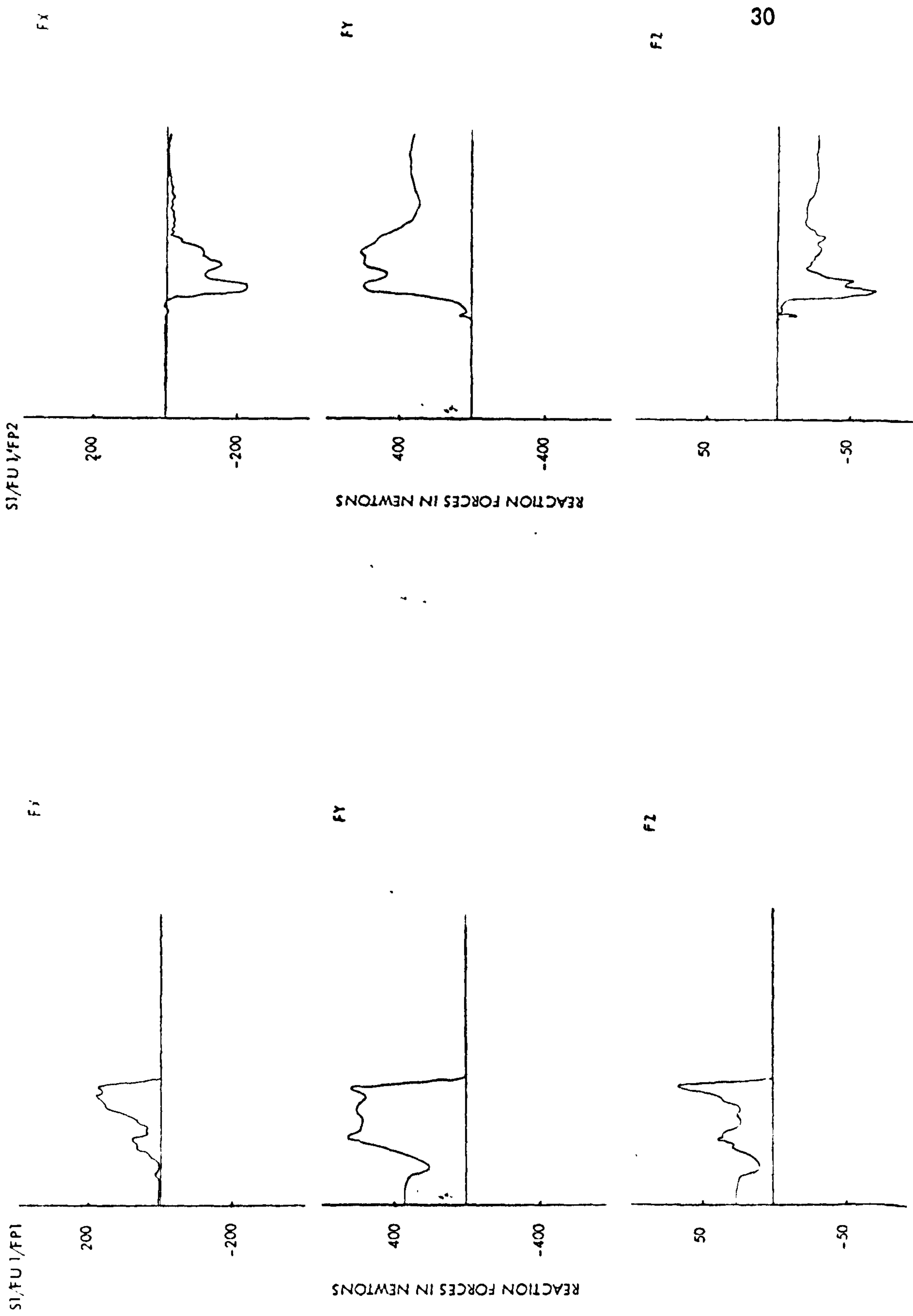


Fig. 5.1



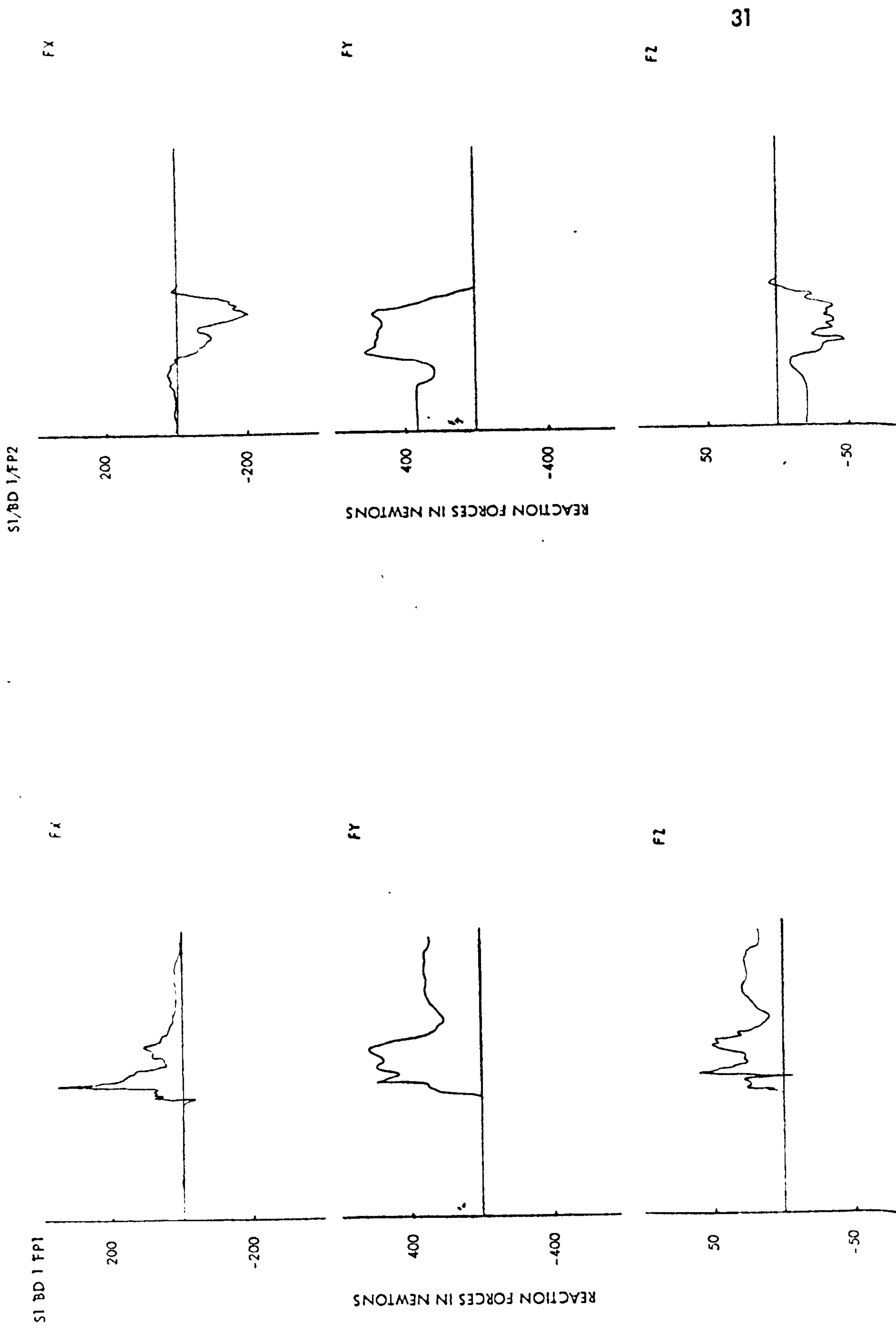


Fig. 5.2

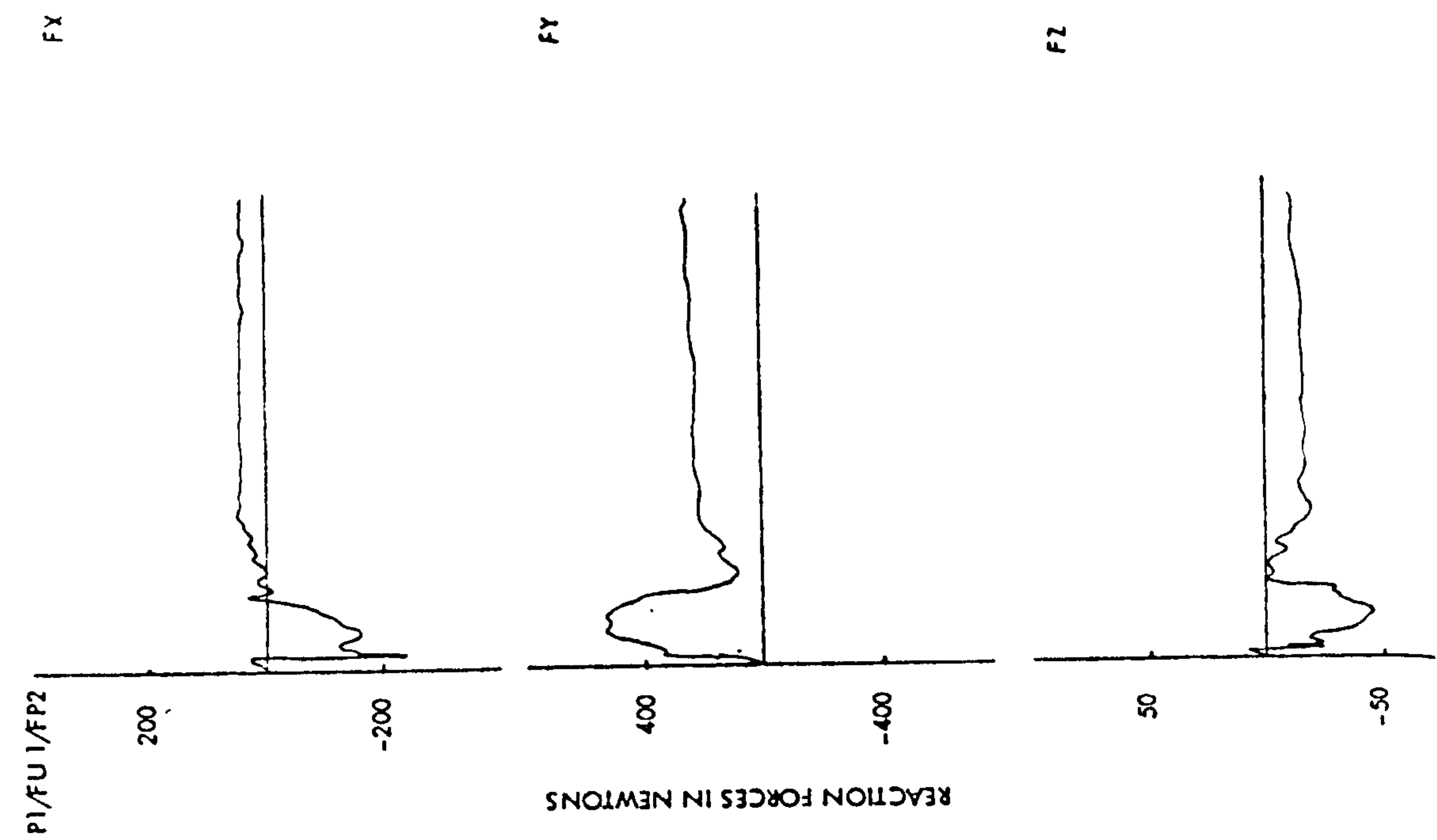


Fig. 5.3

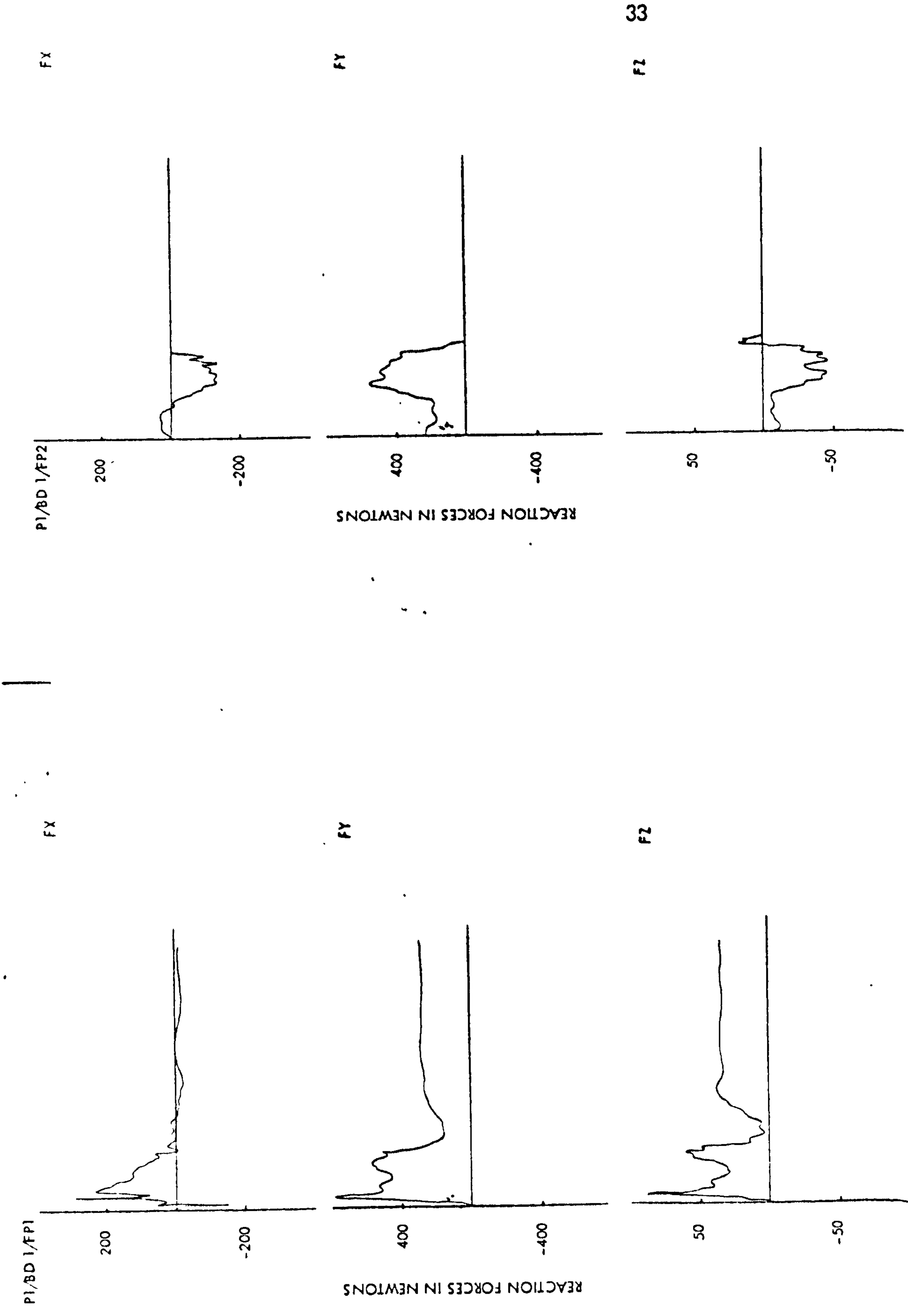


Fig.5.4

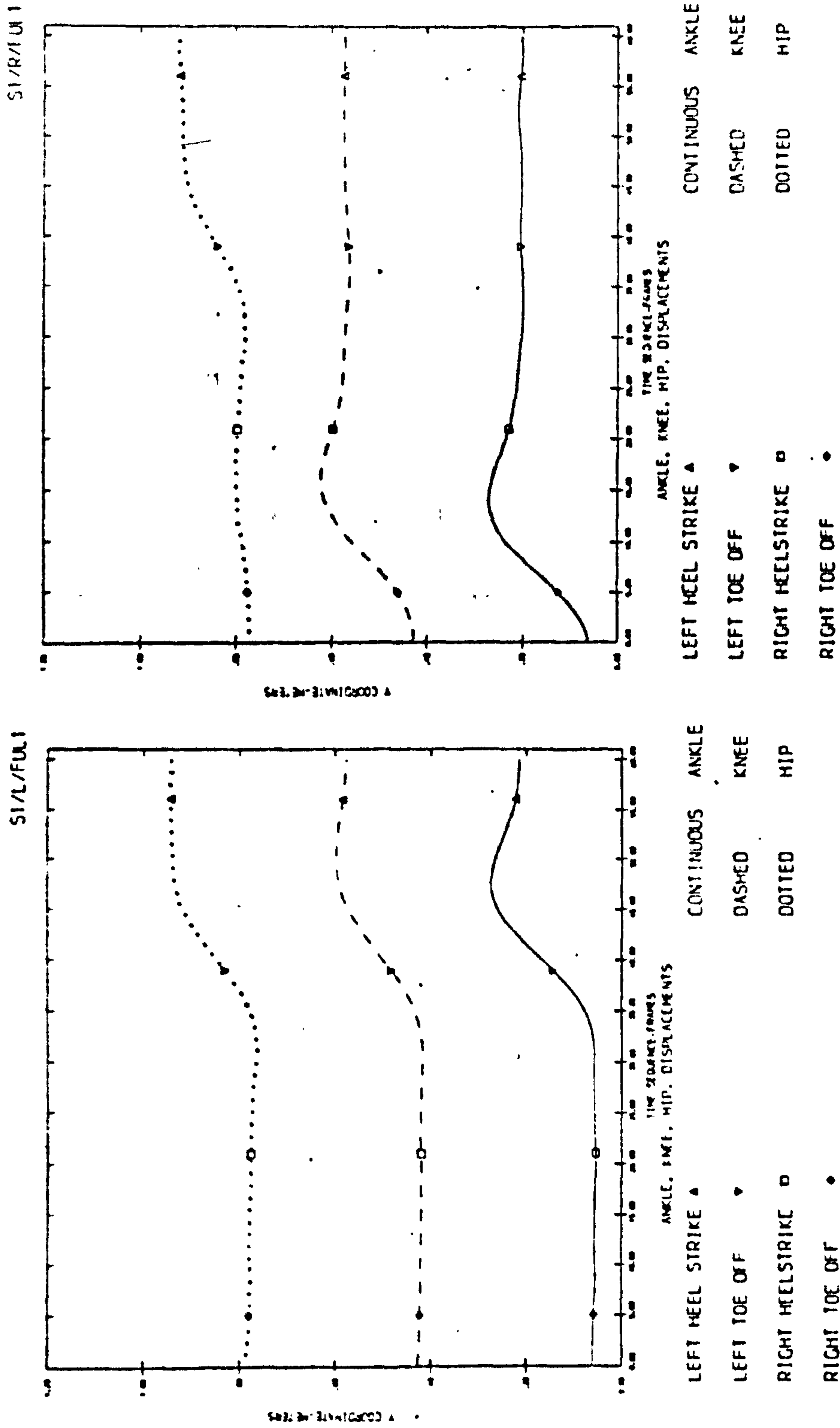


Fig 5.5

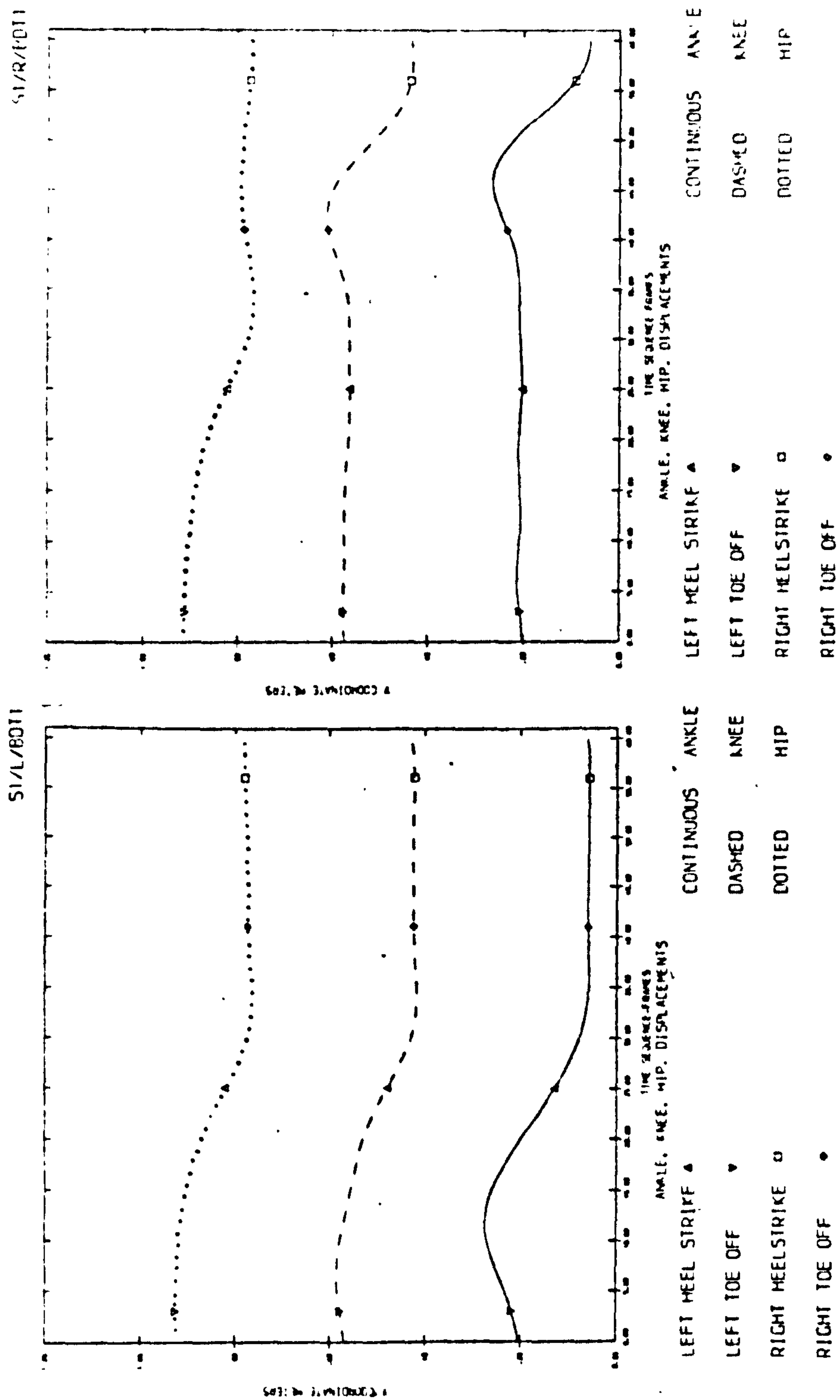


Fig 5.6

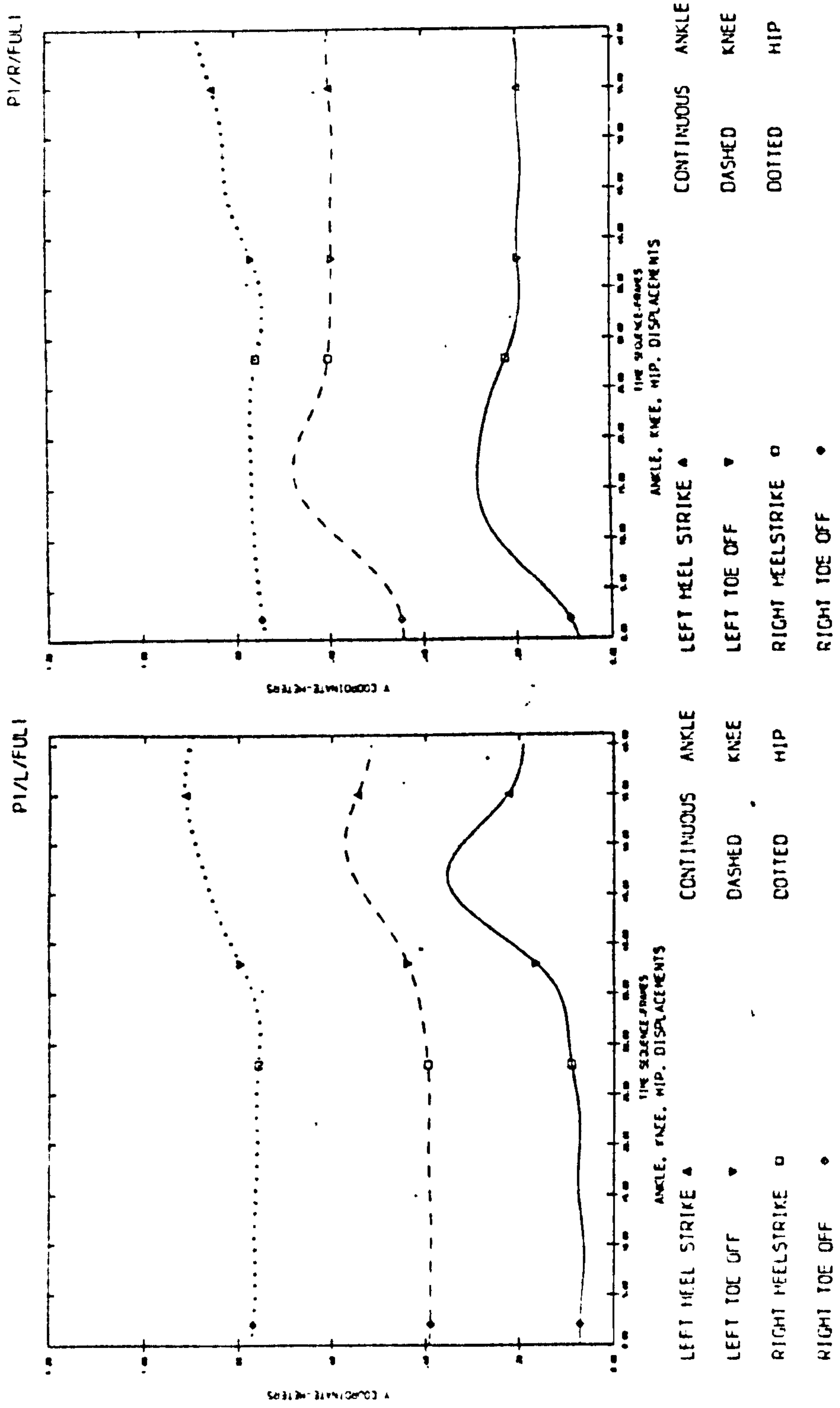


Fig 5.7

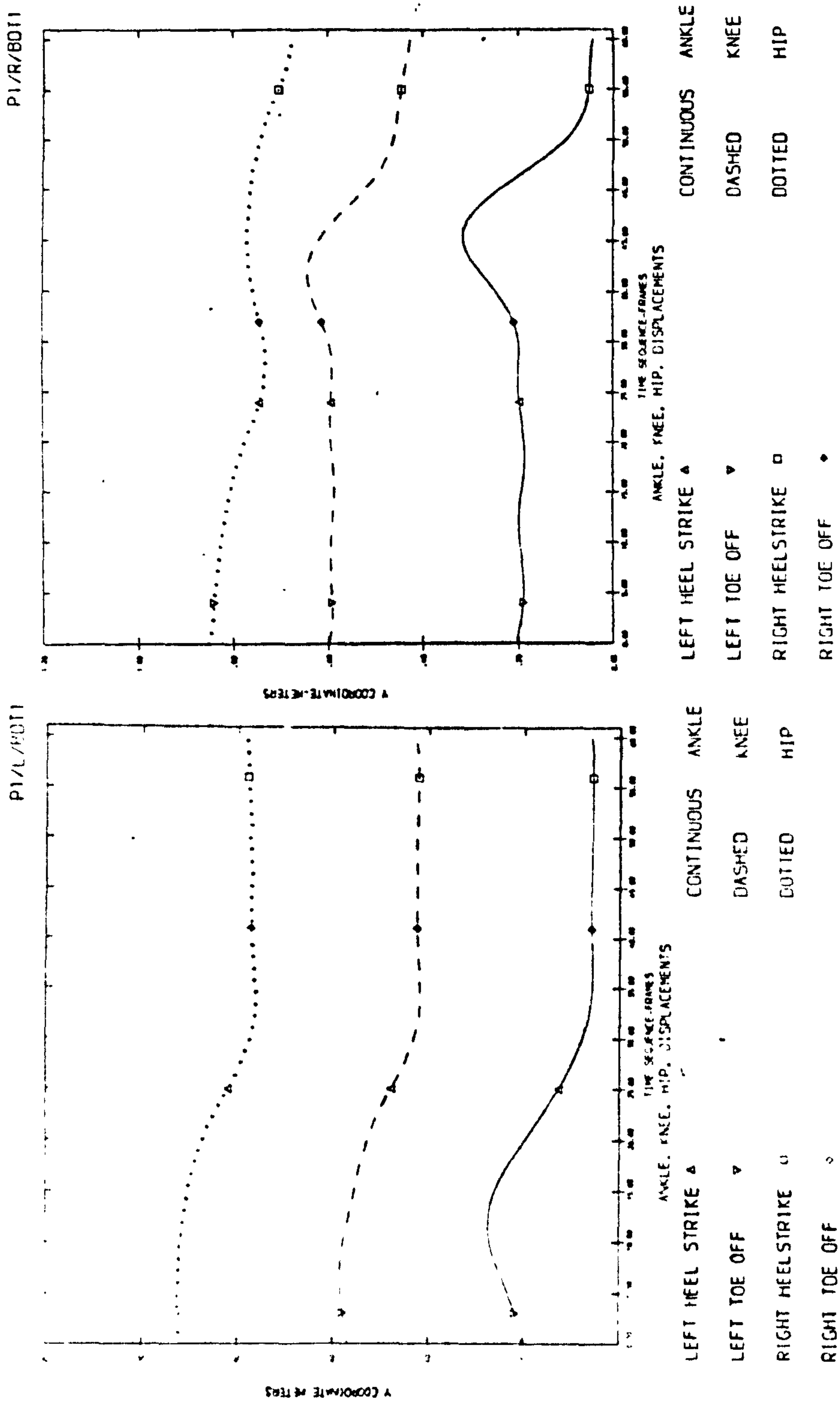


Fig 5. 8

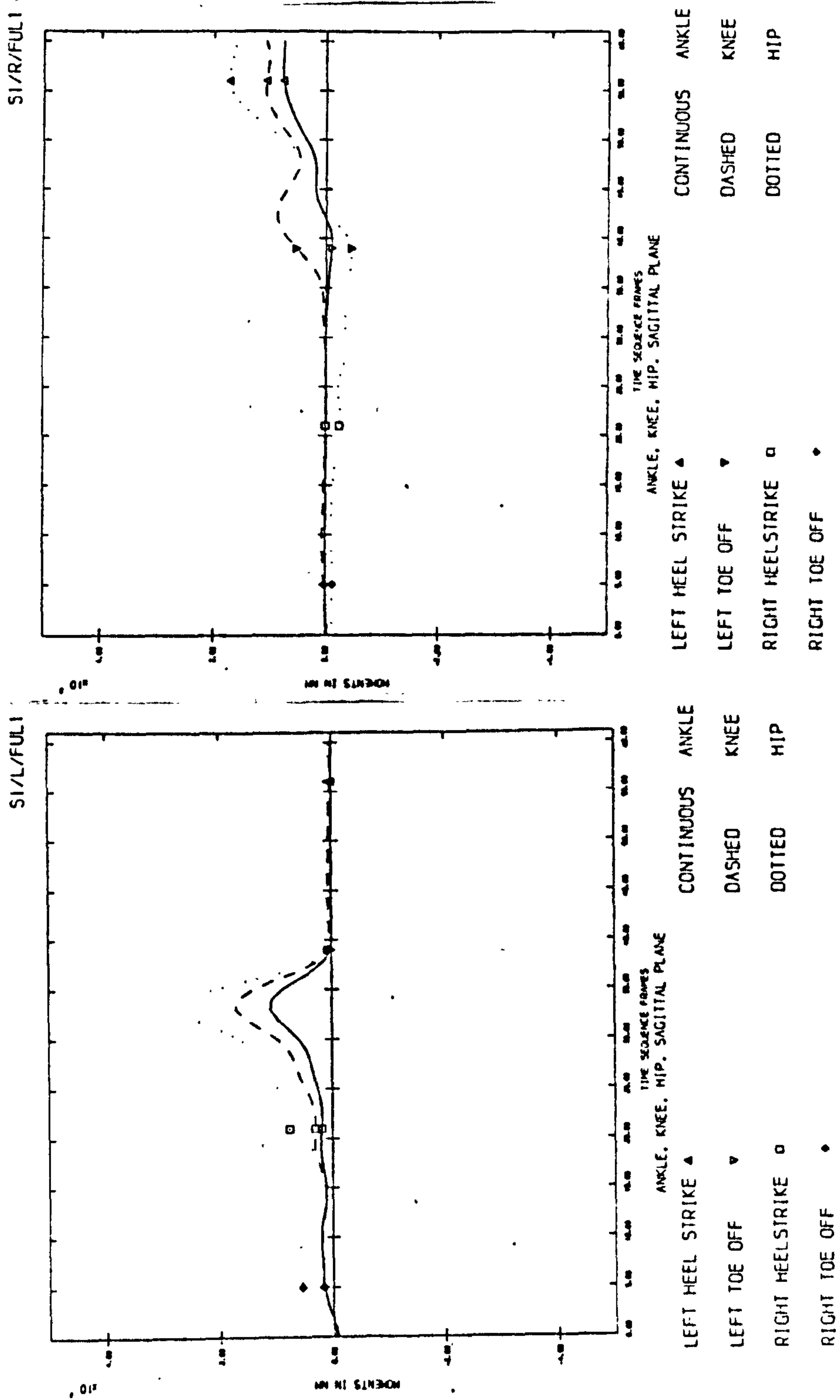


Fig. 5.9



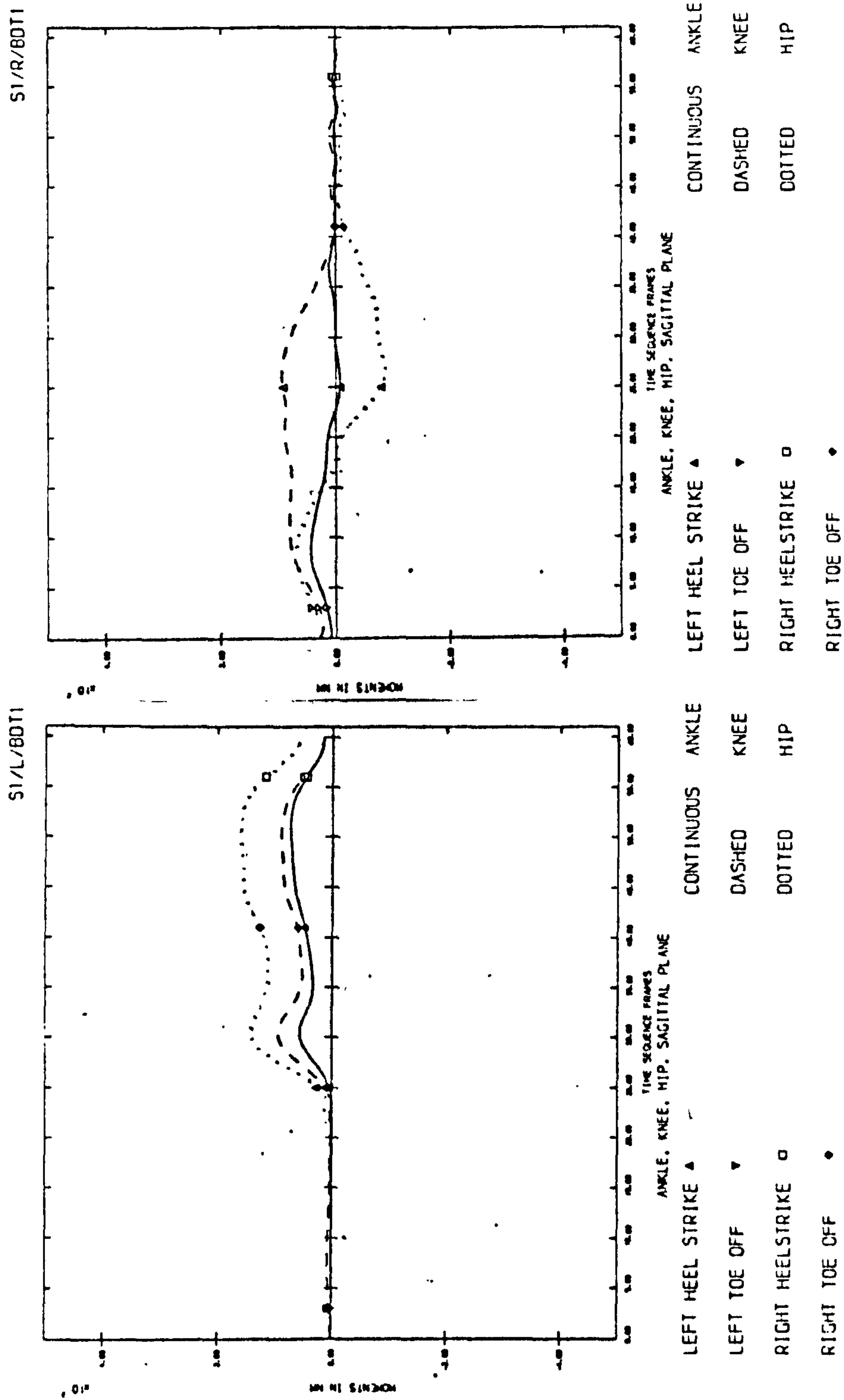


Fig.5.10

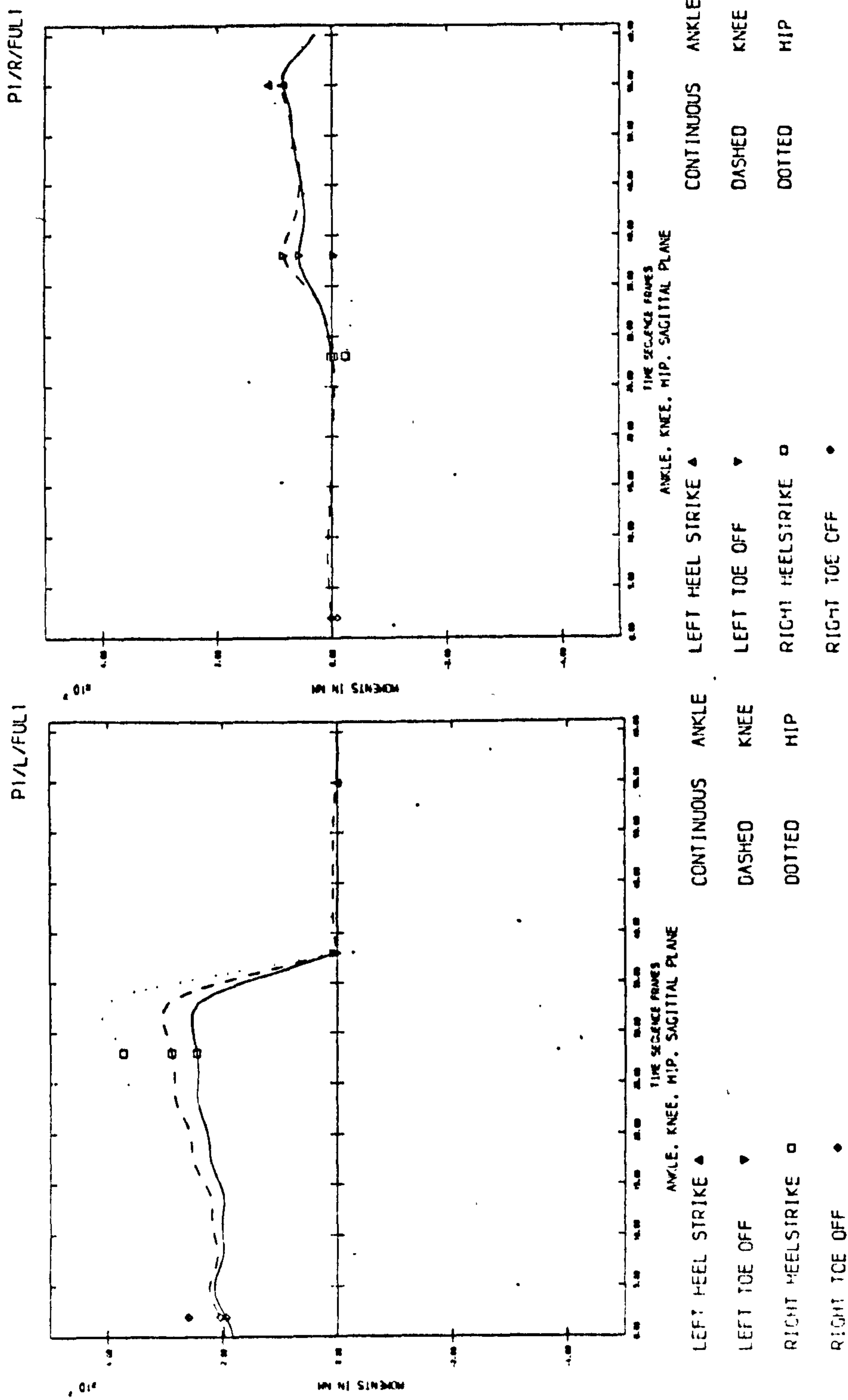


Fig. 5.11

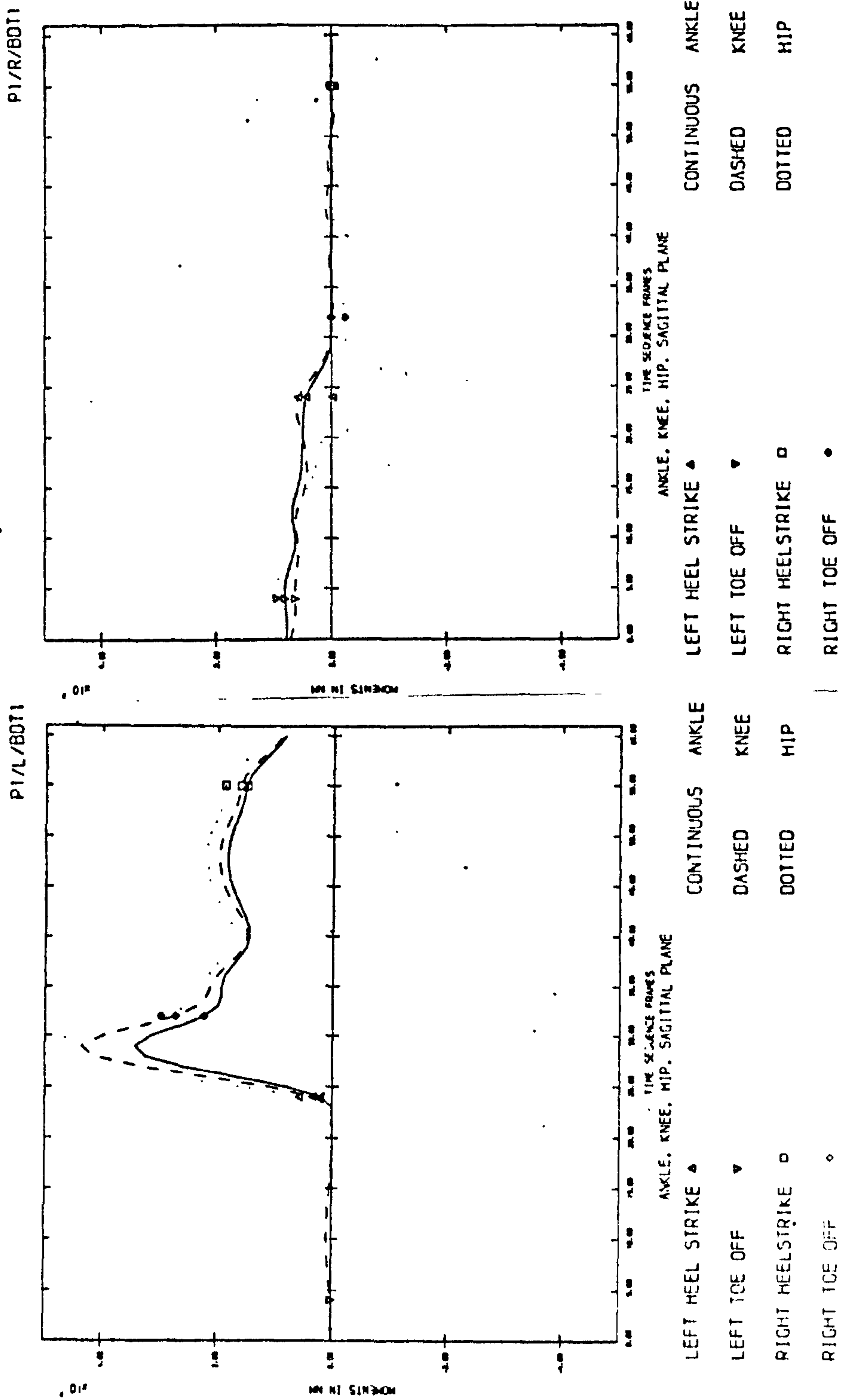


Fig.5.12

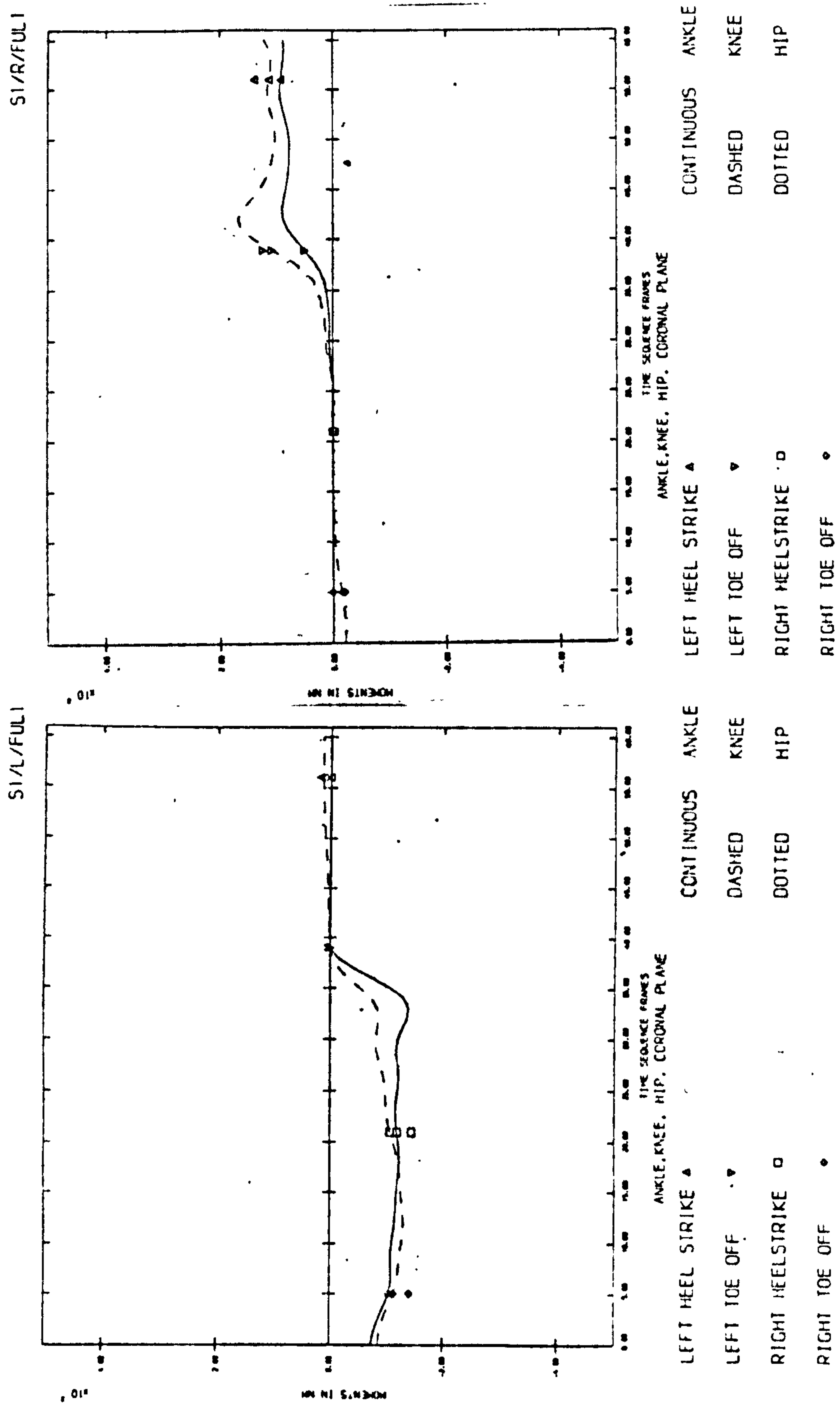


Fig. 5.13

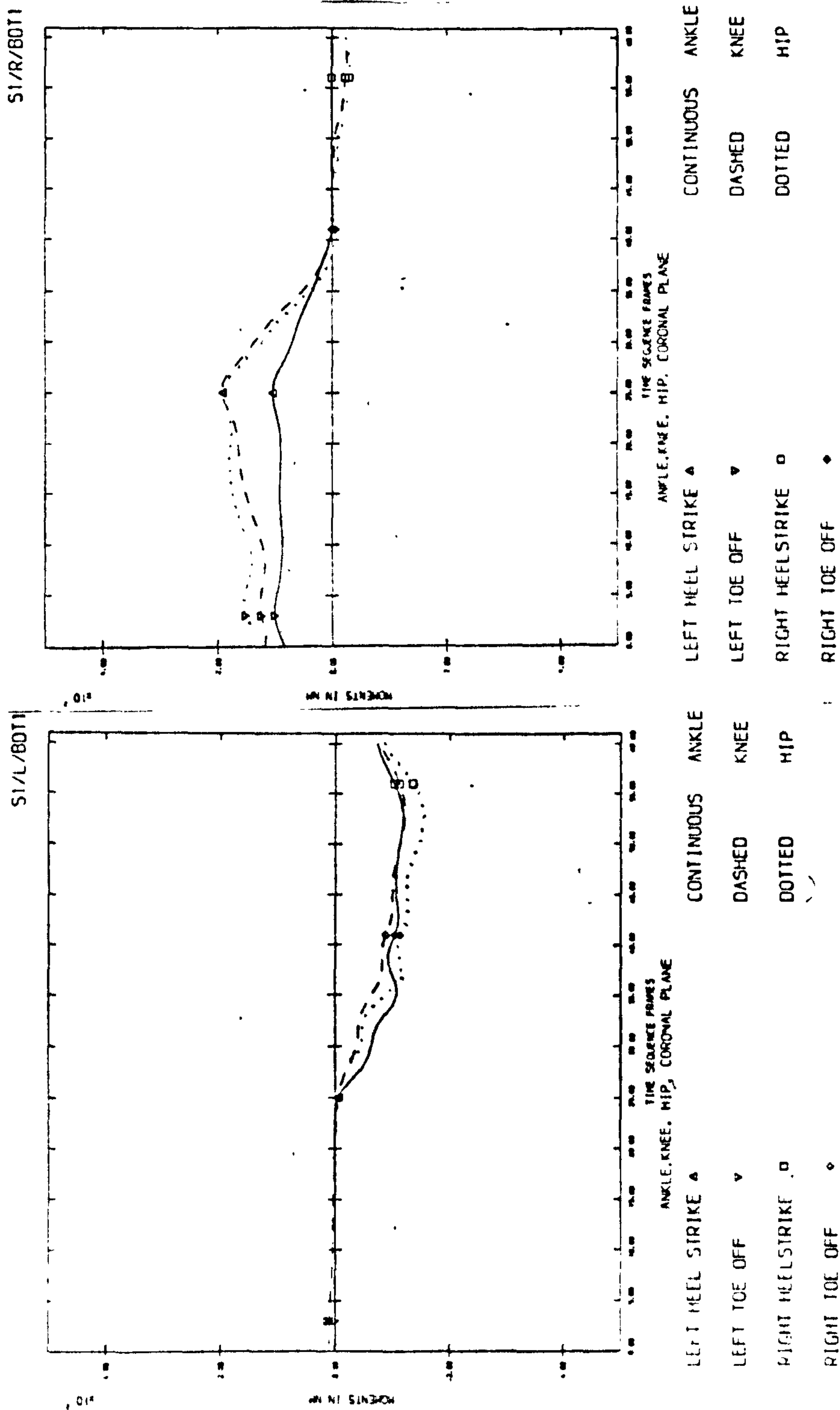


Fig.5.14

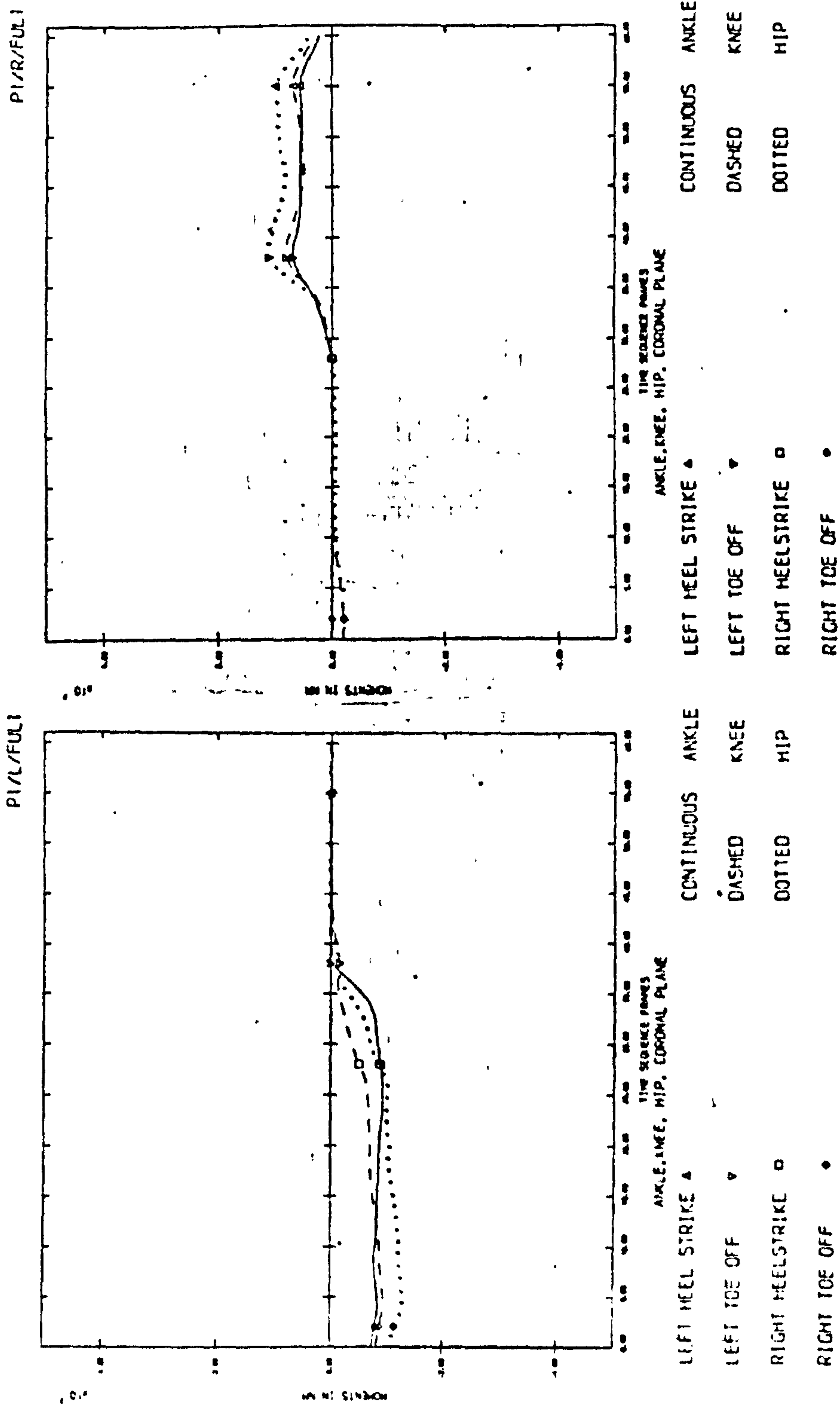


Fig 5.15

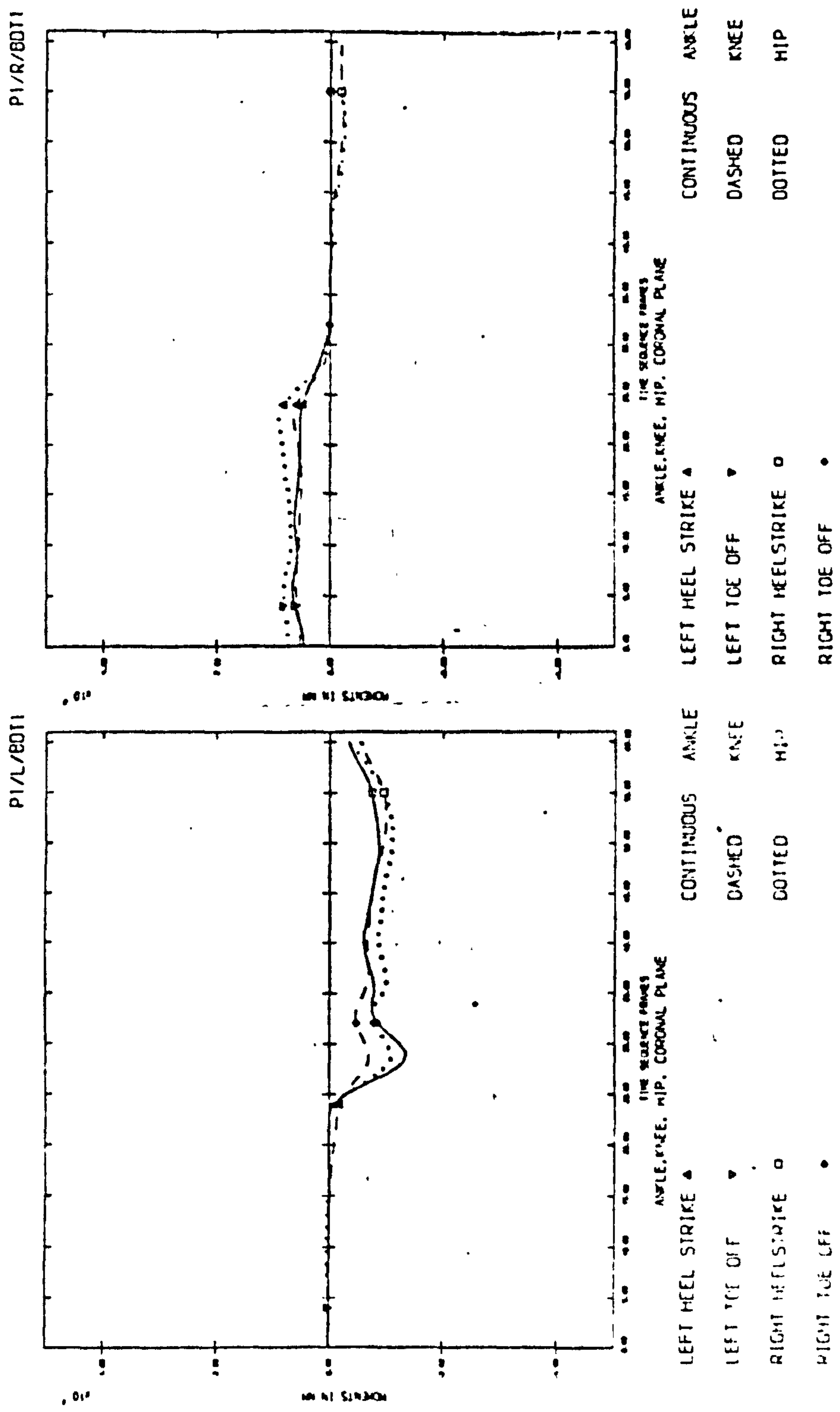


Fig 5.16

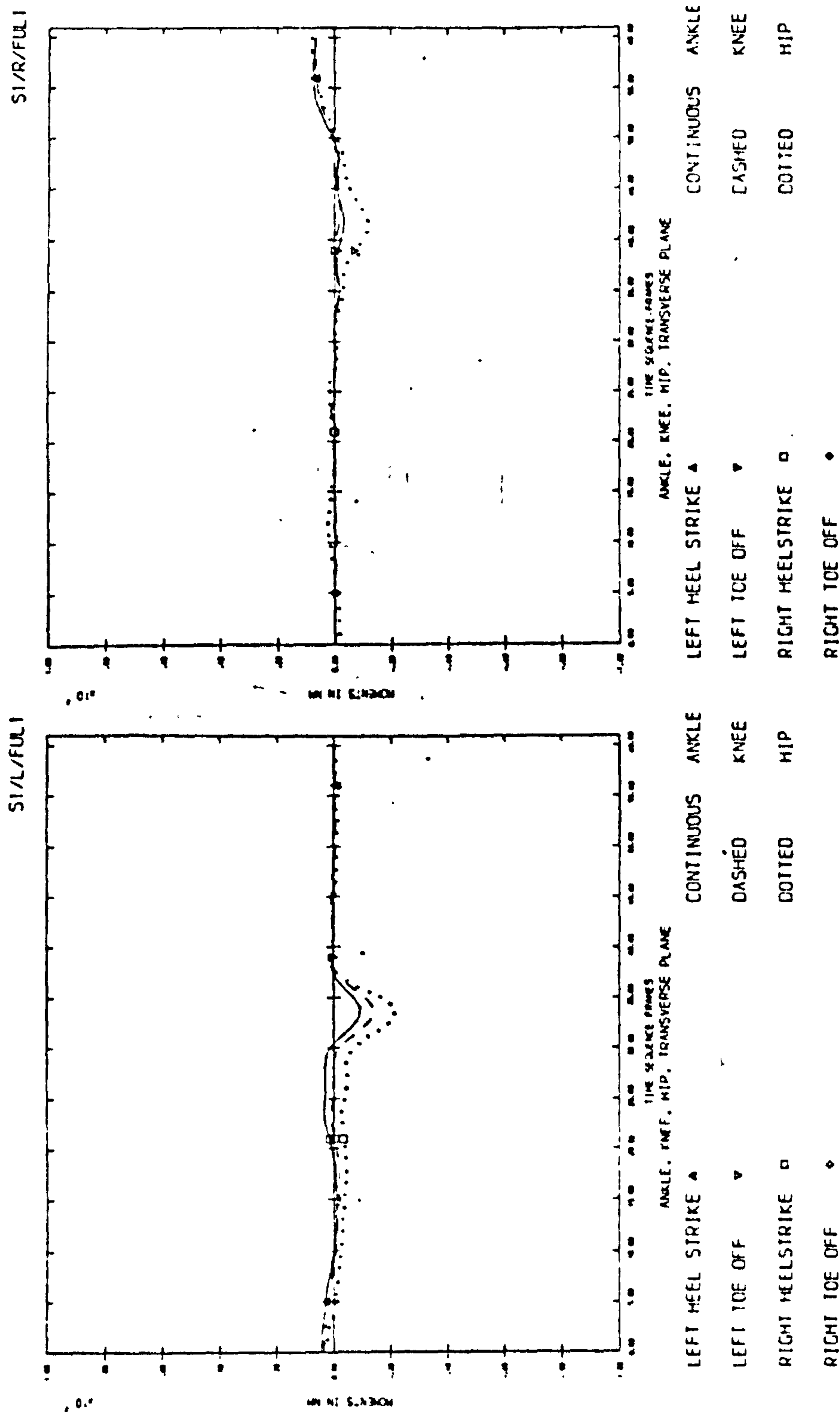


Fig 5.17



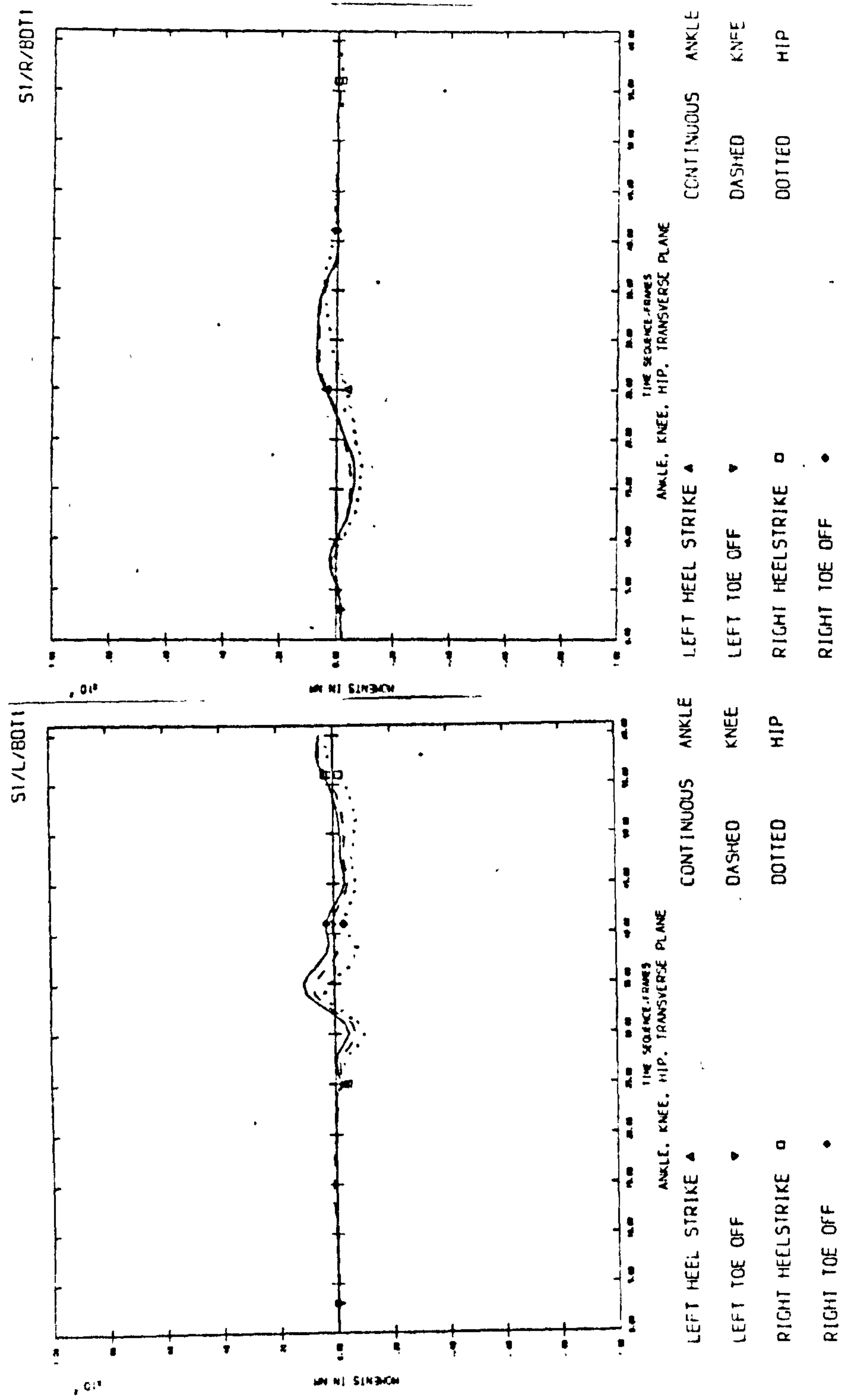


Fig. 5.18

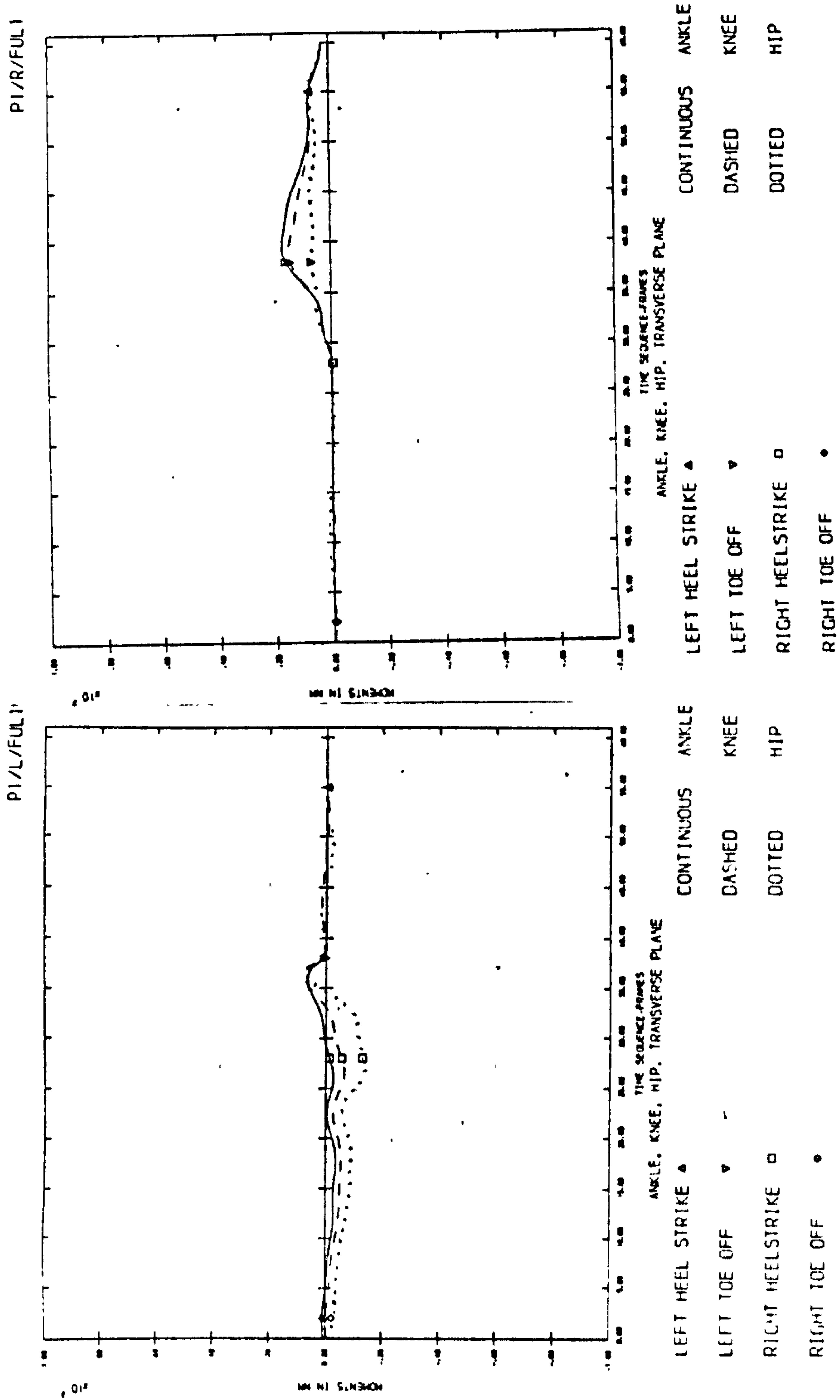


Fig. 5.19

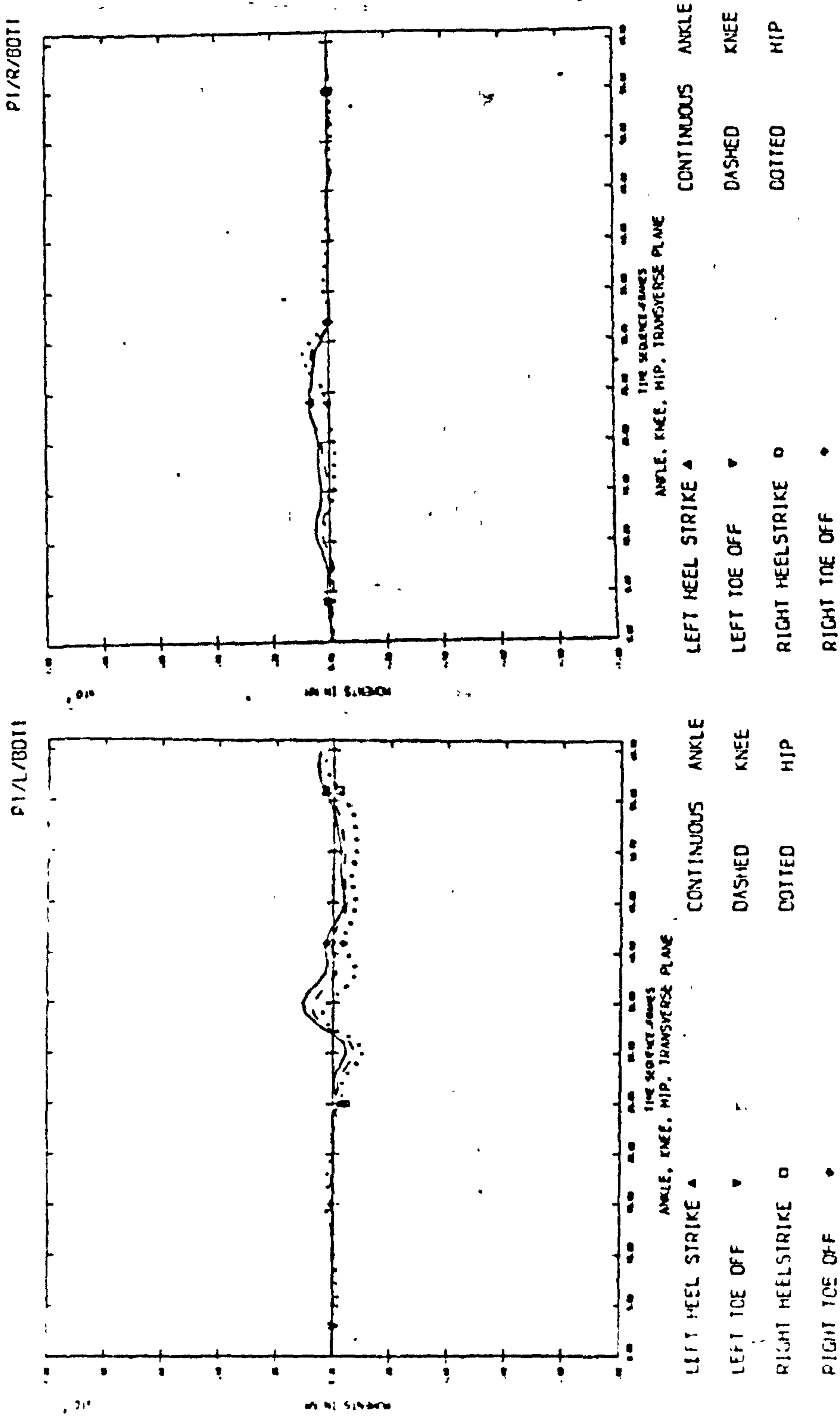


Fig 5.20

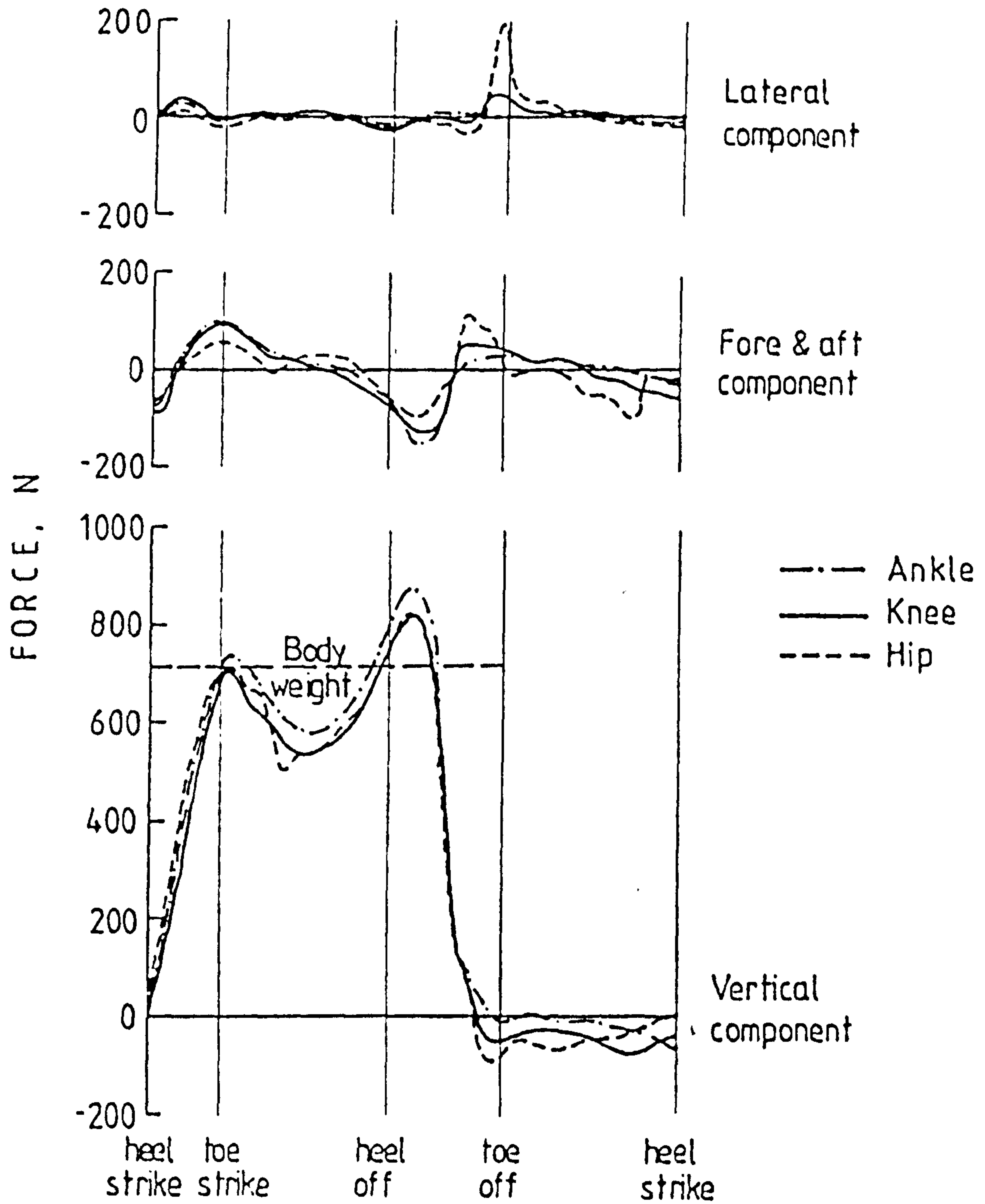


Fig 5.21

Intersegment forces in level walking.

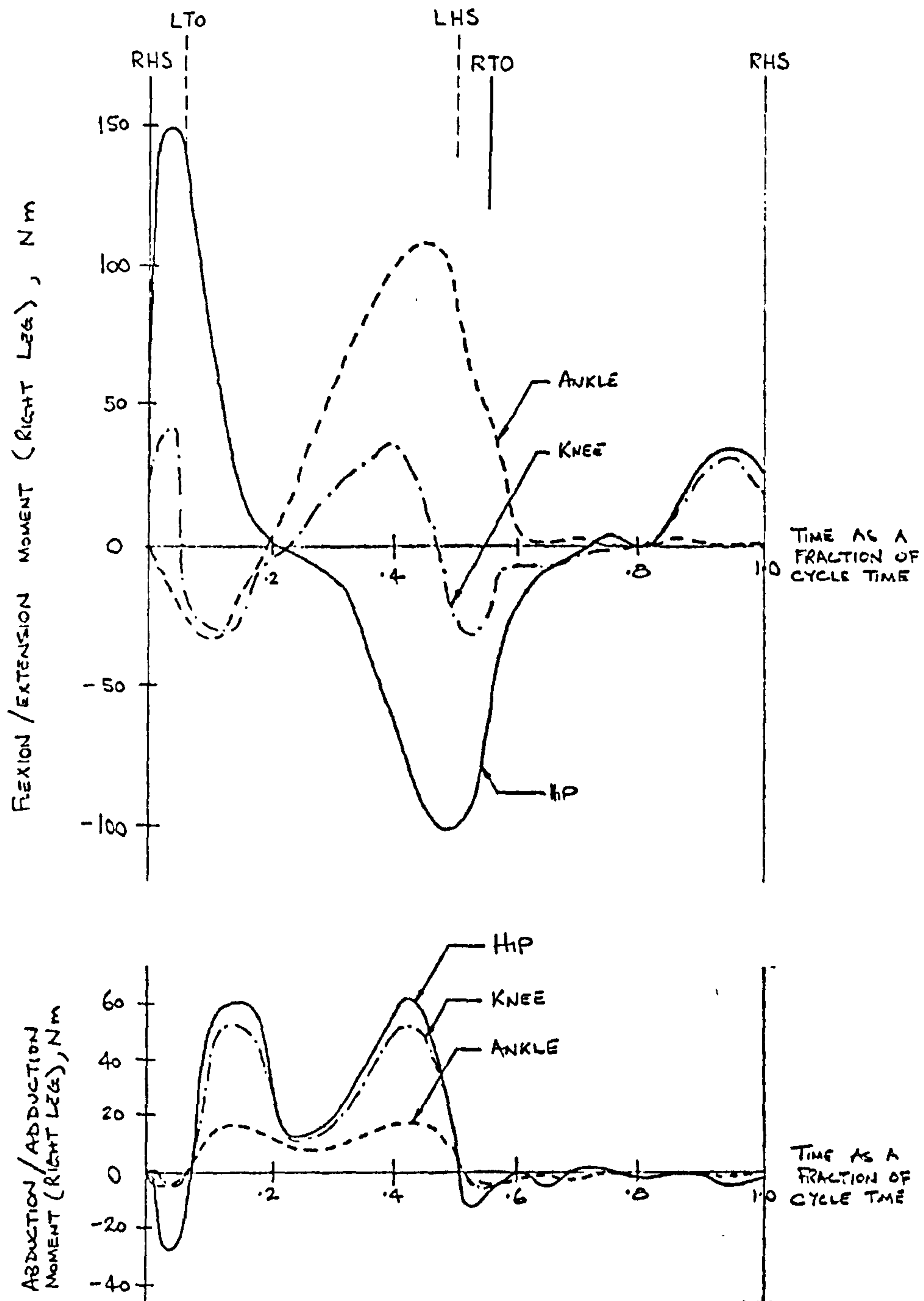


Fig. 5.22

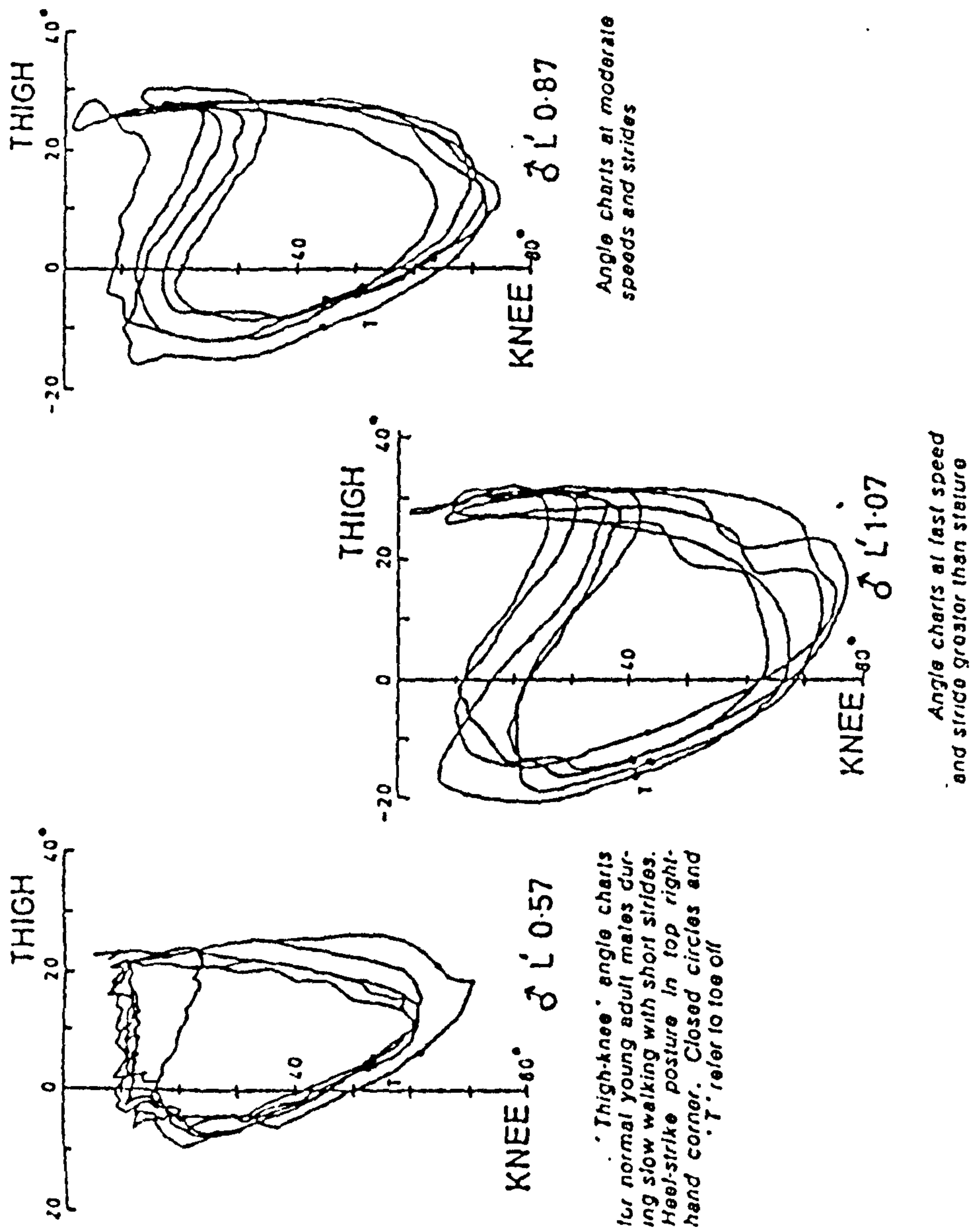
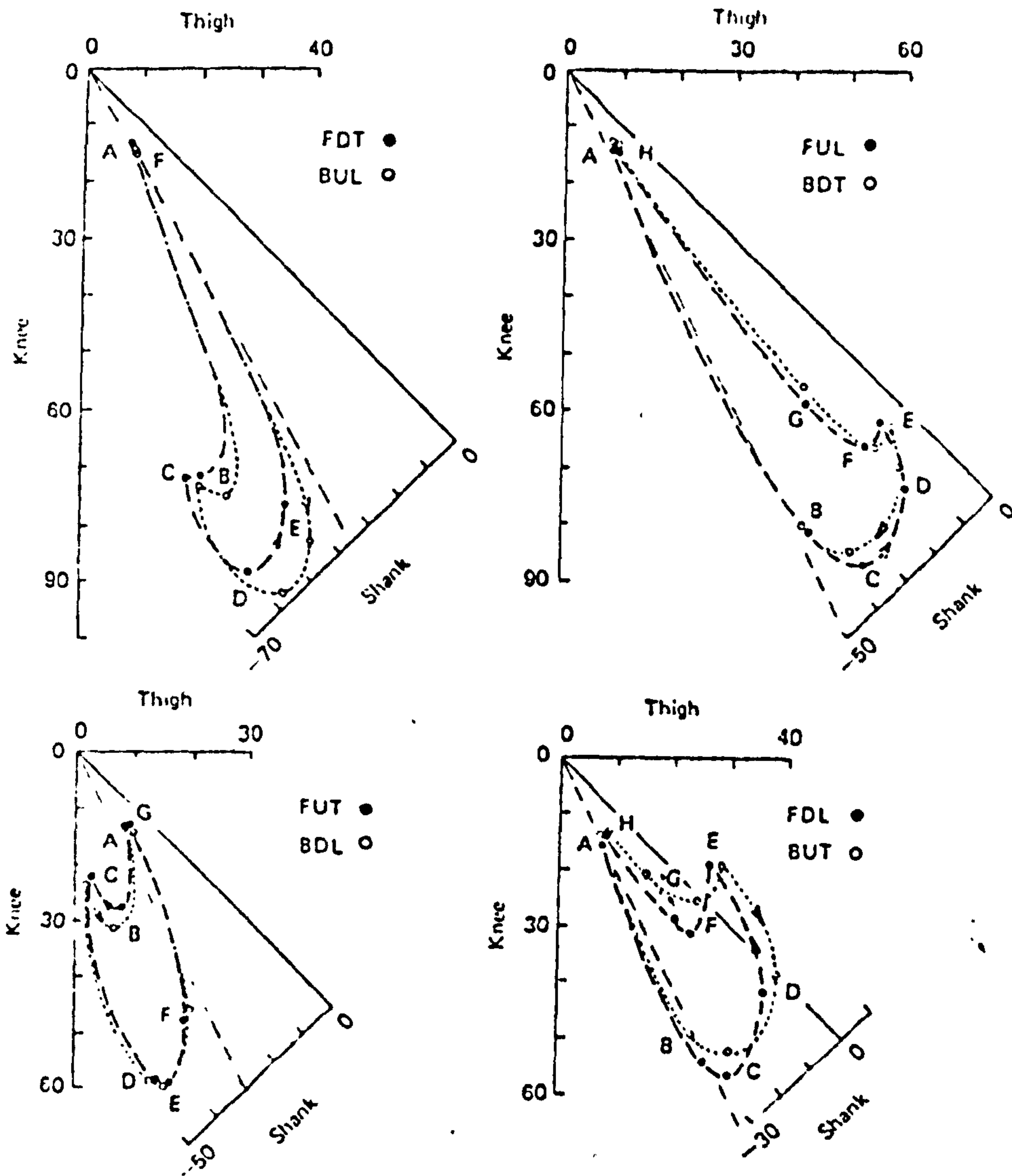


Fig. 5.23



Predicted forms of thigh-knee diagrams to be expected at a relative step height equal to 10% of stature.

Fig 5.24

## 5.2 Raw Data and Calculation of Moment

Sample for some of the raw data from the tests of one normal subject and one patient are presented in Fig. 5.1 to 5.8.

In comparing the forceplate (FP) data for the normals with those for the pathologicals it will be noticed that the forces for the patients showed considerable instability (made apparent by the fluctuations on the force signals) particularly on the y component of force 'Fy' see Fig. 5.1 to 5.4)

Referring to the Fy force trace Fig. 5.1 to 5.4 the initial force value is about 300 N which is about half of the body weight (this value varies, sometimes more and sometimes less than half body weight). It depends on the way the test subject is standing prior to commencement of the experiment.

The pattern of the Fy force has the characteristic double peak shape observed on tests for normal level walking (see Fig. 5.21). The peak value however, is only about 10% above body weight, whereas on walking values between 20% to 40% above body weight have been reported. This of course is due to the fact that only one step is performed and the inertia effects are much smaller than in walking.

It was considered that the Y displacements were the most relevant in the raw data and these are shown in Fig. 5.5 to 5.8. For the FU I manoeuvre (Fig. 5.5) it is noted that the hip rises smoothly as the subject walks on the step, whereas the knee and the ankle displacements show peaks which indicate that the subject attempts to clear the step during the swing phase. The same applies for the BD I manoeuvre. Symmetries for the left and right leg for the two manoeuvres are evident. There are no significant differences between the normals (Fig. 5.5 and 5.6) and the patients tested (Fig. 5.7 and 5.8) in the displacements curves.

From the raw data, the moments in the sagittal, coronal and transverse planes have been calculated and sample graphs for the results for the same subject and patient are presented in Fig. 5.9 to 5.20.

It will be appreciated that a large number of graphs have been obtained, one set for each of the five normal subjects and for each of the five patients tested. In order to allow comparisons between subjects, between patients, between



patients and subjects, between various types of manoeuvres to be made easily, the curves for the same manoeuvres for normals and patients have been superimposed on the same diagram.

During swing phase very small load actions have been noted. These are practically zero at the ankle and very slight at the knee and hip due to inertia effects. Load actions during the swing phase have been reported to be of low magnitude when compared to those obtained during the stance phase of locomotion by several investigators (Paul, 1967 and Frankel and Bressler, 1952).

### 5.3 Moments in the Sagittal Plane

5.3.1 Moments at the ankle joint. The results for the ankle are as follows:

Fig. 5.25 FU O (left and right) for patients and subjects

Fig. 5.26 BD O (left and right) for patients and subjects

Fig. 5.27 FU 1 (left and right) for patients and subjects

Fig. 5.28 BD 1 (left and right) for patients and subjects

Examination of Fig. 5.25 and 5.26 shows that the shapes of the graphs for the zero height step are similar to those obtained using a 10% step height (Fig. 5.27 and 5.28). The patient P1, however showed higher moment values than the other patients in all cases. The following discussion is based on the results of the 10% step test but applies equally well to the zero height step.

Referring to Fig. 5.26 and 5.28, BD O and BD 1 are similar to those for FU O and FU 1 but the graphs are in the reverse order with respect to time; due to the backwards direction of the BD manoeuvre.

On examination of Fig. 5.25 and 5.27, it is evident that the initial negative (plantar flexing moment) that is observed in normal level walking (see Fig. 5.22) is absent. This is because proper heel strike does not obtain in any of the manoeuvres examined in this study. The dorsiflexion moment was in the range of 50 - 100 Nm which is somewhat less than the reported average of 100 to 150 Nm to normal level walking (see Fig. 5.22).

It is evident from Fig. 5.25 to 5.28 for normal subjects that the loading on the two ankles (right and left) is not symmetrical - the loading on the left ankle tends

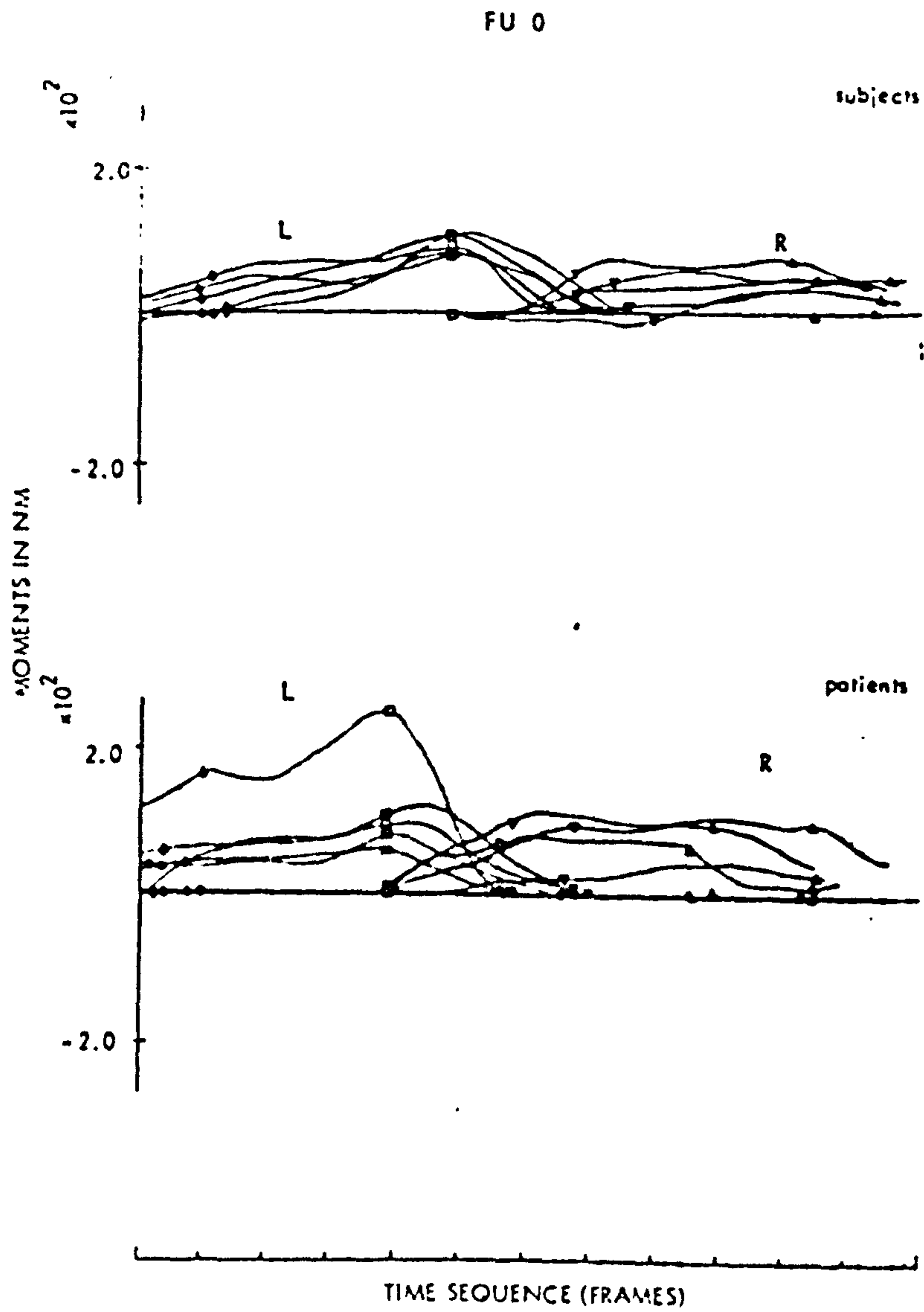


Fig. 5.25 ankle moments sagittal plane

LEFT HEEL STRIKE  $\blacktriangle$

LEFT TOE OFF  $\blacktriangledown$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\diamond$

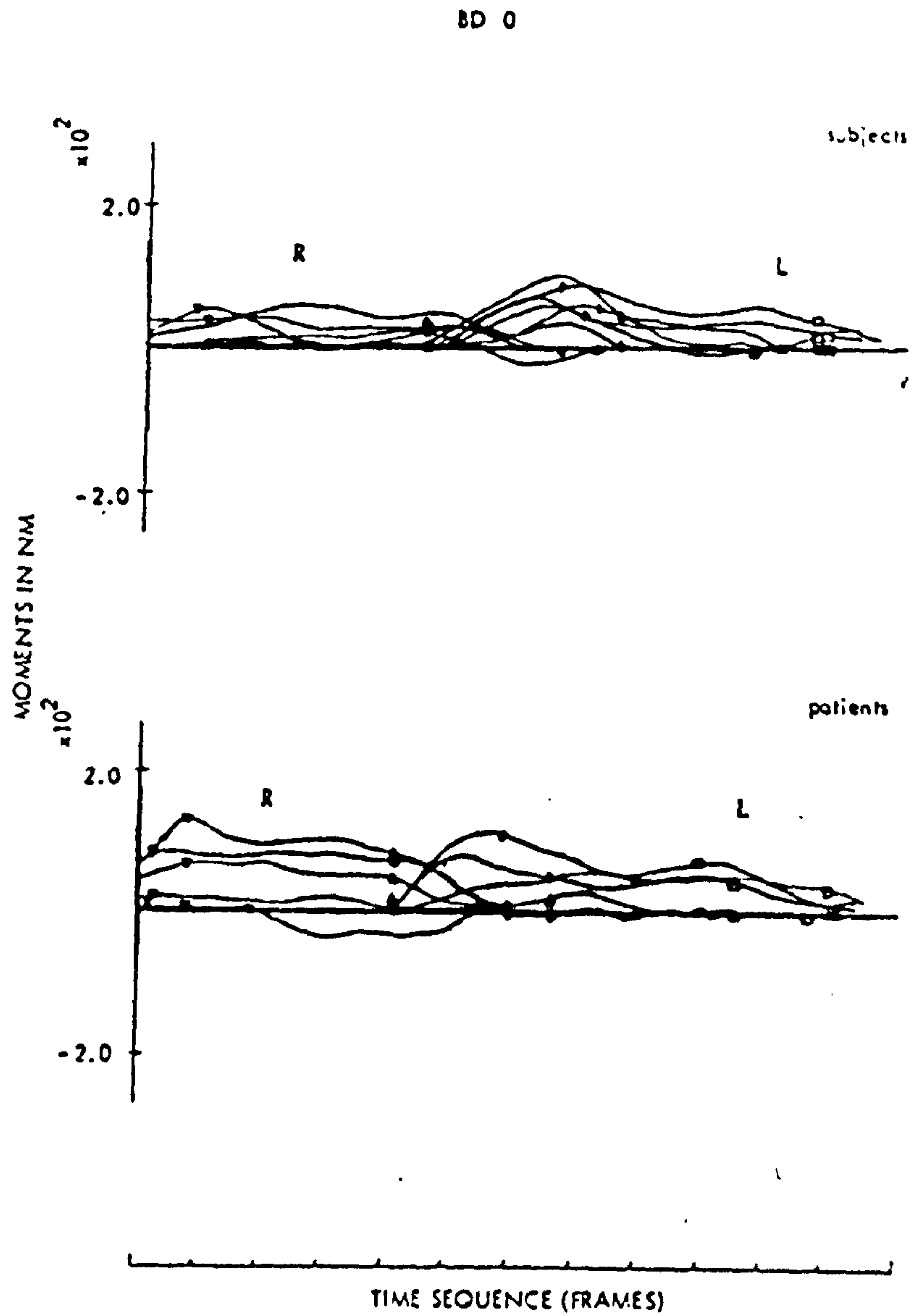


Fig. 5.26 ankle moments sagittal plane

LEFT HEEL STRIKE  $\Delta$

LEFT TOE OFF  $\nabla$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\diamond$

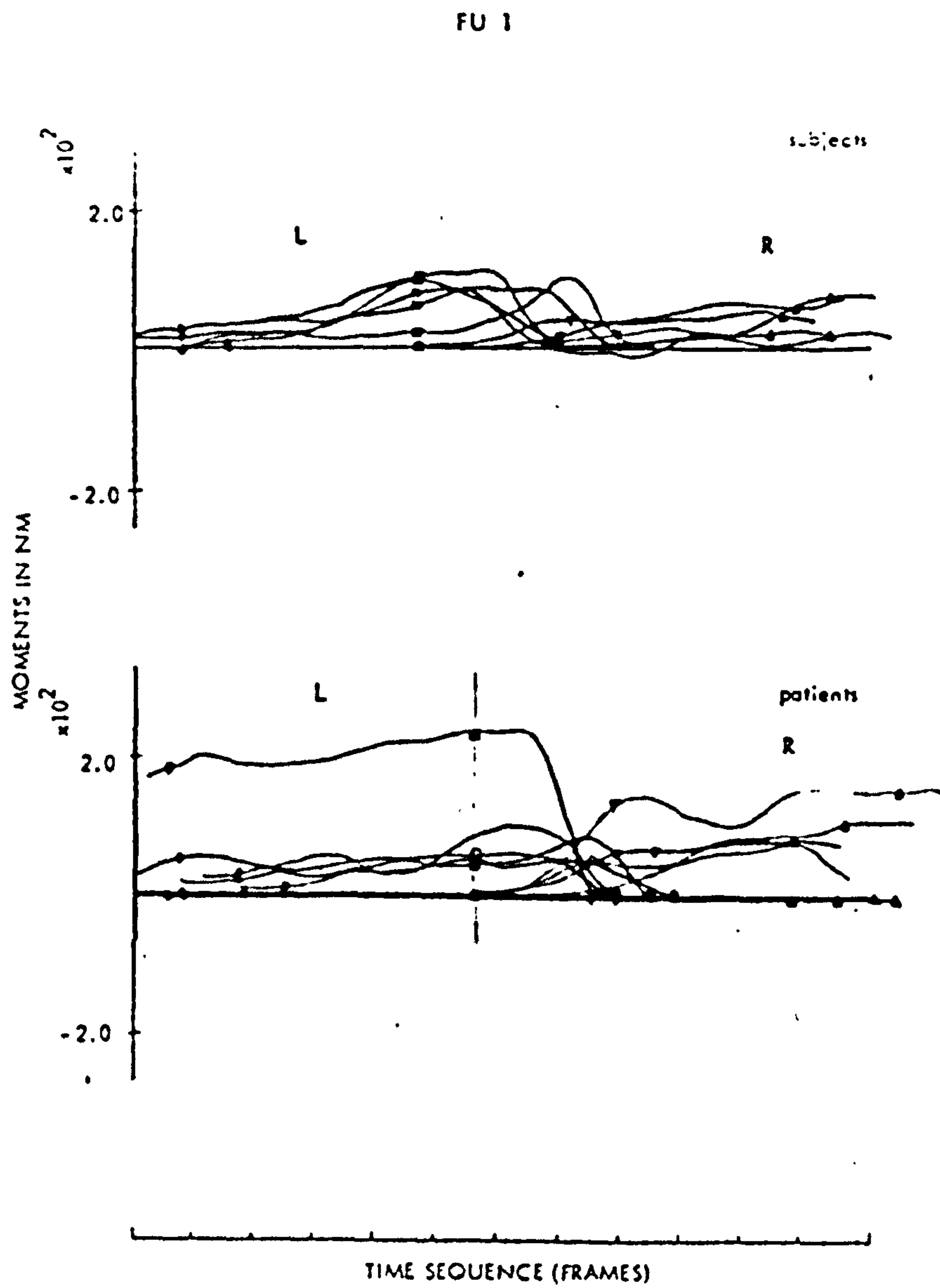


Fig. 5.27 ankle moments sagittal plane

LEFT HEEL STRIKE  $\Delta$

LEFT TOE OFF  $\nabla$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\diamond$

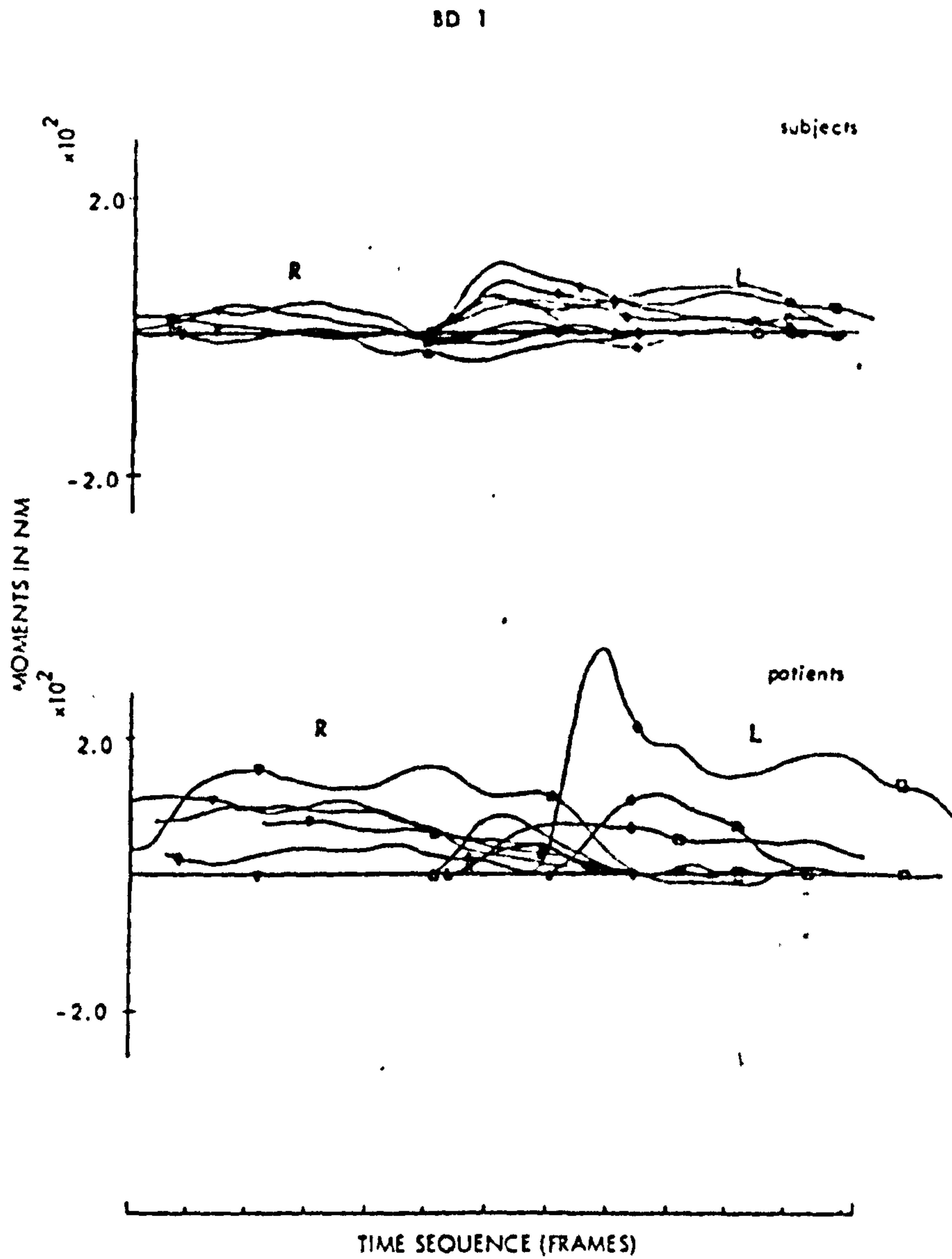


Fig. 5:28 ankle moments sagittal plane

LEFT HEEL STRIKE  $\Delta$

LEFT TOE OFF  $\nabla$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\circ$

to be higher than that on the right. This may be explained as follows: on a FU manoeuvre (zero or 10% height) the left leg being posterior to the body, applies the push off power, and on the BD manoeuvre the left leg is again posterior to the body and decelerates the body on the backwards movement.

In both cases this has the effect of increasing the ground reaction force and hence increasing the ankle moment. In the case of the patients the scatter was so large that trends cannot readily be seen for most patients. However, one patient (P1) displayed high ankle moments with the left ankle moment being higher than the right as in the case of the normals.

This tends to indicate that the ankle joint plays an active part during stepping and therefore one would expect this joint to compensate for knee deficiencies of the contralateral leg.

The temporal parameters of gait, for all patients showed considerably larger scatter than those for the normal subjects.

### 5.3.2 Moments at the knee joint

Fig. 5.29 FU.O (left and right) for patients and subjects

Fig. 5.30 BD.O " " " " " " "

Fig. 5.31 FU 1 " " " " " " "

Fig. 5.32 BD 1 " " " " " " "

On examination of the diagrams 5.29 and 5.31 the moments obtained with zero height step are generally of the same order as those for the 10% step. At first sight this would appear to be rather surprising as one would expect the quadriceps to be more active during a 10% stepping action, resulting in higher moments. However, the ankle results suggest that active plantar flexion by means of gastrocnemius action on the contralateral side (trailing limb) assist the ascending leg and thus reducing the load required by the quadriceps.

The results for the knee moments for the patients (Fig. 5.31 and 5.32) showed considerable scatter when compared to those for the normals. This applies to both zero and 10% height step test. Again patient (P1) showed higher values than the rest of the patients.

On comparing Fig. 5.29 with the graphs obtained from normal subjects during level walking (Fig. 5.20) it is noted that the usual moment curve

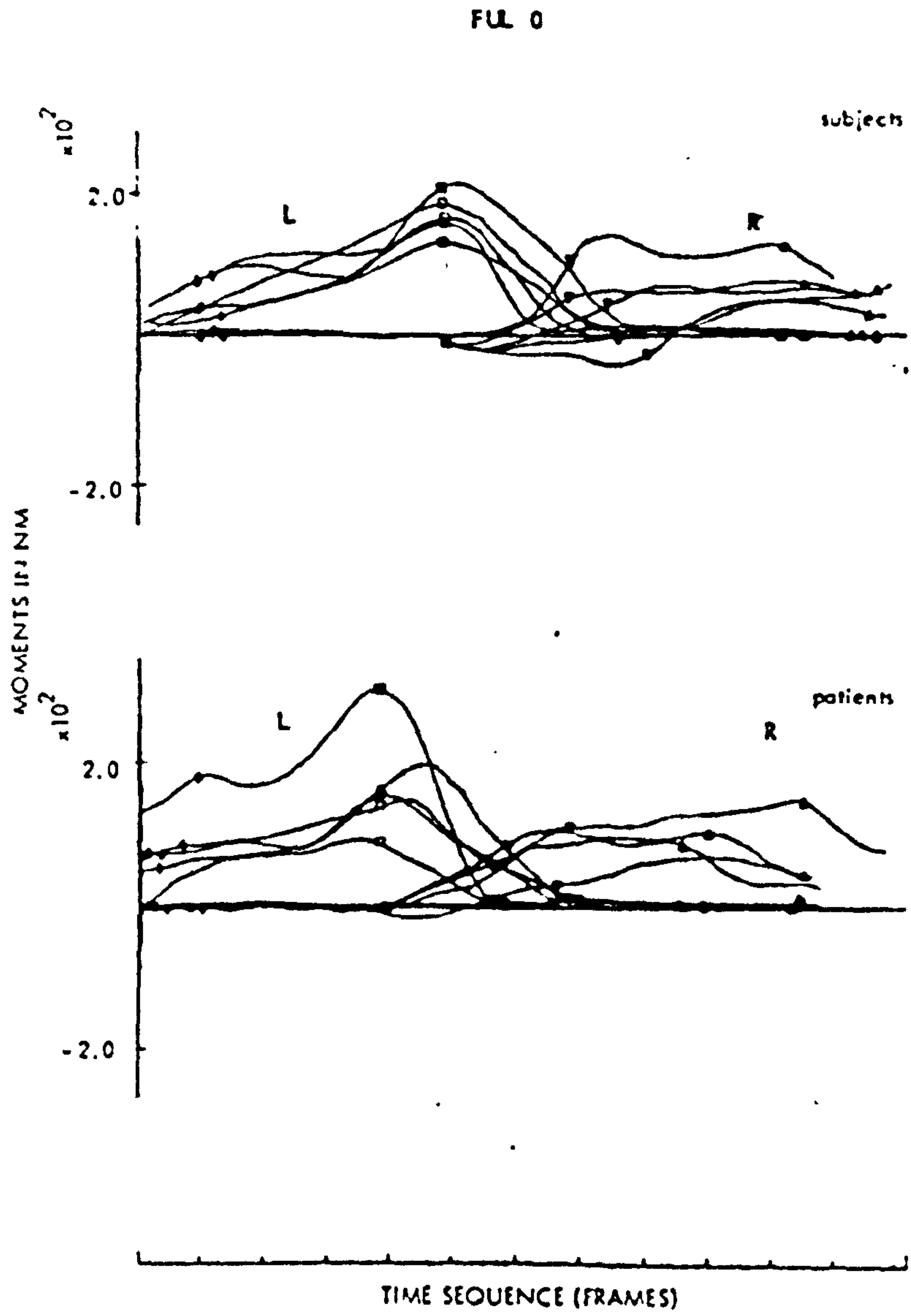


Fig. 5.29 knee moments sagittal plane

LEFT HEEL STRIKE  $\Delta$

LEFT TOE OFF  $\nabla$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\diamond$

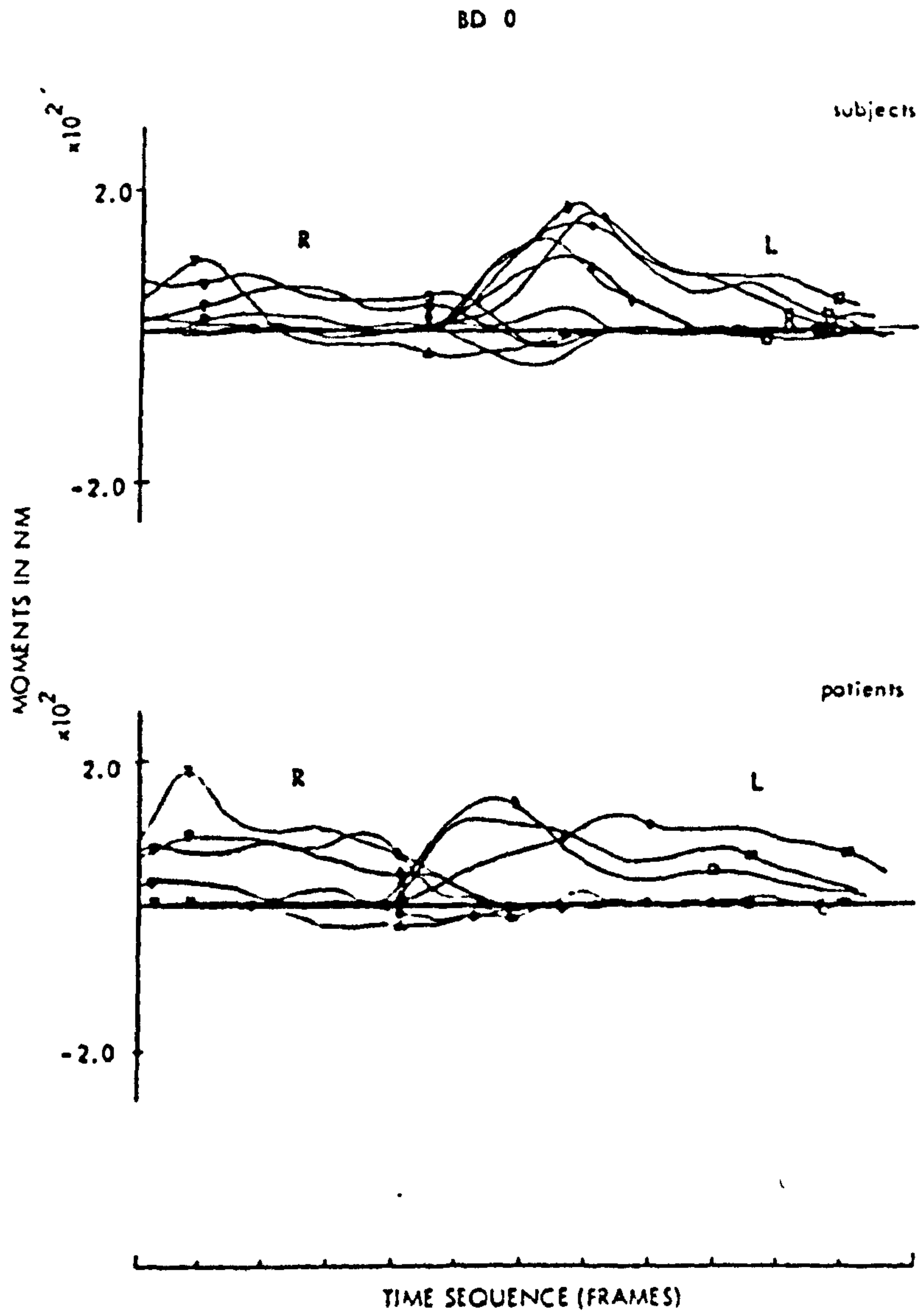


Fig. 5.30 knee moments sagittal plane

- LEFT HEEL STRIKE  $\blacktriangle$
- LEFT TOE OFF  $\blacktriangledown$
- RIGHT HEELSTRIKE  $\square$
- RIGHT TOE OFF  $\diamond$



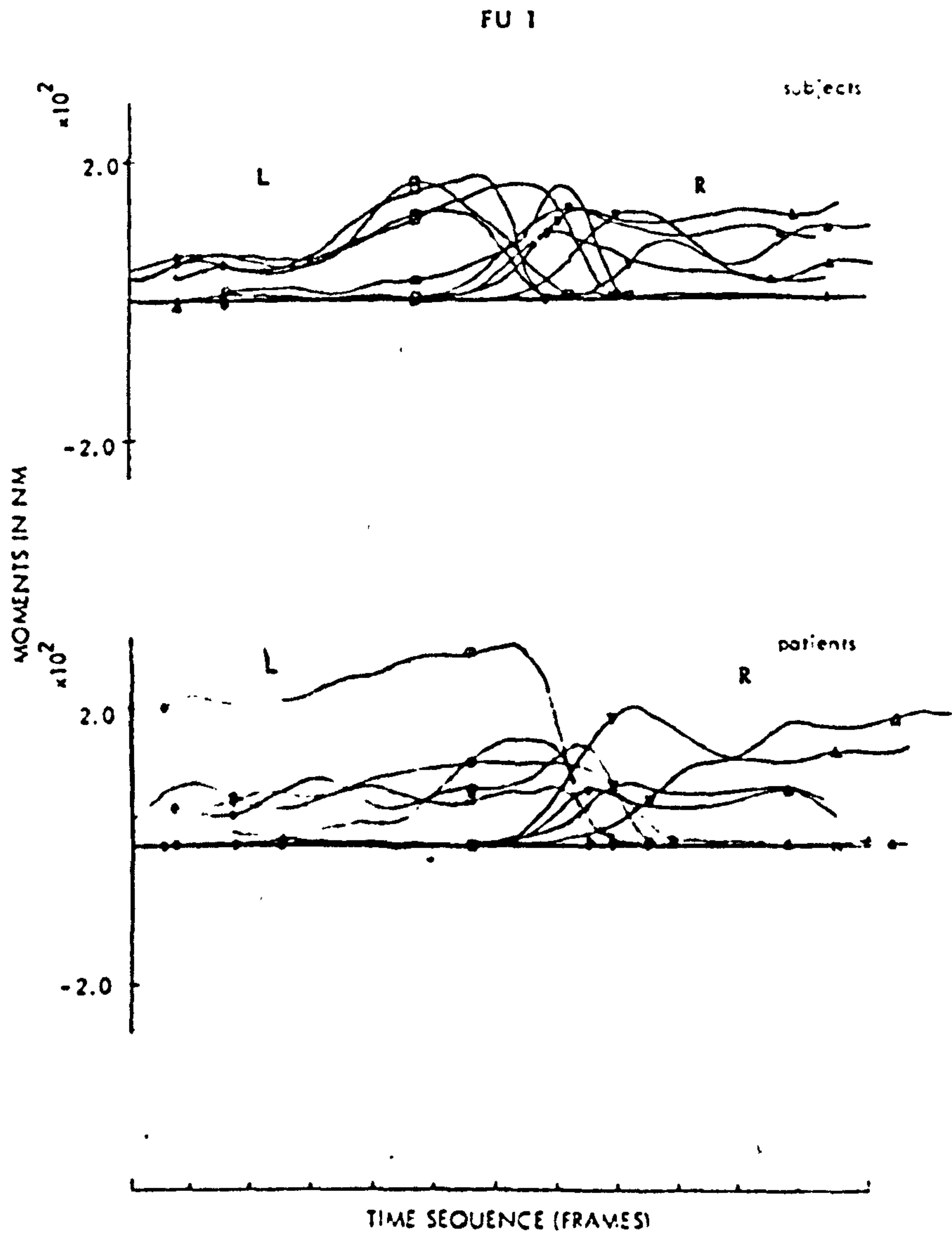


Fig. 5.31 knee moments sagittal plane

LEFT HEEL STRIKE  $\blacktriangle$

LEFT TOE OFF  $\blacktriangledown$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\diamond$

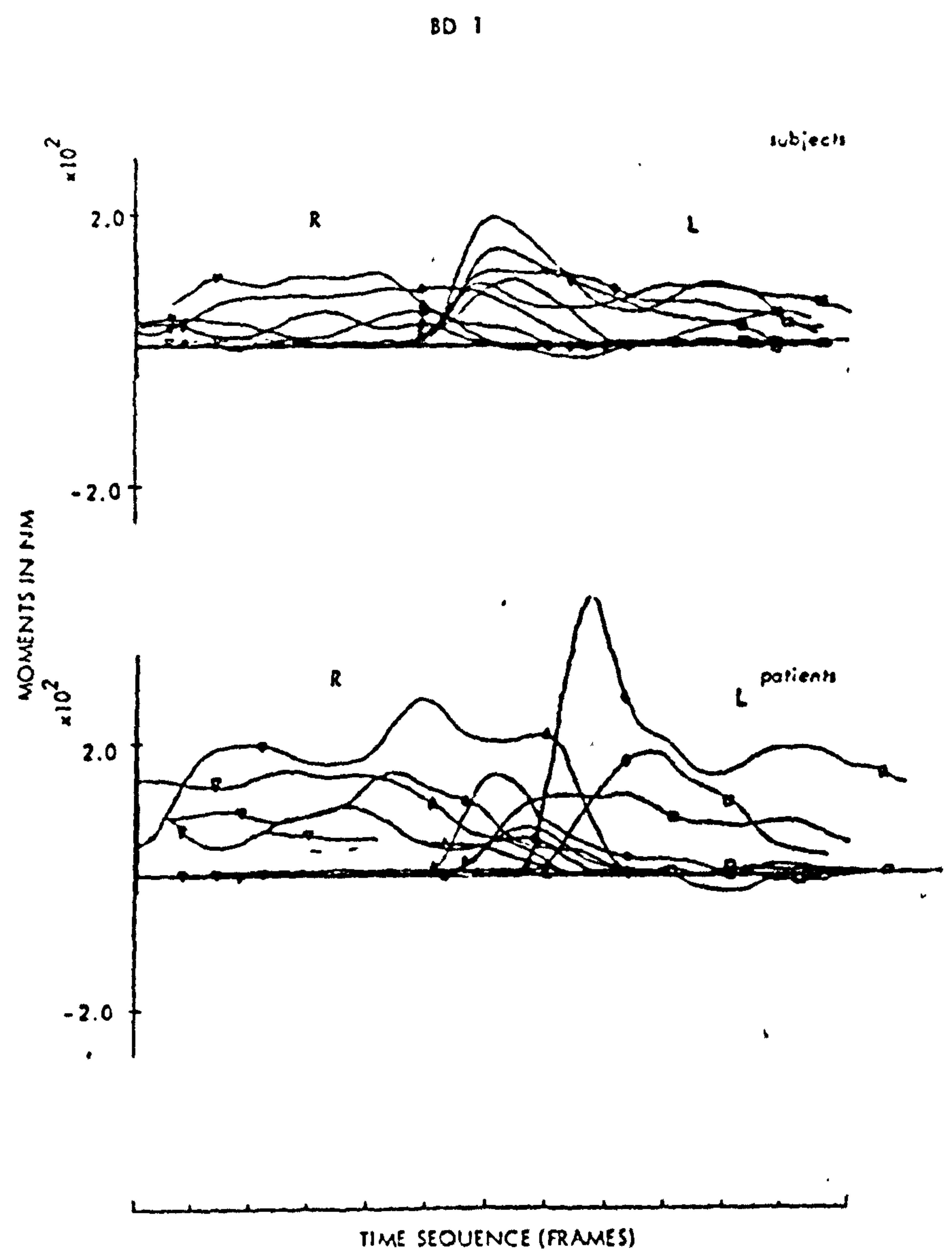


Fig. 5.32 knee moments sagittal plane

- LEFT HEEL STRIKE  $\triangle$
- LEFT TOE OFF  $\nabla$
- RIGHT HEELSTRIKE  $\square$
- RIGHT TOE OFF  $\diamond$

reversal (locking and unlocking of the knee) is only present on the leading leg and at the zero step. The maximum knee extension moment recorded during the test was on the range of 120 to 200 Nm for both zero high and 10% step height. This is much higher than for normal level walking which is of the order of 40 Nm (see Fig. 5.20). It is reckoned that this is due to the fact that in the stepping manoeuvres the knee assumes a hyperextended posture throughout most of the stance phase.

As was pointed out in the case of the ankle, the knee moments are also higher on the left leg than those on the right leg.

Again here, patient P1 has displayed significant differences from the others. At this stage it is not possible to provide an explanation for this.

### 5.3.3- Moments at the hip joint

Fig. 5.33 FL O (left and right) for patients and subjects

Fig. 5.34 BD O " " " " " " "

Fig. 5.35 FU 1 " " " " " " "

Fig. 5.36 BD' 1 " " " " " " "

As in the case of the moments at the knee there were no apparent differences between the results obtained using zero height step and the 10% step height.

From Fig. 5.35 and 5.36 it is noted that the left leg has larger moments than the right during the stance phase. This is due to rigorous extensor activity which is required to stabilize the trunk.

Apart from patient P1 who displayed outstandingly large moments, there was very little difference to be seen between normals and pathologicals.

The graphs are similar to those obtained for normal level walking if it is remembered that they only constitute part of the cycle of level walking. The maximum value has a range of 200 to 250 Nm, which is also (as in the case of the knee) higher than for normal level walking which was about 150 Nm (see Fig. 5.20).

## 5.4 Moments in the Coronal Plane

### 5.4.1 Moments at the ankle joint

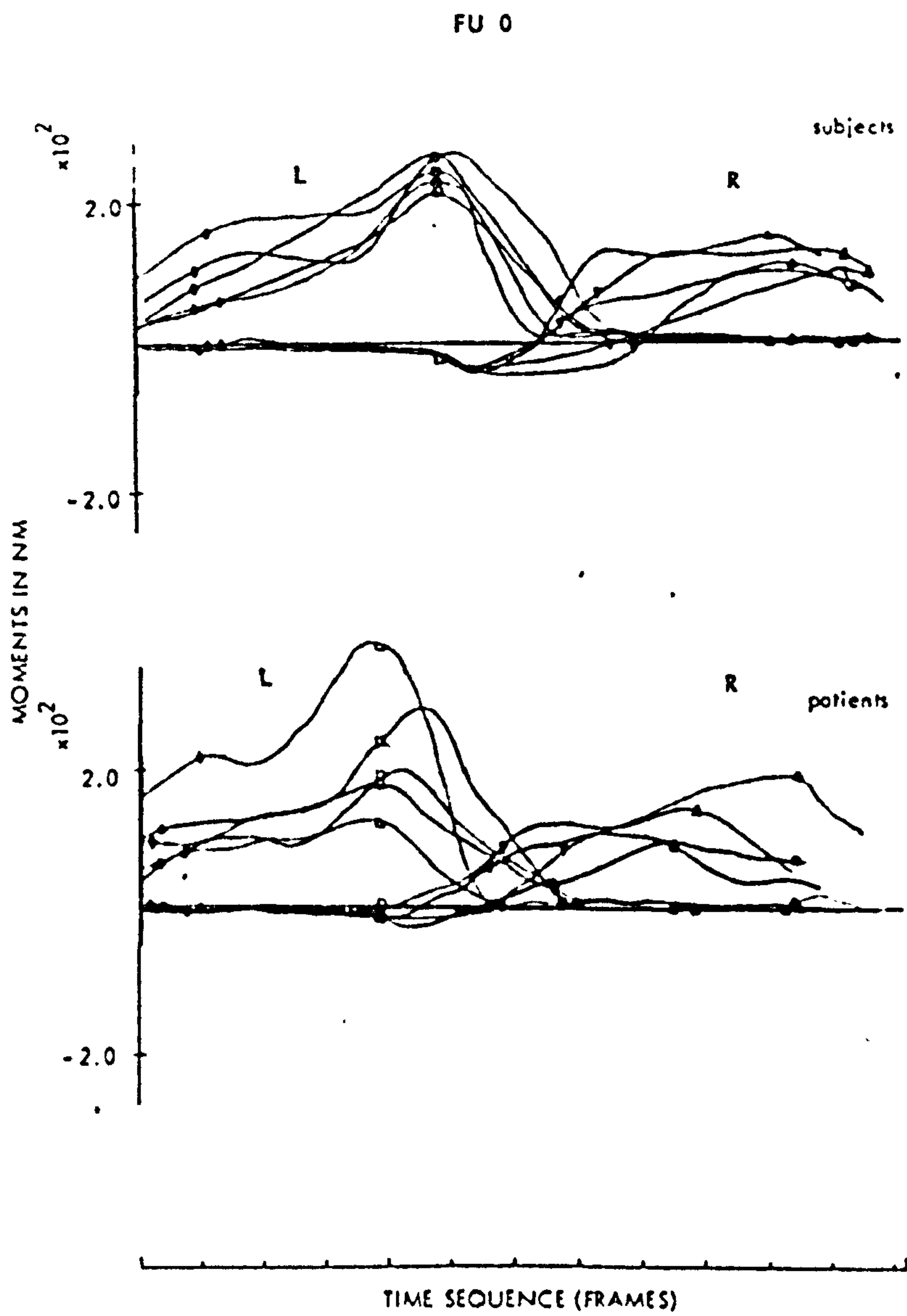


Fig. 5:33 hip moments sagittal plane

LEFT HEEL STRIKE  $\blacktriangle$

LEFT TOE OFF  $\blacktriangledown$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\diamond$

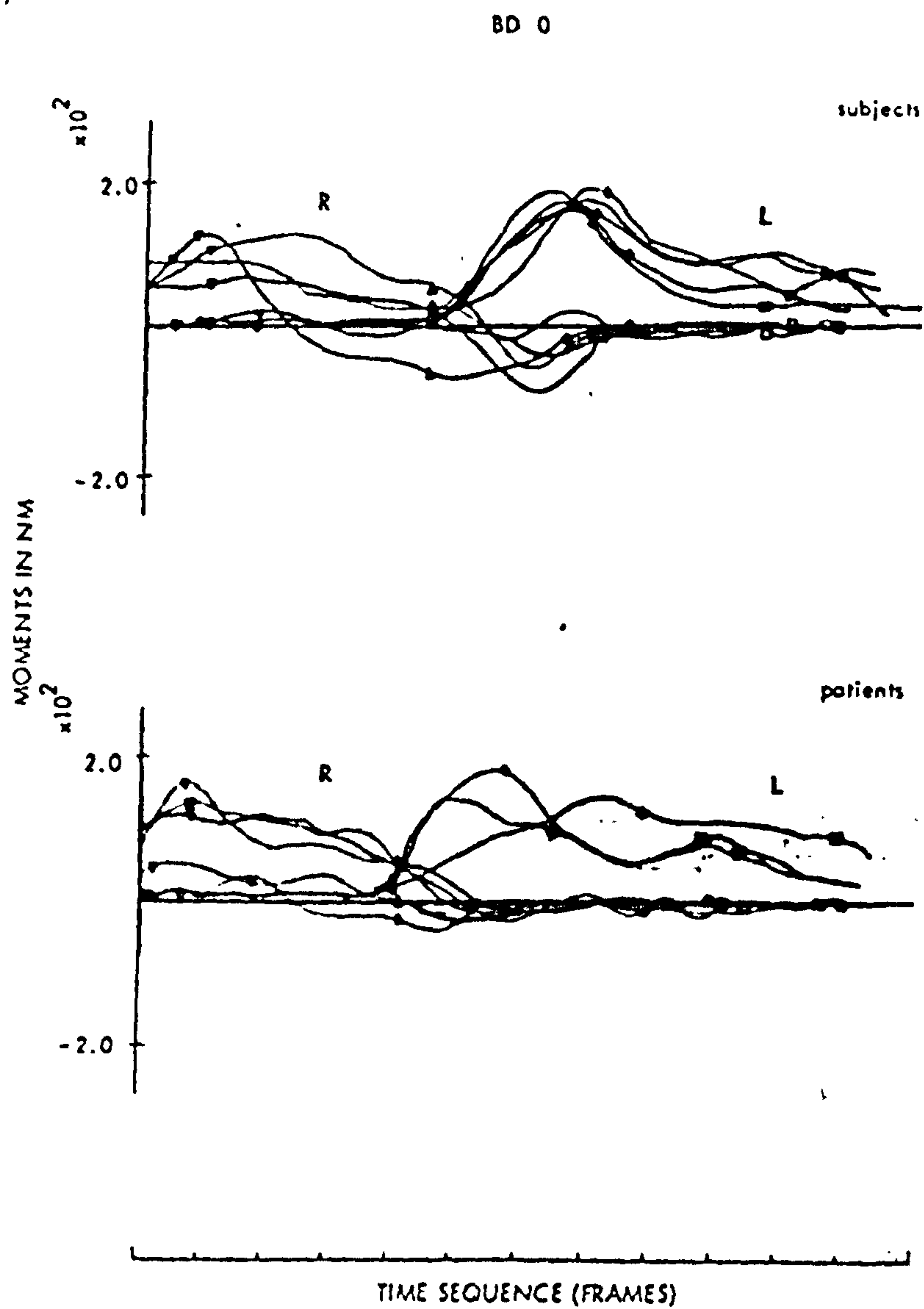


Fig. 5.34 hip moments sagittal plane

LEFT HEEL STRIKE  $\Delta$

LEFT TOE OFF  $\nabla$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\circ$

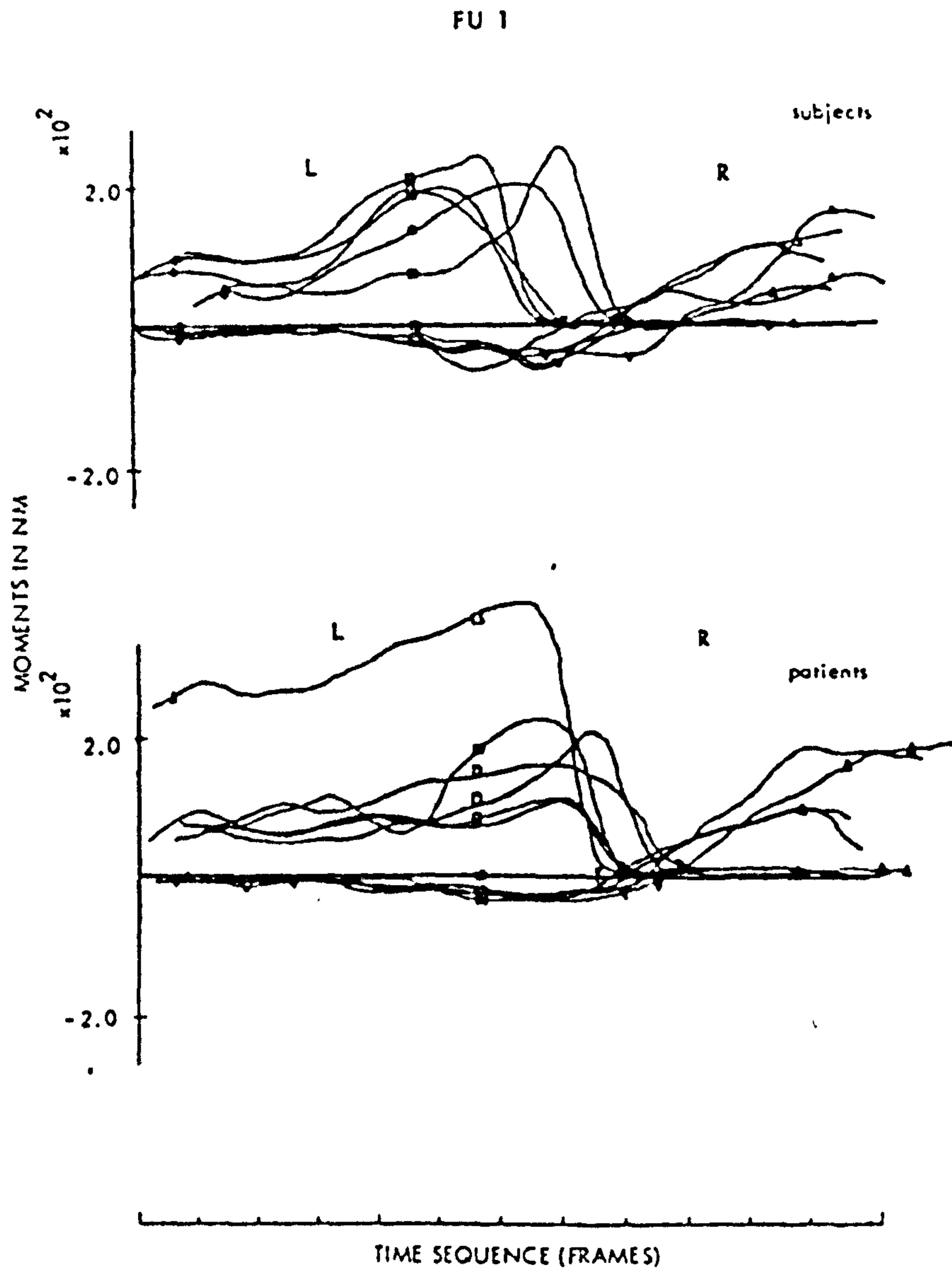


Fig. 5.35 hip moments sagittal plane

LEFT HEEL STRIKE  $\triangle$   
 LEFT TOE OFF  $\nabla$   
 RIGHT HEELSTRIKE  $\square$   
 RIGHT TOE OFF  $\diamond$

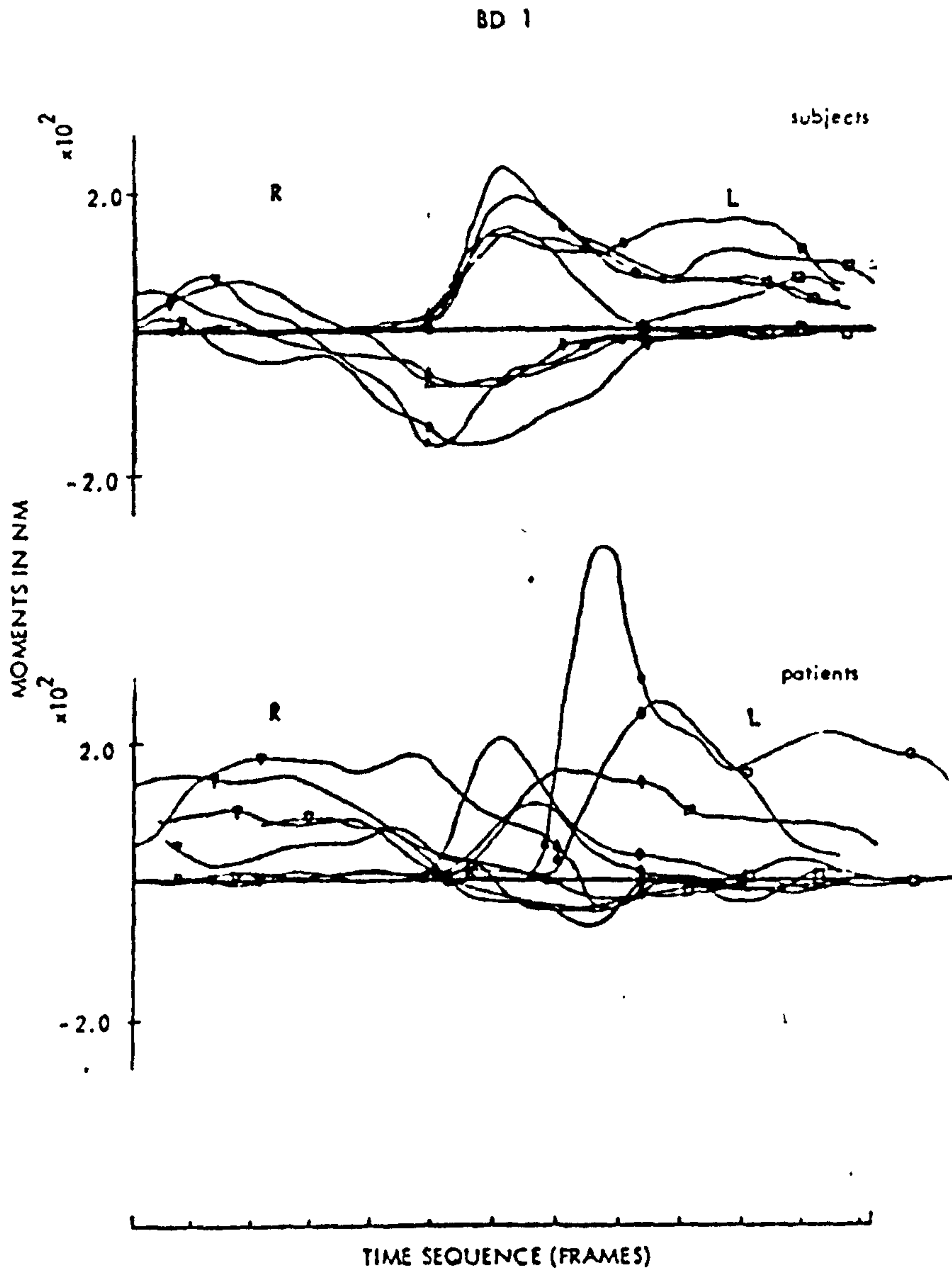


Fig. 5.36 hip moments sagittal plane

LEFT HEEL STRIKE  $\blacktriangle$

LEFT TOE OFF  $\blacktriangledown$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\diamond$

Fig. 5.37 FU O (left and right) for patients and subjects

Fig. 5.38 BD O " " " " " " "

Fig. 5.39 FU 1 " " " " " " "

Fig. 5.40 BD 1 " " " " " " "

All the graphs are very similar, and have the shape that one would expect. Fig. 5.39 the normals for instance have shown that the left ankle the moments are negative during the stance phase, which means that the external force actions tend to invert the ankle. The right leg has positive moments which indicate that the right ankle is also tended to be inverted.

All graphs display a double peak characteristic similarly displayed by the  $F_y$  ground reaction force, which is also to be expected. The  $F_y$  ground force is the force mainly responsible for the production of this moment.

Loading on the left leg is higher than on the right leg, this was noted also on the sagittal moments.

In comparing normals and pathologicals the graphs are very similar, except perhaps that the patients showed lower values. The shape of the curves are similar to those obtained to normal level walking but the maximum value is much higher (120 vs 20 Nm). It is thought that the reason for this is the very wide walking base adopted in stepping.

#### 5.4.2 Moments at the knee joint

Fig. 5.41 FU O (left and right) for patients and subjects

Fig. 5.42 BD O " " " " " " "

Fig. 5.43 FU 1 " " " " " " "

Fig. 5.44 BD 1 " " " " " " "

The graphs for the knee are similar in shape to those of the ankle; which is to be expected. There is more scatter in the results for the knee than the ankle.

#### 5.4.3 Moments at the hip joint

Fig. 4.45 FU O (left and right) for patients and subjects

Fig. 5.46 BD O " " " " " " "

Fig. 5.47 FU 1 " " " " " " "

Fig. 5.48 BD 1 " " " " " " "



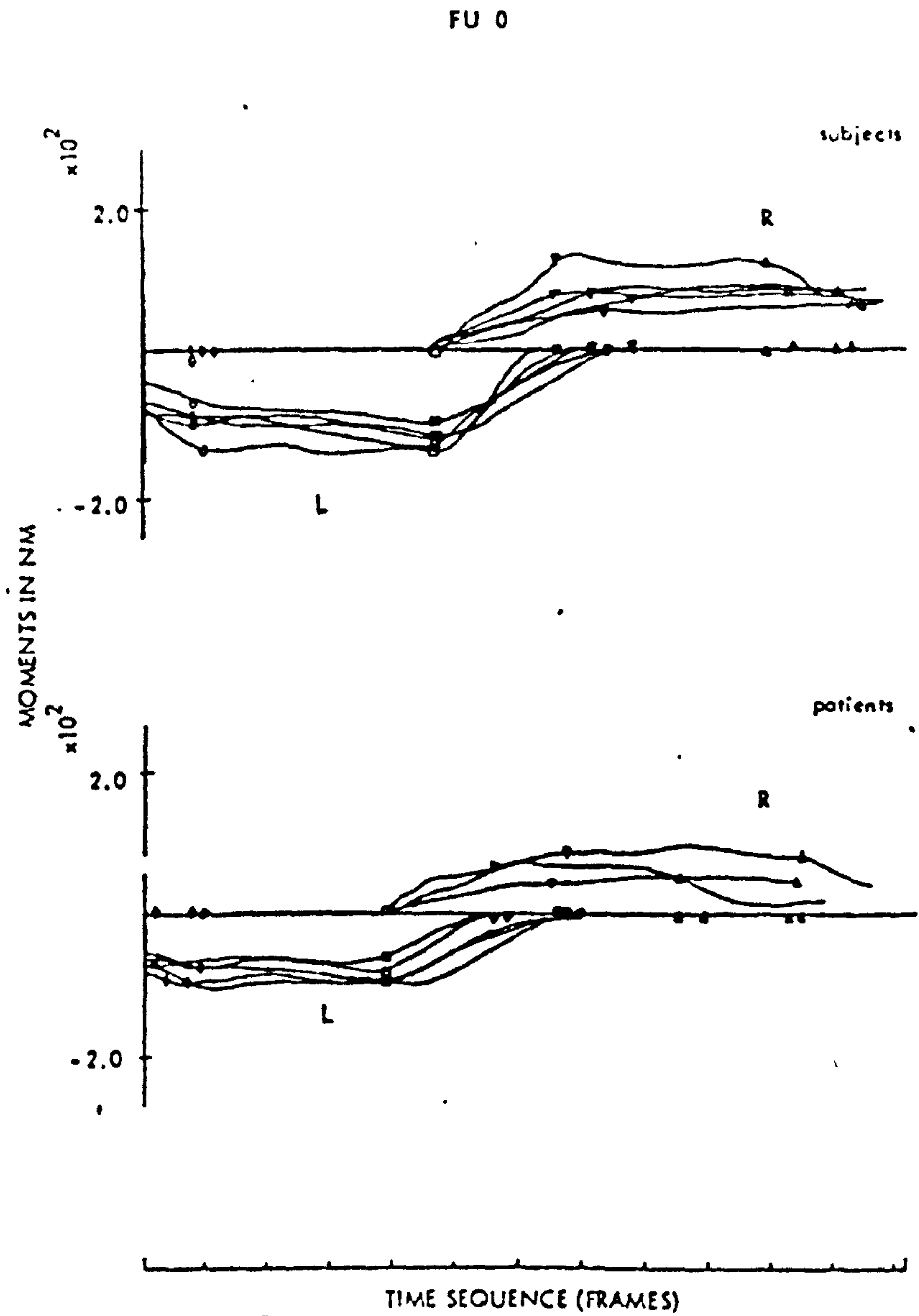


Fig. 5.37 ankle moments coronal plane

LEFT HEEL STRIKE  $\blacktriangle$

LEFT TOE OFF  $\blacktriangledown$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\diamond$

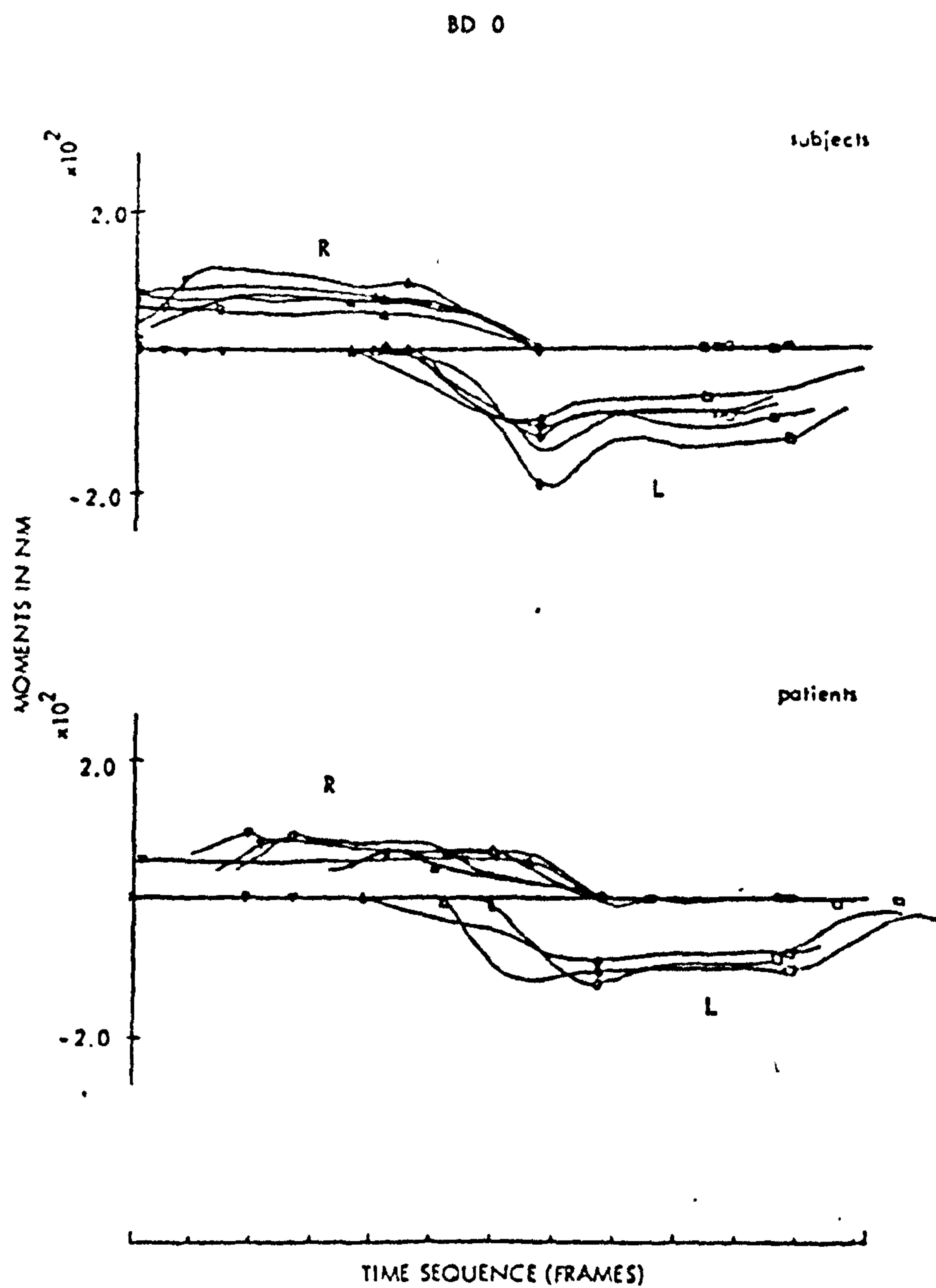


Fig. 5.38 ankle moments coronal plane

LEFT HEEL STRIKE  $\Delta$

LEFT TOE OFF  $\nabla$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\circ$

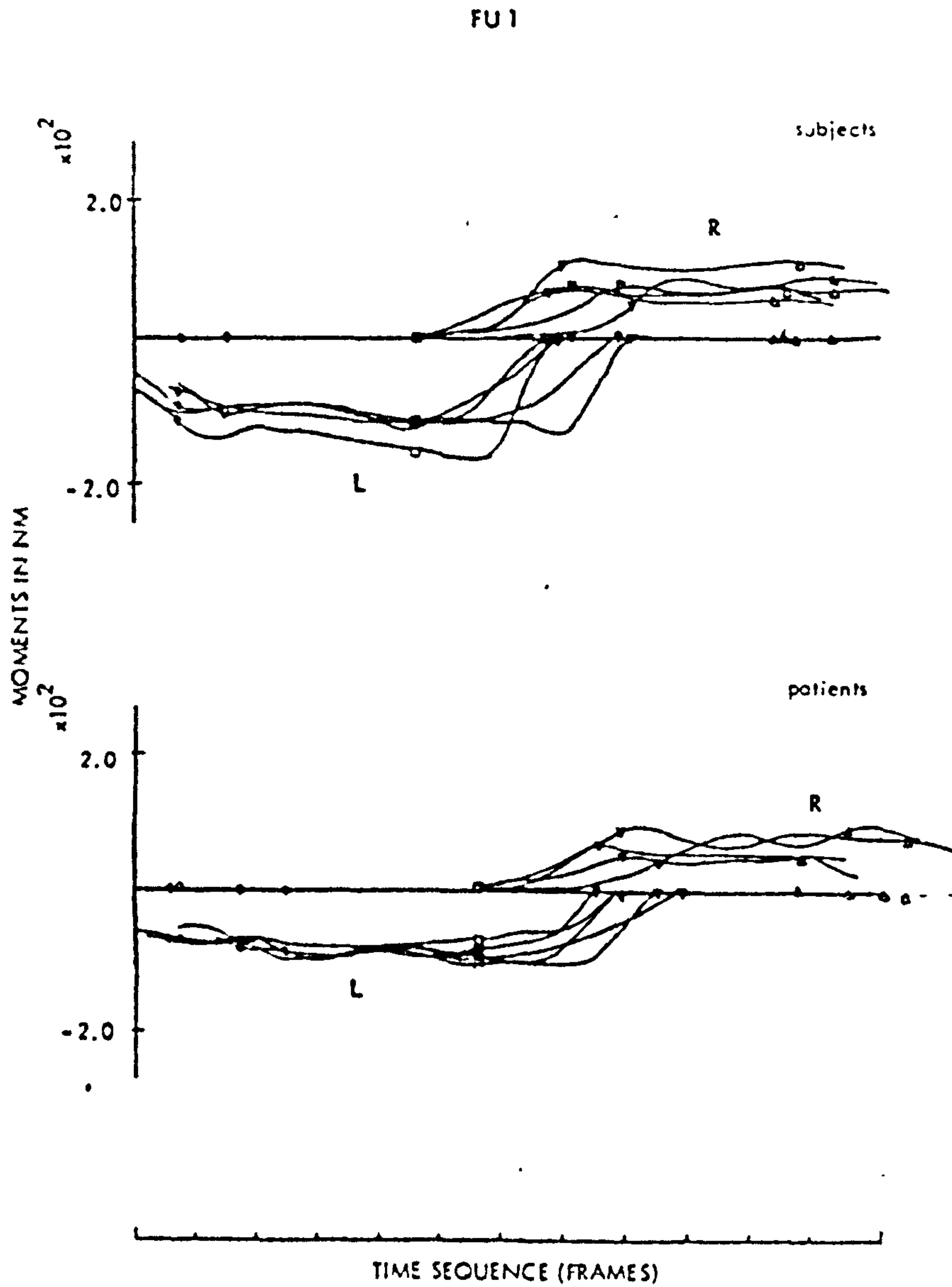


Fig. 5.39 ankle moments coronal plane

- |                  |   |
|------------------|---|
| LEFT HEEL STRIKE | △ |
| LEFT TOE OFF     | ▽ |
| RIGHT HEELSTRIKE | □ |
| RIGHT TOE OFF    | ◇ |

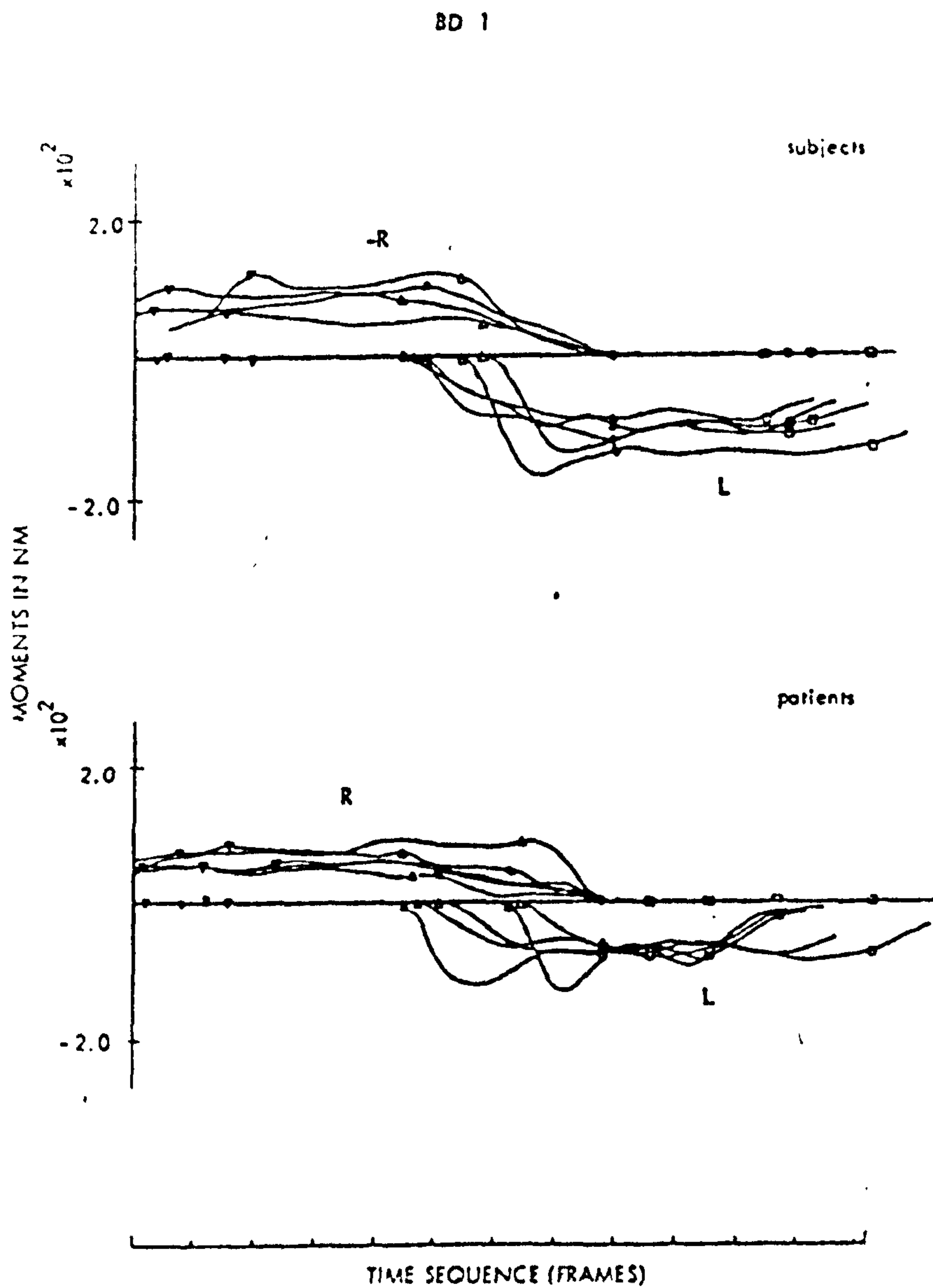


Fig. 5.40 ankle moments coronal plane

- LEFT HEEL STRIKE  $\Delta$
- LEFT TOE OFF  $\nabla$
- RIGHT HEELSTRIKE  $\square$
- RIGHT TOE OFF  $\circ$

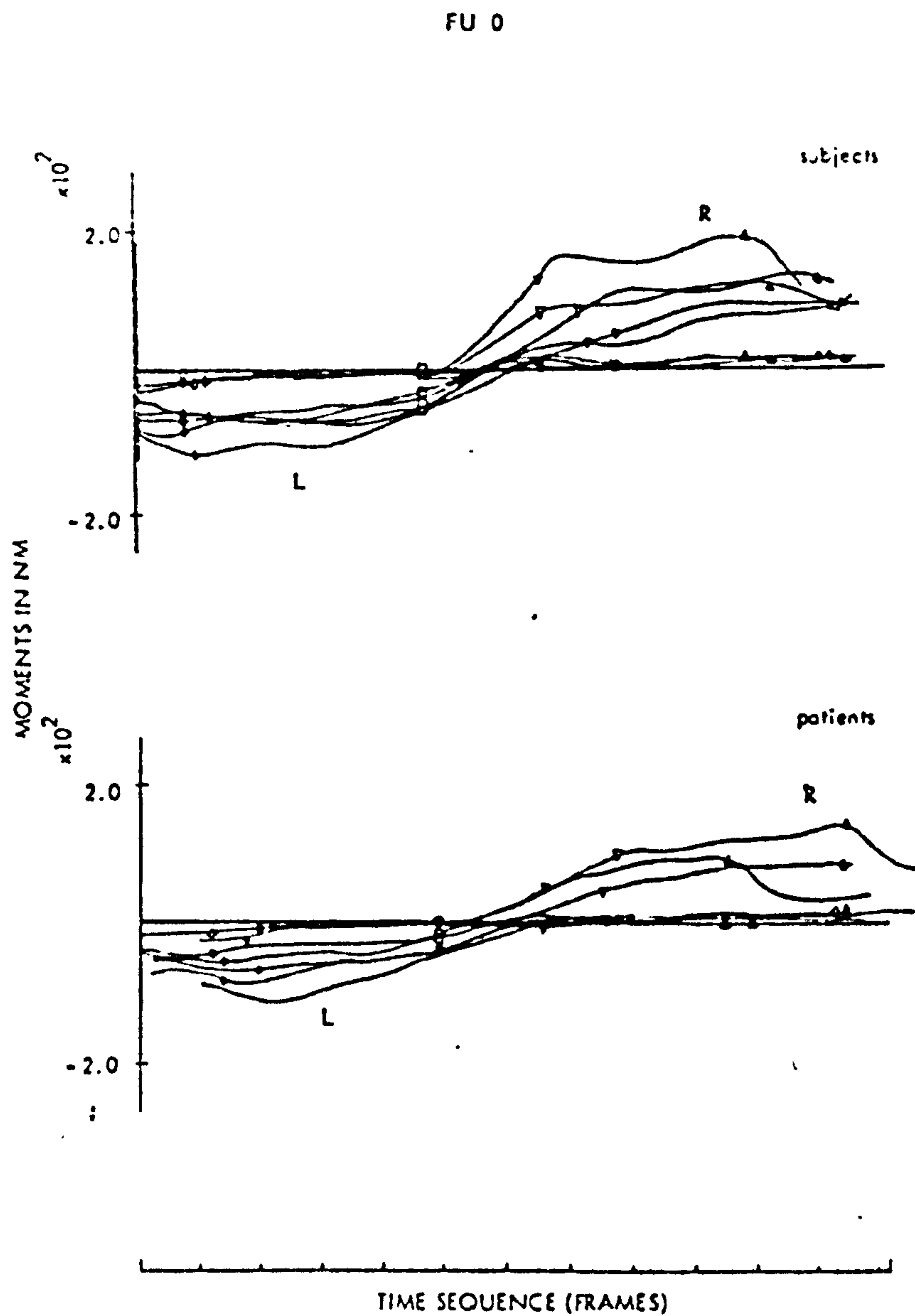


Fig. 5.41 knee moments coronal plane

LEFT HEEL STRIKE  $\Delta$

LEFT TOE OFF  $\nabla$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\diamond$

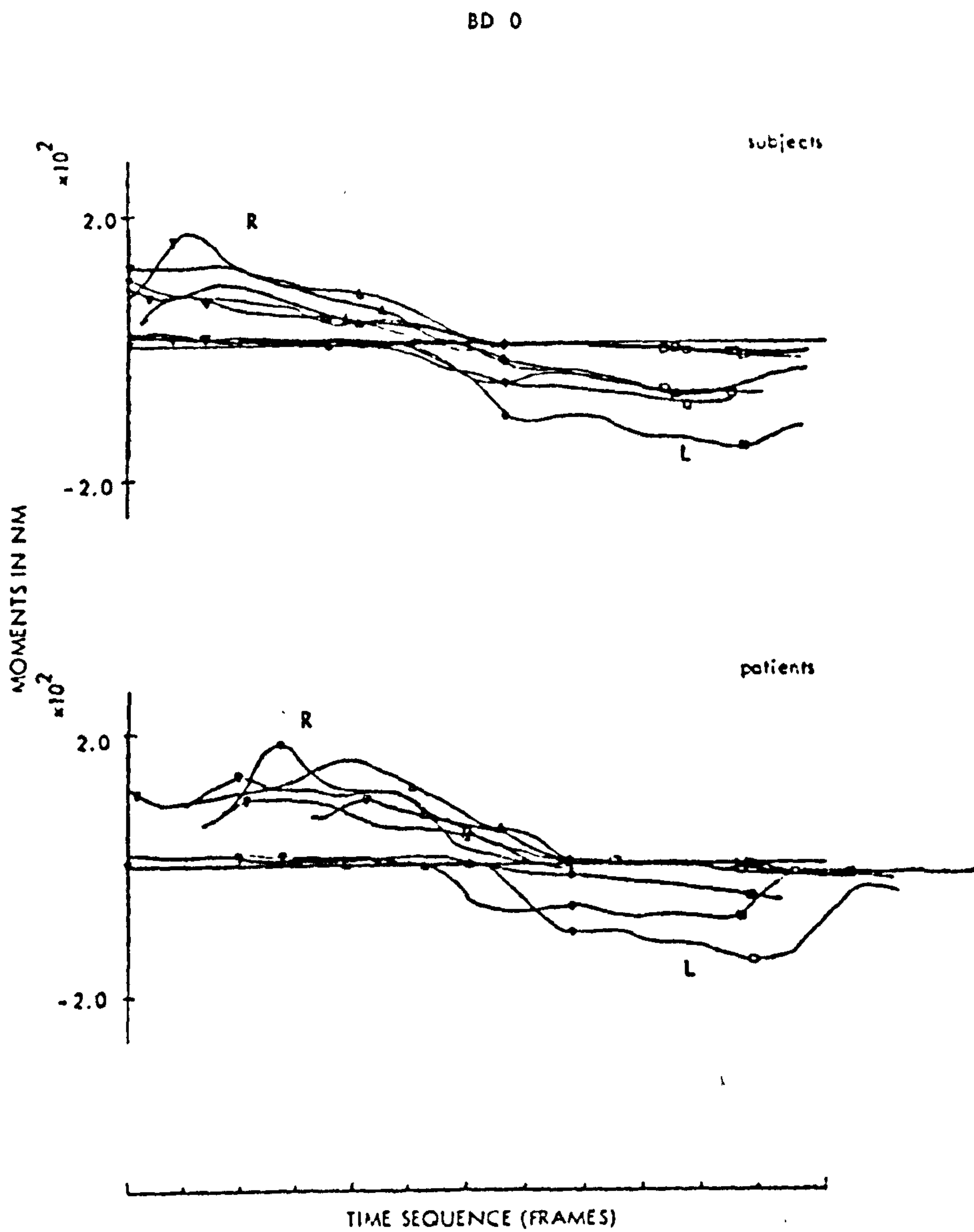


Fig. 5.42 knee moments coronal plane

- LEFT HEEL STRIKE  $\wedge$
- LEFT TOE OFF  $\nabla$
- RIGHT HEELSTRIKE  $\square$
- RIGHT TOE OFF  $\diamond$

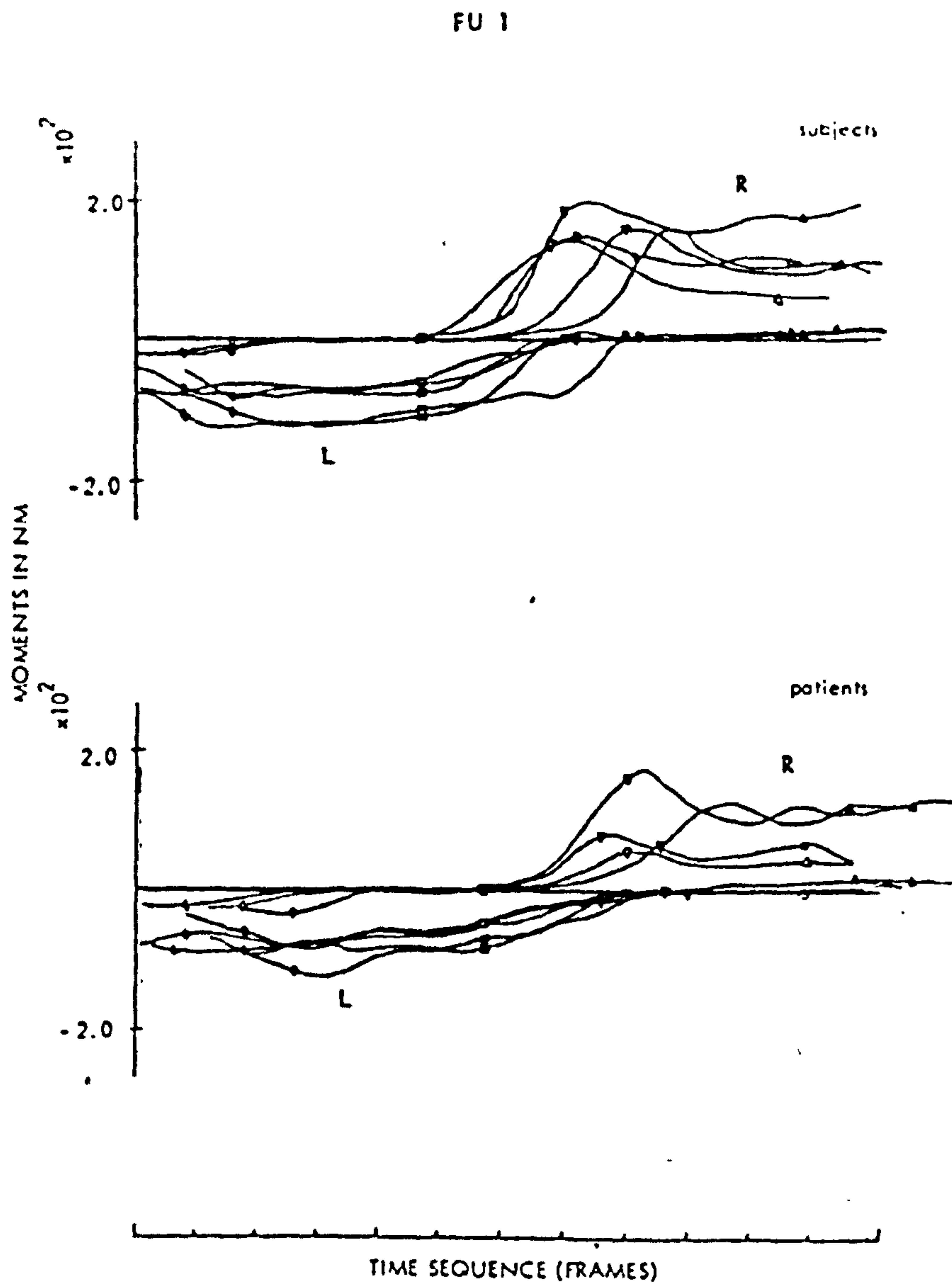


Fig. 5.43 knee moments coronal plane

LEFT HEEL STRIKE	△
LEFT TOE OFF	▽
RIGHT HEELSTRIKE	□
RIGHT TOE OFF	◇

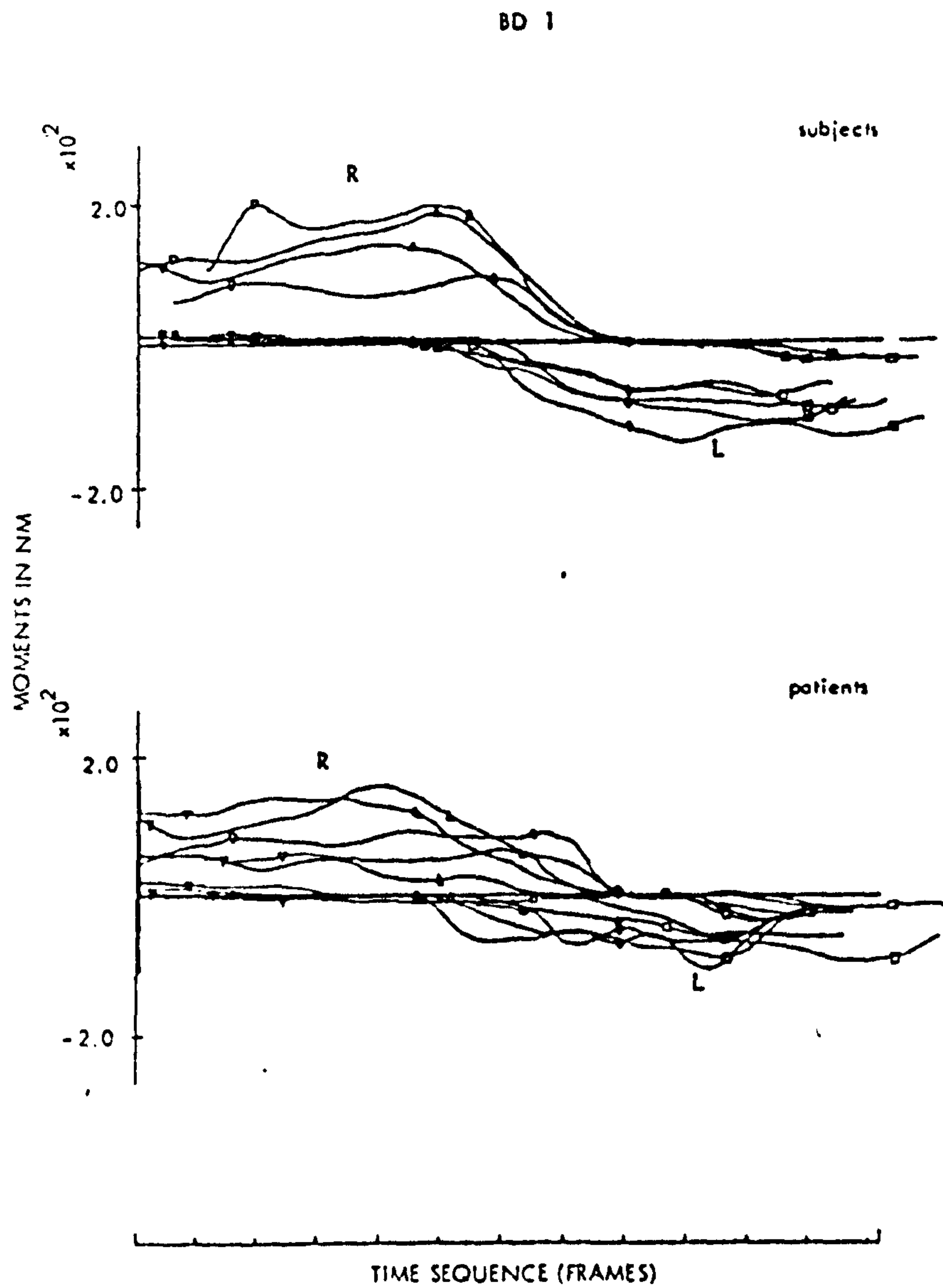


Fig. . 5.44 knee moments coronal plane

LEFT HEEL STRIKE  $\blacktriangle$

LEFT TOE OFF  $\blacktriangledown$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\diamond$



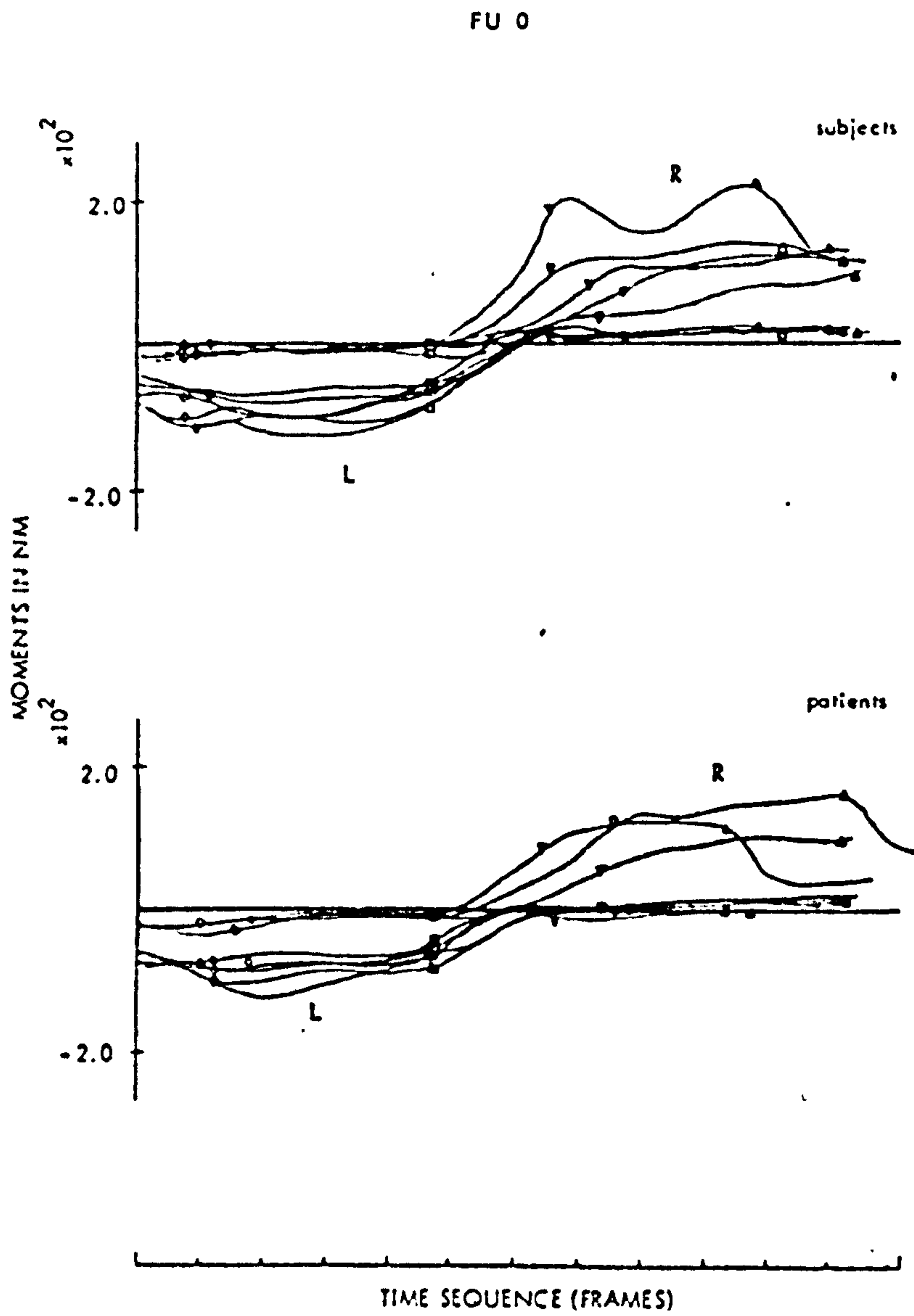


Fig. 5.45 hip moments coronal plane

LEFT HEEL STRIKE  $\blacktriangle$   
 LEFT TOE OFF  $\blacktriangledown$   
 RIGHT HEELSTRIKE  $\square$   
 RIGHT TOE OFF  $\diamond$

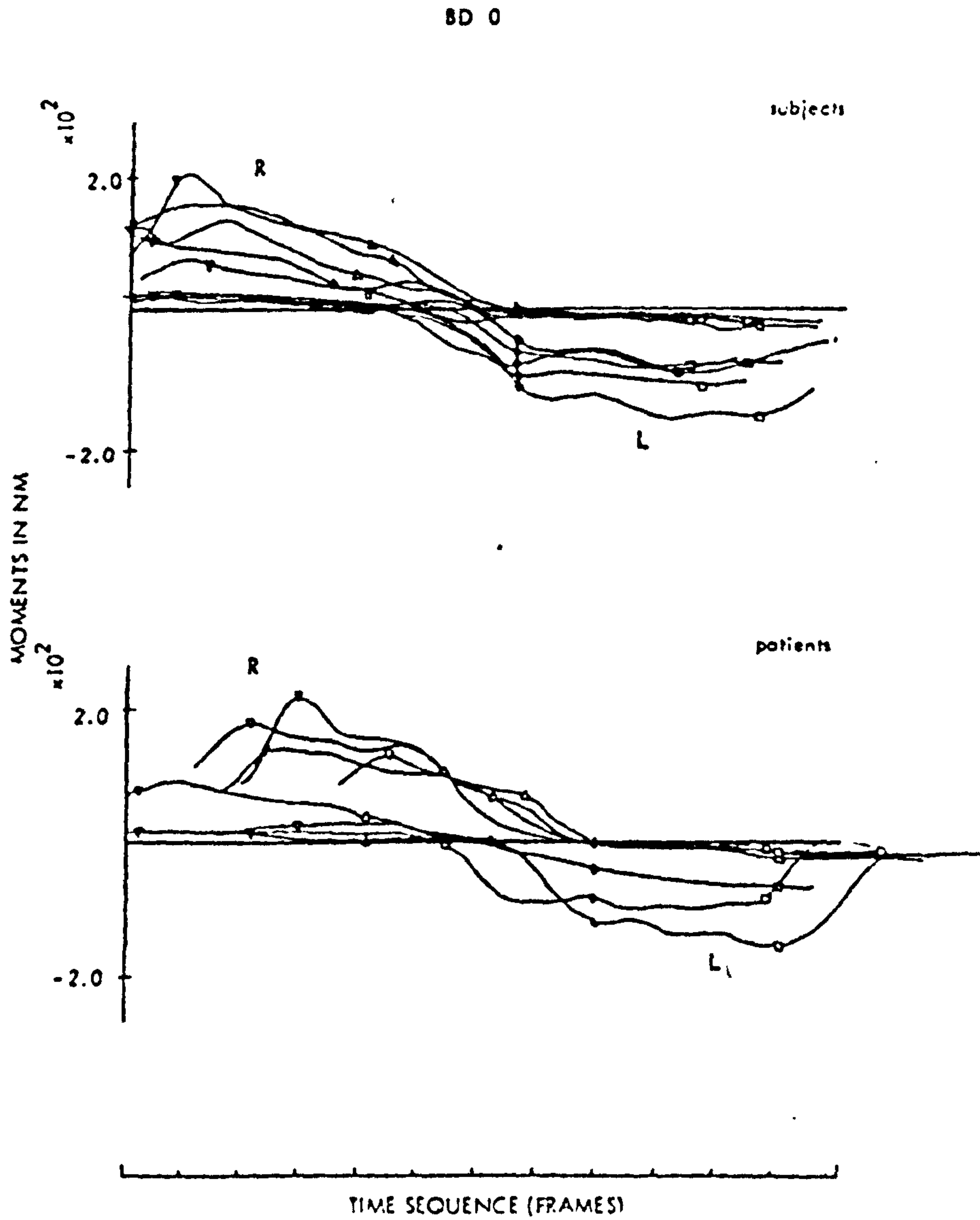


Fig. 5.46 hip moments coronal plane

- LEFT HEEL STRIKE  $\Delta$
- LEFT TOE OFF  $\nabla$
- RIGHT HEELSTRIKE  $\square$
- RIGHT TOE OFF  $\diamond$

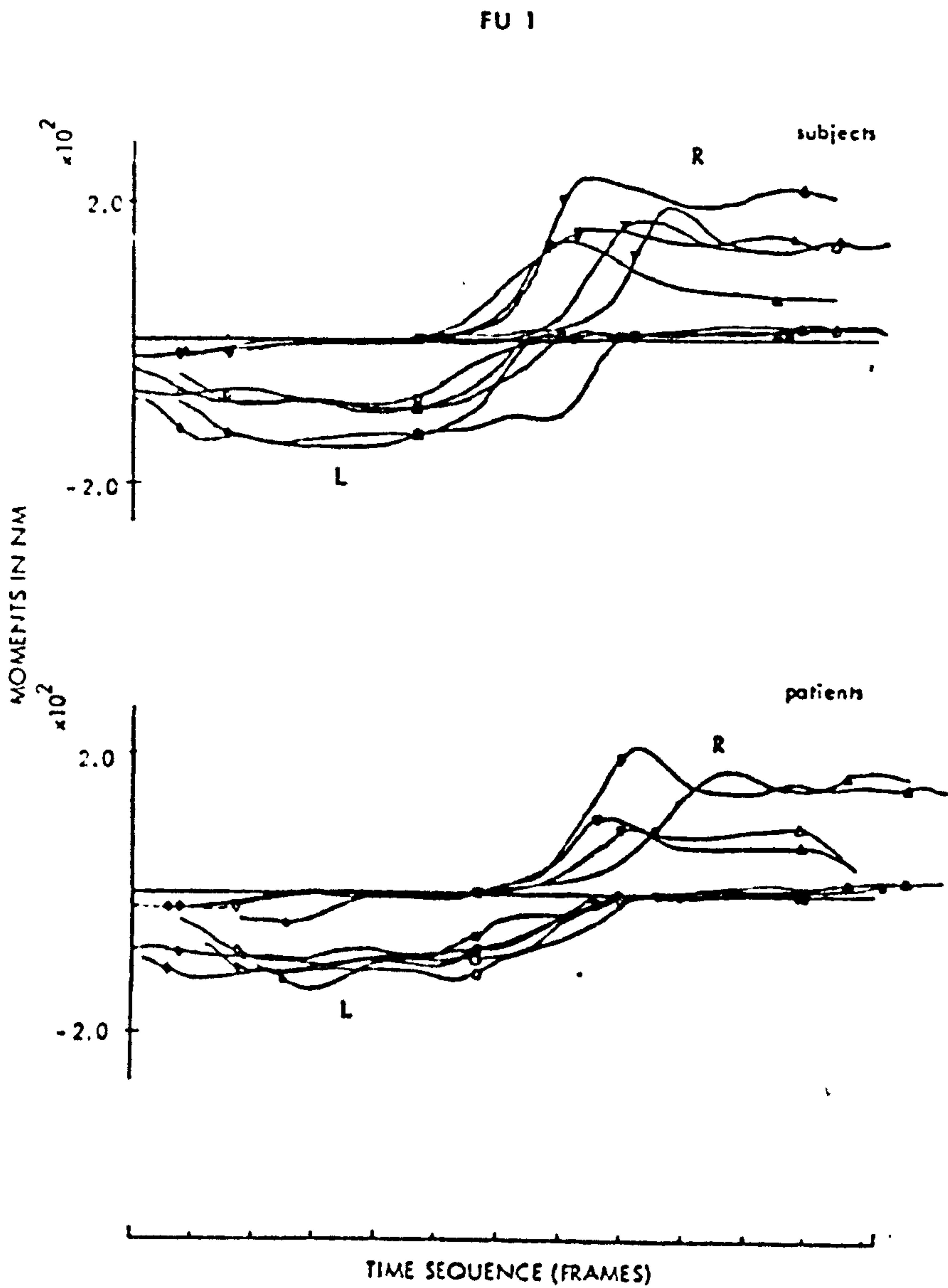


Fig. 5.47 hip moments coronal plane

- |                  |   |
|------------------|---|
| LEFT HEEL STRIKE | ▲ |
| LEFT TOE OFF     | ▼ |
| RIGHT HEELSTRIKE | □ |
| RIGHT TOE OFF    | ◇ |

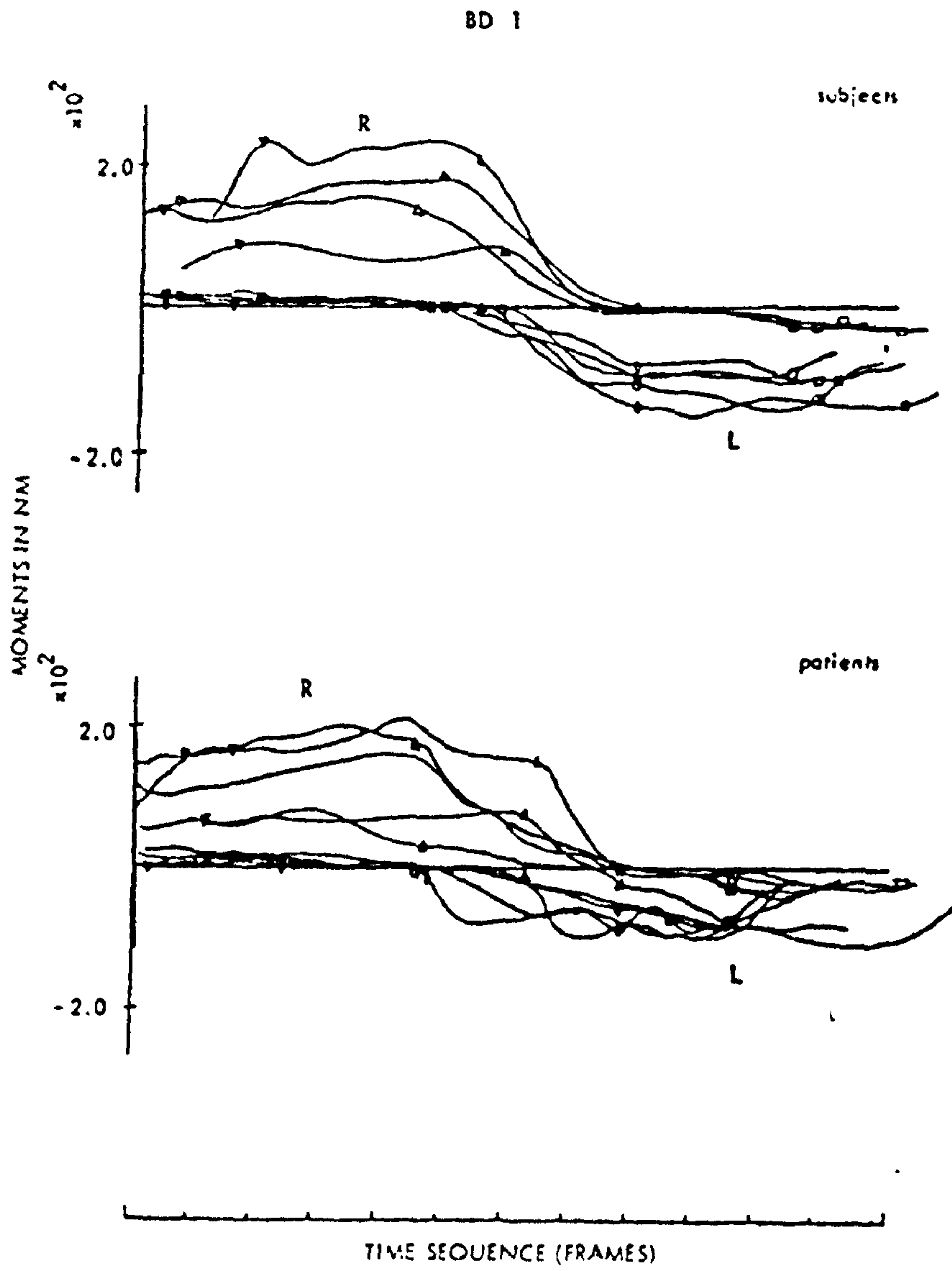


Fig. 5.48 hip moments coronal plane

LEFT HEEL STRIKE  $\blacktriangle$

LEFT TOE OFF  $\blacktriangledown$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\diamond$

Generally, it has been found that for the right leg the hip moment tended to be higher than the knee moment and the knee moment higher than the ankle moment. (see Fig. 5.13). For the left leg there was a tendency for the hip moments to have a higher value than the knee and the ankle moments. However, for the left leg, the knee moments were sometimes above sometimes below the values for the ankle moments.

Fig. 5.45 to 5.48 have the same characteristic shape as those for the ankle and knee, i.e. displaying the same double peak characteristic. Generally, however, the scatter of the curves at the hip level it is much more pronounced than those of the knee and ankle.

The range of hip moments calculated was 200 to 250 Nm whereas for normal level walking values of up to 150 Nm have been recorded (see Fig. 5.22).

### 5.5 Moments in the Transverse Plane

Only sample results for subject S and patient P1 (Fig. 5.17 to 5.20) are shown for the transverse plane moments. Other investigators (University of California 1947) have shown that the torque along the long axis of the limb displayed considerable scatter even for normals. The same effect was observed in the present study. It was therefore decided that it was little to be gained in collecting all the results for normal subjects and patients for this parameter. The maximum torque observed was of the order of 15 Nm for both patients and subjects.

### 5.6 The Angle-Angle Diagrams (Figures 5.49 to 5.56)

It was decided to present the kinematic results of this study in the form of angle-angle diagrams (Fig. 5.23 and 5.24). This decision was taken for two reasons: firstly, these diagrams incorporate a method of normalisation of the data since they eliminate the time variable. Variation in the time taken to perform a certain manoeuvre distorts the shape of the curves and make comparisons between tests difficult. Secondly, it is obvious that the most important features of the kinematics of stepping are the angles between the various limb segments.

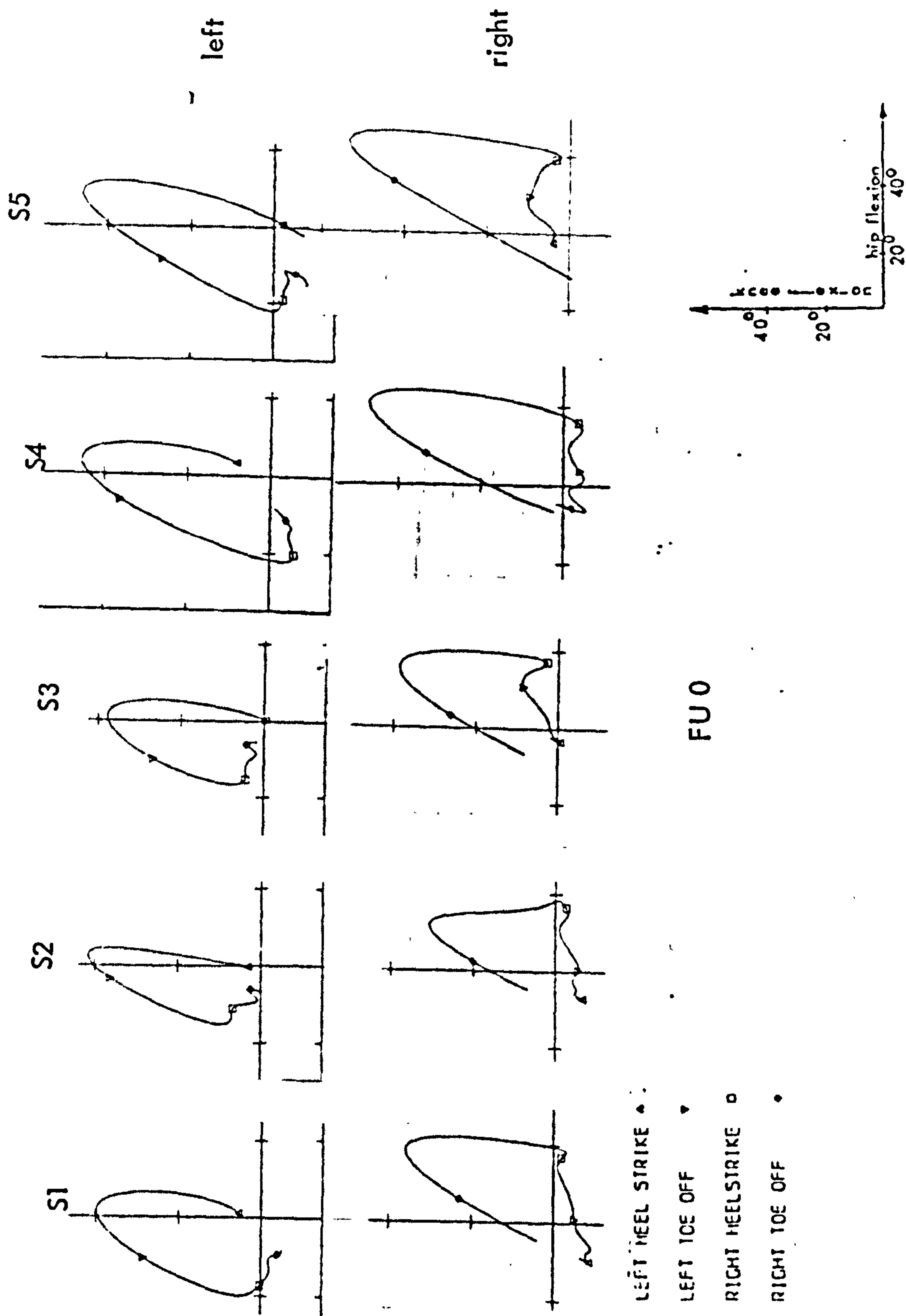


Fig 5.49

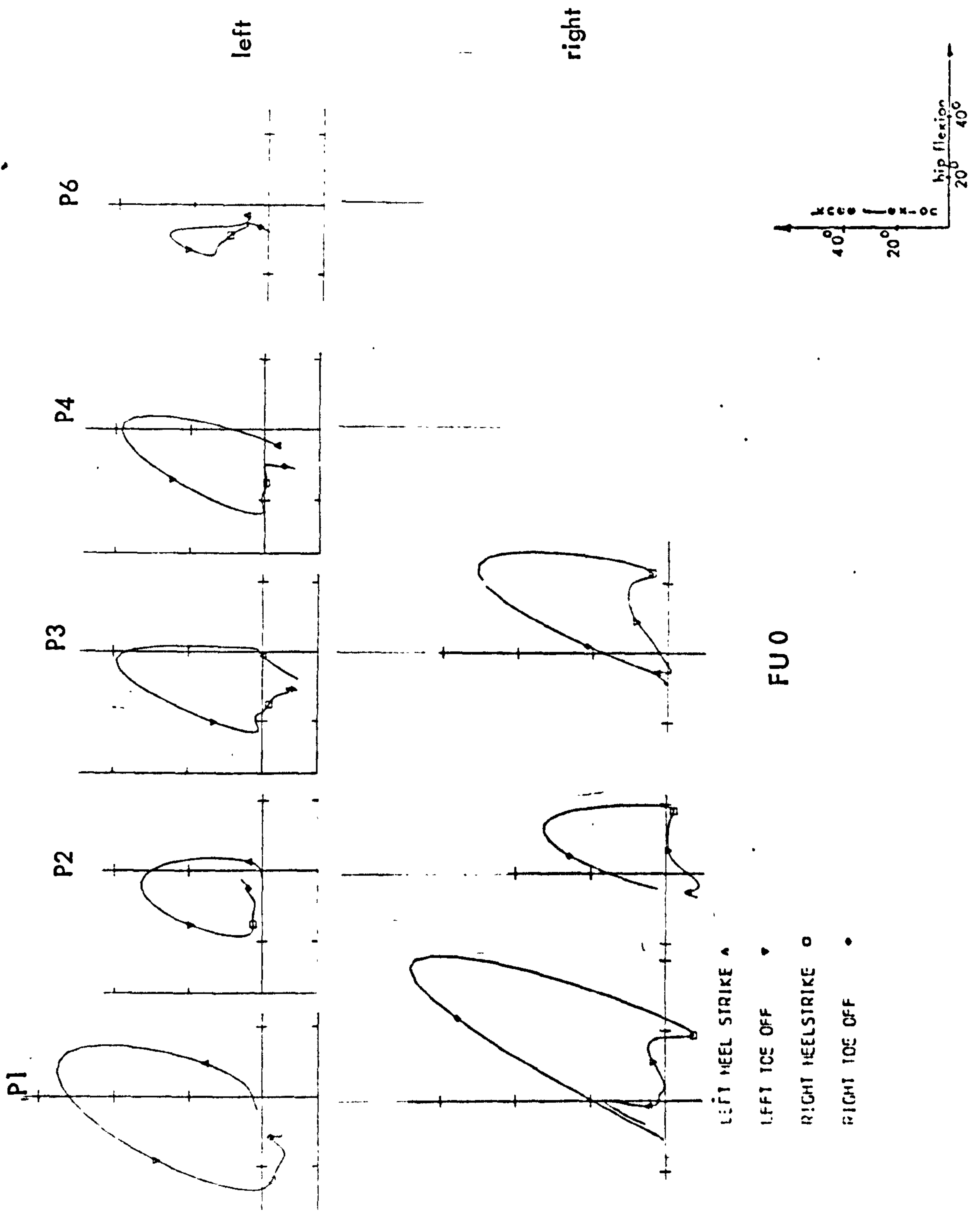


Fig 5.50

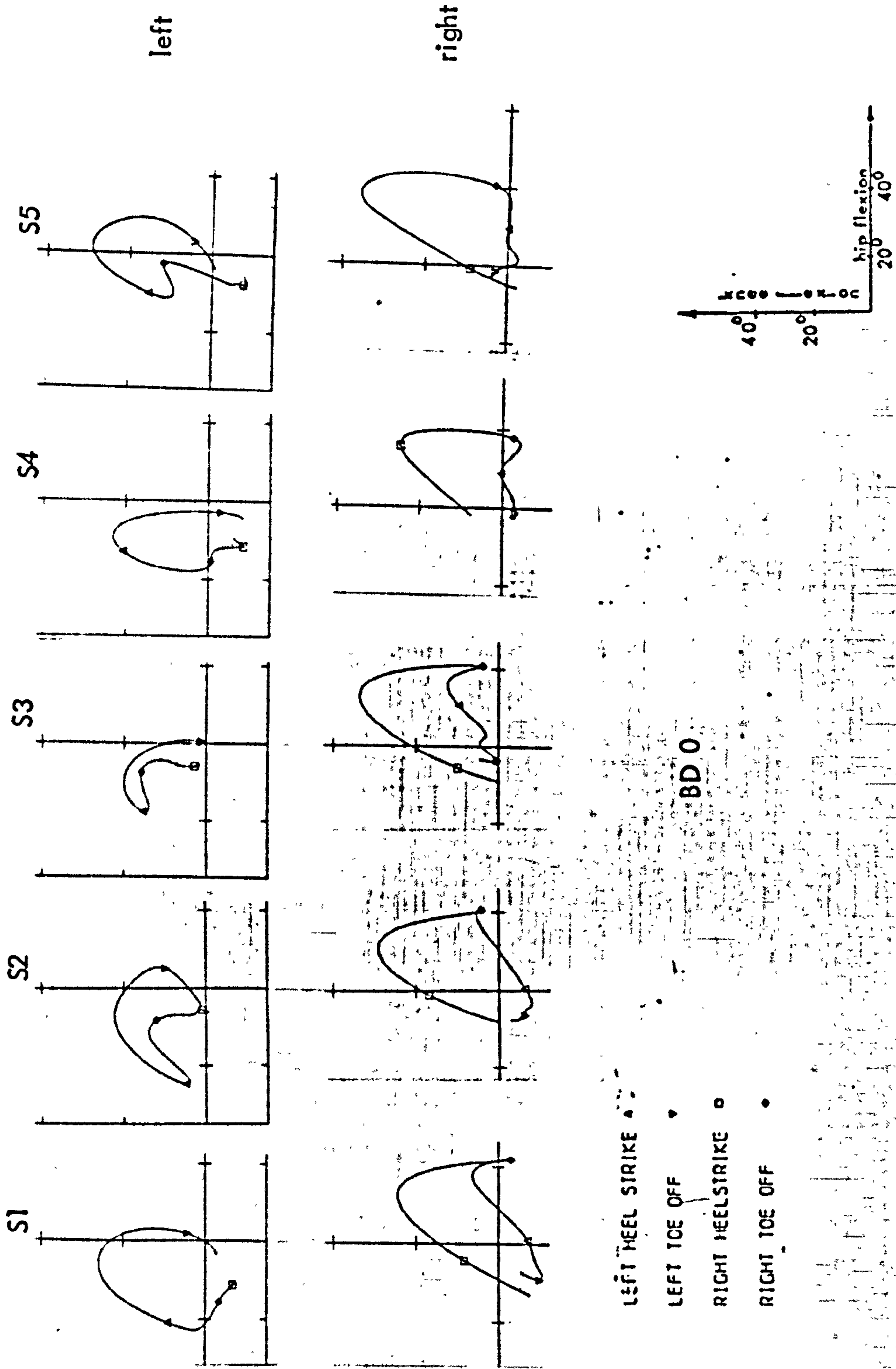


Fig 5.51



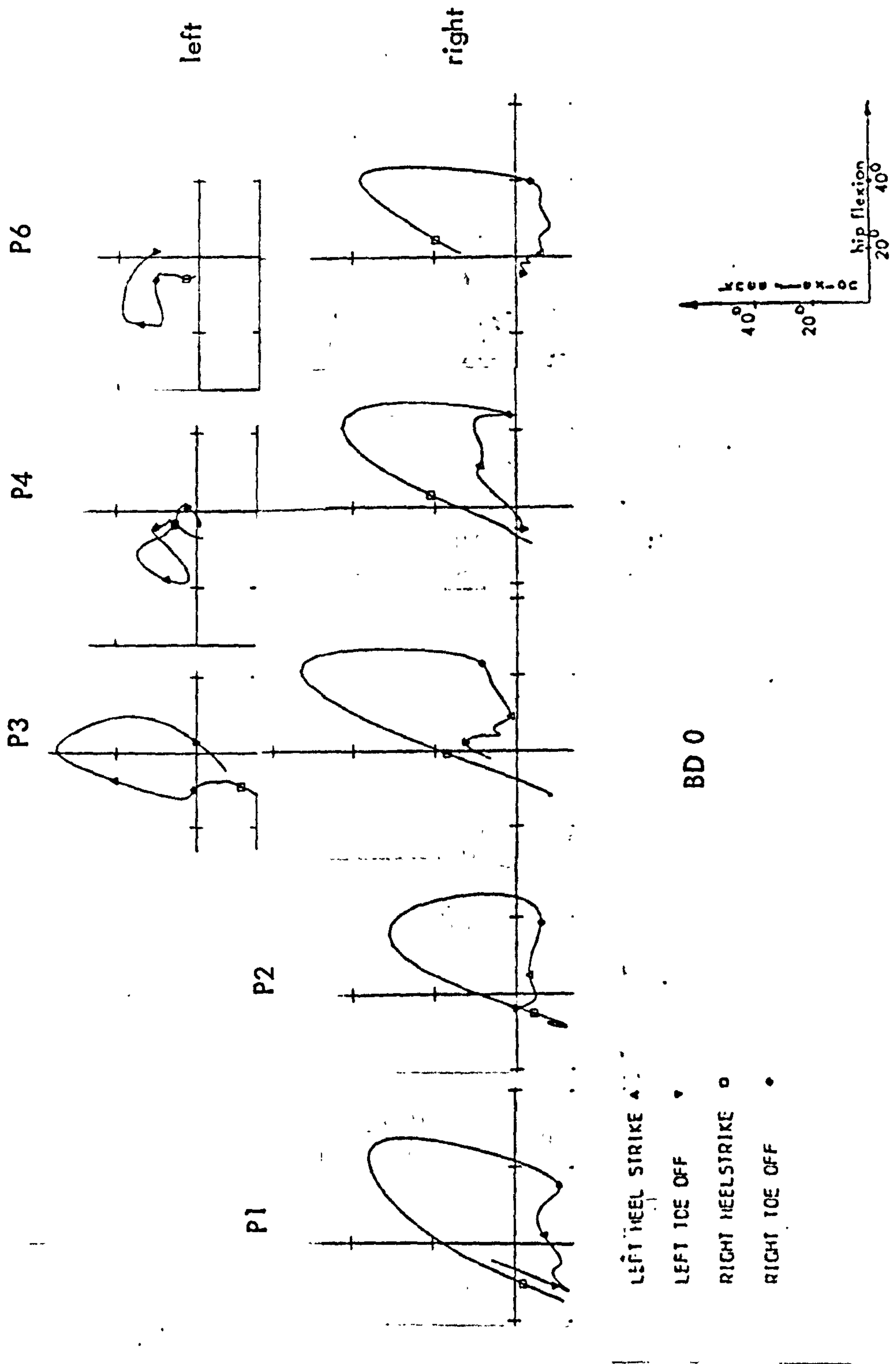


Fig 5.52

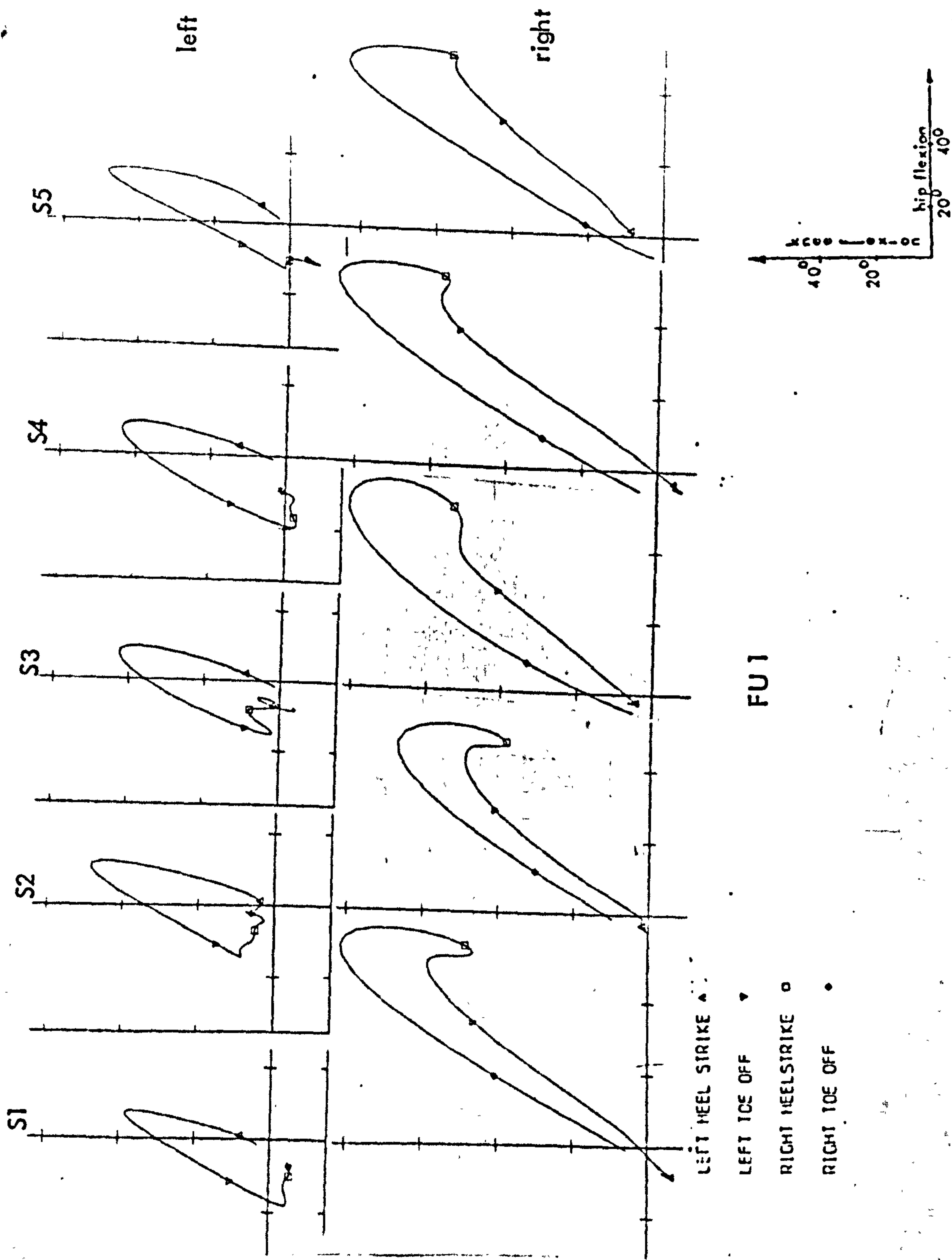


Fig 5.53

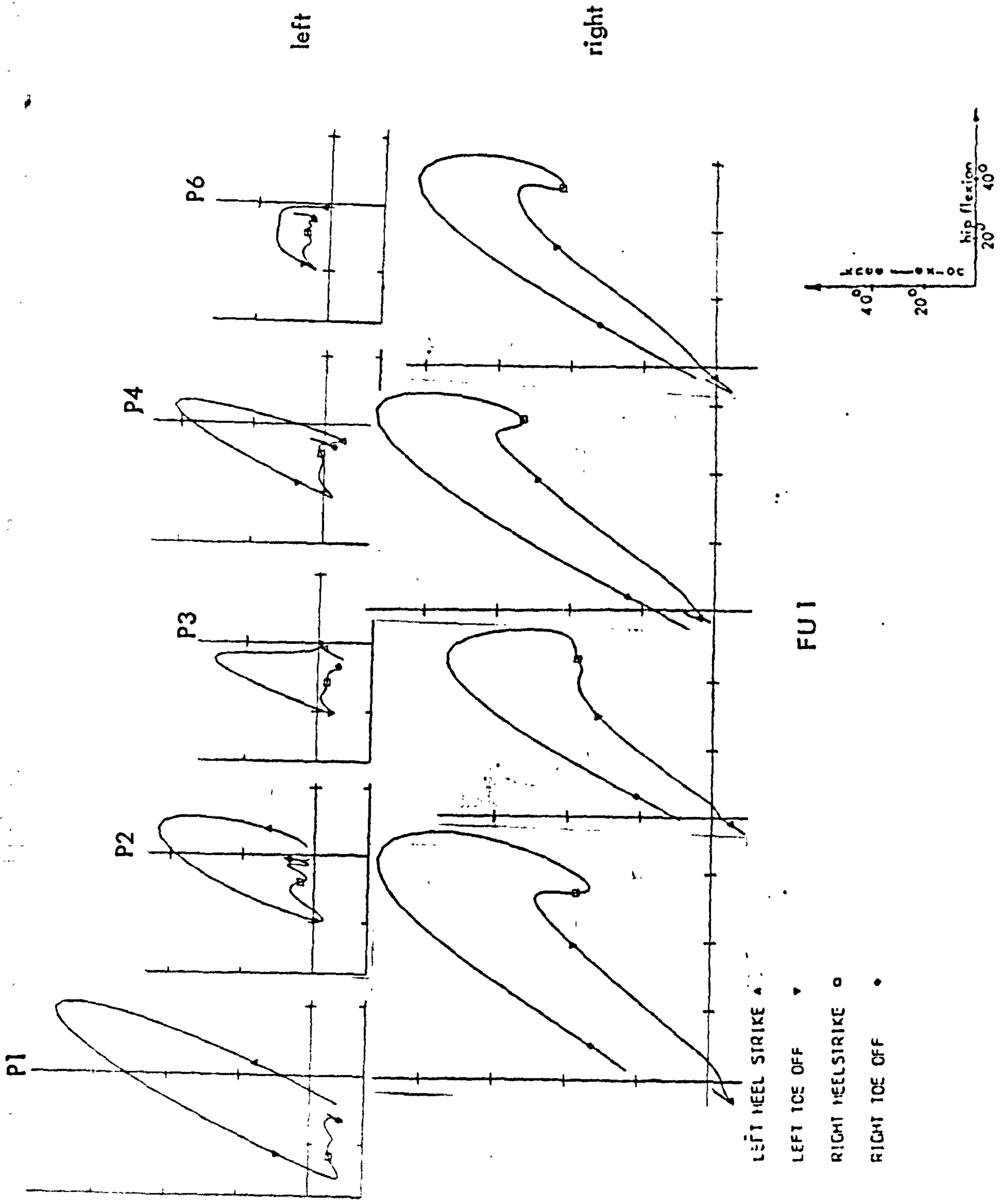


Fig 5.54

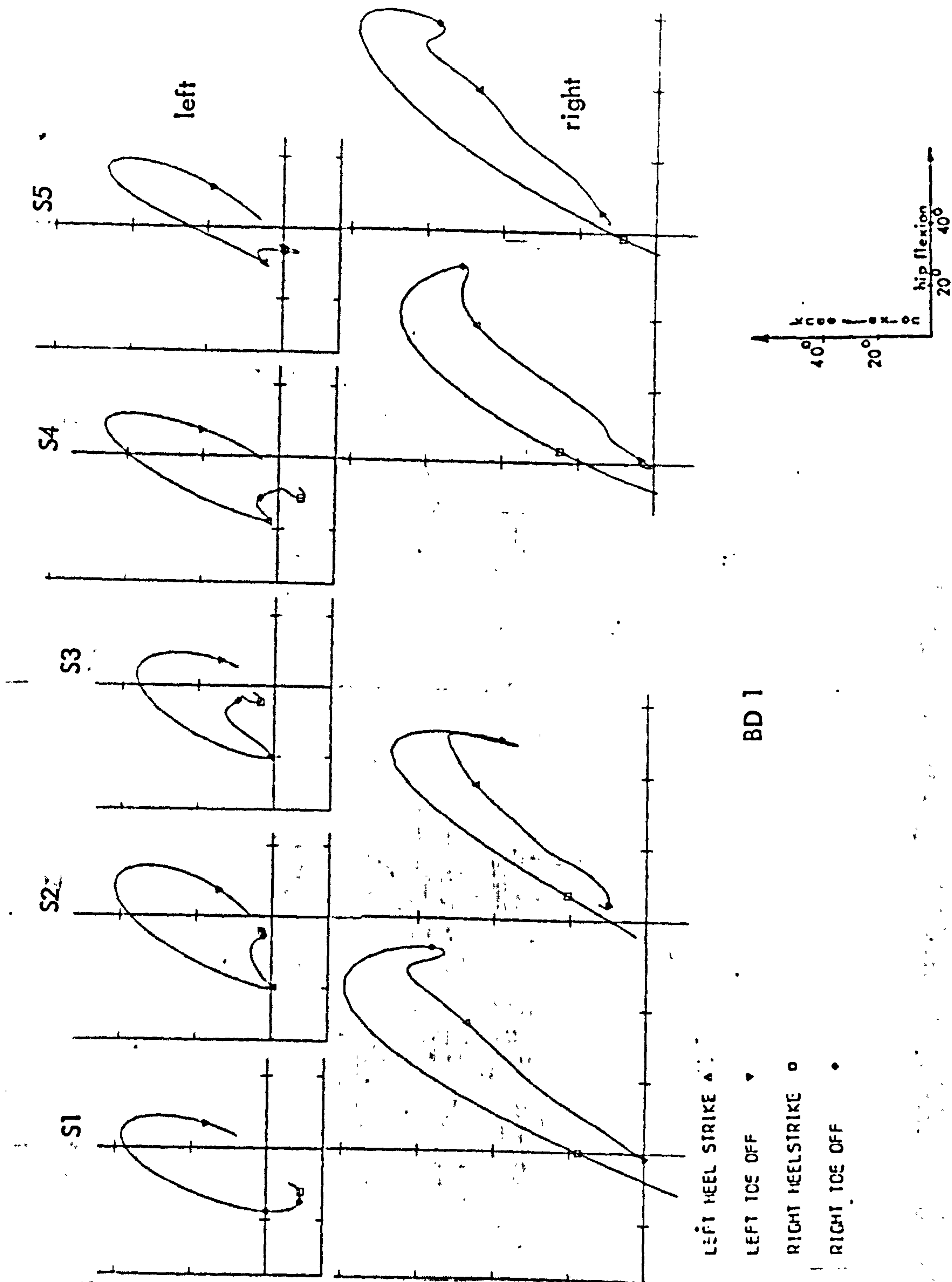


Fig 5.55

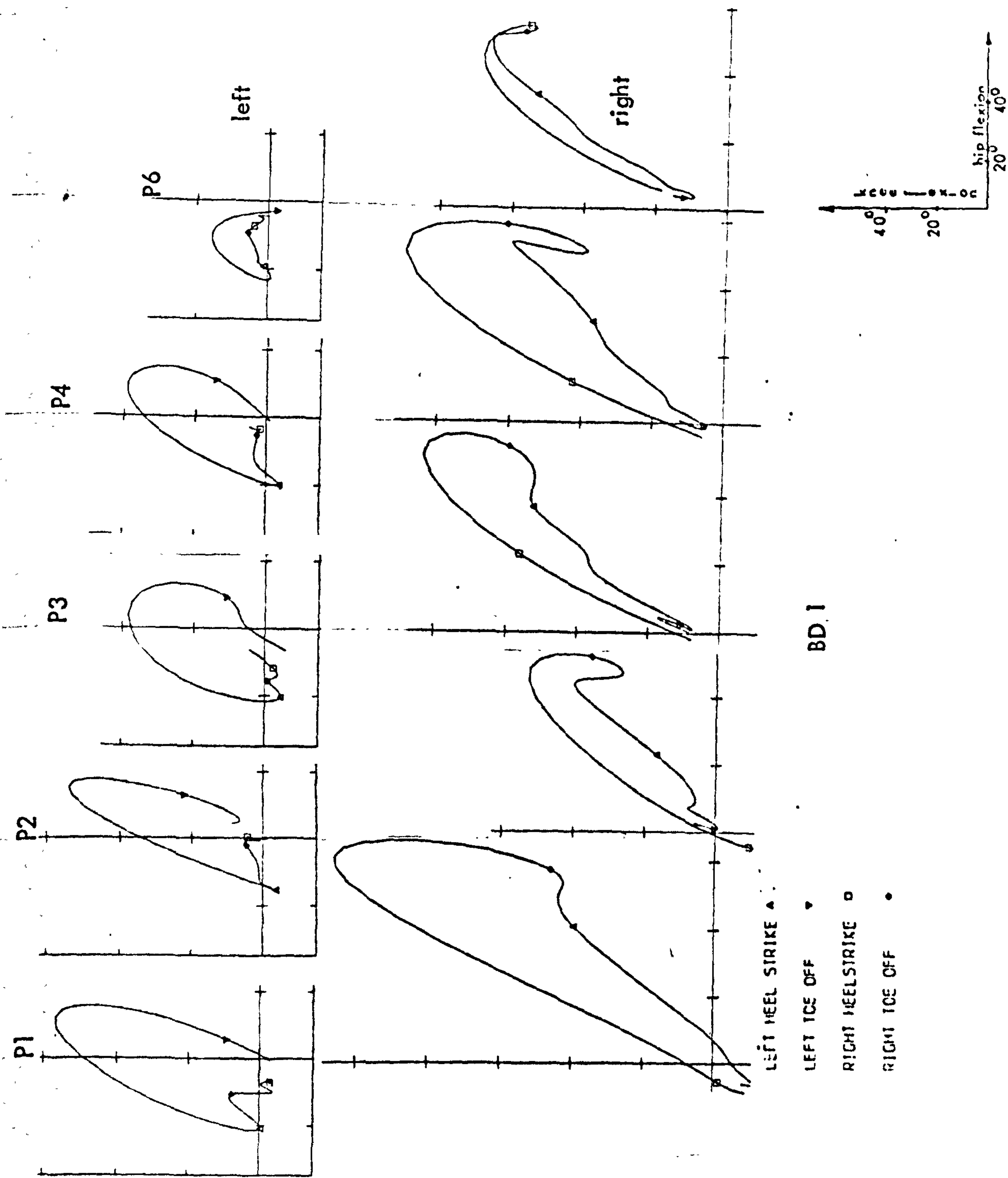


Fig 5.56

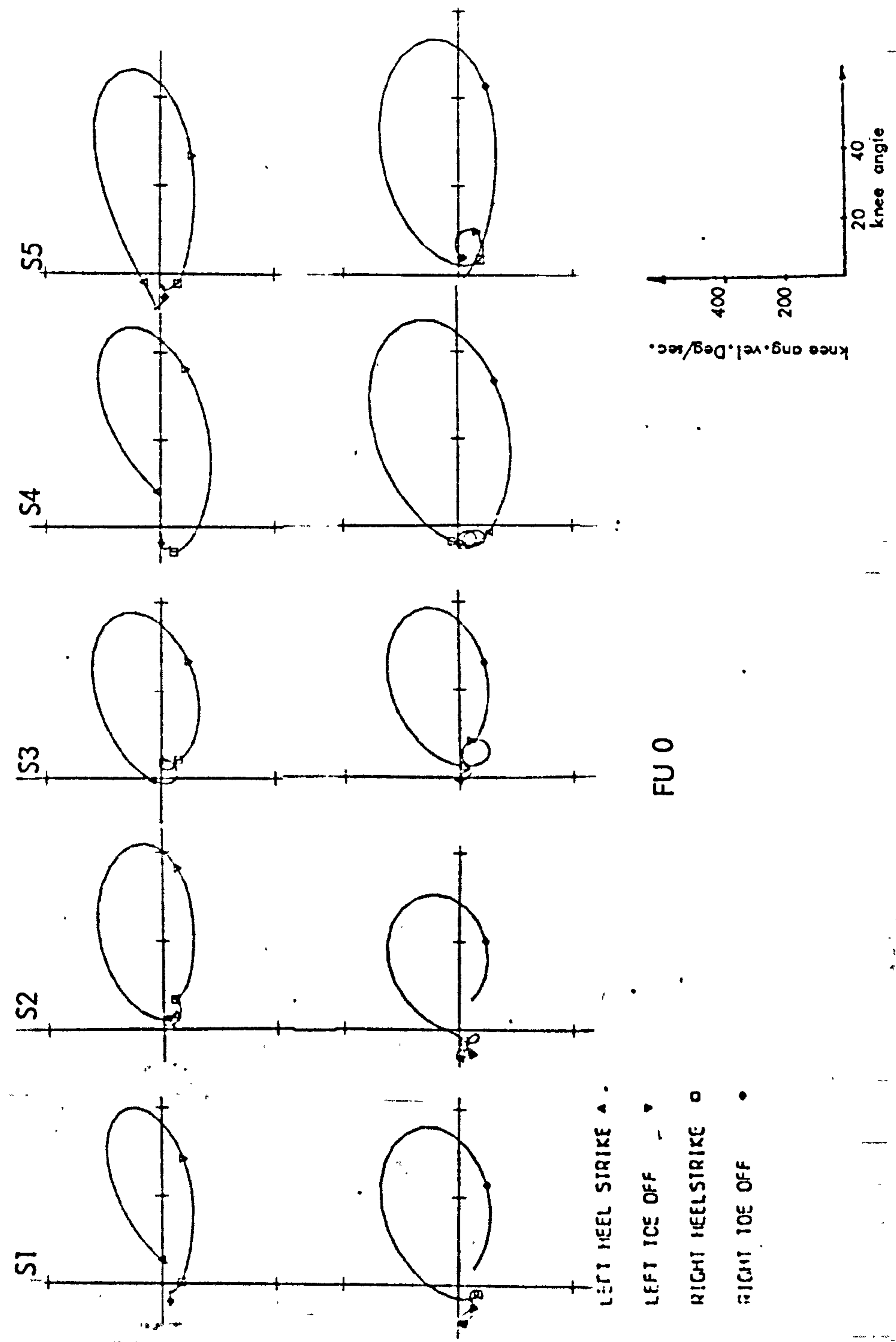


Fig 5.57

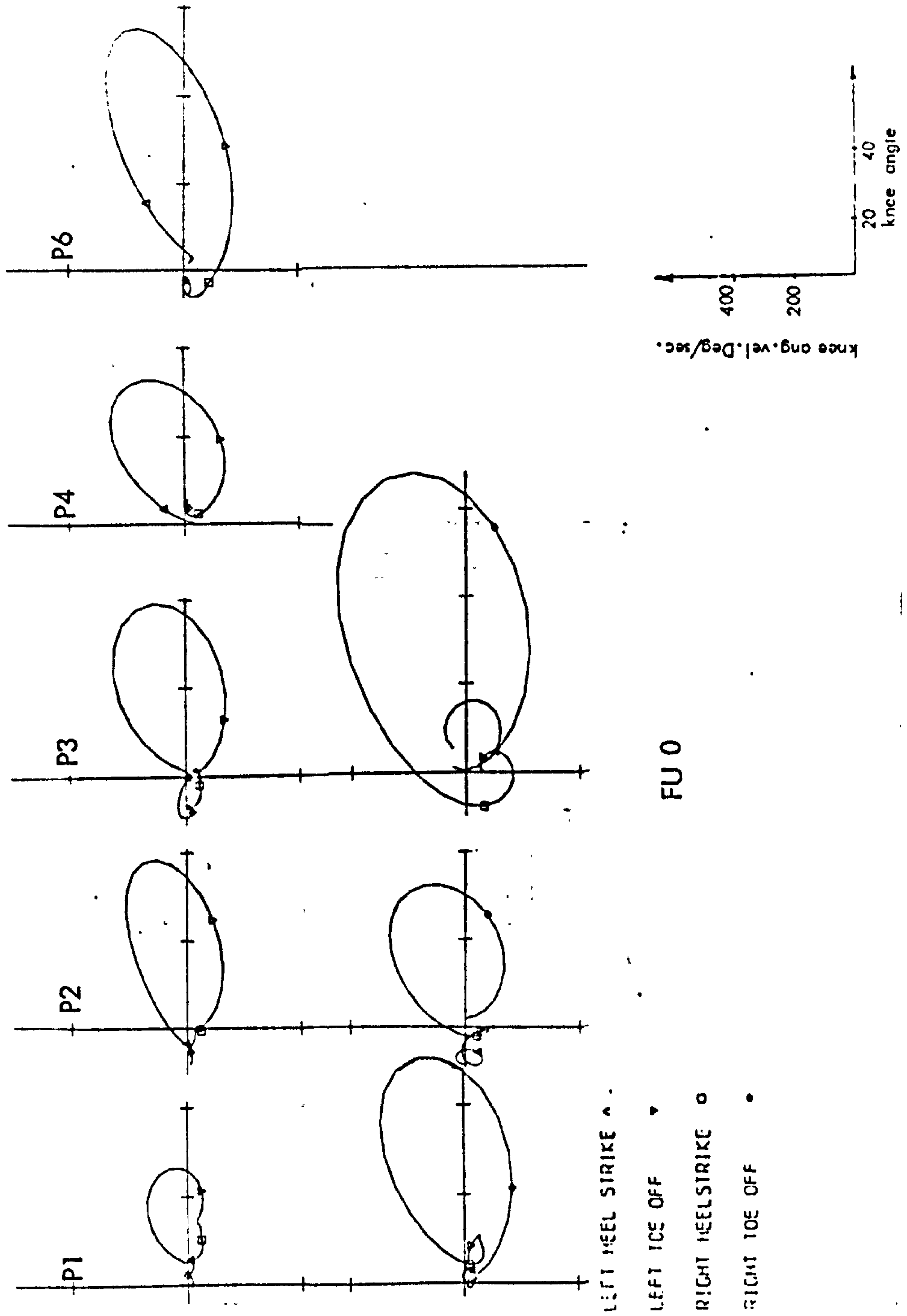


Fig 5.58

0

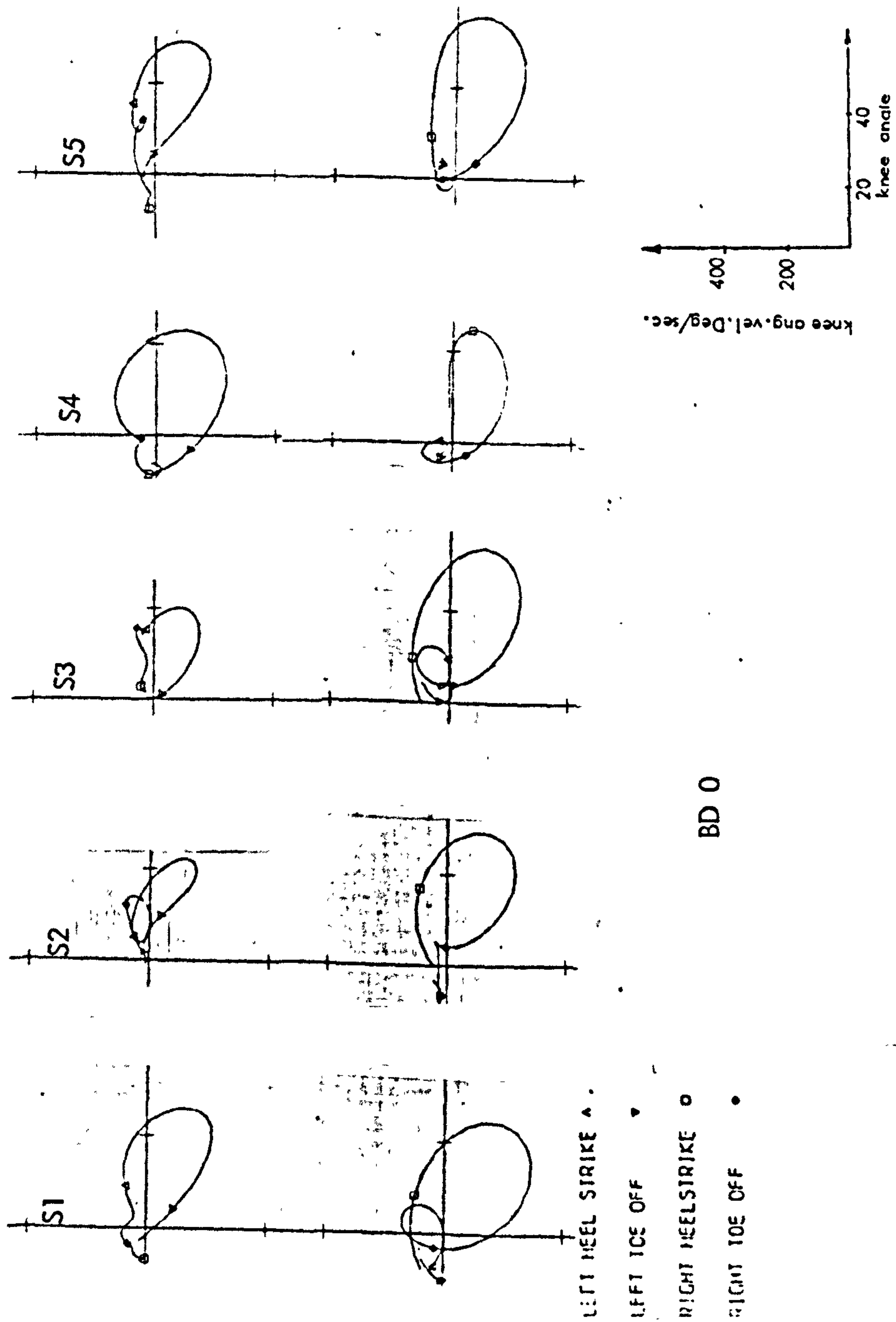


Fig 5.59



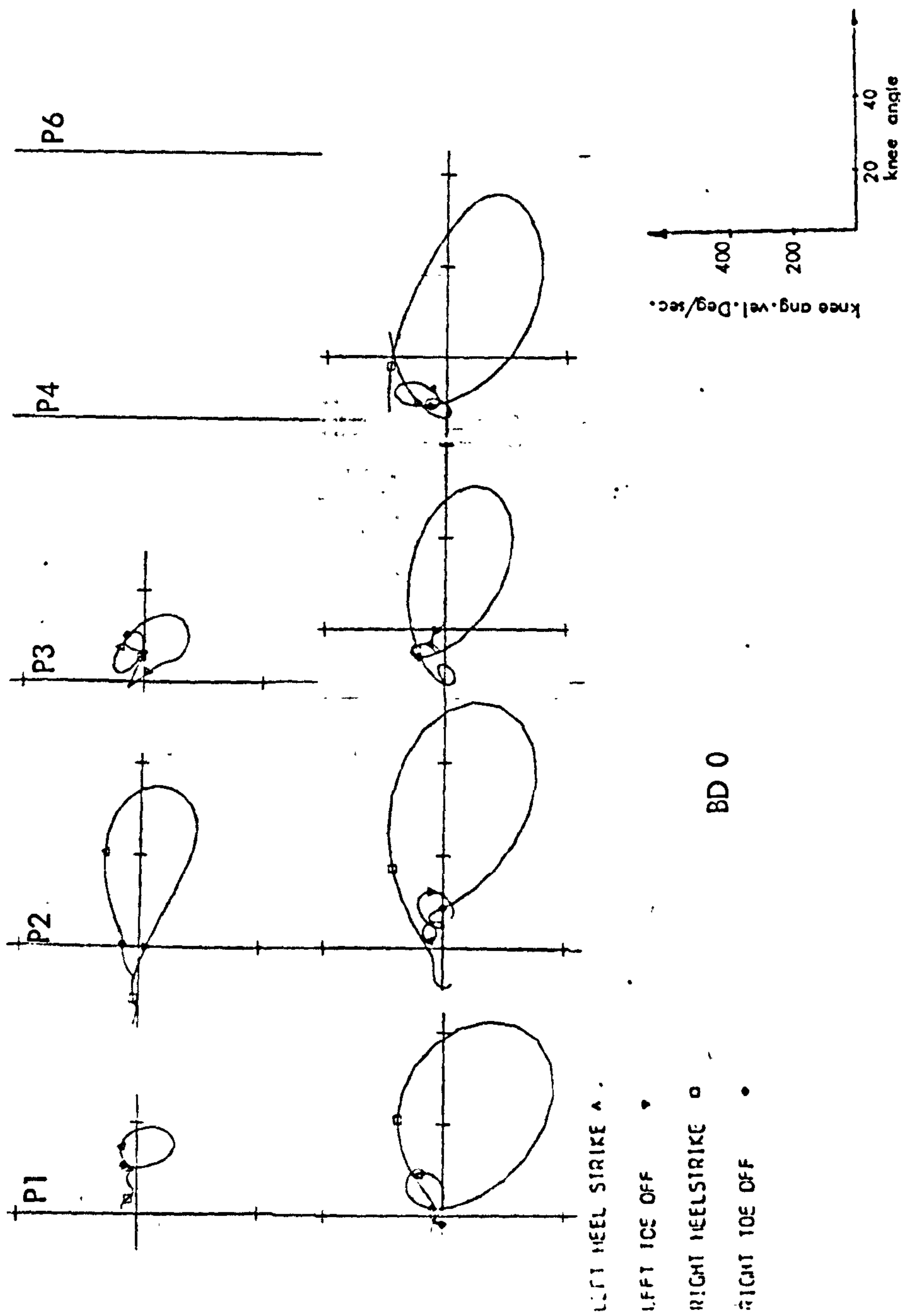
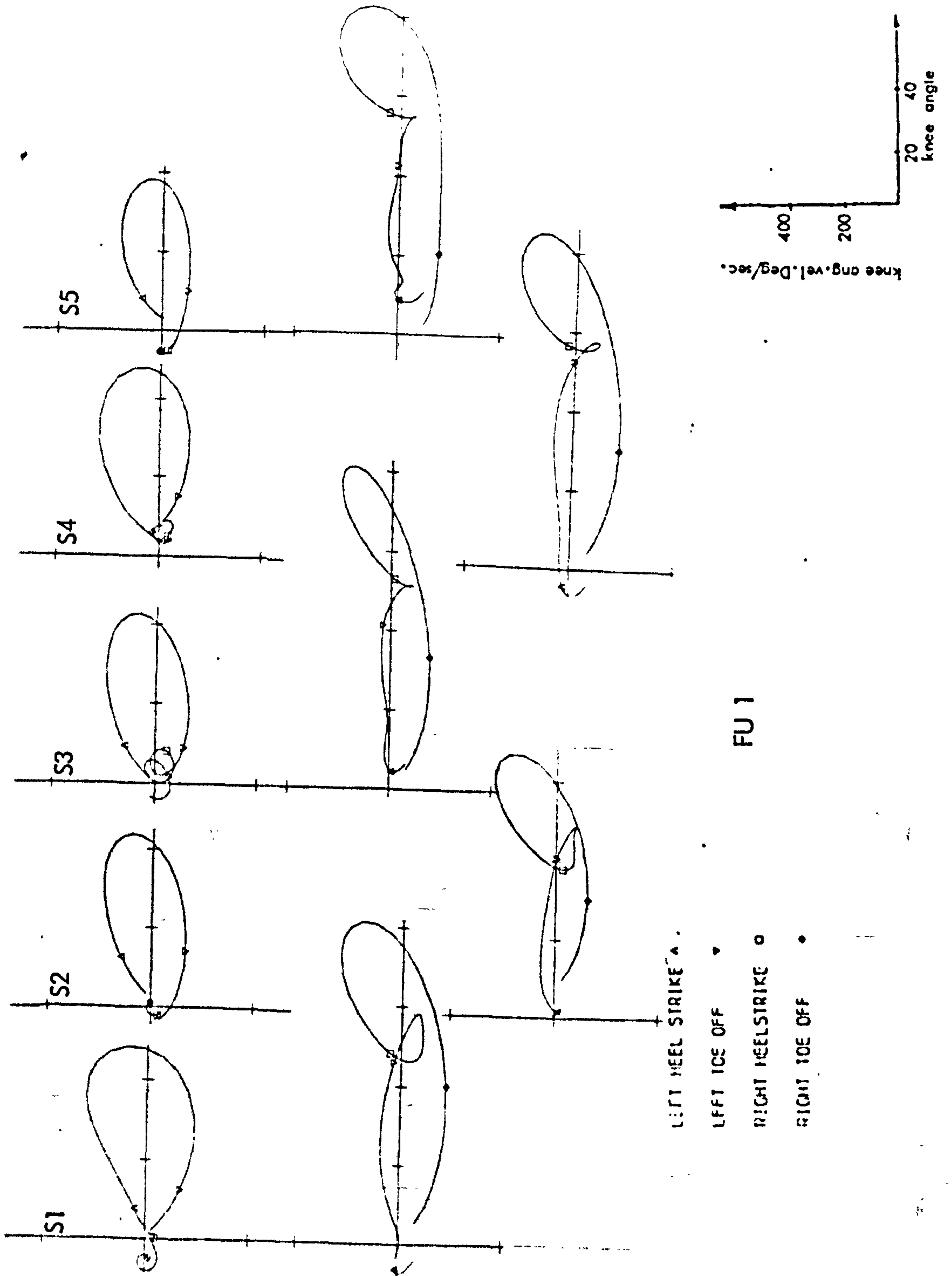


Fig 5.60



Flg 5.61

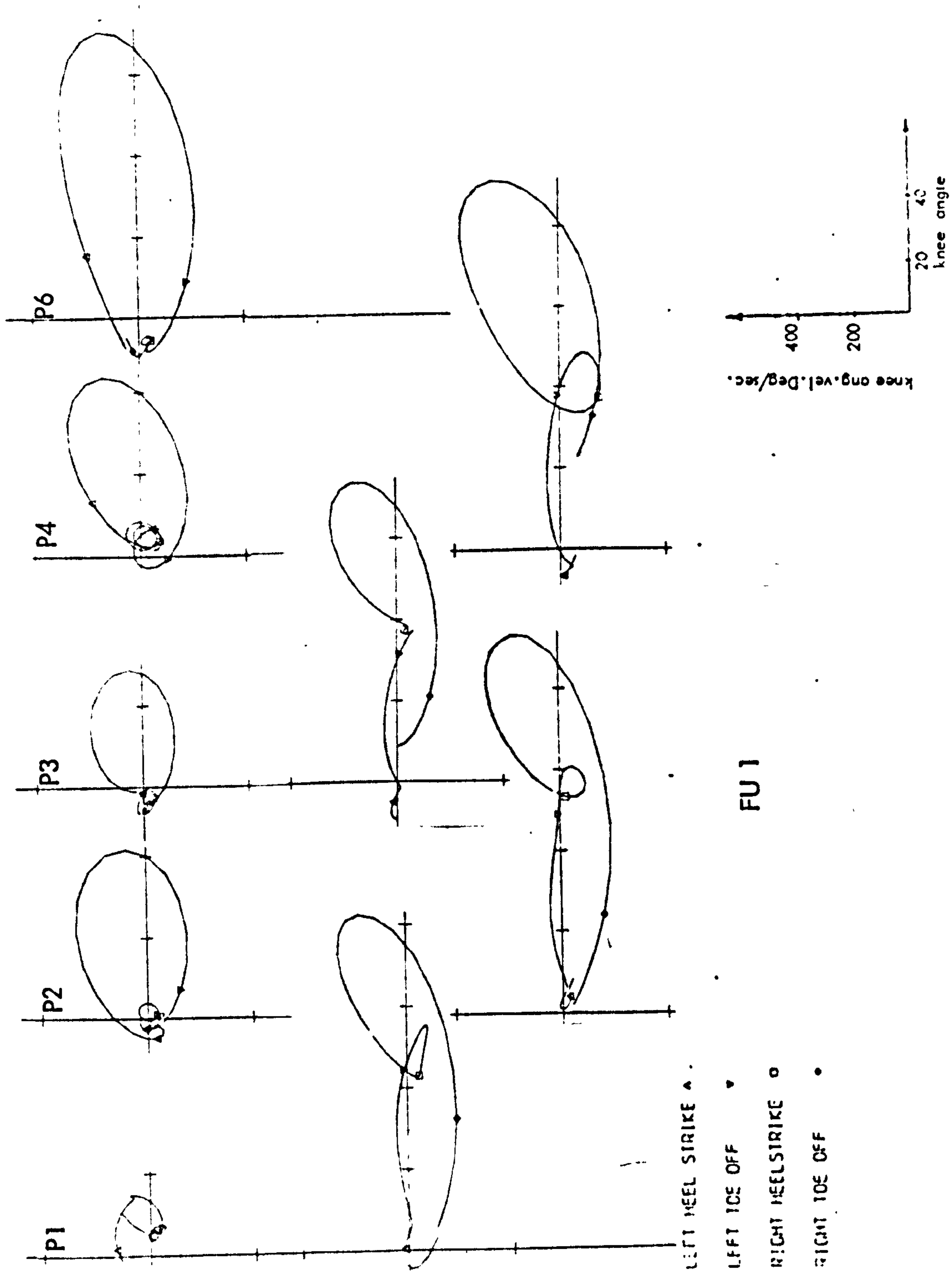


Fig 5.62

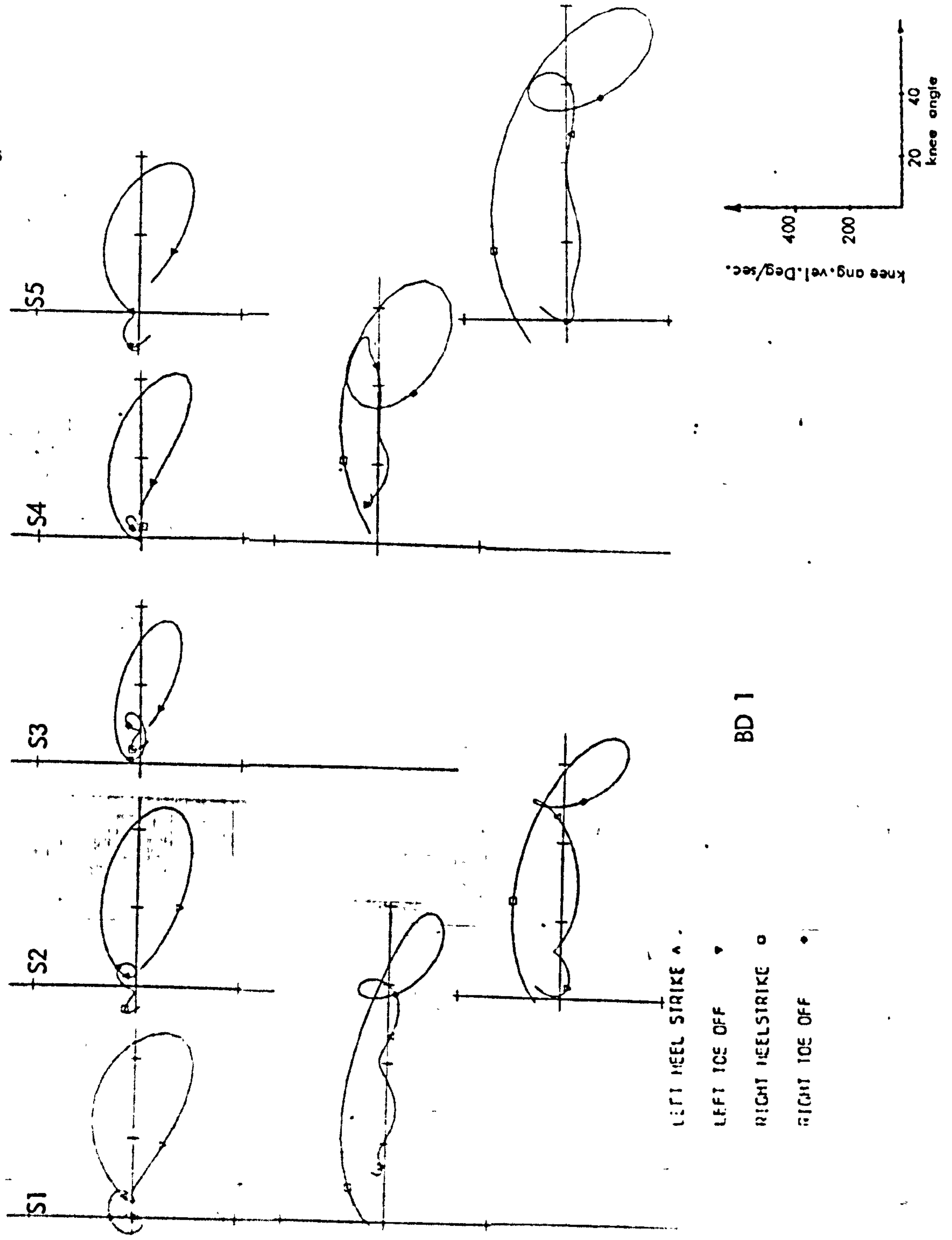


Fig 5.63

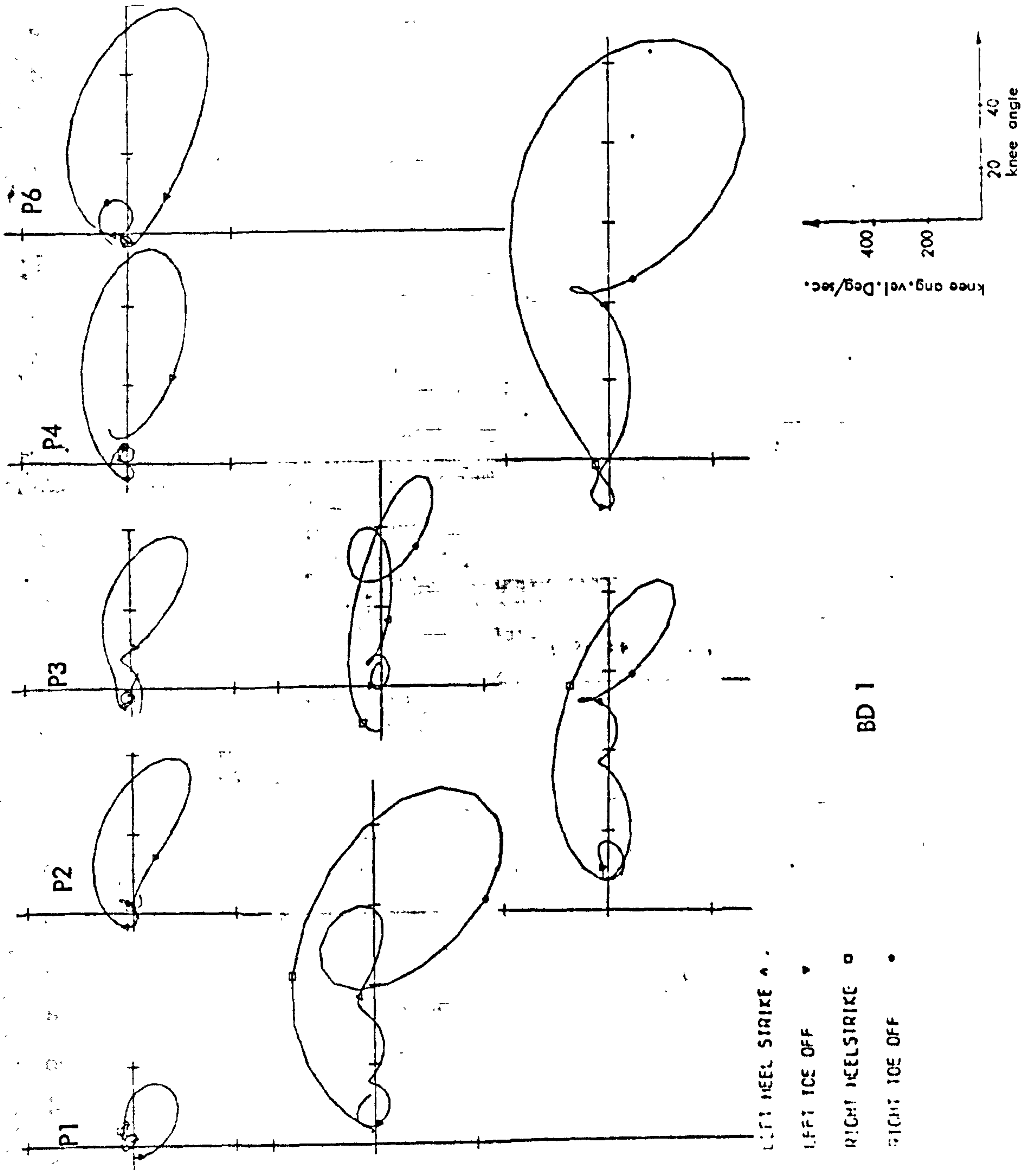


Fig 5.64

This study did not confirm the statement made by Grieve et al (1978) viz: "the similarities between normal conjugate movements seem remarkable and deserve exploration". It can be seen, from the diagrams presented (Fig. 5.53 to 5.56) that these curves for the conjugate pair vary within subject or patient.

It is concluded that the angle-angle diagram, represents a good visual aid for locomotion studies, but does not provide complete information.

### 5.7 Angle-velocity diagrams

Fig. 5.57 to 5.64 show the angular velocity at the knee plotted against knee angle.

These are presented as another way of conveying information. Instability areas can be seen apparent as small loops. These diagrams may prove useful in interpreting the rate of muscle contraction at a particular joint. However, further studies are required towards this end.

### 5.8 Analysis of result for one particular patient, P2 ("within-patient" comparisons)

5.8.1 Introduction The discussion so far has been based by considering all subjects and patients collectively in order to identify trends. The results obtained for one particular patient (selected arbitrarily as patient P2) will be considered in order to allow comparison "within-patient" to be made.

5.8.2 Moments in the sagittal plane Observing the moments in the sagittal plane for the ankle and knee for this patient, remarkable similarity for the curve shapes for these two joints is noted. The most important part in both manoeuvres (FU 1 and BD 1) is the double support phase (shaded area Fig. 5.65 to 5.70) where the body weight is being transferred from one leg to the other. In both cases (FU 1 and BD 1) either for the ankle and knee, the "within patient" analysis confirms the important role of the left leg on the step action. In these figures it is easier to see the result of this affecting all the joints during double support.

The coronal plane moments have confirmed the general discussion. (para. 5.4).

5.8.3 The angle-angle diagrams The thigh-knee diagrams, show differences in shape on first impression. The differences are as follows:

The left leg during FU 1 shows a certain degree of instability Fig 5.71 (oscillations in the knee) while the hip is being extended and the body is pushed forwards. The largest knee flexion on this diagram suggests that the patient is using

his quadriceps in the trailing leg in order to assist the contralateral limb.

Comparing the FU 1 left leg with the BD 1 left leg, shows that in the latter manoeuvre the patient is not using his knee very much, suggesting that the calf group is being responsible for the deceleration of the movement.

However, the FU 1 and BD 1 for the right leg, shows a remarkable difference in the conjugate pairs as described by Grieve et al (1978). It is important to note that in this double stance phase, in the FU 1 manoeuvre, the knee remains "locked" at a certain angle while the hip extends as the body is being translated to the step. In this particular instant the quadriceps group is acting isometrically, in order to provide more stability during the transference of the load from one limb to the other. On the conjugate pair (BD 1) this phenomenon does not occur - gravity assists the manoeuvre and the contralateral limb is the one responsible to support.

In both cases, left and right leg, the limb leading the manoeuvre is the one which produces larger angles during the swing phase. This is due to the necessity to clear the ground (step); the same does not obtain in the trailing limb as the neurosystem had already received the necessary informations.

Grieve et al (1978) emphasise the importance of the shapes of the angle-angle diagram as an aid in itself to assess and interpret pathological cases. It is the author's view that this is an over-simplification when assessing significance of shape changes clinically, unimportant features in locomotion can produce such distortion. In the case (patient P2) analysed it is of interest to note that the difference in shape, of the diagram of the right leg (FU 1 and BD 1) occurs mainly during the swing phase which seems not to be of any importance in the detection of pathological states.

The diagrams without doubt can be of considerable help in the interpretation of human kinematics, but it has to be borne in mind that the whole of the biomechanical complexity of the action is not being reflected in these diagrams and in consequence they have to be used as an accessory tool only.

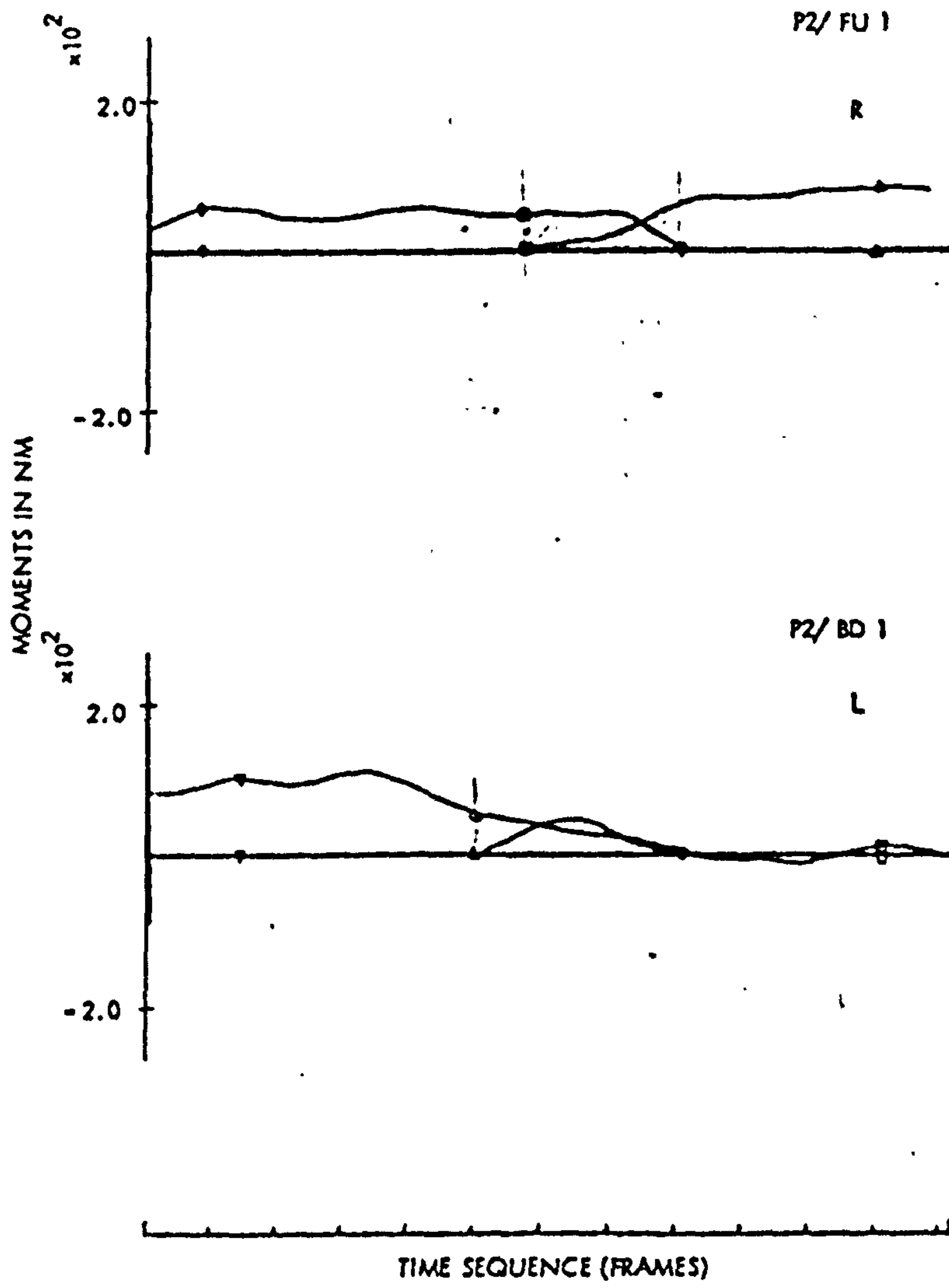
Additionally, presentation of the kinematic data in the form of angle-angle diagrams has the advantage of allowing direct comparisons to be made with the results of the preliminary study on the stepping action carried out using the Polarized light goniometer (Polgon) by D'Angelo and Grieve (1977) and Grieve et al (1978).

Fig. 5.49 and 5.50 show that the angle-angle diagrams produced during zero height step are generally similar to those obtained for walking on the level (see Fig. 5.23) for both left and right legs. However two differences can be seen: a) the zero height stepping diagram does not close completely, as in the case of level walking. This is due to the fact that the step test does not constitute a full cycle (stride) as in locomotion and in the majority of the cases (both for normals and pathologicals) the limbs do not end up with the same posture as at the start of the manoeuvre. b) in the step test it seems that there is a tendency to hyperextend the knee during the stance phase. The latter effect was interpreted as a posture adopted in order to save muscle energy during standing. This is not commonly seen in walking due to large inertia effects.

The BD O manoeuvre (Fig. 5.51 & 5.52) shows familiar curves shapes for the right leg but completely distorted curve shapes for the left leg, for both normals and pathologicals. The inconsistencies in the shapes for this manoeuvre are thought to be due to the unusual nature of this particular stepping movement. It has been observed that a certain subject may choose any convenient posture at a certain moment in time. At first sight it would appear that important features could emerge from such a diagram, but on comparisons with Fig. 5.55 and 5.56 BD 1 which represent the same movement performed on a 10% height step, a more stable diagram is seen (for both normals and pathologicals). When descending from a step, both normals and pathologicals, have less choice in posture than when walking backwards on the level.

For the FU 1 and BD 1 Fig. 5.53 to 5.56 the right leg produces the shape described by Grieve et al (1978) see Fig. 5.24. These curves did not show significant differences between the normals and the pathologicals neither for neither FU 1 nor for BD 1. Nevertheless, differences do occur between the conjugate part of diagrams (FU 1/BD 1) within a certain subject (for both normals and patients).

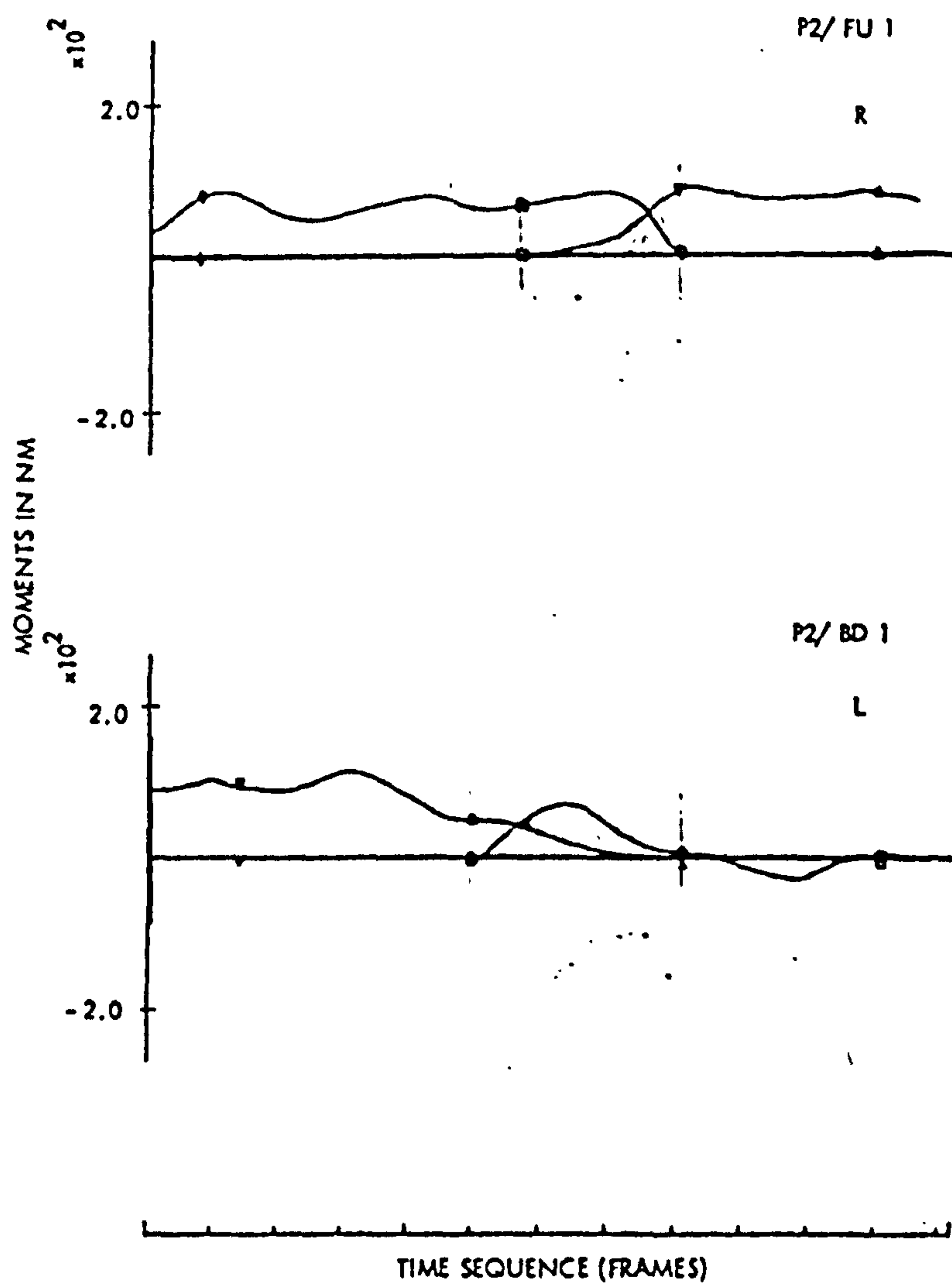




Ankle moments, sagittal plane

Fig. 5.65

- LEFT HEEL STRIKE ▲
- LEFT TOE OFF ▼
- RIGHT HEELSTRIKE □
- RIGHT TOE OFF ◇



Knee moments, sagittal plane

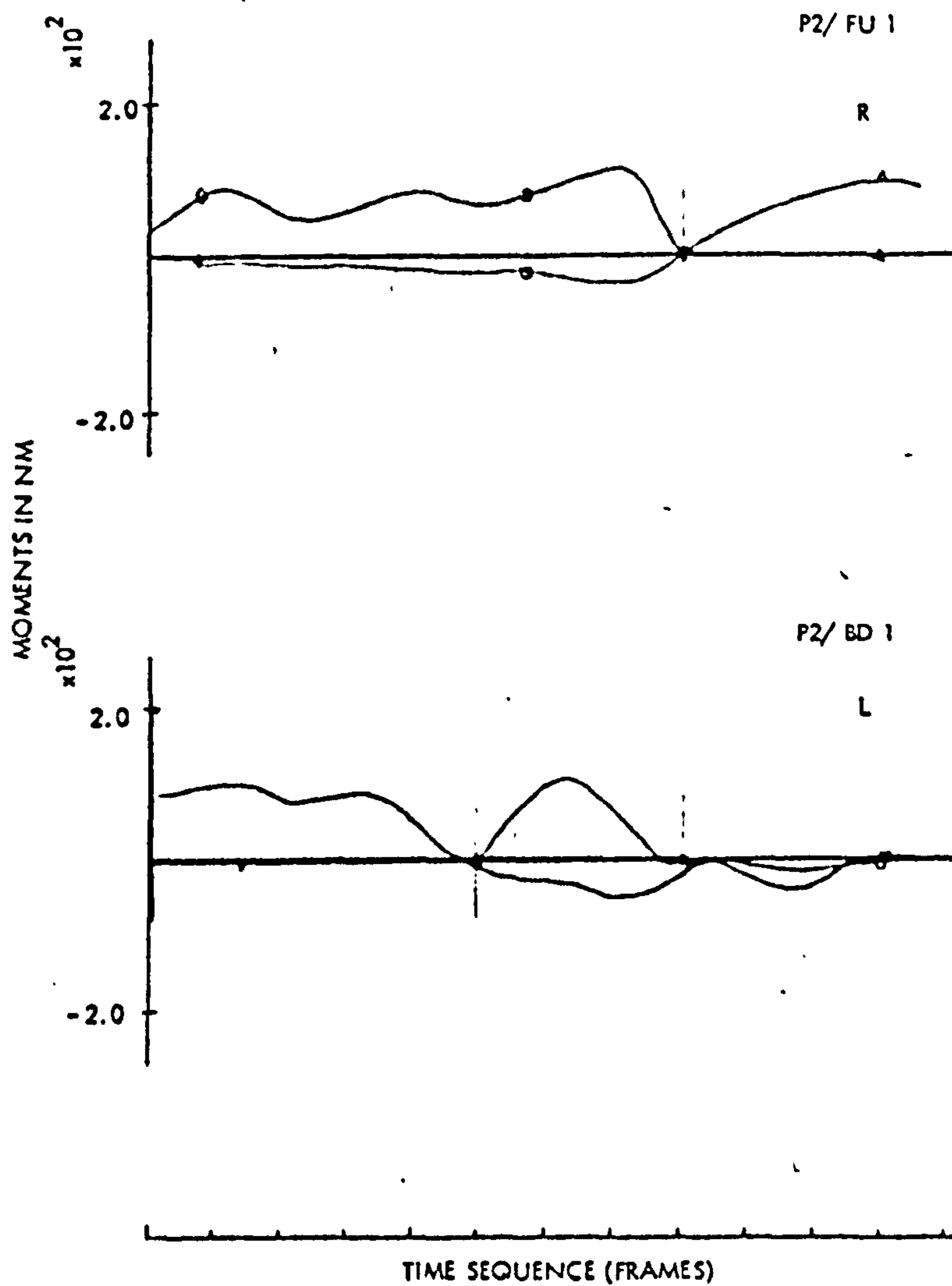
Fig. 5. 66

LEFT HEEL STRIKE  $\blacktriangle$

LEFT TOE OFF  $\blacktriangledown$

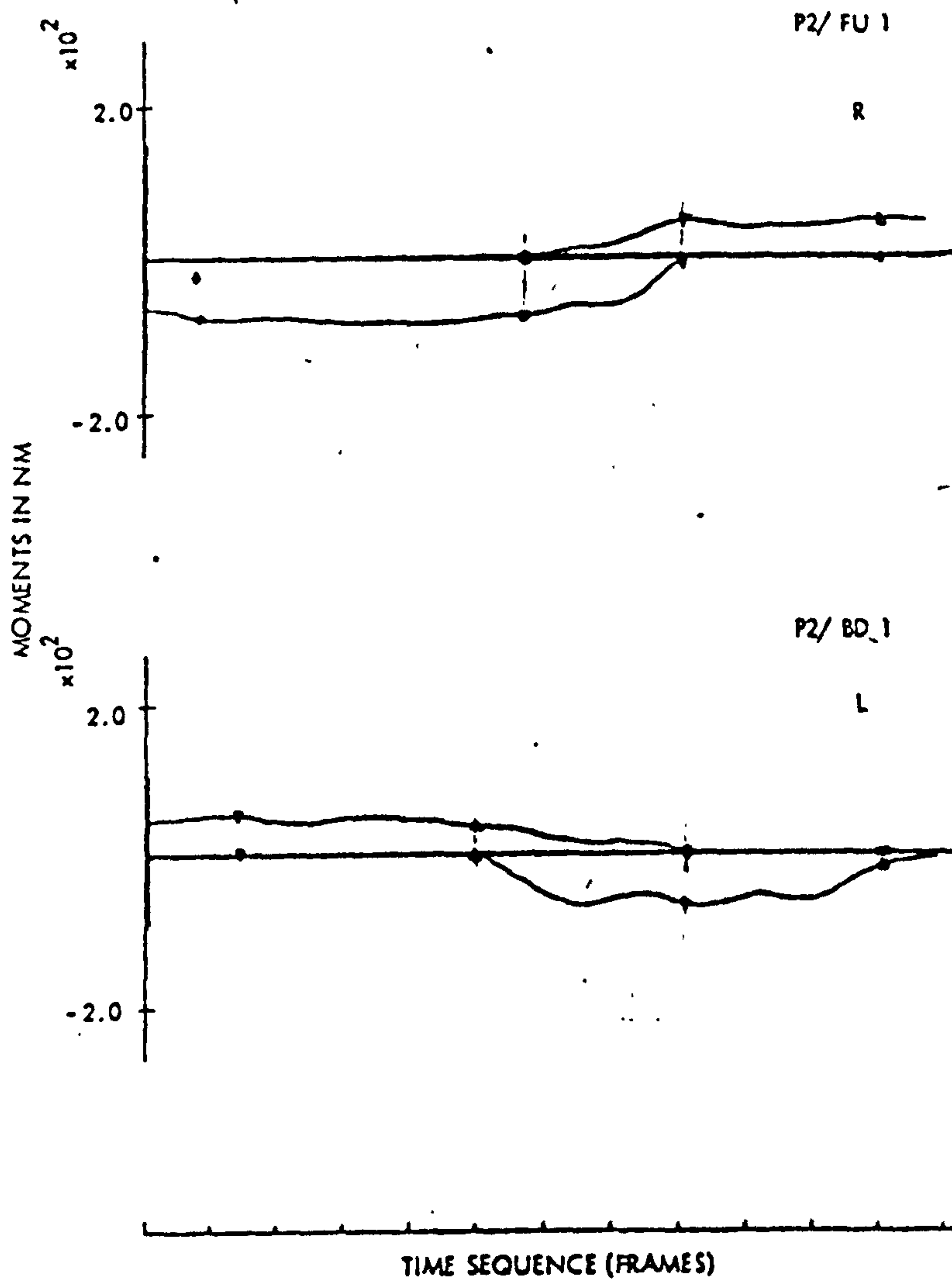
RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\circ$



Hip moments, sagittal plane  
Fig. 5.67

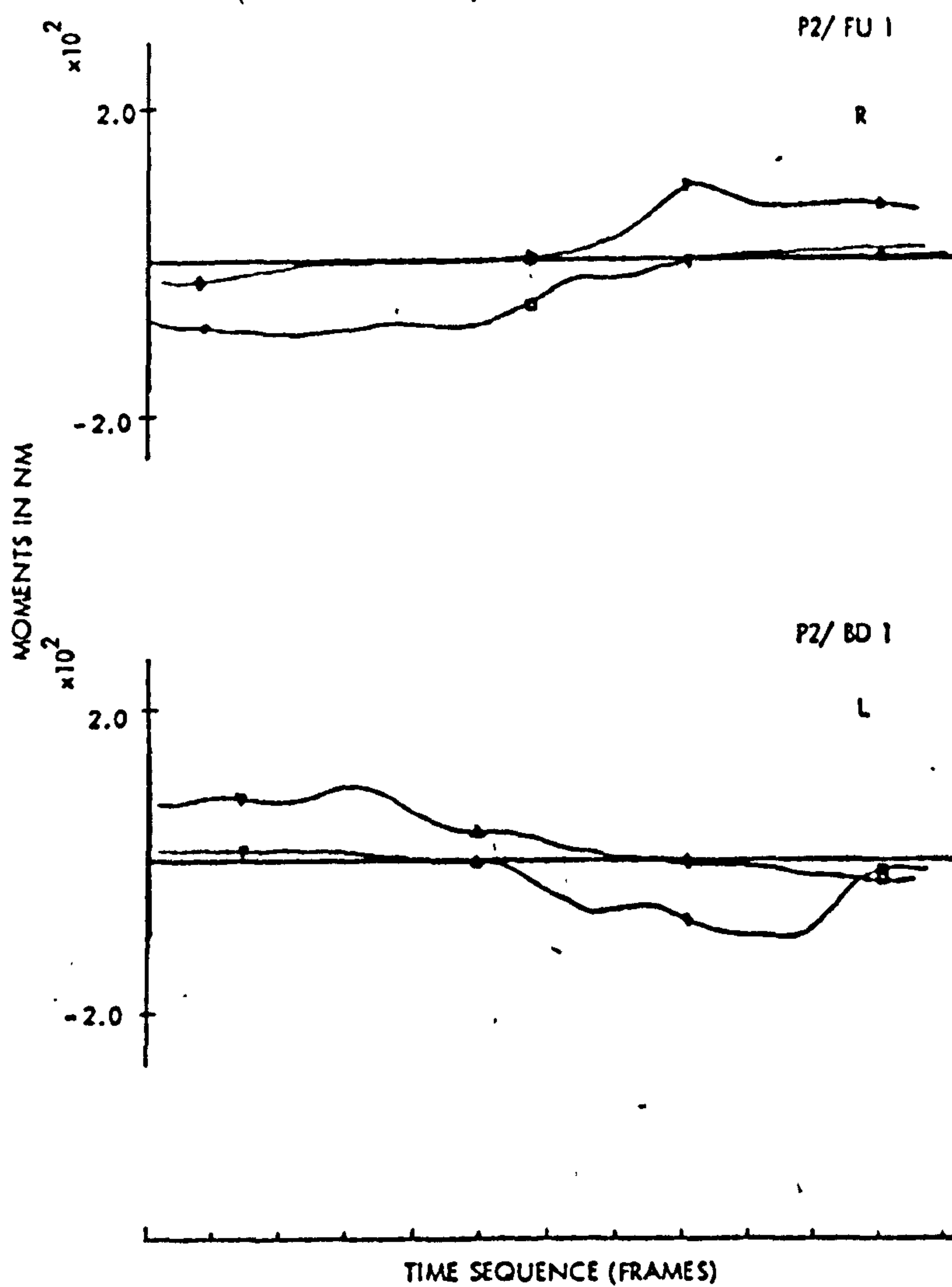
LEFT HEEL STRIKE  $\blacktriangle$   
 LEFT TOE OFF  $\blacktriangledown$   
 RIGHT HEELSTRIKE  $\square$   
 RIGHT TOE OFF  $\diamond$



Ankle moments, coronal plane

Fig. 5. 68

- LEFT HEEL STRIKE  $\wedge$
- LEFT TOE OFF  $\nabla$
- RIGHT HEELSTRIKE  $\square$
- RIGHT TOE OFF  $\circ$



Knee moments, coronal plane

Fig. 5.69

LEFT HEEL STRIKE  $\blacktriangle$

LEFT TOE OFF  $\blacktriangledown$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\circ$

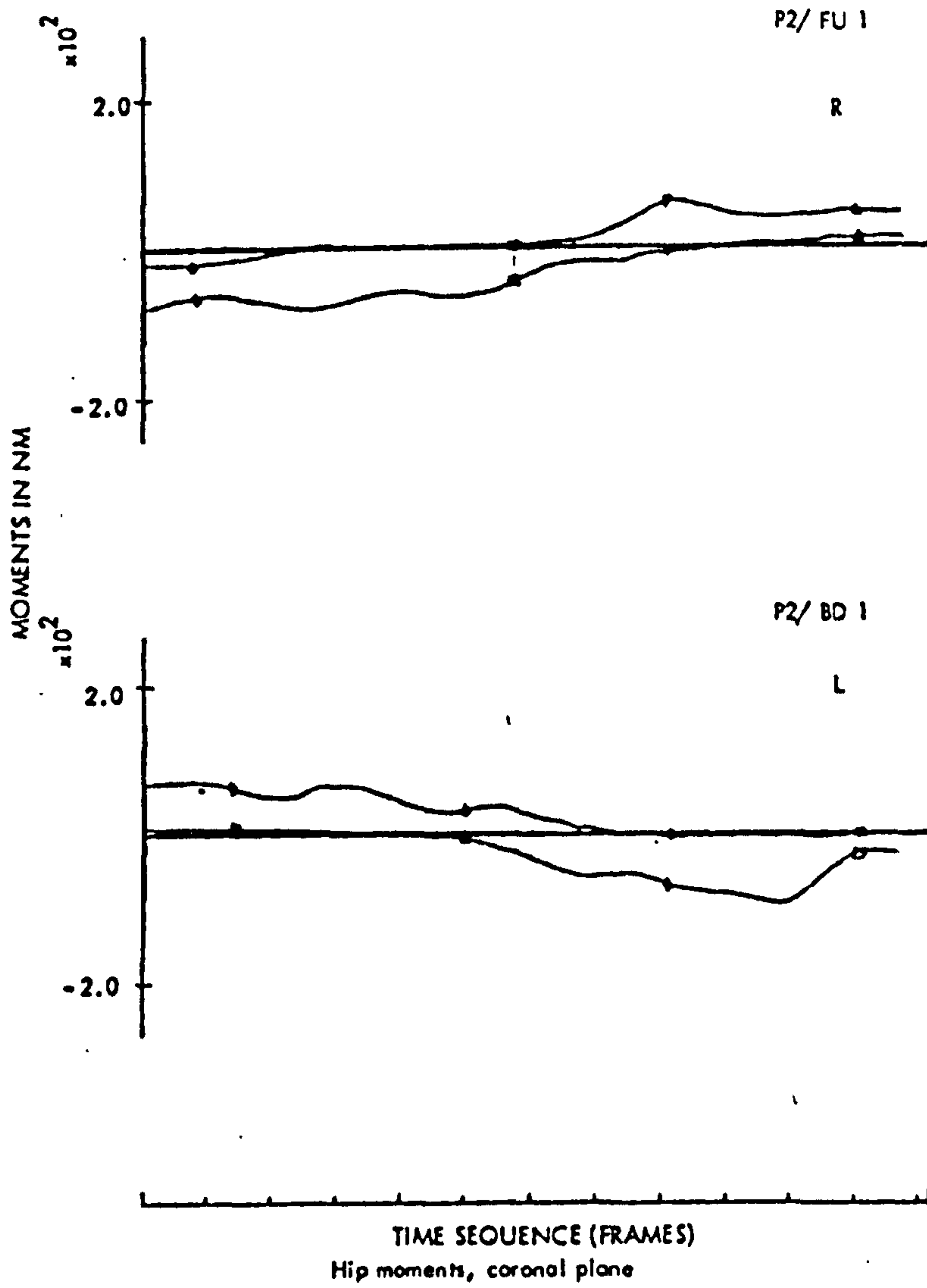


Fig. 5.70

LEFT HEEL STRIKE  $\blacktriangle$   
 LEFT TOE OFF  $\blacktriangledown$   
 RIGHT HEELSTRIKE  $\square$   
 RIGHT TOE OFF  $\diamond$

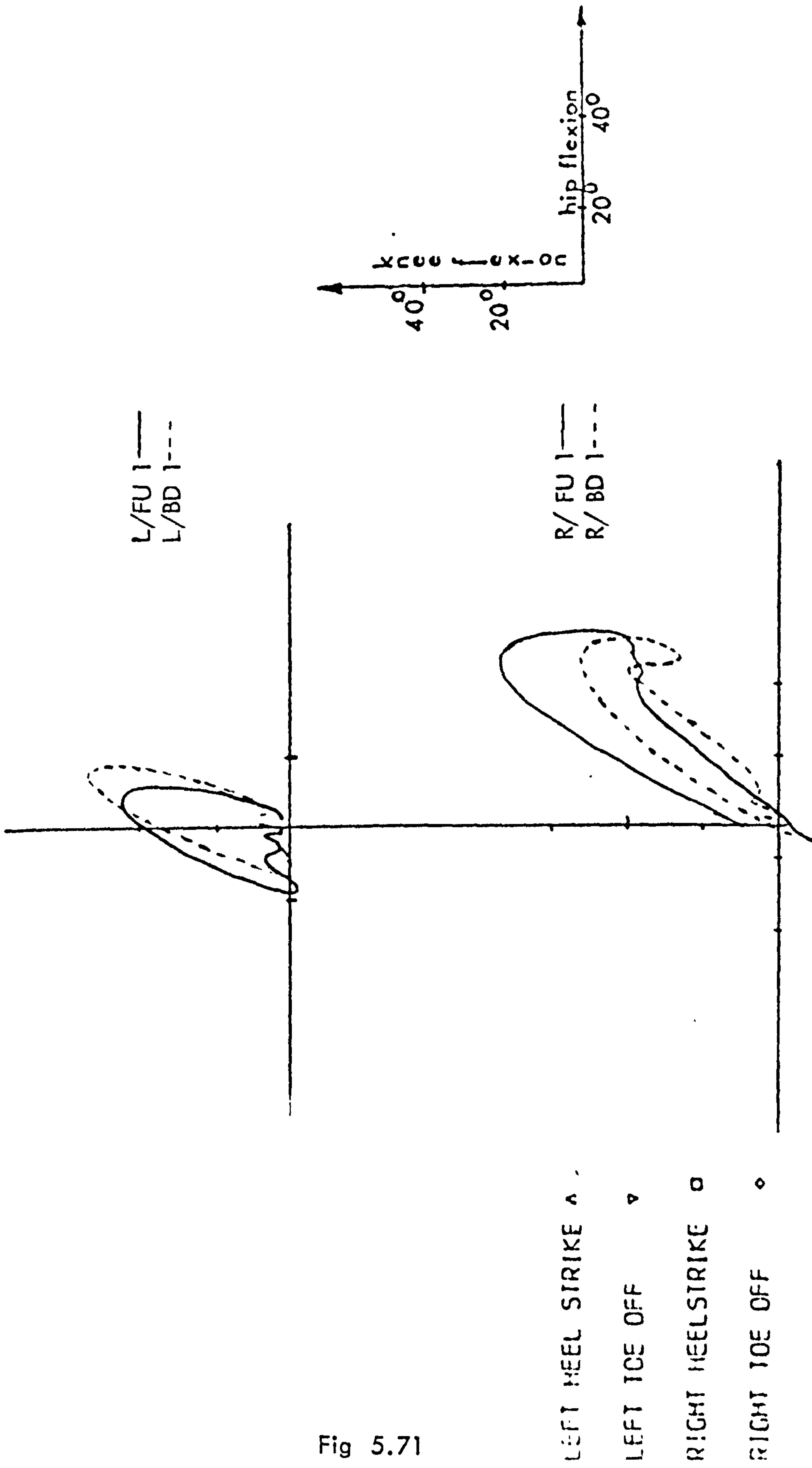


Fig 5.71

LEFT HEEL STRIKE ^  
 LEFT TOE OFF v  
 RIGHT HEEL STRIKE o  
 RIGHT TOE OFF o

L/FU |——  
 L/BD |- - -

R/FU |——  
 R/BD |- - -

CHAPTER 6

CONCLUSIONS



## 6. CONCLUSIONS

There were no significant differences between the moments at ankle, knee or hip for step height of 0% and 10% of patient's height.

The left leg (trailing leg) was found to be always more highly loaded than the right, in both the FU and BD manoeuvres. The calf muscular group seems to play an important role in accelerating the body upwards or absorbing the energy in decelerating the body backwards.

This is a disadvantage in the step test as a patient can mask pathology in the leading leg knee using the gastrocnemius of the trailing leg.

The angle-angle diagrams can be of considerable help in the interpretation of human motion kinematics. However to attempt to interpret pathological conditions from merely the shape of the angle-angle diagrams would be an over simplification. Analysis of the results must be done in conjunction with other information such as force actions, temporal parameters etc. During the stance phase measurement of both the forces and displacements is of importance whereas during swing phase the linear and angular displacements are most relevant. The calculations carried out clearly indicate that the forces due to the inertia effects during the stepping action are negligibly small.

No significant differences were found between the patients and the control subjects. Furthermore, an attempt to interpret "within patient" variations (as suggested by Grieve et al 1978) did not prove fruitful. Similarities in conjugate pairs when using the angle diagrams, were not found.

A positive outcome of significance has been the development of a computer program which accepts data from 2 force plates and a kinematic system and outputs 3 dimensional intersegmental, force actions, and linear and angular displacements in graphical form. This development was necessary in order to handle the enormous amount of data involved and it is now so designed that any modification/improvement considered necessary in the future development of all locomotion testing procedures can be easily accommodated.

It is concluded that the step test in its present form has no application as part of a battery of tests used for clinical purposes. Further exploration

therefore, in this simple form of test, is not recommended. Future investigations should be carried out using a step of variable rise - from zero to a height that the subject/patient is capable of climbing - in order to establish a relationship between step height and the relevant biomechanical parameters.

CHAPTER 7

BIBLIOGRAPHY

## 7. BIBLIOGRAPHY

The publications listed represent all those consulted in the course of the work. However not every one of the cited references are directly referred to in the text.

ABBOTT, B. C., BIGLAND, B. and RITCHIE, J. M. (1952)

The Physiological Cost of Negative Work

J. Physiol. 117 380 - 390

AMAR, J. (1916)

Trottoir Dynamographique

Compt. Rend. Acad. di Sci. 163 130 - 132

AMAR, J. (1917)

Organization Physiologique due Travail, Paris

Cited by University of California (1947)

BASMAJIAN, J. V. (1967)

Muscles Alive. 2nd Edition

Baltimore, Williams and Wilkins and Co.

BATTYE, C. K. and JOSEPH, J. (1966)

An Investigation by Telemetering of the Activity of Some Muscles  
in Walking

Med. and Biol. Engng. Vol. 4 125 - 135

BERUSTEIN, N. (1967)

Biodynamics of Locomotion: In "The Co-ordination and Regulation  
of Movements".

Pergamon, Oxford, England. 196p.

BIGLAND, B. and LIPPOLD, O. C. J. (1954)

Relation Between Forces, Velocity and Integrated Electrical Activity  
In Human Muscle

J. Physiol. 123 214 - 224

BRAUNE, W. and FISCHER, O. (1890)

Cited by University of California (1947)

BRESLER, B. and FRANKEL, J.P. (1950)

The Forces and Moments in the Leg During Level Walking

Trans. ASME 72 No. 1 27 - 36

BRESLER, B. and BERRY, F.R. (1951)

Energy and Power in the Leg During Normal Level Walking

Prosthetic Devices Research Project.

I.E.R. Univ. of California, Berkeley Report Series. 11 Issue 15

May 1951

BRESLER, B., RADCLIFFE, C. W. and BERRY, F.R. (1957)

Energy and Power in the Legs of Above-Knee Amputees During  
Normal Level Walking.

Prosth. Res. Bd. N.R.G. Report Series 11 Issue 31.

Univ. of California, Berkely, May 1957

CAPPOZZO, A., LEO, T. and PEDOTTI, A. (1975)

A General Computing Method for the Analysis of Human Locomotion

J. Biomechanics, Vol. 8 , 307 - 320

CAPPOZZO, A. and LEO, T. (1973)

Biomechanics of Walking Up Stairs

1st CISM-IFTOMM Symp. Theory and Practice of Robots and  
Manipulators, Udine

CARLET, G. (1872)

Essai Experimental sur la Locomotion Humain

Etude de la March

Ann. des Science Nat., Zool. 16 1 - 92

CARNAHAN, B., LUTHER, H.A., WILKES, J.O. (1968)

Applied Numerical Methods

Uohn Wiley & Sons Inc. 604p

✓  
CAVAGNA, G.A. and MARGARIA, R. (1966)

Mechanics of Walking

J. Appl. Physiol. 21 (1) 271 - 278

✓  
CAVAGNA, G. A., SAIBENE, F.P. and MARGARIA, R. (1963)

External Work in Walking

J. Appl. Physiol. 18 1 - 9

CLOSE, J.R., NICKEL, E.D. and TODD, F. N. (1960)

Motor Unit Action Potential Counts and their Significance in Isometric and Isotonic Contractions.

J. Bone and Joint Surgery. 42A 1207 - 1222

COATES, J.E. and MEADE, F. (1960)

The Energy Expenditure and Mechanical Energy Demand in Walking

Ergonomics 3 97

D'ANGELO, M.D. and GRIEVE, D. W. (1977)

Tests of Locomotor Function During Stepping by Means of Polygon

Biomechanics VI - B 363

International Series on Biomechanics, Volume 2B, Edited by

Asmussen, E and Jørgensen, K., University Park Press, Baltimore.

DRILLIS, R. and CONTINI, R. (1966)

Body Segment Parameters.

Office of Vocational Rehabilitation, Dept. Health, Education and

Welfare Report. 1106 - 03. N.Y. Univ. School of Eng. and Sic.,

New York, USA.

EBERHARDT, H. D. and INMAN, V.T. (1951)

An Evaluation of Experimental Procedure used in a Fundamental

Study of Human Gait.

Ann. N.Y. Acad. Sci. 51 1213

EBERHARDT, H. D., INMAN, V. T. and BRESLER, B. (1957)

The Principal Elements of Human Locomotion

In: Klopsteg and Wilson: Human Limbs and their Substitutes.

McGraw Hill, New York. 1954 437 - 471

ELFTMAN, H. (1939)

Forces and Energy changes in the Leg during Walking.

Am. J. Physiol. 125 339 - 356

ELFTMAN, H. (1940)

The Work Done by Muscles in Running

Am. J. Physiol. 129. 672

ELFTMAN, H. (1951)

The Basic Pattern of Human Locomotion

Ann. N.Y. Acad. Sci. 51 Art. 7. 1207 - 1212

ELFTMAN, H. (1966)

Biomechanics of Muscle: With Particular Application to the Studies of Gait

J. Bone and Joint Surgery 48A No. 2 363 - 377

GRIEVE, D. W. (1968)

Gait Patterns and the Speed of Walking

Bio-Medical Engineering 3 119 - 122

GRIEVE, D. W. (1969)

The Assessment of Gait

Physiotherapy. Nov. 452 - 460

GRIEVE, D.W., LEGGETT, D. and WETHERSTONE, B. (1978)

The Analysis of Normal Stepping Movements as a Possible Basis for Locomotor Assessment of the Lower Limbs.

J. Anat. 127.3, 515 - 532

HILL, A. V. (1970)

First and Last Experiments in Muscle Mechanics  
University Press, Cambridge, U.K. 140p

INMAN, V.T. and RALSTON, H. J. (1954)

The Mechanics of Voluntary Muscle  
Chapter 11 in Klopsteg and Wilson: Human Limbs and their  
Substitutes. McGraw Hill, New York. 1954

JORDAN, M. M. (1978)

An Interactive Signal Processing and Analysis Package for use in  
Biomedical Research. PhD Thesis Univ. of Strathclyde, Glasgow.

KATZ, B. (1939)

The Relation Between Force and Speed in Muscular Contraction.  
J. Physiol. 96 45 - 64

KLOPSTEG, P. E. and WILSON, P. D. (1954)

Human Limbs and Their Substitutes.  
New York, McGraw Hill

LAMOREUX, L. (1971)

Kinematic Measurements in the Study of Human Walking  
Bull, Prosth. Research. Spring, 1971, 3 - 84

LANCZOS, C. (1957)

Applied Analysis  
Pitmans, London, 540p

MAREY, E. J. (1874)

Animal Mechanism: A Treatise on Terrestrial and Aerial Locomotion  
New York

MARKS, M. and HIRSCHBERG, G. G. (1958)

Analysis of Hemiplegic Gait  
Ann. N.Y. Acad. Sci. 74. Art. 1 59 - 77



MORRISON, J. B. (1968)

Bioengineering Analysis of Force Actions Transmitted by the Knee Joint  
Bio-Medical Engineering. Vol. 3 No. 4, 164 - 170

MORRISON, J. B. (1970)

The Mechanics of the Knee Joint in Relation to Normal Walking  
J. Biomech. 3 51 - 61

MURRAY, M. P., DROUGHT, A. B., KORY, R.C. (1964)

Walking Patterns of Normal Man  
J. Bone and Joint Surgery 46A No. 2 335 - 360

MURRAY, M. P. (1967)

Gait as a Total Pattern of Movement  
Am. J. Phys. Med. 46 No. 1, 290 - 331

PAUL, J. P. (1965)

Bioengineering Studies of the Forces Transmitted by Joints.  
Part 2. Engineering Analysis.  
In: Biomechanics and Related Bio-Engineering Topics.  
Ed. R.M. Kenedi, Pergamon Press, Oxford. 493p

PAUL, J. P. (1967)

Forces at the Human Hip Joint  
PhD Thesis University of Glasgow

PAUL, J.P. (1970)

The Effect of Walking Speed on the Force Actions Transmitted at  
the hip and Knee Joints.  
Proc. Roy. Soc. Med. LXII 200 - 202

PAUL, J. P. (1971)

Comparison of EMG Signals from Leg Muscles with the Corresponding  
Force Actions from Walkpath Measurements.  
Proc. Conf. on Human Locomotor Engineering. 13 - 25 Inst. Mech.  
Engrs. London

RYDELL, N. (1966)

Forces Acting on the Femoral Head - Prosthesis  
Univ. of Goteborg. Tryckery AB Litotyp. 132p

SAUNDERS, J. B. de C., INMAN, V. T and EBERHARDT, H. D. (1953)

The Major Determinants in Normal and Pathological Gait  
J. Bone and Joint Surgery 35A July, 543 - 558

UNIVERSITY OF CALIFORNIA (1947)

Prosthetic Devices Research Project.

"Fundamental Studies of Human Locomotion and other Information  
Relating to Design of Artificial Limbs". 2 Volumes

WAGNER, E. M. and CATRAINS, J. G. (1954)

New Developments in Lower Extremity Protheses.

Ch. 17 in Klopsteg and Wilson (1954) Human Limbs and their  
Substitutes. McGraw Hill, New York

WILKIE, D. R. (1950)

The Relation Between Force and Velocity in Human Muscle  
J. Physiol. 110 249 - 280

## APPENDICES

- 8.1 Computer Program
- 8.2 Intersegmental Moments for all Subjects  
and patients

## 8.1 Computer Program

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C
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C
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PROGRAM FIFTH(INPUT,OUTPUT,TAPE8,TAPE5=INPUT,TAPE6=OUTPUT)
DIMENSION IR(8),IS(8),XUXU(10),ZUZU(10),IIR(13),IIS(13),
1 XAXA(10),SSX(8),SSY(8),SSFZ(8)
DIMENSION X1(1380),Y1(1380),Z1(1630),Y2(1630)
DIMENSION X1A(8,125),Y1A(8,125),Y2A(10,125),Z1A(10,125)
DIMENSION TXL(3),T(3,3),TD(3,3),VAD(3),EKD(3),HJC(3,125)
DIMENSION XIANTES(10,125),YIANTES(10,125),X(11,125),Y(11,125),
1 Z(11,125)
DIMENSION VLA(3),VLA5TT(3),VLK(3),VLK5TT(3)
DIMENSION VH7C(3),VH7(3),TP(3,3),FT(3,3)
DIMENSION ANKVEL(3,61),ANKACC(3,61),KNEVEL(3,61),KNEACC(3,61),
1 HIPVEL(3,61),HIPACC(3,61),HIPANX(61),DELHOX(61),KNEANX(61),
2 HIPANZ(61),DELHOZ(61),KNEANZ(61),FOTANG(61),FOTVEL(61),
3 FOTACC(61),SHOANG(61),
4 SOMEGX(61),SOMEGZ(61),SALFAX(61),SALFAZ(61),TOMEGX(61),
5 TOMEGZ(61),TALFAX(61),TALFAZ(61),TETAZ(61)
DIMENSION XCGSHA(61),YCGSHA(61),ZCGSHA(61),SXGDD(61),SYGDD(61),
1 SZGDD(61),XCGTHI(61),YCGTHI(61),ZCGTHI(61),TXGDD(61),
2 TYGDD(61),TZGDD(61),XE5T(61),ZEST(61),EMNEEX(61),
3 EMNEEZ(61),EMHIPX(61),EMHIPZ(61),ANKMOX(61),ANKMOZ(61),
4 TQA(61),FXK(61),FYK(61),FZK(61),KNEEMX(61),KNEEMZ(61),
5 FXH(61),FYH(61),FZH(61),HIPMZ(61),HIPMX(61),TQK(61),
6 TOH(61)
DIMENSION FX(61),FY(61),FZ(61),MX(61),MY(61),MZ(61)
DIMENSION FHOLD(3000),TOT060(61)
DIMENSION YY(125),DFUN(61),DDFUN(61)
DIMENSION IDENT(7),ANGDEG(10)
COMMON /ABTFLG/ ABTFL(2)
COMMON /BLOCK1/ SSX(10),SSY(10),SSFZ(10)
COMMON /BLOCK2/ AJC(3,125),KJC(3,125),SXL(3)
COMMON /FHLDBK/ FHOLD
COMMON /LADO/ LEFSID,ISIDE,JSIDE,LSIDE,JBIDE,LBIDE
COMMON /TRY2/ Y2A,Y2
COMMON XIANTES,YIANTES,X1A,Y1A,Z1A,X,Y,Z,MX,XL,ZL
EQUIVALENCE (FHOLD(1),FX(1)),(FHOLD(62),FY(1)),(FHOLD(123),FZ(1))
EQUIVALENCE (FHOLD(184),MX(1)),(FHOLD(245),MY(1)),(FHOLD(306),
1 MZ(1))
INTEGER SFRAME,FFRAME
REAL IIR,IIS,IR,IS,KNEANX,KNEANZ,KNEEMX,KNEEMZ,KJC,KNEVEL
REAL KNEACC,LENGTH,MX,MY,MZ
LOGICAL ABTFL,FUL,LEFSID,NEWMAN,OIDENT
DATA DEGREE / 57.29578 /
DATA HALFPI / 1.570796 /
DATA IFUL/JHFUL/
DATA LAD02 / 3HKLI /
C
C READ IN CONSTANTS FOR PATIENT, AND CALCULATE VECTOR LOCATING HIP-
C JOINT CENTRES FROM DISTANCE BETWEEN A.S.I.SPINES.
C
100 ABTFL(1)=.FALSE.
CALL INPCON(BH,BM,D67,D78,DB6,IDENT(1),NEXTID)
WRITE(6,110)IDENT(1)
110 FORMAT(35HIPATIENT CONSTANTS READ FROM DECK ,A9,1H.)
VH7(1)=D86*0.1829
VH7(2)=D86*0.3049
VH7(3)=D86*0.1219
C
C READ IN STATIC DATA FROM FILM OBSERVATIONS.
C
CALL INPKIN (IR,IS,NCHECK,IDENT(2),NEXTID)
WRITE(6,120)IDENT(2)
120 FORMAT(35H0STATIC SIDE DATA READ FROM DECK ,A9,1H.)
IF(NCHECK.NE.8)CALL ABORT(1)
CALL INPKIN (IIR,IIS,NCHECK,IDENT(3),NEXTID)
WRITE(6,130)IDENT(3)
130 FORMAT(35H0STATIC FRONT DATA READ FROM DECK ,A9,1H.)
IF(NCHECK.NE.13)CALL ABORT(1)
C
C READ IN AND PROCESS FORCE-PLATE DATA, ABORT IF ERROR FLAG SET.

```

```

C
140 ABTFL(2)=.FALSE.
    CALL INFPD(FHOLD,NFPSET,IDENT(4),NEXTID,BM,EVNTPT)
    WRITE(6,144) IDENT(4),EVNTPT
144 FORMAT (35H0FORCE PLATE DATA READ FROM DECK ,A9.1H.,10X,
1 16HEVENT POINTER =,F8.2)
    IF (NFPSET.LE.0) CALL ABORT(2)
C
C READ FRAME NUMBERS FOR EVENTS, AND FRAME COUNT.
C
    CALL INPKMK(LHS,LTO,NH,NTO,NF,IDENT(5),NEXTID)
    WRITE(6,150) IDENT(5)
150 FORMAT(35H0FRAME NUMBERS READ FROM DECK ,A9.1H.)
C
C READ KINEMATIC DATA. >FRAME IS THE NUMBER OF POINTS PER FRAME IN
C SIDE VIEW, INCLUDING THE FIRST THREE POINTS OF THE GRID.
C >FFRAME IS THE SAME FOR THE FRONT VIEW. FOR EACH VIEW THE
C NUMBER OF FRAMES IS CHECKED AGAINST NF.
C
    CALL INPKIN (X1,Y1,N>IDE,IDENT(6),NEXTID)
    WRITE(6,160) IDENT(6)
160 FORMAT(35H0DYNAMIC SIDE DATA READ FROM DECK ,A9.1H.)
    >FRAME=11
    IF ((NF>>FRAME).NE.N>IDE) CALL ABORT(2)
    CALL INPKIN(Z1,Y2,NFRONT,IDENT(7),NEXTID)
    WRITE(6,170) IDENT(7)
170 FORMAT(35H0DYNAMIC FRONT DATA READ FROM DECK ,A9.1H.)
    >FFRAME=13
    IF ((NF>>FFRAME).NE.NFRONT) CALL ABORT(2)
    IF (ABTFL(1).OR.ABTFL(2)) GOTO 890
C
C DETERMINE WHETHER LEFT OR RIGHT, AND SET SIDE-DEPENDENT VALUES AND
C POINTERS.
C
    FUL=0 IDENT(IDENT(6),6,8,IFUL)
    IF (0 IDENT(IDENT(2),3,5,LA002)) GOTO 180
    STEP=0.0
    IF (0 IDENT(IDENT(6),9,9,1H1)) >STEP=0.1*BH
C
    LEF>ID=.FALSE.
    CONST=432.0
    DK7=D67
    IBIDE=2
    JBIDE=1
    LBIDE=2
    KKA=1
    I>IDE=0
    J>IDE=1
    KA=1
    KB=4
    KC=2
    K>IDE=4
    L>IDE=2
    M>IDE=7
    XCONST=0.000322
    YCONST=0.000292
    XL=8.800
    ZL=5.25
    GOTO 190
C
180 LEF>ID=.TRUE.
    CONST=383.0
    DK7=D78
    IBIDE=5
    JBIDE=10
    LBIDE=9
    KKA=9
    I>IDE=5
    J>IDE=6
    KC=10
    L>IDE=7
    KA=7
    KB=10
    K>IDE=7
    M>IDE=2
    XCONST=-0.000329
    YCONST=0.000332
    XL=8.800
    ZL=-3.95
C
C CALCULATE FIXED PELVIC ANGLE, AND SET CAMERA HEIGHT.
C
190 ANGS=ATAN(SQRT(4.0*DK7*DK7-D86*D86)/D86)

```

```

FIFTH700
FIFTH710
FIFTH720
FIFTH730
FIFTH740
FIFTH750
FIFTH760
FIFTH770
FIFTH780
FIFTH790
FIFTH800
FIFTH810
FIFTH820
FIFTH830
FIFTH840
FIFTH850
FIFTH860
FIFTH870
FIFTH880
FIFTH890
FIFTH900
FIFTH910
FIFTH920
FIFTH930
FIFTH940
FIFTH950
FIFTH960
FIFTH970
FIFTH980
FIFTH990
FIFT1000
FIFT1010
FIFT1020
FIFT1030
FIFT1040
FIFT1050
FIFT1060
FIFT1070
FIFT1080
FIFT1090
FIFT1100
FIFT1110
FIFT1120
FIFT1130
FIFT1140
FIFT1150
FIFT1160
FIFT1170
FIFT1180
FIFT1190
FIFT1200
FIFT1210
FIFT1220
FIFT1230
FIFT1240
FIFT1250
FIFT1260
FIFT1270
FIFT1280
FIFT1290
FIFT1300
FIFT1310
FIFT1320
FIFT1330
FIFT1340
FIFT1350
FIFT1360
FIFT1370
FIFT1380
FIFT1390
FIFT1400
FIFT1410
FIFT1420
FIFT1430
FIFT1440
FIFT1450
FIFT1460
FIFT1470
FIFT1480
FIFT1490
FIFT1500
FIFT1510
FIFT1520

```

```

ANGDC=ANGS*57.29577951
HX=0.86
HZ=HX
C
CALL REF(IR(1),IR(2),IR(3),IS(1),IS(2),IS(3),X0,Z0,CD)
Z0=Z0-CONST
DO 200 I=4,8
CALL CHANGE(X0,Z0,CD,IR(I),IS(I),XU,ZU)
ZUZU(I-3)=ZU*YCONST
XUXU(I-3)=XU*XCONST
200 CONTINUE
ANKLEX=XUXU(1)
ANKLEY=ZUZU(1)
AKNEEX=XUXU(2)
AKNEEY=ZUZU(2)
DO 210 I=3,5
II=I+ISIDE-2
SSSX(II)=XUXU(I)
SSSY(II)=ZUZU(I)
210 CONTINUE
C
C . . . AND THE SAME FOR THE FRONT CAMERA.
C
CALL REF(IIR(1),IIR(2),IIR(3),IIS(1),IIS(2),IIS(3),X0,Z0,CD)
Z0=Z0-375.0
DO 220 I=4,13
CALL CHANGE(X0,Z0,CD,IIR(I),IIS(I),XU,ZU)
XAXA(I-3)=-XU*0.000322
220 CONTINUE
ANKLEZ=XAXA(KKA)
AKNEEZ=XAXA(KC)
DO 230 I=1,3
JJ=I+ISIDE
J=I+IISIDE
SSFZ(J)=XAXA(JJ)
230 CONTINUE
C
C IN THE NEXT STAGE THE FIRST THREE POINTS OF EACH FRAME WILL BE USED
C TO CORRECT THE COORDINATES FOR RANDOM DISPLACEMENTS OF THE FRAME.
C
C
C
I1A=1
I1B=I1A
DO 250 I=1,NISIDE,SFRAME
CALL REF(X1(I),X1(I+1),X1(I+2),Y1(I),Y1(I+1),Y1(I+2),X0,Z0,CD)
Z0=Z0-CONST
K=I+3
N=I+SFRAME-1
DO 240 M=K,N
CALL CHANGE(X0,Z0,CD,X1(M),Y1(M),XU,ZU)
C
C X1A(M) AND Y1A(M) REPRESENT THE VALUES OF X AND Y BEFORE PARALLAX
C CORRECTION.
C
C THE NEXT STAGE IS TO CONVERT VANGUARD UNITS TO METRES.
C
C
X1A(I1A,I1B)=XU*XCONST
Y1A(I1A,I1B)=ZU*YCONST
I1A=I1A+1
IF(I1A.LT.9)GOTO 240
I1A=1
I1B=I1B+1
240 CONTINUE
250 CONTINUE
I1A=1
I1B=I1A
DO 270 I=1,NFRONT,FFRAME
CALL REF(Z1(I),Z1(I+1),Z1(I+2),Y2(I),Y2(I+1),Y2(I+2),X0,Z0,CD)
Z0=Z0-375.0
K=I+3
N=I+FFRAME-1
DO 260 M=K,N
CALL CHANGE(X0,Z0,CD,Z1(M),Y2(M),XU,ZU)
C
C Y2 IS NOT USED FURTHER EXCEPT TO PRODUCE THE TABULATED COMPARISONS
C OF SUBROUTINE CHECKY. Z1A IS THE VALUE OF Z BEFORE PARALLAX
C CORRECTION.
C
C
Z1A(I1A,I1B)=-XU*0.000322
Y2A(I1A,I1B)=ZU*0.000322
I1A=I1A+1
IF(I1A.LT.11) GOTO 260
I1A=1

```

FIFT1530  
FIFT1540  
FIFT1550  
FIFT1560  
FIFT1570  
FIFT1580  
FIFT1590  
FIFT1600  
FIFT1610  
FIFT1620  
FIFT1630  
FIFT1640  
FIFT1650  
FIFT1660  
FIFT1670  
FIFT1680  
FIFT1690  
FIFT1700  
FIFT1710  
FIFT1720  
FIFT1730  
FIFT1740  
FIFT1750  
FIFT1760  
FIFT1770  
FIFT1780  
FIFT1790  
FIFT1800  
FIFT1810  
FIFT1820  
FIFT1830  
FIFT1840  
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FIFT2090  
FIFT2100  
FIFT2110  
FIFT2120  
FIFT2130  
FIFT2140  
FIFT2150  
FIFT2160  
FIFT2170  
FIFT2180  
FIFT2190  
FIFT2200  
FIFT2210  
FIFT2220  
FIFT2230  
FIFT2240  
FIFT2250  
FIFT2260  
FIFT2270  
FIFT2280  
FIFT2290  
FIFT2300  
FIFT2310  
FIFT2320  
FIFT2330  
FIFT2340  
FIFT2350

```

      I18=I18+1
260 CONTINUE
270 CONTINUE
C
C IN THE NEXT STEP THE COORDINATES ARE STORED IN THE ARRAYS XIANTE,
C YIANTE WITH A COMMON RELATIONSHIP BETWEEN SUBSCRIPTS AND THE
C TARGETS ON THE PATIENT. THE THREE INITIAL GRID POINTS ON EACH
C FRAME ARE ELIMINATED.
C
      DO 290 K=5,SFRAME
      DO 280 I=1,NF
      XIANTE((K-4),I)=X1A((K-2),I)
      YIANTE((K-4),I)=Y1A((K-2),I)
280 CONTINUE
290 CONTINUE
      IF(.NOT.LEFSID)GOTO 320
      DO 310 K=1,4
      DO 300 I=1,NF
      XIANTE((K+6),I)=XIANTE(K,I)
      YIANTE((K+6),I)=YIANTE(K,I)
300 CONTINUE
310 CONTINUE
      CALL CHECKY(YIANTE,10,Y2A,10,NF,KA,KB)
C
C SUBROUTINES PARALA AND PIRILI CORRECT FOR PARALLAX, RESPECTIVELY FOR
C THE KINEMATIC AND STATIC COORDINATES. XL, ZL AND HX ARE THE
C CAMERA DISTANCES (FRONT, SIDE, AND HEIGHT RESPECTIVELY). IT IS
C IMPORTANT TO NOTE THAT FOR THE LEFT CAMERA THE VALUE OF ZL IS
C NEGATIVE, TO KEEP THE CORRECT SIGN IN THE EQUATIONS.
C
320 CALL PARALA(KA,KB,NF)
      CALL CHECKY(Y,11,Y2,10,NF,KA,KB)
      CALL PIRILI(SSX(I>SIDE+1),SSY(I>SIDE+1),SSFZ(I>SIDE+1),XL,ZL,HX)
C
C AKNEE(X,Y,Z) AND ANKLE(X,Y,Z) ARE THE CENTRES OF THE JOINTS
C TAKEN FROM THE STATIC SHOT. VLA(X,Y,Z) AND VLK(X,Y,Z) ARE THOSE
C AFTER PARALLAX CORRECTION. VLA(J) AND VLK(J) ARE THE VECTORS
C FROM MARKER 1 TO THE CENTRE OF THE ANKLE AND KNEE JOINTS.
C
C SUBROUTINE POROLO CORRECTS PARALLAX FOR THE JOINT CENTRES.
C
      CALL POROLO(VLAX,VLAY,VLAZ,ANKLEX,ANKLEY,ANKLEZ,ZL,XL,HX)
      CALL POROLO(VLKX,VLKY,VLKZ,AKNEEX,AKNEEY,AKNEEZ,ZL,XL,HX)
      VLA(1)=VLAX-SSX(JSIDE)
      VLA(2)=VLAY-SSY(JSIDE)
      VLA(3)=VLAZ-SSFZ(JSIDE)
      VLK(1)=VLKX-SSX(JSIDE)
      VLK(2)=VLKY-SSY(JSIDE)
      VLK(3)=VLKZ-SSFZ(JSIDE)
C
C T IS THE MATRIX WHICH RELATES THE GROUND AND SHANK SYSTEMS.
C
      CALL TSTAT(T)
C
C THE VECTOR TXL DEFINES THE FORWARD DIRECTION OF THE SHANK.
C
      TXL(1)=T(1,1)
      TXL(2)=T(2,1)
      TXL(3)=T(3,1)
C
C VLA&STAT AND VLK&STAT REPRESENT VLA AND VLK AT STATIC CONFIGURATION
C IN THE SHANK SYSTEM.
C
      CALL AMULT(T,VLA,VLA&STAT)
      CALL AMULT(T,VLK,VLK&STAT)
C
C CALCULATE THE COORDINATES OF THE KNEE AND ANKLE JOINT CENTRES.
C
      DO 340 I=1,NF
C
C THE SUBROUTINE THAT WILL CALCULATE T DYNAMICALLY.
C
      CALL T&MAT(I,T,X,Y,Z)
C
C THE ARRAY TD IS T TRANSPOSED (TO THE GROUND SYSTEM).
C
      DO 330 J=1,3
      TD(J,J)=T(J,J)
330 CONTINUE
      TD(1,2)=T(2,1)
      TD(1,3)=T(3,1)
      TD(2,1)=T(1,2)
      TD(2,3)=T(3,2)

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FIFT2400
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FIFT3000
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FIFT3100
FIFT3110
FIFT3120
FIFT3130
FIFT3140
FIFT3150
FIFT3160
FIFT3170
FIFT3180

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      TD(3,1)=T(1,3)
      TD(3,2)=T(2,3)
      CALL AMULT(TD, TXL, >XL)
      CALL AMULT(TD, VLASTT, VAD)
      CALL AMULT(TD, VLKSTT, EKD)
      AJC(1,1)=VAD(1)+X(JBIDE,I)
      AJC(2,1)=VAD(2)+Y(JBIDE,I)
      AJC(3,1)=VAD(3)+Z(JBIDE,I)
      KJC(1,1)=EKD(1)+X(JBIDE,I)
      KJC(2,1)=EKD(2)+Y(JBIDE,I)
      KJC(3,1)=EKD(3)+Z(JBIDE,I)
      CALL FMAT(I,FT)
C
C CALCULATION OF THE COORDINATES OF THE TAIL MARKER (M).
C
      AQUAD=(X1A(M>IDE,I)**2+(HZ-Y1A(M>IDE,I))**2)/(ZL*ZL)+1.
      BQUAD=2.0*((X1A(M>IDE,I)*(X(K>IDE,I)-X1A(M>IDE,I))
1      (Y(K>IDE,I)-Y1A(M>IDE,I))*(Y1A(M>IDE,I)-HZ))/ZL
2      -Z(K>IDE,I))
      CQUAD=-DK7*DK7*(X(K>IDE,I)-X1A(M>IDE,I))**2+
1      (Y(K>IDE,I)-Y1A(M>IDE,I))**2+Z(K>IDE,I)**2
C
C NOW CALCULATE THE ROOTS.
C
      CALL ROOT>(RX1,RX2,AQUAD,BQUAD,CQUAD)
C
C X(11,I), Y(11,I), Z(11,I) ARE THE FINAL COORDINATES OF THE
C TAIL MARKER.
C
      Z(11,I)=RX1
      IF(.NOT.LEF>ID)RX1=-RX1
      X(11,I)=X1A(M>IDE,I)+RX1*X1A(M>IDE,I)/ZL
      Y(11,I)=Y1A(M>IDE,I)+RX1*(Y1A(M>IDE,I)-HZ)/ZL
C
C DYNAMIC ANGLES - ANGDI IS IN RADIANS AND AGDC IS IN DEGREES.
C
      ANGDI=ACOS(ABS((Z(K>IDE,I)-Z(11,I))/DK7))
      ANGDC=ANGDI*57.29577951
C
C NOTE THAT TP IS THE PELVIS ROTATION MATRIX.
C
      TP(1,1)=COS(ANGDI-ANGD)
      TP(1,2)=0.0
      TP(1,3)=SIN(ANGDI-ANGD)
      TP(2,1)=0.0
      TP(2,2)=1.0
      TP(2,3)=0.0
      TP(3,1)=-SIN(ANGDI-ANGD)
      TP(3,2)=0.0
      TP(3,3)=COS(ANGDI-ANGD)
      CALL AMULT(TP,VH7,VH7C)
C
C MULTIPLY THE VECTOR VH7 BY THE MATRIX TP TO GIVE VH7C, THE VECTOR
C LOCATING THE HIP JOINT CENTRE FROM THE A.S.I.S. MARKER AT TIME T.
C
      IF(LEF>ID)VH7C(3)=-VH7C(3)
      HJC(1,I)=X(K>IDE,I)-VH7C(1)
      HJC(2,I)=Y(K>IDE,I)-VH7C(2)
      HJC(3,I)=Z(K>IDE,I)-VH7C(3)
340 CONTINUE
      CALL TABLE1(IDENT(6),AJC,KJC,HJC,NF)
C
      IF (LEF>ID) GOTO 410
      J=1
      K=2
      YF=0.037*STEP
      CX1=.30
      CZ1=.20
      GOTO 420
410 J=8
      K=7
      YF=0.037
      CX1=-.30
      CZ1=-.20
420 CONTINUE
      ND=NF
      NC=61
C
      IF (LEF>ID) GOTO 422
      IF (FUL) GOTO 421
      NSYNCH=NEARST(EVNTPT+1.5)-NT0
      GOTO 424
421 NSYNCH=NEARST(EVNTPT+1.5)-NH>

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 FIFTJ950  
 FIFTJ960  
 FIFTJ970  
 FIFTJ980  
 FIFTJ990  
 FIFT4000  
 FIFT4010

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GOTO 424
422 IF (FUL) GOTO 423
    NSYNCH=NEARST(EVNTPT*1.5)-LMS
    GOTO 424
423 NSYNCH=NEARST(EVNTPT*1.5)-LTO
424 CONTINUE
C
DO 430 I=1,ND
430 SHOANG(I)=ATAN2((Y1A(J,I)-HJC(2,I)),(X1A(J,I)-HJC(1,I)))
    CALL SMOOTH(50HSHOULDER ANGLE SAGITTAL PLANE***
1 1,ND,SHOANG(I),1,NC,SHOANG(I),DFUN,DDFUN,0)
    DO 440 I=1,NC
440 SHOANG(I)=SHOANG(I)*DEGREE
    CALL SMOOTH(50HSHOULDER JOINT CENTRE X COMPONENT***
1 3,ND,AJC(1,1),3,NC,AJC(1,1),ANKVEL(1,1),ANKACC(1,1),0)
    CALL SMOOTH(50HSHOULDER JOINT CENTRE Y COMPONENT***
1 3,ND,AJC(2,1),3,NC,AJC(2,1),ANKVEL(2,1),ANKACC(2,1),0)
    CALL SMOOTH(50HSHOULDER JOINT CENTRE Z COMPONENT***
1 3,ND,AJC(3,1),3,NC,AJC(3,1),ANKVEL(3,1),ANKACC(3,1),0)
C
CALL SMOOTH(50HKNEE JOINT CENTRE X COMPONENT***
1 3,ND,KJC(1,1),3,NC,KJC(1,1),KNEVEL(1,1),KNEACC(1,1),0)
CALL SMOOTH(50HKNEE JOINT CENTRE Y COMPONENT***
1 3,ND,KJC(2,1),3,NC,KJC(2,1),KNEVEL(2,1),KNEACC(2,1),0)
CALL SMOOTH(50HKNEE JOINT CENTRE Z COMPONENT***
1 3,ND,KJC(3,1),3,NC,KJC(3,1),KNEVEL(3,1),KNEACC(3,1),0)
C
CALL SMOOTH(50HHIP JOINT CENTRE X COMPONENT***
1 3,ND,HJC(1,1),3,NC,HJC(1,1),HIPVEL(1,1),HIPACC(1,1),0)
CALL SMOOTH(50HHIP JOINT CENTRE Y COMPONENT***
1 3,ND,HJC(2,1),3,NC,HJC(2,1),HIPVEL(2,1),HIPACC(2,1),0)
CALL SMOOTH(50HHIP JOINT CENTRE Z COMPONENT***
1 3,ND,HJC(3,1),3,NC,HJC(3,1),HIPVEL(3,1),HIPACC(3,1),0)
CALL SMOOTH(50HFORCE-PLATE DATA FX***
1 1,ND,FHOLD(NSYNCH),1,NC,FHOLD(1),HIPMX(1),HIPMZ(1),10)
CALL SMOOTH(50HFORCE-PLATE DATA FY ***
1 1,ND,FHOLD(NSYNCH+NFP*ET),1,NC,FHOLD(62),HIPMX(1),HIPMZ(1),10)
CALL SMOOTH(50HFORCE-PLATE DATA FZ ***
1 1,ND,FHOLD(NSYNCH+NFP*ET*2),1,NC,FHOLD(123),HIPMX(1),HIPMZ(1),
2 10)
CALL SMOOTH(50HFORCE-PLATE DATA MX ***
1 1,ND,FHOLD(NSYNCH+NFP*ET*3),1,NC,FHOLD(184),HIPMX(1),HIPMZ(1),
2 10)
CALL SMOOTH(50HFORCE-PLATE DATA MY ***
1 1,ND,FHOLD(NSYNCH+NFP*ET*4),1,NC,FHOLD(245),HIPMX(1),HIPMZ(1),
2 10)
CALL SMOOTH(50HFORCE-PLATE DATA MZ ***
1 1,ND,FHOLD(NSYNCH+NFP*ET*5),1,NC,FHOLD(306),HIPMX(1),HIPMZ(1),
2 10)
DO 510 I=1,NC
HIPANX(I)=ATAN2((KJC(1,I)-HJC(1,I)),(HJC(2,I)-KJC(2,I)))
OELHOX(I)=ATAN2((AJC(1,I)-KJC(1,I)),(KJC(2,I)-AJC(2,I)))
KNEANX(I)=HIPANX(I)-OELHOX(I)
HIPANZ(I)=ATAN2((KJC(3,I)-HJC(3,I)),(HJC(2,I)-KJC(2,I)))
OELHOZ(I)=ATAN2((AJC(3,I)-KJC(3,I)),(KJC(2,I)-AJC(2,I)))
KNEANZ(I)=HIPANZ(I)-OELHOZ(I)
NZPRNT=0
WRITE(6,500)
ANGDEG(1)=HIPANX(I)*DEGREE
ANGDEG(2)=OELHOX(I)*DEGREE
ANGDEG(3)=KNEANX(I)*DEGREE
ANGDEG(4)=HIPANZ(I)*DEGREE
ANGDEG(5)=OELHOZ(I)*DEGREE
ANGDEG(6)=KNEANZ(I)*DEGREE
WRITE(6,500)I,(ANGDEG(IAD),IAD=1,6)
500 FORMAT(1H ,14,10F12.2)
510 CONTINUE
C
C THE FOOT ANGLE IS MEASURED WITH RESPECT TO THE HORIZONTAL. IT IS
C IMPORTANT TO NOTE THAT THE SHANK ANGLE (WITH RESPECT TO THE
C VERTICAL) HAS TO BE ADDED.
C
C CALL SUBROUTINE REGR FOR THE FOOT IN ORDER TO PRODUCE THE SAME NUMBER
C OF OUTPUT VALUES.
C
DO 520 I=1,NF
520 FOTANG(I)=ATAN2((Y1A(J,I)-Y1A(K,I)),(X1A(J,I)-X1A(K,I)))
    CALL SMOOTH(50HFOOT ANGLE SAGITTAL PLANE***
1 1,ND,FOTANG(I),1,NC,FOTANG(I),FOTVEL(1),FOTACC(1),0)
    DO 530 I=1,NC
530 FOTANG(I)=OELHOX(I)*HALFPI-FOTANG(I)
530 CONTINUE
C

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C CALCULATION OF THE TRUNK ANGLE.
C
C ANTHROPOMETRY.  BM = BODY MASS,  TM = THIGH MASS,  SFM = SHANK AND
C   FOOT MASS.  THE LIMB SEGMENT MASSES ARE OBTAINED IN PROPORTION
C   TO BODY MASS.
C
  SFL=BM*.285
  TL=BM*.530-SFL
  TGRAVT=.427*TL
  SGRAVT=.467*SFL
  TM=.0946*BM
  SFM=.0590*BM
C
C TK = THIGH RADIUS OF GYRATION.  SFK = RADIUS OF GYRATION FOR THE
C   SHANK AND FOOT.
C
  TK=.23*TL
  TINERT=TK*TK*TM
  SFK=.29*SFL
  SFINER=SFK*SFK*SFM
  WEIGSF=SFM*.981
  WEIGT=TM*.81
C
C VELOCITY AND ACCELERATION AT THE SHANK CENTRE OF GRAVITY.
C
  DO 600 I=1,NC
  SVX=ANKVEL(1,I)-KNEVEL(1,I)
  SVY=ANKVEL(2,I)-KNEVEL(2,I)
  SVZ=ANKVEL(3,I)-KNEVEL(3,I)
  SAX=ANKACC(1,I)-KNEACC(1,I)
  SAY=ANKACC(2,I)-KNEACC(2,I)
  SAZ=ANKACC(3,I)-KNEACC(3,I)
  SLONG=1.0/SFL
  SRATIO=SLONG*SGRAVT
  SCOSX=CO5(OELHOX(I))
  SCOSZ=CO5(OELHOZ(I))
  SSENX=5IN(OELHOX(I))
  SSENZ=5IN(OELHOZ(I))
  XCOMS=SGRAVT*SSENX
  YCOMS=SGRAVT*SCOSX
  ZCOMS=SGRAVT*SSENZ
  XCGSHA(I)=KJC(1,I)+XCOMS
  YCGSHA(I)=KJC(2,I)-YCOMS
  ZCGSHA(I)=KJC(3,I)+ZCOMS
  STVX=SVX*SCOSX
  STVY=SVY*SSENX
  STVZ=SVZ*SCOSZ
  STVYZ=SVY*SSENZ
  STVINX=STVX+STVY
  STVINZ=STVZ+STVYZ
  SOMEGX(I)=STVINX*SLONG
  SOMEGZ(I)=STVINZ*SLONG
  SACCX=5AX*SCOSX
  SACCY=5AY*SSENX
  SACCZ=5AZ*SCOSZ
  SACCYZ=5AY*SSENZ
  SACINX=SACCX+SACCY
  SACINZ=SACCZ+SACCYZ
  SALFAX(I)=SACINX*SLONG
  SALFAZ(I)=SACINZ*SLONG
  SXGDD(I)=KNEACC(1,I)+SRATIO*5AX
  SYGDD(I)=KNEACC(2,I)+SRATIO*5AY
  SZGDD(I)=KNEACC(3,I)+SRATIO*5AZ
  TVX=KNEVEL(1,I)-HIPVEL(1,I)
  TVY=KNEVEL(2,I)-HIPVEL(2,I)
  TVZ=KNEVEL(3,I)-HIPVEL(3,I)
  TAX=KNEACC(1,I)-HIPACC(1,I)
  TAY=KNEACC(2,I)-HIPACC(2,I)
  TAZ=KNEACC(3,I)-HIPACC(3,I)
  TLONG=1.0/TL
  TRATIO=TLONG*TGRAVT
  TCO5X=CO5(HIPANX(I))
  TCO5Z=CO5(HIPANZ(I))
  TSENX=5IN(HIPANX(I))
  TSENZ=5IN(HIPANZ(I))
  XCOMT=TGRAVT*TSENX
  YCOMT=TGRAVT*TCO5X
  ZCOMT=TGRAVT*TSENZ
  XCGTHI(I)=HJC(1,I)+XCOMT
  YCGTHI(I)=HJC(2,I)-YCOMT
  ZCGTHI(I)=HJC(3,I)+ZCOMT
  TTVX=TVX*TCO5X
  TTVY=TVY*TSENX

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TTVZ=TVZ*TCOSZ
TTVYZ=TVY*TSENZ
TTVINX=TTVX*TTVY
TTVINZ=TTVZ*TTVY
TOMEGX(I)=TTVINX*TLONG
TOMEGZ(I)=TTVINZ*TLONG
TACCX=TAX*TCOSX
TACCY=TAY*TSENZ
TACCZ=TAZ*TCOSZ
TACCYZ=TAY*TSENZ
TACINX=TACCX*TACCY
TACINZ=TACCZ*TACCY
TALFAX(I)=TACINX*TLONG
TALFAZ(I)=TACINZ*TLONG
TXGDD(I)=HIPACC(1,I)*TRATIO*TAX
TYGDD(I)=HIPACC(2,I)*TRATIO*TAY
TZGDD(I)=HIPACC(3,I)*TRATIO*TAZ
600 CONTINUE
ANF=NF
RHS=NHS
RTO=NTO
ALHS=LHS
ALTO=LTO
SA=1./(ANF-1.)
NHS=INT(1.5+60.*(RHS-1.5)*SA)
RTO=INT(1.5+60.*(RTO-1.5)*SA)
LHS=INT(1.5+60.*(ALHS-1.5)*SA)
LTO=INT(1.5+60.*(ALTO-1.5)*SA)
DO 700 I=1,NC
XPROV=(MZ(I)*FX(I)*YF)/FY(I)
ZPROV=(FZ(I)*YF-MX(I))/FY(I)
XEST(I)=XPROV*CX
ZEZT(I)=ZPROV*CZ
700 CONTINUE
DO 710 I=1,NC
TOTO60(I)=FLOAT(I-1)
EMNEEX(I)=SFINER*SALFAX(I)
EMNEEZ(I)=SFINER*SALFAZ(I)
EMHIPX(I)=TINERT*TALFAX(I)
EMHIPZ(I)=TINERT*TALFAZ(I)
710 CONTINUE
DO 770 I=1,NC
C
C I IS THE NUMBER OF FRAMES FOR THE STANCE PHASE (FORCE PLATE).
C
IF (LEFSID) GOTO 730
IF (FUL) GOTO 720
IF (I.LE.NHS) GOTO 740
GOTO 750
720 IF (I.GE.NHS) GOTO 740
GOTO 750
730 IF (FUL) GOTO 734
IF (I.GE.LHS) GOTO 740
GOTO 750
734 IF (I.GE.LTO) GOTO 750
C
C ANKLE MOMENTS.
C
740 CONTINUE
E=FY(I)*(XEST(I)-AJC(1,I))
EE=FY(I)*(ZEZT(I)-AJC(3,I))
ANKMOZ(I)=FX(I)*AJC(2,I)*E
ANKMOX(I)=FZ(I)*AJC(2,I)*EE
TOA(I)=FX(I)*(AJC(3,I)-ZEZT(I))+FZ(I)*(AJC(1,I)-XEST(I))*
1 MY(I)
C
C KNEE MOMENTS.
C
FXK(I)=FX(I)+SFH*TXGDD(I)
FYK(I)=WEIGSF*FY(I)+SFH*TYGDD(I)
FZK(I)=FZ(I)+SFH*TZGDD(I)
BB=FY(I)*(AJC(2,I)-YCGSHA(I))
BBB=FY(I)*(ZCGSHA(I)-AJC(1,I))
AA=FX(I)*(AJC(2,I)-YCGSHA(I))
AAAA=FY(I)*(XCGSHA(I)-AJC(1,I))
GOTO 760
750 E=0.0
EE=0.0
ANKMOZ(I)=0.0
ANKMOX(I)=0.0
TOA(I)=0.0
FXK(I)=SFH*TXGDD(I)
FYK(I)=WEIGSF*FY(I)+SFH*TYGDD(I)

```

FIFT5680  
FIFT5690  
FIFT5700  
FIFT5710  
FIFT5720  
FIFT5730  
FIFT5740  
FIFT5750  
FIFT5760  
FIFT5770  
FIFT5780  
FIFT5790  
FIFT5800  
FIFT5810  
FIFT5820  
FIFT5830  
FIFT5840  
FIFT5850  
FIFT5860  
FIFT5870  
FIFT5880  
FIFT5890  
FIFT5900  
FIFT5910  
FIFT5920  
FIFT5930  
FIFT5940  
FIFT5950  
FIFT5960  
FIFT5970  
FIFT5980  
FIFT5990  
FIFT6000  
FIFT6010  
FIFT6020  
FIFT6030  
FIFT6040  
FIFT6050  
FIFT6060  
FIFT6070  
FIFT6080  
FIFT6090  
FIFT6100  
FIFT6110  
FIFT6120  
FIFT6130  
FIFT6140  
FIFT6150  
FIFT6160  
FIFT6170  
FIFT6180  
FIFT6190  
FIFT6200  
FIFT6210  
FIFT6220  
FIFT6230  
FIFT6240  
FIFT6250  
FIFT6260  
FIFT6270  
FIFT6280  
FIFT6290  
FIFT6300  
FIFT6310  
FIFT6320  
FIFT6330  
FIFT6340  
FIFT6350  
FIFT6360  
FIFT6370  
FIFT6380  
FIFT6390  
FIFT6400  
FIFT6410  
FIFT6420  
FIFT6430  
FIFT6440  
FIFT6450  
FIFT6460  
FIFT6470  
FIFT6480  
FIFT6490  
FIFT6500

```

FZK(I)=5FM*SZGDD(I)
BB=0.0
BBBB=0.0
AA=0.0
AAAA=0.0
760 CONTINUE
A=FXK(I)*(YCGSHA(I)-KJC(2,I))
AAA=FYK(I)*(KJC(1,I)-XCGSHA(I))
KNEEMZ(I)=ANKMOZ(I)+EMNEEX(I)+A*AA+AAA+AAAA
B=FZK(I)*(YCGSHA(I)-KJC(2,I))
BBB=FYK(I)*(KJC(1,I)-ZCGSHA(I))
KNEEMX(I)=ANKMOX(I)+EMNEEZ(I)+B*BB+BBB+BBBB
C
C HIP MOMENTS.
C
FXH(I)=FXK(I)+TM*TXGDD(I)
FYH(I)=FYK(I)+WEIGT *TM*TYGDD(I)
FZH(I)=FZK(I)+TM*TZGDD(I)
C=FXH(I)*(YCGTHI(I)-HJC(2,I))
CC=FYH(I)*(HJC(1,I)-XCGTHI(I))
CCC=FXK(I)*(KJC(2,I)-YCGTHI(I))
CCCC=FYK(I)*(XCGTHI(I)-KJC(1,I))
HIPMZ(I)=KNEEMZ(I)+EMHIPX(I)+C+CC+CCC+CCCC
D=FZH(I)*(YCGTHI(I)-HJC(2,I))
DD=FYH(I)*(HJC(3,I)-ZCGTHI(I))
DDD=FZK(I)*(KJC(2,I)-YCGTHI(I))
DDDD=FYK(I)*(ZCGTHI(I)-KJC(3,I))
HIPMX(I)=KNEEMX(I)+EMHIPZ(I)+D+DD+DDD+DDDD
C
C KNEE.
C
TOK(I)=TQA(I)+FZK(I)*(XCGSHA(I)-KJC(1,I))+FZ(I)*(AJC(1,I)
1 -XCGSHA(I))+FXK(I)*(KJC(3,I)-ZCGSHA(I))+FX(I)*(ZCGSHA(I)
2 -AJC(3,I))
C
C HIP.
C
TQH(I)=TOK(I)+FZH(I)*(XCGTHI(I)-HJC(1,I))+FZK(I)*(KJC(1,I)
1 -XCGTHI(I))+FXH(I)*(HJC(3,I)-ZCGTHI(I))+FXK(I)*(ZCGTHI(I)
2 -KJC(3,I))
HIPANX(I)=HIPANX(I)*DEGREE
KNEANX(I)=KNEANX(I)*DEGREE
SOMEGX(I)=SOMEGX(I)*DEGREE
TOMEGX(I)=TOMEGX(I)*DEGREE
FOTANG(I)=FOTANG(I)*DEGREE
WRITE (6,500)
WRITE (6,500)NZPRNT,ANKMOZ(I),ANKMOX(I),KNEEMZ(I),KNEEMX(I),
1 HIPMZ(I),HIPMX(I),TQA(I),TOK(I),TQH(I)
770 CONTINUE
DO 780 I=1,NC
780 WRITE(6,500)I,FOTANG(I)
CALL GRPTTT(IDENT(6),40HANKLE,KNEE, HIP, CORONAL PLANE
1 20H TIME SEQUENCE FRAMES,20H MOMENTS IN NM .61,TOT060,
2 10HANKLE .1,ANKMOX(I),
3 10HKNEE .1,KNEEMX(I),
4 10HHIP .1,HIPMX(I),
5 LHS,LTO,NHS,NT0,0.0,61.0,-500.0,500.0)
CALL GRPTTT(IDENT(6),40HANKLE, KNEE, HIP, TRANSVERSE PLANE
1 20H TIME SEQUENCE-FRAMES,20H MOMENTS IN NM .61,TOT060,
2 10HANKLE .1,TQA(I),
3 10HKNEE .1,TOK(I),
4 10HHIP .1,TQH(I),
5 LHS,LTO,NHS,NT0,0.0,61.0,-100.0,100.0)
CALL GRPHDT(IDENT(6),40HHIP ANGLE X KNEE ANGLE, SAGITTAL PLANE
1 20H HIP ANGLE .20H KNEE ANGLE .61,
2 HIPANX(I),1,KNEANX(I),LHS,LTO,NHS,NT0,-35.,120.,-15.,120.)
CALL GRPHDT(IDENT(6),40H HIP ANGULAR VELOCITY, SAGITTAL PLANE
1 20H TIME .20H HIP-VEL. DEG/SEC. .61,TOT060,
2 1,TOMEGX(I),LHS,LTO,NHS,NT0,0.,61.,-500.0,500.0)
CALL GRPHDT(IDENT(6),40HKNEE ANGLE X KNEE ANG-VEL. SAGITTAL PLA.
1 20H KNEE ANGLE .20HANG-VEL DEG/SEC. .61,KNEANX(I),
2 1,SOMEGX(I),LHS,LTO,NHS,NT0,-20.,120.,-500.0,500.0)
CALL GRPHDT(IDENT(6),40HKNEE ANGLE X KNEE MOMENTS, SAGIT. PLANE
1 20H ANGLES/DEG. .20H MOMENTS IN NM .61,KNEANX(I),
2 1,KNEEMZ(I),LHS,LTO,NHS,NT0,-20.,120.,-500.,500.)
CALL GRPHDT(IDENT(6),40HKNEE ANG. VELOC. - SAGITTAL PLANE
1 20H TIME SEQUENCE-FRAMES,20HKNEE-VEL. DEG/SEC. .61,TOT060,
2 1,SOMEGX(I),LHS,LTO,NHS,NT0,0.,61.,-500.0,500.0)
C
CALL GRPTTT(IDENT(6),40HANKLE, KNEE, HIP, DISPLACEMENTS
1 20H TIME SEQUENCE-FRAMES,20H Y COORDINATE-METERS,61,TOT060,
2 10HANKLE .3,AJC(2,I),
3 10HKNEE .3,KJC(2,I),

```

```

FIFT6510
FIFT6520
FIFT6530
FIFT6540
FIFT6550
FIFT6560
FIFT6570
FIFT6580
FIFT6590
FIFT6600
FIFT6610
FIFT6620
FIFT6630
FIFT6640
FIFT6650
FIFT6660
FIFT6670
FIFT6680
FIFT6690
FIFT6700
FIFT6710
FIFT6720
FIFT6730
FIFT6740
FIFT6750
FIFT6760
FIFT6770
FIFT6780
FIFT6790
FIFT6800
FIFT6810
FIFT6820
FIFT6830
FIFT6840
FIFT6850
FIFT6860
FIFT6870
FIFT6880
FIFT6890
FIFT6900
FIFT6910
FIFT6920
FIFT6930
FIFT6940
FIFT6950
FIFT6960
FIFT6970
FIFT6980
FIFT6990
FIFT7000
FIFT7010
FIFT7020
FIFT7030
FIFT7040
FIFT7050
FIFT7060
FIFT7070
FIFT7080
FIFT7090
FIFT7100
FIFT7110
FIFT7120
FIFT7130
FIFT7140
FIFT7150
FIFT7160
FIFT7170
FIFT7180
FIFT7190
FIFT7200
FIFT7210
FIFT7220
FIFT7230
FIFT7240
FIFT7250
FIFT7260
FIFT7270
FIFT7280
FIFT7290
FIFT7300
FIFT7310
FIFT7320
FIFT7330

```



```

RETURN                                     AMULT170
END                                         AMULT180

SUBROUTINE CALFPD(X,NSETS,IDENT,NPNT)
C
C CONVERTS FORCE-PLATE DATA, READ AS VOLTAGES BY INFPD, INTO FORCES
C OR MOMENTS IN S.I. UNITS. THE PARAMETERS CORRESPOND TO THOSE OF
C INFPD. EACH INPUT VALUE IS MULTIPLIED BY A FACTOR MADE UP AS
C FOLLOWS.
C
C IN THE CASE OF THE FIRST FORCE-PLATE -
C
C   FOR FORCE  FX1 THE FACTOR IS  1. * 10. * 20. * H / 512.
C   FY1       1. * 10. * 100. * H / 512.
C   FZ1      -1. * 5. * 20. * H / 512.
C   MX1       1. * 8. * 100. * H * .264/512.
C   MY1       1. * 5. * 20. * H * .264/512.
C   MZ1      -1. * 8. * 100. * H * .264/512.
C
C FOR THE SECOND FORCE-PLATE ONLY THE FIRST (SIGN) TERM DIFFERS, AND
C FOLLOWS THE PATTERN -1. I. 1. -I. I. 1. READING DOWNWARDS.
C
C FOR CONTROL SUBJECTS H HAS THE VALUE 2.5, AND FOR CLINICAL CASES IT
C IS 1.0.
C
C   DIMENSION FBASIC(6),FACTOR(6),X(NPNT)
C   INTEGER FP2,P
C   LOGICAL QIDENT
C   DATA FBASIC(1) / 0.3906250 /
C   DATA FBASIC(2) / 1.9531250 /
C   DATA FBASIC(3) / 0.1953125 /
C   DATA FBASIC(4) / 0.4125000 /
C   DATA FBASIC(5) / 0.0515625 /
C   DATA FBASIC(6) / 0.4125000 /
C   DATA FP2 / 3HFP2 /
C   DATA P / 1HP /
C
C   DO 100 J=1,6
C   FACTOR(J)=FBASIC(J)
100 CONTINUE
C   NFP=3
C   IF (QIDENT(IDENT,3.5,FP2)) NFP=1
C   FACTOR(NFP)=-FACTOR(NFP)
C   FACTOR(NFP+3)=-FACTOR(NFP+3)
C   IF (QIDENT(IDENT,1,1,P)) GOTO 120
C   DO 110 J=1,6
C   FACTOR(J)=2.5*FACTOR(J)
110 CONTINUE
120 JFIRST=1
C   JLAST=NSETS
C   DO 140 K=1,6
C   DO 130 J=JFIRST,JLAST
C   X(J)=X(J)*FACTOR(K)
130 CONTINUE
C   JFIRST=JFIRST+NSETS
C   JLAST=JLAST+NSETS
140 CONTINUE
C   RETURN
C   END
C
C   SUBROUTINE CHANGE(X0,Z0,CD,X,Z,XU,ZU)
C   SD=SIGN(CD)
C   CO=COS(CD)
C   XU=(X-X0)*CO+(Z-Z0)*SD
C   ZU=-(X-X0)*SD+(Z-Z0)*CO
C   RETURN
C   END
C
C   SUBROUTINE CHECKY(Y1,NSUBY1,Y2,NSUBY2,NF,NTARG1,NTARG2)
C
C   DIMENSION IDIFF(13),Y1(NSUBY1,NF),Y2(NSUBY2,NF)
C   DATA IBLANK / 1H /
C
C   WRITE (6,100) (IBLANK,J,J=NTARG1,NTARG2)
100 FORMAT (6H1FRAME,A1,5(13H ** TARGET ,I2,3H **,A1,3X))
C   WRITE (6,110) (IBLANK,J=NTARG1,NTARG2)
110 FORMAT (5H NO.,5(A1,21H Y1 Y2 DIFF ))
C   DO 150 J=1,NF
C   IF (MOD(J,5).EQ.1) WRITE(6,120)
120 FORMAT (1H )

```

CALFPD10  
 CALFPD20  
 CALFPD30  
 CALFPD40  
 CALFPD50  
 CALFPD60  
 CALFPD70  
 CALFPD80  
 CALFPD90  
 CALFP100  
 CALFP110  
 CALFP120  
 CALFP130  
 CALFP140  
 CALFP150  
 CALFP160  
 CALFP170  
 CALFP180  
 CALFP190  
 CALFP200  
 CALFP210  
 CALFP220  
 CALFP230  
 CALFP240  
 CALFP250  
 CALFP260  
 CALFP270  
 CALFP280  
 CALFP290  
 CALFP300  
 CALFP310  
 CALFP320  
 CALFP330  
 CALFP340  
 CALFP350  
 CALFP360  
 CALFP370  
 CALFP380  
 CALFP390  
 CALFP400  
 CALFP410  
 CALFP420  
 CALFP430  
 CALFP440  
 CALFP450  
 CALFP460  
 CALFP470  
 CALFP480  
 CALFP490  
 CALFP500  
 CALFP510  
 CALFP520  
 CALFP530  
 CALFP540  
 CALFP550  
 CALFP560

CHANGE10  
 CHANGE20  
 CHANGE30  
 CHANGE40  
 CHANGE50  
 CHANGE60  
 CHANGE70

CHCKY 10  
 CHCKY 20  
 CHCKY 30  
 CHCKY 40  
 CHCKY 50  
 CHCKY 60  
 CHCKY 70  
 CHCKY 80  
 CHCKY 90  
 CHCKY100  
 CHCKY110  
 CHCKY120





```

TERM=1.
130 TEMP=SUM
    TERM=TERM*(TOP/BOT)*XC
    SUM=SUM+TERM
    TOP=TOP+1.
    BOT=BOT+1.
    IF(SUM-TEMP) 140,140,130
140 FPROB=ABS(CON*SGN*EXP(A*ALOG(X)+B*ALOG(XC)+ALGAMA(AB)-ALGAMA(A)
    1 -ALGAMA(B))*SUM/B)
150 RETURN
160 F=1.000001
    FPROB=1000000.
    RETURN
    END

```

FPROB440  
FPROB450  
FPROB460  
FPROB470  
FPROB480  
FPROB490  
FPROB500  
FPROB510  
FPROB520  
FPROB530  
FPROB540  
FPROB550  
FPROB560  
FPROB570

```

SUBROUTINE GRPHOT(IDENT,LABEL,XLABEL,YLABEL,NPNTS,X,NSUBI,Y,LHS,
1 LTO,NHS,NTD,XMIN,XMAX,YMIN,YMAX)
INTEGER XLABEL,YLABEL
INTEGER YALAB
DIMENSION LABEL(4),XLABEL(2),YLABEL(2),X(NPNTS),Y(NSUBI),NPNTS)
DATA NOY / 1 /
DATA YALAB / 10H NO LABEL /
WRITE (8,100) IDENT,LABEL
100 FORMAT (5A10)
WRITE (8,110) XLABEL,YLABEL
110 FORMAT (2A10,10X,2A10)
WRITE (8,120) NPNTS,NOY
120 FORMAT (2I5)
WRITE (8,130) LHS,LTO,NHS,NTD
130 FORMAT (4I5)
WRITE (8,140) XMIN,XMAX,YMIN,YMAX
140 FORMAT (4E15.6)
WRITE (8,150) (X(J),J=1,NPNTS)
WRITE (8,160) YALAB
150 FORMAT (5E15.6)
160 FORMAT (1A10)
WRITE (8,150) (Y(I,J),J=1,NPNTS)
RETURN
END

```

GPH1T 10  
GPH1T 20  
GPH1T 30  
GPH1T 40  
GPH1T 50  
GPH1T 60  
GPH1T 70  
GPH1T 80  
GPH1T 90  
GPH1T100  
GPH1T110  
GPH1T120  
GPH1T130  
GPH1T140  
GPH1T150  
GPH1T160  
GPH1T170  
GPH1T180  
GPH1T190  
GPH1T200  
GPH1T210  
GPH1T220  
GPH1T230  
GPH1T240

```

SUBROUTINE GRPTTT(IDENT,LABEL,XLABEL,YLABEL,NPNTS,X,YALAB,NSUBIA,
1 YA,YBLAB,NSUBIB,YB,YCLAB,NSUBIC,YC,LHS,LTO,NHS,NTD,
2 XMIN,XMAX,YMIN,YMAX)
INTEGER XLABEL,YLABEL
INTEGER YALAB,YBLAB,YCLAB
DIMENSION LABEL(4),XLABEL(2),YLABEL(2),X(NPNTS),YA(NSUBIA),NPNTS)
DIMENSION YB(NSUBIB),NPNTS),YC(NSUBIC),NPNTS)
DATA NOY / 3 /
WRITE (8,100) IDENT,LABEL
100 FORMAT (5A10)
WRITE (8,110) XLABEL,YLABEL
110 FORMAT (2A10,10X,2A10)
WRITE (8,120) NPNTS,NOY
120 FORMAT (2I5)
WRITE (8,130) LHS,LTO,NHS,NTD
130 FORMAT (4I5)
WRITE (8,140) XMIN,XMAX,YMIN,YMAX
140 FORMAT (4E15.6)
150 FORMAT (5E15.6)
WRITE (8,150) (X(J),J=1,NPNTS)
WRITE (8,160) YALAB
WRITE (8,150) (YA(I,J),J=1,NPNTS)
WRITE (8,160) YBLAB
WRITE (8,150) (YB(I,J),J=1,NPNTS)
WRITE (8,160) YCLAB
WRITE (8,150) (YC(I,J),J=1,NPNTS)
160 FORMAT (1A10)
RETURN
END

```

GPH3T 10  
GPH3T 20  
GPH3T 30  
GPH3T 40  
GPH3T 50  
GPH3T 60  
GPH3T 70  
GPH3T 80  
GPH3T 90  
GPH3T100  
GPH3T110  
GPH3T120  
GPH3T130  
GPH3T140  
GPH3T150  
GPH3T160  
GPH3T170  
GPH3T180  
GPH3T190  
GPH3T200  
GPH3T210  
GPH3T220  
GPH3T230  
GPH3T240  
GPH3T250  
GPH3T260  
GPH3T270  
GPH3T280  
GPH3T290

```

SUBROUTINE INPCON(HEIGHT,AMASS,D67,D78,D86,IDENT,NEXTID)
C
C READS FROM A LINE OF AN UPDATE COMPILE FILE, AS DATA STREAM 5, FIVE
C REAL VARIABLES CHARACTERISTIC OF THE PATIENT WITH MARKERS
C AFFIXED, IN SF10.3 FORMAT, PLUS THE DECK IDENTIFIER FROM COLUMNS
C 74 TO 82 IN A9 FORMAT. THE FIVE VALUES ARE -
C
C          HEIGHT - IN METRES.
C          AMASS  - MASS IN KG..
C          D67   - ) DISTANCES IN METRES BETWEEN MARKERS ON THE PELVIS.
C

```

INPCUN10  
INPCUN20  
INPCUN30  
INPCUN40  
INPCUN50  
INPCUN60  
INPCUN70  
INPCUN80  
INPCUN90  
INPCU100



```

100 READ (5,110) LNCH,LINE,IDCHEK
110 FORMAT (4A7,T1,4(I5,2X),T74,A9)
    IF (EOF(5).NE.0) GOTO 190
    IF (IDLOC.NE.0) GOTO 120
    IDLOC=IDCHEK
120 IF (IDLOC.EQ.IDCHEK) GOTO 125
    IF (.NOT.QIDENT(IDCHEK,1,5,FCORR)) GOTO 200
125 DO 130 J=1,4
    IF (LNCH(5-J).NE.IBLANK) GOTO 140
130 CONTINUE
    IF (NXREAD.EQ.NLASTB) GOTO 100
    GOTO 160
140 JVALS=5-J
    DO 150 J=1,JVALS
    NXREAD=NXREAD+1
    X(NXREAD)=FLOAT(LINE(J))
150 CONTINUE
    IF (JVALS.EQ.4) GOTO 100
160 NBLOCK=NBLOCK+1
    IF (NBLOCK.NE.1) GOTO 170
    NSLOC=NXREAD
    NLASTB=NXREAD
    GOTO 100
170 IF (NBLOCK.GT.6) GOTO 220
    IF (NXREAD.NE.(NLASTB+NSLOC)) GOTO 220
    NLASTB=NXREAD
    GOTO 100
180 NSLOC=-NSLOC
    EVNTPT=0.
    GOTO 210
190 IDCHEK=0
200 IF (NBLOCK.EQ.6) GOTO 210
    IF (NBLOCK.NE.5) GOTO 180
    IF (NXREAD.NE.(NLASTB+NSLOC)) GOTO 180
210 NSETS=NSLOC
    IDENT=IDLOC
    NEXTID=IDCHEK
    IF (NSETS.LE.0) RETURN
    NPNTS=6*NSETS
    CALL CALFPO(X,NSETS,IDENT,NPNTS)
    CALL QEVENT(X,NSETS,IDENT,AMASS,EVNTPT)
    RETURN
220 NSLOC=-NSLOC
230 READ (5,240) IDCHEK
240 FORMAT (T74,A9)
    IF (EOF(5).EQ.0.) GOTO 250
    IDCHEK=0
250 IF (IDCHEK.EQ.IDLOC) GOTO 230
    GOTO 210
    END

```

```

SUBROUTINE INPKIN(X,Y,N,IDENT,NEXTID)
C
C READS X AND Y CO-ORDINATES COMPRISING KINETIC DATA, FROM UPDATE
C COMPILE FILE. DATA ARE READ IN SEQUENCE X(1),Y(1),X(2),Y(2),
C . . . X(N),Y(N). X AND Y DATA ARE ON STREAM 5 IN FORMAT
C J(I5,IX,I5,IX) WHERE 0.LE.J.LE.6. DECK NAME IS READ FROM COLS.
C 74 TO 82 AND IS RETURNED IN A9 FORMAT AS IDENT. READING STOPS
C WHEN A NEW DECK IDENTIFIER IS FOUND AND THIS IS RETURNED AS
C NEXTID. N CONTAINS NUMBER OF PAIRS READ. TO AVOID LOSS OF
C DATA AND OTHER PROBLEMS THE FIRST TWO LINES OF EACH DECK SHOULD
C BE BLANK. IF END-OF-FILE IS READ NEXTID IS SET TO ZERO.
C
C TO PROVIDE HORIZONTAL CO-ORDINATES OF A COMMON ORDER OF MAGNITUDE,
C DESPITE VARIATION IN THE WAY THE REFERENCE GRID HAS BEEN USED,
C THESE CO-ORDINATES ARE MODIFIED. AN OFFSET XDIFF, CONSTANT FOR
C A GIVEN DECK AND BASED ON PATIENT P1 DATA, IS ADDED TO THE THREE
C REFERENCE VALUES FOR EACH FRAME.
C
C FOR THREE SPECIAL DECKS FOR WHICH THE REFERENCE GRID TREATMENT WAS
C GROSSLY ATYPICAL, MEAN P1 VALUES ARE INSERTED WITH ADJUSTMENT
C ONLY FOR TRANSLATORY DISPLACEMENT OF EACH FRAME.
C
C CORRECTION IDENTIFIERS OF WHICH THE FIRST FIVE CHARACTERS ARE KCORR
C ARE IGNORED AFTER THE FIRST LINE. THE FIRST LINE ITSELF (WHICH
C WILL NORMALLY BE BLANK) MUST BEAR THE TRUE DECKNAME AS
C IDENTIFIER.
C
DIMENSION LINE(12),LNCH(6),PIX(3,3),PIXBAR(3),PIY(3,3),SPECID(3)
DIMENSION X(1380),Y(1380)
INTEGER UCAM(3)
LOGICAL FIRST,QIDENT

```

```

INPFP390
INPFP400
INPFP410
INPFP420
INPFP430
INPFP440
INPFP450
INPFP460
INPFP470
INPFP480
INPFP490
INPFP500
INPFP510
INPFP520
INPFP530
INPFP540
INPFP550
INPFP560
INPFP570
INPFP580
INPFP590
INPFP600
INPFP610
INPFP620
INPFP630
INPFP640
INPFP650
INPFP660
INPFP670
INPFP680
INPFP690
INPFP700
INPFP710
INPFP720
INPFP730
INPFP740
INPFP750
INPFP760
INPFP770
INPFP780
INPFP790
INPFP800
INPFP810
INPFP820
INPFP830
INPFP840
INPFP850
INPFP860
INPFP870
INPFP880
INPKIN10
INPKIN20
INPKIN30
INPKIN40
INPKIN50
INPKIN60
INPKIN70
INPKIN80
INPKIN90
INPKI100
INPKI110
INPKI120
INPKI130
INPKI140
INPKI150
INPKI160
INPKI170
INPKI180
INPKI190
INPKI200
INPKI210
INPKI220
INPKI230
INPKI240
INPKI250
INPKI260
INPKI270
INPKI280
INPKI290
INPKI300
INPKI310

```

DATA IBLANK / 6H /	INPK1320
DATA KCORR / SHKCORR /	INPK1330
DATA PIX(1,1) / +4588. /; PIY(1,1) / +5960. /	INPK1340
DATA PIX(2,1) / +4588. /; PIY(2,1) / +3290.1 /	INPK1350
DATA PIX(3,1) / +5701. /; PIY(3,1) / +3289.7 /	INPK1360
DATA PIX(1,2) / +4776.3 /; PIY(1,2) / +5935. /	INPK1370
DATA PIX(2,2) / +4781.7 /; PIY(2,2) / +2847.5 /	INPK1380
DATA PIX(3,2) / +5600. /; PIY(3,2) / +2845.8 /	INPK1390
DATA PIX(1,3) / +4064.5 /; PIY(1,3) / +6145. /	INPK1400
DATA PIX(2,3) / +4031.5 /; PIY(2,3) / +3279.2 /	INPK1410
DATA PIX(3,3) / +4720. /; PIY(3,3) / +3272.6 /	INPK1420
DATA PIXBAR(1) / +4588. /	INPK1430
DATA PIXBAR(2) / +4779.0 /	INPK1440
DATA PIXBAR(3) / +4048.0 /	INPK1450
DATA QCAM(1) / 3HKL1 /	INPK1460
DATA QCAM(2) / 3HKR2 /	INPK1470
DATA QCAM(3) / 3HKF3 /	INPK1480
DATA SPECID(1) / 9H>1KF3FUL0 /	INPK1490
DATA SPECID(2) / 9H>3KLIFUL0 /	INPK1500
DATA SPECID(3) / 9H>3KLIBDT0 /	INPK1510
C	INPK1520
NLOC=0	INPK1530
FIRST=.TRUE.	INPK1540
IDENT=0	INPK1550
C	INPK1560
100 READ (5,110) LNCH,LINE,NXTLOC	INPK1570
110 FORMAT (6(6X,A6),T1,12(15,1X),1X,A9)	INPK1580
IF (EOF(5).NE.0.) GOTO 150	INPK1590
IF (.NOT.FIRST) GOTO 120	INPK1600
FIRST=.FALSE.	INPK1610
IDLOC=NXTLOC	INPK1620
IDENT=NXTLOC	INPK1630
120 IF (NXTLOC.EQ.IDLOC) GOTO 130	INPK1640
IF (.NOT.OIDENT(NXTLOC,1,5,KCORR)) GOTO 160	INPK1650
130 DO 140 K=1,6	INPK1660
IF (LNCH(K).EQ.IBLANK) GOTO 100	INPK1670
NLOC=NLOC+1	INPK1680
X(NLOC)=FLOAT(LINE(2*K-1))	INPK1690
Y(NLOC)=FLOAT(LINE(2*K))	INPK1700
140 CONTINUE	INPK1710
GOTO 100	INPK1720
C	INPK1730
150 NXTLOC=0	INPK1740
160 NEXTID=NXTLOC	INPK1750
N=NLOC	INPK1760
DO 170 J=1,3	INPK1770
IF (.NOT.OIDENT(IDLOC,3,5,QCAM(J))) GOTO 170	INPK1780
KCAM=J	INPK1790
GOTO 180	INPK1800
170 CONTINUE	INPK1810
CALL ABORT	INPK1820
180 NSTEP=11+2*(KCAM/3)	INPK1830
DO 190 J=1,3	INPK1840
IF (OIDENT(IDLOC,1,9,SPECID(J))) GOTO 240	INPK1850
190 CONTINUE	INPK1860
XSUM=0.	INPK1870
NX=0	INPK1880
DO 210 J=1,NLOC,NSTEP	INPK1890
DO 200 K=1,2	INPK1900
JPKL1=J*K-1	INPK1910
XSUM=XSUM+X(JPKL1)	INPK1920
200 CONTINUE	INPK1930
NX=NX+2	INPK1940
210 CONTINUE	INPK1950
XBAR=XSUM/FLOAT(NX)	INPK1960
XBARX=PIXBAR(KCAM)	INPK1970
IF (KCAM.NE.1) GOTO 214	INPK1980
IF (OIDENT(IDLOC,1,1,1H>)) GOTO 214	INPK1990
IF (OIDENT(IDLOC,1,2,2HP6)) GOTO 214	INPK1000
XBARX=5546.0	INPK1010
214 XDIFF=XBARX-XBAR	INPK1020
DO 230 J=1,NLOC,NSTEP	INPK1030
DO 220 K=1,3	INPK1040
JPKL1=J*K-1	INPK1050
X(JPKL1)=X(JPKL1)+XDIFF	INPK1060
220 CONTINUE	INPK1070
230 CONTINUE	INPK1080
RETURN	INPK1090
C	INPK1100
240 WRITE (6,250) IDLOC	INPK1110
250 FORMAT (11H0*** DECK ,A9,34H REQUIRED SPECIAL PROCESSING. ***)	INPK1120
XSUM=0.	INPK1130
YSUM=0.	INPK1140

```

      NX=0
      DO 270 J=1,NLOC,NSTEP
      DO 260 K=1,3
      JPKL1=J+K-1
      XSUM=XSUM+X(JPKL1)
      YSUM=YSUM+Y(JPKL1)
260  CONTINUE
      NX=NX+3
270  CONTINUE
      XBAR=XSUM/FLOAT(NX)
      YBAR=YSUM/FLOAT(NX)
      DO 300 J=1,NLOC,NSTEP
      XSUM=0.
      YSUM=0.
      DO 280 K=1,3
      JPKL1=J+K-1
      XSUM=XSUM+X(JPKL1)
      YSUM=YSUM+Y(JPKL1)
280  CONTINUE
      XDIFF=XSUM/3.-XBAR
      YDIFF=YSUM/3.-YBAR
      DO 290 K=1,3
      JPKL1=J+K-1
      X(JPKL1)=PIX(K,KCAM)+XDIFF
      Y(JPKL1)=PIY(K,KCAM)+YDIFF
290  CONTINUE
300  CONTINUE
      RETURN
      END

```

INPK1150  
INPK1160  
INPK1170  
INPK1180  
INPK1190  
INPK1200  
INPK1210  
INPK1220  
INPK1230  
INPK1240  
INPK1250  
INPK1260  
INPK1270  
INPK1280  
INPK1290  
INPK1300  
INPK1310  
INPK1320  
INPK1330  
INPK1340  
INPK1350  
INPK1360  
INPK1370  
INPK1380  
INPK1390  
INPK1400  
INPK1410  
INPK1420  
INPK1430

```

      SUBROUTINE INPKMK(LHS,LTO,IRHS,IRTO,NFRAME,IDENT,NEXTID)

```

INPKMK10  
INPKMK20  
INPKMK30  
INPKMK40  
INPKMK50  
INPKMK60  
INPKMK70  
INPKMK80  
INPKMK90  
INPKM100  
INPKM110  
INPKM120  
INPKM130  
INPKM140  
INPKM150  
INPKM160  
INPKM170  
INPKM180  
INPKM190  
INPKM200  
INPKM210  
INPKM220  
INPKM230  
INPKM240  
INPKM250  
INPKM260  
INPKM270  
INPKM280  
INPKM290  
INPKM300  
INPKM310  
INPKM320  
INPKM330  
INPKM340  
INPKM350  
INPKM360  
INPKM370  
INPKM380  
INPKM390  
INPKM400  
INPKM410  
INPKM420  
INPKM430  
INPKM440  
INPKM450  
INPKM460  
INPKM470  
INPKM480  
INPKM490  
INPKM500  
INPKM510  
INPKM520

```

C
C READS FROM A LINE OF AN UPDATE COMPILE FILE, AS DATA STREAM 5, FIVE
C INTEGERS MARKING EVENTS IN KINEMATIC DATA, IN 5110 FORMAT, PLUS
C THE DECK IDENTIFIER FROM COLUMNS 74 TO 82 IN A9 FORMAT. THE
C FIVE INTEGERS ARE -
C
C      LHS - FRAME NUMBERS (FIRST = 1) OF FIRST FRAME AFTER (OR
C           AT) LEFT HEEL STRIKE.
C      LTO - THE SAME, FOR LEFT TOE-OFF.
C      IRHS - THE SAME, FOR RIGHT HEEL STRIKE.
C      IRTO - THE SAME FOR RIGHT TOE-OFF.
C      NFRAME - THE TOTAL NUMBER OF FRAMES EXPOSED IN EACH CAMERA
C              FOR THE MANOEUVRE.
C
C IDENT CONTAINS THE DECK NAME FROM WHICH DATA ARE READ. LEADING
C BLANK, OR TRAILING, LINES ARE SKIPPED, AND READING STOPS WHEN THE
C FIRST LINE OF THE FOLLOWING DECK IS READ. THE IDENTIFIER OF
C THAT DECK IS RETURNED AS NEXTID. IF END-OF-FILE IS READ, NEXTID
C IS RETURNED AS ZERO.
C
C CORRECTION IDENTIFIERS OF WHICH THE FIRST FIVE CHARACTERS ARE M CORR
C ARE IGNORED AFTER THE FIRST LINE. THE FIRST LINE ITSELF (WHICH
C WILL NORMALLY BE BLANK) MUST BEAR THE TRUE DECKNAME AS
C IDENTIFIER.
C
C ON ERROR LHS IS RETURNED NEGATIVE.
C
C DIMENSION LINE(7)
C LOGICAL QIDENT
C DATA IBLANK / 10H /
C DATA M CORR / 5H M CORR /
C
      IDENT=0
      LHS=-1
100  READ (5,110) LINE
110  FORMAT (A10,T1,5I10,T74,A9)
      IF (EOF(5).NE.0.) GOTO 130
      IF (IDENT.EQ.0) IDENT=LINE(7)
      IF (IDENT.EQ.LINE(7)) GOTO 120
      IF (.NOT.QIDENT(LINE(7),1,5,M CORR)) GOTO 140
120  IF (LHS.GE.0) GOTO 100
      IF (LINE(1).EQ.IBLANK) GOTO 100
      LHS=LINE(2)
      LTO=LINE(3)
      IRHS=LINE(4)
      IRTO=LINE(5)
      NFRAME=LINE(6)
      GOTO 100
130  LINE(7)=0
140  NEXTID=LINE(7)
      RETURN

```

```

END                                                    INPKM530

INTEGER FUNCTION NEARST(X)                            NEARST10
C                                                     NEARST20
C RETURNS THE NEAREST INTEGER TO THE ARGUMENT X.    NEARST30
C                                                     NEARST40
C                                                     NEARST50
C                                                     NEARST60
C                                                     NEARST70

NEARST=IFIX(X+.5IGN(0.5,X))
RETURN
END

LOGICAL FUNCTION NEWMAN(ID1, ID2)                    NEWMAN10
C                                                     NEWMAN20
C COMPARE THE FIRST TWO CHARACTERS (TWELVE BITS) IN TWO WORDS, AND
C RETURNS THE VALUE .TRUE. IF THEY DIFFER, AND .FALSE. IF THEY ARE
C THE SAME.
C                                                     NEWMAN30
C                                                     NEWMAN40
C                                                     NEWMAN50
C                                                     NEWMAN60
C                                                     NEWMAN70
C                                                     NEWMAN80
C                                                     NEWMAN90

NEWMAN=(ID1.AND.MASK(12)).NE.(ID2.AND.MASK(12))
RETURN
END

SUBROUTINE NUREGR(ND>BD1, ND, YEXT, NC>BD1, NC, FUN, DFUN, DDFUN, NK)
DIMENSION YEXT(NDSBD1, ND), FUN(NCSBD1, NC), DFUN(NCSBD1, NC),
I   DDFUN(NCSBD1, NC)
DIMENSION SUMCY(30), SUMSY(30)
DIMENSION A(30), B(30), SUMSQR(31)
REAL ICPEXT
COMMON /SMOOTH/ A, B, C, COVERT, GRAD, GRDEXT, ICPEXT, STEP, SUMSQR, YM, YO
DATA T / 0.020000000 /
DATA TWOPI / 6.283185307 /
N=ND-1
RINT=FLOAT(N)
NA=(ND-3)/2
IF (NA.GT.30) NA=30
IF (NA.GT.(NK+NK)) NA=NK+NK
C=TWOPI/RINT
COVERT=C/T
STEP=(YEXT(1,ND)-YEXT(1,1))
GRAD=STEP/RINT
YO=YEXT(1,1)-GRAD
SUMY=0.
SUMYSQ=0.
DO 100 K=1,NA
SUMCY(K)=0.
SUMSY(K)=0.
100 CONTINUE
DO 120 I=1,N
YI=YEXT(1,I)-YO-GRAD*FLOAT(I)
SUMY=SUMY+YI
SUMYSQ=SUMYSQ+YI*YI
XI=C*FLOAT(I-1)
DO 110 K=1,NA
ARG=K*XI
SUMCY(K)=SUMCY(K)+COS(ARG)*YI
SUMSY(K)=SUMSY(K)+SIN(ARG)*YI
110 CONTINUE
120 CONTINUE
YM=SUMY/RINT
CYY=SUMYSQ-SUMY*YM
SUMSQR(1)=CYY
DO 130 K=1,NA
A(K)=SUMCY(K)*(2./RINT)
B(K)=SUMSY(K)*(2./RINT)
CYY=CYY-A(K)*SUMCY(K)-B(K)*SUMSY(K)
SUMSQR(K+1)=CYY
130 CONTINUE
RC=NC-1
CC=TWOPI/RC
GRADC=GRAD*RINT/RC
ICPEXT=YEXT(1,1)*YM
YOCYM=ICPEXT-GRADC
GRDEXT=GRAD/T
DO 150 I=1,NC
FUN(I,I)=YOCYM+GRADC*FLOAT(I)
DFUN(1,I)=GRDEXT
DDFUN(1,I)=0.
CCII=CC*FLOAT(I-1)
DO 140 K=1,NK
RK=FLOAT(K)
FREQ=RK*COVERT
SN=SIN(RK*CCII)

```

```

CS=COS(RK*CCI)
HOLD=A(K)*CS+B(K)*SN
FUN(I,I)=FUN(I,I)+HOLD
DFUN(I,I)=DFUN(I,I)+FREQ*(-A(K)*SN+B(K)*CS)
DDFUN(I,I)=DDFUN(I,I)-FREQ*FREQ*HOLD
140 CONTINUE
150 CONTINUE
RETURN
END

```

NUREG610  
NUREG620  
NUREG630  
NUREG640  
NUREG650  
NUREG660  
NUREG670  
NUREG680  
NUREG690

```

SUBROUTINE PARALA(KA,KB,NF)
DIMENSION XIANTES(10,125),YIANTES(10,125),X1A(8,125),
1 Y1A(8,125),Z1A(10,125),X(11,125),Y(11,125),Z(11,125)
COMMON XIANTES,YIANTES,X1A,Y1A,Z1A,X,Y,Z,HX,XL,ZL
COMMON /TRYZ/ Y2A(10,125),Y2(10,125),Y2FILL(380)
DO 110 J=KA,KB
DO 100 I=1,NF
DO=XIANTES(J,I)*Z1A(J,I)
RE=XL*ZL
RMI=XIANTES(J,I)*RE-DO*XL
FA=RE-DO
X(J,I)=RMI/FA
SOL=Z1A(J,I)*X(J,I)
SI=SOL/XL
Z(J,I)=Z1A(J,I)-SI
DOO=YIANTES(J,I)*Z(J,I)
REE=HX*Z(J,I)
REMI=(DOO-REE)/ZL
Y(J,I)=YIANTES(J,I)-REMI
Y2(J,I)=Y2A(J,I)-(Y2A(J,I)-HX)*X(J,I)/XL
100 CONTINUE
110 CONTINUE
RETURN
END

```

PARALA10  
PARALA20  
PARALA30  
PARALA40  
PARALA50  
PARALA60  
PARALA70  
PARALA80  
PARALA90  
PARAL100  
PARAL110  
PARAL120  
PARAL130  
PARAL140  
PARAL150  
PARAL160  
PARAL170  
PARAL180  
PARAL190  
PARAL200  
PARAL210  
PARAL220  
PARAL230  
PARAL240

```

SUBROUTINE PIRILI(SSSX,SSSY,SSFZ,XL,ZL,HX,LADO)
DIMENSION SSSX(3),SSSY(3),SSFZ(3)
COMMON /BLOCKI/ SSSX(10),SSSY(10),SSFZ(10)
COMMON /LADO/ LEFSID,ISIDE,JSIDE,LSIDE,JBIDE,LBIDE
LOGICAL LEFSID
DO 1 I=1,3
J=JSIDE+I
DA=SSSX(I)*SSFZ(I)
RE=XL*ZL
RMI=SSSX(I)*RE-DA*XL
FA=RE-DA
SSX(J)=RMI/FA
SOL=SSFZ(I)*SSSX(J)
SI=SOL/XL
SFZ(J)=SSFZ(I)-SI
DOA=SSSY(I)*SFZ(J)
REE=HX*SFZ(J)
REMI=(DOA-REE)/ZL
SSY(J)=SSSY(I)-REMI
1 CONTINUE
RETURN
END

```

PIRIL110  
PIRIL120  
PIRIL130  
PIRIL140  
PIRIL150  
PIRIL160  
PIRIL170  
PIRIL180  
PIRIL190  
PIRIL100  
PIRIL110  
PIRIL120  
PIRIL130  
PIRIL140  
PIRIL150  
PIRIL160  
PIRIL170  
PIRIL180  
PIRIL190  
PIRIL200  
PIRIL210  
PIRIL220

```

SUBROUTINE POROLO(X,Y,Z,A,B,C,ZL,XL,HX)
X=(A*XL*ZL-A*C*XL)/(XL*ZL-C*A)
Z=C-C*X/XL
Y=B-(B*Z-HX*Z)/ZL
RETURN
END

```

POROLO10  
POROLO20  
POROLO30  
POROLO40  
POROLO50  
POROLO60

```

SUBROUTINE QEVENT(X,NSETS,IDENT,AMASS,EVENTPT)
C
C PROCESSES FORCE PLATE DATA, AFTER READING BY INPPFD AND CONVERSION TO
C S.I. UNITS BY CALFPD. DATA ARE SEARCHED FROM THE ZERO-LOAD END
C TO LOCATE ITS LIMIT AT HEEL-STRIKE OR TOE-OFF. LOCATION IS
C RETURNED, AS SUBSCRIPT OF X COINCIDING WITH EVENT, IN EVENTPT.
C THIS HAS TYPE REAL AND THUS INCLUDES A FRACTIONAL PART.
C
C MEAN VALUE OF ZERO-LOAD REGION IS THEN CALCULATED AND VALUES ARE
C ADJUSTED TO THIS ZERO DATUM. THE ADJUSTED DATA ARE RELOCATED TO
C FILL THE WHOLE ARRAY OF 500 BY 6 WORDS, SUPPLYING ZERO FILL AT
C THE END WITH NO FOOT CONTACT.
C
DIMENSION FOLD(500,6),LABEL(2),X(NSETS,6)

```

QEVENT10  
QEVENT20  
QEVENT30  
QEVENT40  
QEVENT50  
QEVENT60  
QEVENT70  
QEVENT80  
QEVENT90  
QEVENT100  
QEVENT110  
QEVENT120  
QEVENT130  
QEVENT140

```

LOGICAL BACKWD,QIDENT
COMMON /FHLD BK/ F HOLD
DATA LABEL(1) / 8H FORWARD /
DATA LABEL(2) / 8HBACKWARD /
C
BACKWD=QIDENT(IDENT,3,8,6HFP1FUL).OR.QIDENT(IDENT,3,8,6HFP2BDT)
CRIT=5.0*AMASS
NSTPLI=NSETS+1
JJ=1
IF(BACKWD) JJ=NSTPLI-JJ
CRITL=X(JJ,2)+0.1*CRIT
XSUM=0.
C
C SEARCH (FORWARD OR BACKWARD) FOR BREAK FROM ZERO-LOAD LEVEL.
C
DO 120 J=1,NSETS
JJ=J
IF (BACKWD) JJ=NSTPLI-JJ
XNOW=X(JJ,2)
IF (J.EQ.1) GOTO 110
IF (XNOW.GE.CRITL) GOTO 80
IF (XLAST.GE.CRITL) GOTO 90
IF (XNOW.LE.XLAST) GOTO 100
80 XLAST=XNOW
90 XLEVEL=XSUM/FLOAT(JLEVEL)
JTEST=JLEVEL+7
TEST=XLEVEL+CRIT
IF ((J.LT.JTEST).AND.(XNOW.LT.TEST)) GOTO 120
JTSTL=J-1
GOTO 130
C
100 IF ((JLEVEL+1).EQ.J) GOTO 110
JLEVEL=JLEVEL+1
JJ=JLEVEL
IF (BACKWD) JJ=NSTPLI-JJ
XSUM=XSUM+X(JJ,2)
GOTO 100
110 JLEVEL=J
XLAST=XNOW
XSUM=XSUM+XNOW
120 CONTINUE
GOTO 300
C
C SEARCH COMPLETE. JLEVEL POINTS TO LAST ELEMENT BEFORE RISE STARTS.
C XLEVEL IS MEAN VALUE UP TO AND INCLUDING THAT POINT. JTSTL
C POINTS TO LAST ELEMENT BEFORE TEST POINT WHERE LOAD EXCEEDS CRIT
C (I.E. ABOUT HALF THE PATIENT'S WEIGHT).
C
C TREATMENT NOW DEPENDS ON THE STEEPNESS OF THE RISE.
C
130 CONTINUE
WRITE (6,140) JLEVEL,JTSTL,XLEVEL
140 FORMAT (1H,60X,19H*** QEVENT CHECK -,2I6,F10.4,4H *** )
IF (JTSTL-JLEVEL-1) 150,160,170
C
C VERY STEEP. SET POINTER HALF WAY ACROSS GAP.
C
150 EVNTPF=FLOAT(JLEVEL)+0.5
B=0.
GOTO 200
C
C STEEP. SET POINTER BY HOW FAR FIRST POINT HAS JUMPED, UP TO HALFWAY.
C
160 JJ=JTSTL
IF (BACKWD) JJ=NSTPLI-JJ
EVNTPF=FLOAT(JTSTL)-(X(JJ,2)-XLEVEL)/(CRIT+CRIT)
B=0.
GOTO 200
C
C GRADUAL. FIT STRAIGHT LINE THROUGH POINTS JLEVEL TO JTSTL. AND
C USE INTERCEPT WITH XLEVEL.
C
170 TSUM=0.
TTSUM=0.
TXSUM=0.
XSUM=0.
XXSUM=0.
DO 180 J=JLEVEL,JTSTL
JJ=J
IF (BACKWD) JJ=NSTPLI-JJ
XNOW=X(JJ,2)
TJ=FLOAT(J)
TSUM=TSUM+TJ

```

QEVEN150  
QEVEN160  
QEVEN170  
QEVEN180  
QEVEN190  
QEVEN200  
QEVEN210  
QEVEN220  
QEVEN230  
QEVEN240  
QEVEN250  
QEVEN260  
QEVEN270  
QEVEN280  
QEVEN290  
QEVEN300  
QEVEN310  
QEVEN320  
QEVEN330  
QEVEN340  
QEVEN350  
QEVEN360  
QEVEN370  
QEVEN380  
QEVEN390  
QEVEN400  
QEVEN410  
QEVEN420  
QEVEN430  
QEVEN440  
QEVEN450  
QEVEN460  
QEVEN470  
QEVEN480  
QEVEN490  
QEVEN500  
QEVEN510  
QEVEN520  
QEVEN530  
QEVEN540  
QEVEN550  
QEVEN560  
QEVEN570  
QEVEN580  
QEVEN590  
QEVEN600  
QEVEN610  
QEVEN620  
QEVEN630  
QEVEN640  
QEVEN650  
QEVEN660  
QEVEN670  
QEVEN680  
QEVEN690  
QEVEN700  
QEVEN710  
QEVEN720  
QEVEN730  
QEVEN740  
QEVEN750  
QEVEN760  
QEVEN770  
QEVEN780  
QEVEN790  
QEVEN800  
QEVEN810  
QEVEN820  
QEVEN830  
QEVEN840  
QEVEN850  
QEVEN860  
QEVEN870  
QEVEN880  
QEVEN890  
QEVEN900  
QEVEN910  
QEVEN920  
QEVEN930  
QEVEN940  
QEVEN950  
QEVEN960  
QEVEN970



```

TTSUM=TTSUM+TJ*TJ
TXSUM=TXSUM+TJ*XNOW
XSUM=XSUM+XNOW
XXSUM=XXSUM+XNOW*XNOW
180 CONTINUE
FN=FLOAT(JTSTL1-JLEVEL+1)
B=(TXSUM*FN-TSUM*XSUM)/(TTSUM*FN-TSUM*TSUM)
A=(XSUM-B*TSUM)/FN
EVNTPT=(XLEVEL-A)/B
WRITE (6,190) TSUM,TTSUM, TXSUM,XSUM,XXSUM,A,B,EVNTPT
190 FORMAT (28H0*** QEVENT BY LINEAR FIT -.5E20.10,4H ***/1H0.67X,
1 3E20.10,4H ***)
C
C EVENT LOCATED. INVERT IF NECESSARY, THEN ADJUST DATUM.
C
200 J2=JLEVEL-1
IF (J2.LE.0) J2=1
IF (.NOT. BACKWD) GOTO 210
EVNTPT=FLOAT(NSTPL1)-EVNTPT
J1=NSTPL1-J2
J2=NSETS
GOTO 220
210 J1=1
220 FACTOR=1./FLOAT(J2-J1+1)
JFILL=500-NSETS
DO 290 K=1,6
KINV=7-K
XSUM=0.
DO 230 J=J1,J2
XSUM=XSUM+X(J,KINV)
230 CONTINUE
XDATUM=FACTOR*XSUM
IF (KINV.EQ.2) XDATM2=XDATUM
IF (.NOT.BACKWD) GOTO 260
DO 240 J=1,NSETS
FHOLD(J,KINV)=X(J,KINV)-XDATUM
240 CONTINUE
DO 250 J=NSTPL1,500
FHOLD(J,KINV)=0.
250 CONTINUE
GOTO 290
260 DO 270 J=1,NSETS
JINV=NSTPL1-J
JJ=JINV+JFILL
FHOLD(JJ,KINV)=X(JINV,KINV)-XDATUM
270 CONTINUE
DO 280 J=1,JFILL
FHOLD(J,KINV)=0.0
280 CONTINUE
290 CONTINUE
IF (.NOT.BACKWD) EVNTPT=EVNTPT+FLOAT(JFILL)
NSHOLD=NSETS
NSETS=500
GOTO 320
C
C SYNCHRONIZATION FAILURE ROUTINE.
C
300 WRITE (6,310) IDENT
310 FORMAT (53H0SYNCHRONIZATION FAILURE IN QEVENT, WHILE PROCESSING ,
1 SHDECK ,A9)
CALL ABORT(2)
RETURN
C
C WRITE GRAPH PLOTTING INFORMATION TO TAPEB
C
320 J=1
IF (BACKWD) J=2
WRITE (8,330) IDENT,LABEL(J)
330 FORMAT (A9,4X,A8,29H-SEARCHING SYNCHRONIZATION )
IF (H.EQ.0) GOTO 350
IF (BACKWD) GOTO 340
J1=JLEVEL
J2=JTSTL1
GOTO 360
340 J1=NSTPL1-JTSTL1
J2=NSTPL1-JLEVEL
GOTO 360
350 J1=0
J2=0
360 WRITE (8,370) NSHOLD,J1,J2
370 FORMAT (J16)
FMIN=0.
FMAX=0.

```

QEVEN980  
QEVEN990  
QEVE1000  
QEVE1010  
QEVE1020  
QEVE1030  
QEVE1040  
QEVE1050  
QEVE1060  
QEVE1070  
QEVE1080  
QEVE1090  
QEVE1100  
QEVE1110  
QEVE1120  
QEVE1130  
QEVE1140  
QEVE1150  
QEVE1160  
QEVE1170  
QEVE1180  
QEVE1190  
QEVE1200  
QEVE1210  
QEVE1220  
QEVE1230  
QEVE1240  
QEVE1250  
QEVE1260  
QEVE1270  
QEVE1280  
QEVE1290  
QEVE1300  
QEVE1310  
QEVE1320  
QEVE1330  
QEVE1340  
QEVE1350  
QEVE1360  
QEVE1370  
QEVE1380  
QEVE1390  
QEVE1400  
QEVE1410  
QEVE1420  
QEVE1430  
QEVE1440  
QEVE1450  
QEVE1460  
QEVE1470  
QEVE1480  
QEVE1490  
QEVE1500  
QEVE1510  
QEVE1520  
QEVE1530  
QEVE1540  
QEVE1550  
QEVE1560  
QEVE1570  
QEVE1580  
QEVE1590  
QEVE1600  
QEVE1610  
QEVE1620  
QEVE1630  
QEVE1640  
QEVE1650  
QEVE1660  
QEVE1670  
QEVE1680  
QEVE1690  
QEVE1700  
QEVE1710  
QEVE1720  
QEVE1730  
QEVE1740  
QEVE1750  
QEVE1760  
QEVE1770  
QEVE1780  
QEVE1790  
QEVE1800

```

IF (BACKWD) GOTO380
J1=JFILL+1
J2=500
GOTO 390
380 J1=1
J2=NSHOLD
390 DO 400 J=J1,J2
IF (FHOLD(J,2).GT.FMAX) FMAX=FHOLD(J,2)
IF (FHOLD(J,2).LT.FMIN) FMIN=FHOLD(J,2)
400 CONTINUE
WRITE (8,410) EVNTPT,FMIN,EVNTPT,FMAX
410 FORMAT (5E15,6)
IF (8.EQ.0.) GOTO 430
A=A-XDATH2
IF (.NOT.BACKWD) A=A-B*FLOAT(JFILL)
TMIN=(FMIN-A)/B
TMAX=(FMAX-A)/B
IF (.NOT.BACKWD) GOTO 420
TMIN=FLOAT(NS>TPL1)-TMIN
TMAX=FLOAT(NS>TPL1)-TMAX
420 T1=FLOAT(J1)
T2=FLOAT(J2)
XLEVEL=XLEVEL-XDATH2
WRITE (8,410) T1,XLEVEL,T2,XLEVEL
WRITE (8,410) TMIN,FMIN,TMAX,FMAX
430 WRITE (8,440) (J,J=J1,J2)
440 FORMAT (5(16,9H,0000E+00))
WRITE (8,410) (FHOLD(J,2),J=J1,J2)
RETURN
END

```

QEVE1810  
QEVE1820  
QEVE1830  
QEVE1840  
QEVE1850  
QEVE1860  
QEVE1870  
QEVE1880  
QEVE1890  
QEVE1900  
QEVE1910  
QEVE1920  
QEVE1930  
QEVE1940  
QEVE1950  
QEVE1960  
QEVE1970  
QEVE1980  
QEVE1990  
QEVE2000  
QEVE2010  
QEVE2020  
QEVE2030  
QEVE2040  
QEVE2050  
QEVE2060  
QEVE2070  
QEVE2080  
QEVE2090  
QEVE2100

```

LOGICAL FUNCTION QIDENT(IDENT,ICOL1,ICOL2,ICOMP)
C COMPARES THE CHARACTERS ICOL1 TO ICOL2 OF THE CHARACTER STRING IDENT
C WITH THE CORRESPONDING LEFTMOST (ICOL2-ICOL1+1) CHARACTERS OF
C ICOMP, AND RETURNS THE VALUE .TRUE. IF THE SAME, .FALSE. IF
C DIFFERENT.
C FOR EXAMPLE, QIDENT(8HSHAMBLES,2,4,3HAM) IS .TRUE..
C
NBITS=6*(ICOL2-ICOL1+1)
M>KBIT=.NOT.MASK(60-NBITS)
IDLOC=SHIFT(IDENT,(6*ICOL2))
ICLOC=SHIFT(ICOMP,NBITS)
QIDENT=(IDLOC.AND.M>KBIT).EQ.(ICLOC.AND.M>KBIT)
RETURN
END

```

QIDENT10  
QIDENT20  
QIDENT30  
QIDENT40  
QIDENT50  
QIDENT60  
QIDENT70  
QIDENT80  
QIDENT90  
QIDENT100  
QIDENT110  
QIDENT120  
QIDENT130  
QIDENT140  
QIDENT150  
QIDENT160

```

SUBROUTINE REF(PX1,PX2,PX3,PZ1,PZ2,PZ3,X0,Z0,CD)
Z32=PZ3-PZ2
X32=PX3-PX2
AM=Z32/X32
CL=(PX3*PZ2-PX2*PZ3)/X32
X0=(PX1+AM*(PZ1-CL))/(1.+AM*AM)
Z0=AM*X0+CL
CD=ATAN(AM)
RETURN
END

```

REF 10  
REF 20  
REF 30  
REF 40  
REF 50  
REF 60  
REF 70  
REF 80  
REF 90  
REF 100

```

SUBROUTINE ROOTS(RX1,RX2,A,B,C)
HBY2A=0.5*B/A
DI>C=(HBY2A)**2-C/A
IF(DI>C.GE.0.)GOTO 1
RX1=-HBY2A
RX2=100.0
GOTO4
1 ROOT=SQRT(DI>C)
RX1=-HBY2A-ROOT
RX2=0.0
4 RETURN
END

```

ROOTS 10  
ROOTS 20  
ROOTS 30  
ROOTS 40  
ROOTS 50  
ROOTS 60  
ROOTS 70  
ROOTS 80  
ROOTS 90  
ROOTS100  
ROOTS110  
ROOTS120

```

SUBROUTINE SMOOTH(LABEL,ND>BD1,ND,Y,NC>BD1,NC,FUN,DFUN,DDFUN,NK)
C PROVIDES AN INTERFACE THROUGH WHICH THE HARMONIC ANALYSIS ROUTINE
C NUREGR IS CALLED.
C
DIMENSION LABEL(5),Y(ND>BD1,ND),FUN(NC>BD1,NC),DFUN(NC>BD1,NC),
1 DDFUN(ND>BD1,NC)

```

SMOOTH10  
SMOOTH20  
SMOOTH30  
SMOOTH40  
SMOOTH50  
SMOOTH60  
SMOOTH70

```

DIMENSION A(30),B(30),SUMSQ(31),HOLDY(320)
REAL ICPEXT
COMMON /SMOOTH/ A,B,C,COVERT,GRAD,GRDXT,ICPEXT,STEP,SUMSQ,YM,YO
C
WRITE (6,90)
90 FORMAT (1H0)
WRITE (6,100) LABEL
100 FORMAT (52H SMOOTHING AND DIFFERENTIATION BY FOURIER REGRESSION,
1 7H = ,SA10/1H )
IF (NK.EQ.0) NK=NEAREST(FLOAT(ND-1)/20.)
JTOP=5
IF (JTOP.GT.NC) JTOP=NC
IF (JTOP.GT.ND) JTOP=ND
DO 150 J=1,ND
HOLDY(J)=Y(1,J)
150 CONTINUE
CALL NUREGR(ND>BD1,ND,Y,NC>BD1,NC,FUN,DFUN,DDFUN,NK)
C*
WRITE (6,200) ND,NC,NK
200 FORMAT (25HNUMBER OF DATA POINTS =,I4,10X,10HNUMBER OF ,
1 16HFITTED POINTS =I4,10X,25HDEGREE OF FITTED MODEL =,I4)
C*
WRITE (6,210) ICPEXT,GRDXT,STEP
210 FORMAT (13HINTERCEPT =,E14.5,12X,18HLINEAR GRADIENT =,E14.5,
1 8X,14HSTEP LENGTH =,E14.5)
C*
WRITE (6,220)
220 FORMAT (49HDEGREE COSINE SINE MODULUS,
1 53H RESIDUAL DEGREE> RESIDUAL RESIDUAL,
2 25H PROB2. MODULUS*/
3 58H NK COEFFT COEFFT SUM,
4 52H>QUARE> FREEDOM VARIANCE >TD.DEVN ,
5 17H OMEGA**2)
NA=(ND-4)/2
IF (NA.GT.30) NA=30
IF (NA.GT.(NK+NK)) NA=NK+NK
NDEGF=ND-3
VARNCE=SUMSQ(1)/FLOAT(NDEGF)
STDEV=SQRT(VARNCE)
C*
WRITE (6,230) SUMSQ(1),NDEGF,VARNCE,STDEV
230 FORMAT (5H0 0.45X,E15.5,18,2E15.5)
DO 270 J=1,NA
F2=(SUMSQ(J)-SUMSQ(J+1))/(VARNCE+VARNCE)
PROB2=1.
IF (F2.GT.1.) PROB2=FPROB(F2,2,NDEGF)
NDEGF=NDEGF-2
VARNCE=SUMSQ(J+1)/FLOAT(NDEGF)
STDEV=SQRT(VARNCE)
OMEGA=COVERT*FLOAT(J)
RMOD=SQRT(A(J)*A(J)+B(J)*B(J))
SQMOD=OMEGA*OMEGA*RMOD
C*
IF (MOD(J,5).EQ.1) WRITE (6,240)
240 FORMAT (1H )
C*
WRITE (6,250) J,A(J),B(J),RMOD,SUMSQ(J+1),NDEGF,VARNCE,STDEV,
C*
1 PROB2,SQMOD
250 FORMAT (1H ,I4,4E15.5,18,2E15.5,F11.4,E13.3)
C*
IF (J.EQ.NK) WRITE (6,260)
260 FORMAT (1H.,127X,6H*****)
270 CONTINUE
TSTEP1=0.02
TSTEP2=TSTEP1*FLOAT(ND-1)/FLOAT(NC-1)
C*
WRITE (6,280)
280 FORMAT(1H0/47H ***** INPUT *****
1 29HOUTPUT *****/19H TIME VALUE,
2 41H TIME VALUE VELOCITY,
3 17H ACCELERATION)
C*
DO 300 J=1,JTOP
C*
T1=TSTEP1*FLOAT(J-1)
C*
T2=TSTEP2*FLOAT(J-1)
C*
IF (MOD(J,5).EQ.1) WRITE (6,240)
C*
WRITE (6,290) T1,HOLDY(J),T2,FUN(1,J),DFUN(1,J),DDFUN(1,J)
290 FORMAT (1H ,F5.2,E15.5,F10.4,3E15.5)
300 CONTINUE
WRITE (6,310)
310 FORMAT (1H0/50H FRAME TIME INPUT FITTED,
1 33H RESIDUAL RESID. //22H NO. (SECONDS) ,
2 51H VALUE VALUE DIFFERENCE ,
3 13H>TD.DEVIATION/1H )
YOYM=Y0+YM
STDEV=SQRT(SUMSQ(NK+1)/FLOAT(ND-NK-NK-3))
RCHECK=0.
SCHECK=0.
DO 350 I=1,ND
YCHECK=YOYM+GRAD*FLOAT(I)
C(I)=C*FLOAT(I-1)
TIME=0.02*FLOAT(I-1)
SMOOTH80
SMOOTH90
SMOOTH100
SMOOTH110
SMOOTH120
SMOOTH130
SMOOTH140
SMOOTH150
SMOOTH160
SMOOTH170
SMOOTH180
SMOOTH190
SMOOTH200
SMOOTH210
SMOOTH220
SMOOTH230
SMOOTH240
SMOOTH250
SMOOTH260
SMOOTH270
SMOOTH280
SMOOTH290
SMOOTH300
SMOOTH310
SMOOTH320
SMOOTH330
SMOOTH340
SMOOTH350
SMOOTH360
SMOOTH370
SMOOTH380
SMOOTH390
SMOOTH400
SMOOTH410
SMOOTH420
SMOOTH430
SMOOTH440
SMOOTH450
SMOOTH460
SMOOTH470
SMOOTH480
SMOOTH490
SMOOTH500
SMOOTH510
SMOOTH520
SMOOTH530
SMOOTH540
SMOOTH550
SMOOTH560
SMOOTH570
SMOOTH580
SMOOTH590
SMOOTH600
SMOOTH610
SMOOTH620
SMOOTH630
SMOOTH640
SMOOTH650
SMOOTH660
SMOOTH670
SMOOTH680
SMOOTH690
SMOOTH700
SMOOTH710
SMOOTH720
SMOOTH730
SMOOTH740
SMOOTH750
SMOOTH760
SMOOTH770
SMOOTH780
SMOOTH790
SMOOTH800
SMOOTH810
SMOOTH820
SMOOTH830
SMOOTH840
SMOOTH850
SMOOTH860
SMOOTH870
SMOOTH880
SMOOTH890
SMOOTH900

```

```

DO 320 J=1,NK
RJC11=FLOAT(J)*C11
YCHECK=YCHECK+A(J)*COS(RJC11)+B(J)*SIN(RJC11)
320 CONTINUE
YDIFF=HOLDY(I)-YCHECK
RATIO=YDIFF/SIDEV
RCHECK=RCHECK+RATIO
SCHECK=SCHECK+RATIO*RATIO
IF (ABS(RATIO).GT.2.3)
1WRITE (6,330) I,TIME,HOLDY(I),YCHECK,YDIFF,RATIO
330 FORMAT (1H ,I4,F13.3,E18.5,2E16.5,F13.2)
C* IF (MOD(I,5).EQ.0) WRITE (6,330)
C* IF (I.EQ.ND) GOTO 350
C* IF (MOD(I,50).EQ.0) WRITE (6,340)
C*340 FORMAT (1H1/1H0)
350 CONTINUE
WRITE (6,360) RCHECK,SCHECK
360 FORMAT (1H0,32X,35H>UM> OF RATIO> AND THEIR SQUARE> -.2F13.2)
RETURN
END

```

```

SUBROUTINE TABLE1(ID,AJC,KJC,HJC,NF)
C
C IMPROVED TABULATION OF JOINT CENTRE CO-ORDINATES.
C
REAL KJC
DIMENSION AJC(3,NF),KJC(3,NF),HJC(3,NF)
C
LABEL=(ID.AND.7777 0077 0077 7777 7700B) .OR.
* 0000 5000 5000 0000 0057B
WRITE(6,100)
100 FORMAT(1H1/1H ,20X,39HCARTESIAN CO-ORDINATES OF JOINT CENTRES)
LINES=23
DO 150 J=1,NF
IF(J.EQ.1)WRITE(6,110)
110 FORMAT(31H0FRAME ***** ANKLE *****4X
* 21H***** KNEE *****4X,21H***** HIP *****/
* 5H NO.3125H X Y Z)
LINES=LINES+1
IF(MOD(J,5).NE.1)GOTO 140
WRITE(6,120)
120 FORMAT(1H ,I4,2X,3F8.4,1X,3F8.4,1X,3F8.4,1X,2F8.4)
LINES=LINES+1
IF(LINES.LT.58) GOTO 140
WRITE(6,130)LABEL
130 FORMAT(1H1,A10)
WRITE(6,110)
WRITE(6,120)
LINES=6
140 SHANK=SQRT((AJC(1,J)-KJC(1,J))**2+(AJC(2,J)-KJC(2,J))**2+(AJC(3,J)-
1 -KJC(3,J))**2)
THIGH=SQRT((KJC(1,J)-HJC(1,J))**2+(KJC(2,J)-HJC(2,J))**2+(KJC(3,J)-
1 -HJC(3,J))**2)
WRITE(6,120)J,(AJC(K,J),K=1,3),(KJC(K,J),K=1,3),(HJC(K,J),K=1,3)
1 SHANK,THIGH
150 CONTINUE
RETURN
END

```

```

SUBROUTINE TMAT(I,T,X,Y,Z)
DIMENSION T(3,3),X(11,125),Y(11,125),Z(11,125)
COMMON /BLOCK2/ AJC(3,125),KJC(3,125),XL(3)
COMMON /LADO/ LEFIDE,IIDE,JIDE,LSIDE,JBIDE,LBIDE
LOGICAL LEFIDE
VKMX=X((IIDE+3),I)-X(JBIDE,I)
VKMY=Y((IIDE+3),I)-Y(JBIDE,I)
VKMZ=Z((IIDE+3),I)-Z(JBIDE,I)
VLKX=X(JBIDE,I)-X(LBIDE,I)
VLKY=Y(JBIDE,I)-Y(LBIDE,I)
VLKZ=Z(JBIDE,I)-Z(LBIDE,I)
S=-(VKMX*VLKX+VKMY*VLKY+VKMZ*VLKZ)/(VKMX*VKMX+VKMY*VKMY+VKMZ*VKMZ)
CL1=-VLKX-S*VKMX
CM1=-VLKY-S*VKMY
CN1=-VLKZ-S*VKMZ
CL=SQRT(CL1*CL1+CM1*CM1+CN1*CN1)
T(1,1)=CL1/CL
T(1,2)=CM1/CL
T(1,3)=CN1/CL
CM=SQRT(VKMX*VKMX+VKMY*VKMY+VKMZ*VKMZ)
T(2,1)=VKMX/CM
T(2,2)=VKMY/CM

```

```

T(2,3)=VKMZ/CM
T(3,1)=T(1,2)*T(2,3)-T(1,3)*T(2,2)
T(3,2)=T(1,3)*T(2,1)-T(1,1)*T(2,3)
T(3,3)=T(1,1)*T(2,2)-T(1,2)*T(2,1)
RETURN
END
TMAT 230
TMAT 240
TMAT 250
TMAT 260
TMAT 270
TMAT 280

SUBROUTINE TSTAT(T)
DIMENSION T(3,3)
COMMON /BLOCK1/ S>X(10),S>Y(10),S>FZ(10)
COMMON /LADO/ LEFSID,I>IDE,J>IDE,LSIDE,JBIDE,LBIDE
LOGICAL LEFSID
VKMX=S>X(I>IDE+3)-S>X(J>IDE)
VKMY=S>Y(I>IDE+3)-S>Y(J>IDE)
VKMZ=S>FZ(I>IDE+3)-S>FZ(J>IDE)
VLKX=S>X(J>IDE)-S>X(LSIDE)
VLKY=S>Y(J>IDE)-S>Y(LSIDE)
VLKZ=S>FZ(J>IDE)-S>FZ(LSIDE)
S=- (VKMX*VLKX+VKMY*VLKY+VKMZ*VLKZ)/(VKMX*VKMX+VKMY*VKMY+VKMZ*VKMZ)
CL1=-VLKX-S*VKMX
CM1=-VLKY-S*VKMY
CN1=-VLKZ-S*VKMZ
CL=CL1*CL1+CM1*CM1+CN1*CN1
CL=SQR(T(CL))
T(1,1)=CL1/CL
T(1,2)=CM1/CL
T(1,3)=CN1/CL
CL2=VKMX
CM2=VKMY
CN2=VKMZ
CM=CL2*CL2+CM2*CM2+CN2*CN2
CM=SQR(T(CM))
T(2,1)=CL2/CM
T(2,2)=CM2/CM
T(2,3)=CN2/CM
C
C THE CROSS PRODUCT TO DEFINE THE 3RD AXIS
C
T(3,1)=T(1,2)*T(2,3)-T(1,3)*T(2,2)
T(3,2)=T(1,3)*T(2,1)-T(1,1)*T(2,3)
T(3,3)=T(1,1)*T(2,2)-T(1,2)*T(2,1)
RETURN
END
TSTAT 10
TSTAT 20
TSTAT 30
TSTAT 40
TSTAT 50
TSTAT 60
TSTAT 70
TSTAT 80
TSTAT 90
TSTAT100
TSTAT110
TSTAT120
TSTAT130
TSTAT140
TSTAT150
TSTAT160
TSTAT170
TSTAT180
TSTAT190
TSTAT200
TSTAT210
TSTAT220
TSTAT230
TSTAT240
TSTAT250
TSTAT260
TSTAT270
TSTAT280
TSTAT290
TSTAT300
TSTAT310
TSTAT320
TSTAT330
TSTAT340
TSTAT350
TSTAT360

PROGRAM CHKRD (INPUT,OUTPUT,TAPE5=INPUT,TAPE6=OUTPUT)
DIMENSION IR(8),IS(8),XUXU(10),ZUZU(10),IIR(13),IIS(13),
1 XAXA(10),S>X(8),S>Y(8),S>FZ(8)
DIMENSION X1(1320),Y1(1320),Z1(1560),Y2(1560)
DIMENSION IDENT(6)
INTEGER SFRAME,FFRAME
REAL IIR,IIS,IR,IS,KJC,KNEVEL,KNEACC
LOGICAL LEFSID,NEWMAN,QIDENT
COMMON /CHECK/ NCHECK,NF,SFRAME,NSIDE,NFBY11,FFRAME,NFRONT,NFBY13
DATA LAD02/3HKLI/
CHKRD 10
CHKRD 20
CHKRD 30
CHKRD 40
CHKRD 50
CHKRD 60
CHKRD 70
CHKRD 80
CHKRD 90
CHKRD100
CHKRD110
CHKRD120
CHKRD130
CHKRD140
CHKRD150
CHKRD160
CHKRD170
CHKRD180
CHKRD190
CHKRD200
CHKRD210
CHKRD220
CHKRD230
CHKRD240
CHKRD250
CHKRD260
CHKRD270
CHKRD280
CHKRD290
CHKRD300
CHKRD310
CHKRD320
CHKRD330
CHKRD340
CHKRD350
CHKRD360

C READ IN CONSTANTS FOR PATIENT, AND CALCULATE VECTOR LOCATING HIP-
C JOINT CENTRES FROM DISTANCE BETWEEN A.S.I. SPINES.
C
100 CALL INPCON(BH,BM,D67,D78,D86,IDENT(1),NEXTID)
WRITE(6,110)IDENT(1)
CHKRD150
CHKRD160
110 FORMAT(35HIPATIENT CONSTANT> READ FROM DECK ,A9,1H.)
CHKRD170
CHKRD180
C READ IN STATIC DATA FROM FILM OBSERVATIONS.
C
CALL INPKIN (IR,IS,NCHECK,IDENT(2),NEXTID)
WRITE(6,120)IDENT(2)
CHKRD210
CHKRD220
120 FORMAT(35H STATIC >IDE DATA READ FROM DECK ,A9,1H.)
CHKRD230
CHKRD240
IF(NCHECK.NE.8)CALL ABORT
CALL INPKIN (IIR,IIS,NCHECK,IDENT(3),NEXTID)
WRITE(6,130)IDENT(3)
CHKRD250
CHKRD260
130 FORMAT(35H STATIC FRONT DATA READ FROM DECK ,A9,1H.)
CHKRD270
CHKRD280
IF(NCHECK.NE.13)CALL ABORT
CHKRD290
C READ FRAME NUMBERS FOR EVENTS, AND FRAME COUNT.
C
140 CALL INPKMK(LH>,LTO,NH>,NTO,NF,IDENT(4),NEXTID)
WRITE(6,150)IDENT(4)
CHKRD320
CHKRD330
150 FORMAT(35H FRAME NUMBERS READ FROM DECK ,A9,1H.)
CHKRD340
CHKRD350
C READ KINEMATIC DATA. SFRAME IS THE NUMBER OF POINTS PER FRAME IN
C >IDE VIEW, INCLUDING THE FIRST THREE POINTS OF THE GRID.
CHKRD360
CHKRD370

```

```

C   FFRAME IS THE SAME FOR THE FRONT VIEW.  FOR EACH VIEW THE
C   NUMBER OF FRAMES IS CHECKED AGAINST NF.
C
C   CALL INPKIN (X1,Y1,N>SIDE,IDENT(5),NEXTID)
C   WRITE(6,160)IDENT(5)
160  FORMAT(35H DYNAMIC >SIDE DATA READ FROM DECK ,A9,1H.)
C   >FRAME=11
C   IF((NF>>FRAME).NE.N>SIDE)CALL ABORT
C   CALL INPKIN(Z1,Y2,NFRONT,IDENT(6),NEXTID)
C   WRITE(6,170)IDENT(6)
170  FORMAT(35H DYNAMIC FRONT DATA READ FROM DECK ,A9,1H.)
C   FFRAME=13
C   IF((NF>>FFRAME).NE.NFRONT)CALL ABORT
C
C   IF(NEXTID.EQ.0)STOP
C   IF(NEWMAN(IDENT(2),NEXTID))GOTO 100
C   WRITE(6,900)IDENT(1)
900  FORMAT(35HOPATIENT CONSTANT> RETAINED FROM ,A9,1H.)
C   WRITE(6,910)IDENT(2)
910  FORMAT(35H STATIC >SIDE DATA RETAINED FROM ,A9,1H.)
C   WRITE(6,920)IDENT(3)
920  FORMAT(35H STATIC FRONT DATA RETAINED FROM ,A9,1H.)
C   GOTO 140
C   END

PROGRAM COMPARE(TAPE1,TAPE2,OUTPUT,TAPE6=OUTPUT)
C
C COMPARES THE TWO CODED FILES> TAPE1 AND TAPE2.  WRITES TO OUTPUT.
C LINE LENGTH PROCESSED IS 80 CHARACTER>.  NUMBER OF BAD LINES>
C COMPARED IS LIMITED TO MAXBAD, SET ON LINE COMPAR90.
C
C   DIMENSION L1(8),L2(8)
C   DATA LINCNT / 0 /
C   DATA MAXBAD / 20 /
C
C   REWIND 1
C   REWIND 2
100  READ (1,110) L1
110  FORMAT (8A10)
C   READ (2,110) L2
C   IF (EOF(1).NE.0.) GOTO 160
C   IF (EOF(2).NE.0.) GOTO 190
C   LINCNT=LINCNT+1
C   DO 120 J=1,8
C   IF (L1(J).NE.L2(J)) GOTO 130
120  CONTINUE
C   GOTO 100
130  WRITE (6,140) LINCNT,L1,L2
140  FORMAT (5H0LINE,I4,9H MISMATCH,4X,8A10/1H ,21X,8A10)
C   MAXBAD=MAXBAD-1
C   IF (MAXBAD.NE.0) GOTO 100
C   WRITE (6,150)
150  FORMAT (22H0COMPARISON ABANDONED./1H0)
C   STOP
160  IF (EOF(2).EQ.0.) GOTO 180
C   WRITE (6,170) LINCNT
170  FORMAT (23H0COMPARISON COMPLETE. ,15,17H LINES PROCESSED./1H0)
C   STOP
180  NDIST=1
C   GOTO 200
190  NDIST=2
200  WRITE (6,210) NDIST,LINCNT
210  FORMAT (24H0UNEQUAL LENGTH>.  FILE,12,11H ENDS AFTER,15,
C   , 7H LINES>./1H0)
C   STOP
C   END

SUBROUTINE CH11TB(NAMEX,NAMEY,X,Y,NDIM1,NDIM2)
C
C TABULATES PAIRS OF CO-ORDINATES IN THE ARRAYS X(NDIM1,NDIM2) AND
C Y(NDIM1,NDIM2).  THE ACTUAL VALUES OF X(J,1),Y(J,1),J=1,NDIM1)
C ARE LISTED FIRST, FOLLOWED BY SCALED DIFFERENCES> BETWEEN
C SUCCESSIVE CORRESPONDING ELEMENTS.  NDIM1 MUST BE .LE. 11.
C
C NAMEX, NAMEY ARE LEFT-JUSTIFIED CHARACTER STRINGS IDENTIFYING THE
C VARIABLE> TABULATED.  A POSSIBLE CALL MIGHT HAVE THE FORM -
C
C   CALL CH11TB(5HXX123,5HY123,XX123,YY123,9,120)
C
C   DIMENSION LDIFFS(22),X(NDIM1,NDIM2),Y(NDIM1,NDIM2)
C   DATA IBLANK / 4H /

```

CHKRD380  
CHKRD390  
CHKRD400  
CHKRD410  
CHKRD420  
CHKRD430  
CHKRD440  
CHKRD450  
CHKRD460  
CHKRD470  
CHKRD480  
CHKRD490  
CHKRD500  
CHKRD510  
CHKRD520  
CHKRD530  
CHKRD540  
CHKRD550  
CHKRD560  
CHKRD570  
CHKRD580  
CHKRD590  
CHKRD600  
CHKRD610

COMPAR10  
COMPAR20  
COMPAR30  
COMPAR40  
COMPAR50  
COMPAR60  
COMPAR70  
COMPAR80  
COMPAR90  
COMPA100  
COMPA110  
COMPA120  
COMPA130  
COMPA140  
COMPA150  
COMPA160  
COMPA170  
COMPA180  
COMPA190  
COMPA200  
COMPA210  
COMPA220  
COMPA230  
COMPA240  
COMPA250  
COMPA260  
COMPA270  
COMPA280  
COMPA290  
COMPA300  
COMPA310  
COMPA320  
COMPA330  
COMPA340  
COMPA350  
COMPA360  
COMPA370  
COMPA380  
COMPA390  
COMPA400  
COMPA410

CH11TB10  
CH11TB20  
CH11TB30  
CH11TB40  
CH11TB50  
CH11TB60  
CH11TB70  
CH11TB80  
CH11TB90  
CH11T100  
CH11T110  
CH11T120  
CH11T130  
CH11T140

```

C
  IF (NDIM1.LE.11) GOTO 110
  WRITE (6,100) NDIM1
100 FORMAT (34HODIMENSION TOO LARGE FOR CHKTBL  =,16)
  RETURN
C
110 WRITE (6,120) NAMEX,NAMEY
120 FORMAT (18H1ARRAY X HAS NAME ,A7,22H AND ARRAY Y HAS NAME ,A7/1H )
  DO 140 J=1,NDIM1
  WRITE (6,130) J,X(J,1),J,Y(J,1)
130 FORMAT (3H0X(,12,7H,1)  =,E15.6,15X,2HY(,12,7H,1)  =,E15.6)
140 CONTINUE
  IF (NDIM2.EQ.1) RETURN
  DIFMAX=0.
  DO 160 J=2,NDIM2
  DO 150 K=1,NDIM1
  DIFF=ABS(X(K,J)-X(K,(J-1)))
  IF (DIFF.GT.DIFMAX) DIFMAX=DIFF
  DIFF=ABS(Y(K,J)-Y(K,(J-1)))
  IF (DIFF.GT.DIFMAX) DIFMAX=DIFF
150 CONTINUE
160 CONTINUE
  AFACTR=ALOG10(999./DIFMAX)
  IF (AFACTR.LT.0.) AFACTR=AFACTR-1.
  FACTOR=10.**INT(AFACTR)
C
  WRITE (6,170) FACTOR
170 FORMAT (1H0/38H DIFFERENCES ARE TABULATED IN THE FORM,1PE7.0,
  * 42H*(X(J,N)-X(J,N-1))) IN THE FOLLOWING TABLE./1H )
  WRITE (6,180) (IBLANK,J,J,J=1,NDIM1)
180 FORMAT (4H N ,9(A4,2H0X,11,4H DY,11),2(A3,2H0X,12,3H DY,12))
  WRITE (6,200)
  LTOP=NDIM1+NDIM1
  LINES=LTOP+9
  DO 220 J=2,NDIM2
  DO 190 K=1,NDIM1
  KK=K+K
  LDIFFS(KK-1)=NEAREST(FACTOR*(X(K,J)-X(K,(J-1))))
  LDIFFS(KK)=NEAREST(FACTOR*(Y(K,J)-Y(K,(J-1))))
190 CONTINUE
  WRITE (6,200) J,(LDIFFS(L),L=1,LTOP)
200 FORMAT (1H ,13,11(17,15))
  IF (MOD(J,5).NE.0) GOTO 220
  WRITE (6,200)
  LINES=LINES+6
  IF (LINES.LT.58) GOTO 220
  WRITE (6,210)
210 FORMAT (1H1)
  WRITE (6,180) (IBLANK,L,L,L=1,NDIM1)
  WRITE (6,200)
  LINES=LINES+3
220 CONTINUE
C
  WRITE (6,210)
  RETURN
  END

  SUBROUTINE CH13TB(NAMEX,NAMEY,X,Y,NDIM1,NDIM2)
C
C TABULATES PAIRS OF CO-ORDINATES IN THE ARRAYS X(NDIM1,NDIM2) AND
C Y(NDIM1,NDIM2). THE ACTUAL VALUES OF X(J,1),Y(J,1),J=1,NDIM1)
C ARE LISTED FIRST, FOLLOWED BY SCALED DIFFERENCES BETWEEN
C SUCCESSIVE CORRESPONDING ELEMENTS. NDIM1 MUST BE .LE. 13.
C
C NAMEX, NAMEY ARE LEFT-JUSTIFIED CHARACTER STRINGS IDENTIFYING THE
C VARIABLES TABULATED. A POSSIBLE CALL MIGHT HAVE THE FORM -
C
C CALL CH13TB(5HXX123,5HY123,XX123,YY123,13,120)
C
C DIMENSION LDIFFS(26),X(NDIM1,NDIM2),Y(NDIM1,NDIM2)
C DATA IBLANK / 4H /
C
C IF (NDIM1.LE.13) GOTO 110
  WRITE (6,100) NDIM1
100 FORMAT (34HODIMENSION TOO LARGE FOR CHKTBL  =,16)
  RETURN
C
110 WRITE (6,120) NAMEX,NAMEY
120 FORMAT (18H1ARRAY X HAS NAME ,A7,22H AND ARRAY Y HAS NAME ,A7/1H )
  DO 140 J=1,NDIM1
  WRITE (6,130) J,X(J,1),J,Y(J,1)
130 FORMAT (3H0X(,12,7H,1)  =,E15.6,15X,2HY(,12,7H,1)  =,E15.6)

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```

140 CONTINUE
    IF (NDIM2.EQ.1) RETURN
    DIFMAX=0.
    DO 160 J=2,NDIM2
    DO 150 K=1,NDIM1
    DIFF=ABS(X(K,J)-X(K,(J-1)))
    IF (DIFF.GT.DIFMAX) DIFMAX=DIFF
    DIFF=ABS(Y(K,J)-Y(K,(J-1)))
    IF (DIFF.GT.DIFMAX) DIFMAX=DIFF
150 CONTINUE
160 CONTINUE
    AFACTR=ALOG10(999./DIFMAX)
    IF (AFACTR.LT.0.) AFACTR=AFACTR-1.
    FACTOR=10.**INT(AFACTR)
C
    WRITE (6,170) FACTOR
170 FORMAT (1H0/38H DIFFERENCES ARE TABULATED IN THE FORM,1PE7.0,
    * 42H*(X(J,N)-X(J,N-1)) IN THE FOLLOWING TABLE./1H )
    WRITE (6,180) (1BLANK,J,J=1,NDIM1)
180 FORMAT (4H N ,9(A2,2HDX,11,4H DY,11),4(A1,2HDX,12,3H DY,12))
    WRITE (6,200)
    LTOP=NDIM1+NDIM1
    LINES=LTOP+9
    DO 220 J=2,NDIM2
    DO 190 K=1,NDIM1
    KK=K+K
    LDIFF=(KK-1)*NEARST(FACTOR*(X(K,J)-X(K,(J-1))))
    LDIFF=(KK)*NEARST(FACTOR*(Y(K,J)-Y(K,(J-1))))
190 CONTINUE
    WRITE (6,200) J,(LDIFF(L),L=1,LTOP)
200 FORMAT (1H ,13,13(15,15))
    IF (MOD(J,5).NE.0) GOTO 220
    WRITE (6,200)
    LINES=LINES+6
    IF (LINES.LT.58) GOTO 220
    WRITE (6,210)
210 FORMAT (1H1)
    WRITE (6,180) (1BLANK,L,L=1,NDIM1)
    WRITE (6,200)
    LINES=3
220 CONTINUE
C
    WRITE (6,210)
    RETURN
    END

PROGRAM DRVFPD(INPUT,OUTPUT,TAPES=INPUT,TAPE6=OUTPUT)
C
C DRIVES INPFPD/CALFPD/LISFPD TO PRODUCE FORCE-PLATE LISTINGS.
C
    DIMENSION X(1920)
100 CALL INPFPD(X,NSETS,IDENT,NEXTID)
    NPNTS=6*NSETS
    CALL LISFPD(X,NSETS,IDENT,NPNTS)
    IF (NEXTID.NE.0) GOTO 100
    STOP
    END
DRVFPD10
DRVFPD20
DRVFPD30
DRVFPD40
DRVFPD50
DRVFPD60
DRVFPD70
DRVFPD80
DRVFPD90
DRVFP100
DRVFP110

PROGRAM DRVQVT(INPUT,OUTPUT,TAPES=INPUT,TAPE6=OUTPUT,TAPER)
C
C
C PULLS OFF FORCE PLATE DATA TO DRIVE OEVENT.
C
    DIMENSION X(3000)
100 CALL INPFPD(X,NSETS,IDENT,NEXTID)
    WRITE (6,144) IDENT,EVNPT
144 FORMAT (35HFORCE PLATE DATA READ FROM DECK ,A9,1H.,10X,
    1 16HEVENT POINTER =,F8.2)
    NPNTS=6*NSETS
    IF (NEXTID.NE.0) GOTO 100
    STOP
    END
10
20
30
40
50
60
70
80
90
100
110
120
130

PROGRAM FIDDLE(TAPES,TAPE6,OUTPUT)
C
C PROCESSES SOURCE DATA FOR NON-STANDARD DECKS SJKLIFULO AND SJKLIHOTO.
C THESE HAVE ONLY TEN TARGETS PER FRAME AND ARE MODIFIED BY FIDDLE,
C WHICH REPEATS THE FIRST TARGET CO-ORDINATES TO ESTABLISH AN
C ELEVEN TARGET STRUCTURE.
C
C FIDDLE READS AN UPDATE COMPILE FILE (USING INPKIN) AND WRITES
FIDDLE10
FIDDLE20
FIDDLE30
FIDDLE40
FIDDLE50
FIDDLE60
FIDDLE70
FIDDLE80

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C      A NEW SOURCE FILE.
C
      DIMENSION X(2000),Y(2000),NX(2000),NY(2000)
100 CALL INPKIN(X,Y,N,IDENT,NEXTID)
110 WRITE(6,120)IDENT
120 FORMAT(6H'DECK',A9/1H /1H )
      DO 130 J=1,N
      NX(J)=NEARST(X(J))
      NY(J)=NEARST(Y(J))
130 CONTINUE
      WRITE(6,140) (NX(J),NY(J),NX(J),NY(J),(NX(J+K),NY(J+K),K=1,9),
      * J=1,N,10)
140 FORMAT(12(1H+,I4,1X),1H )
      IF (NEXTID.NE.0) GOTO 100
      REWIND 6
      STOP
      END

      PROGRAM FPDTBL(INPUT,OUTPUT,TAPE8,TAPES=INPUT,TAPE6=OUTPUT)
C
C  LISTS FORCE-PLATE DATA, UNSMOOTHED BUT CONVERTED TO ABSOLUTE UNITS
C  AND SYNCHRONIZED.
C
C  USES SUBROUTINES CALFPD,INPCON,INFPD,INPKMK,NEARST,NEWMAN,OEVENT,
C  QIDENT
C
      DIMENSION EVNTPT(2),FP1(3000),FP2(3000),IDENT(4),MARK(4),
1  MKLABL(4),NSYNCH(2)
      LOGICAL FUL,NEWMAN,QIDENT
      COMMON /FHLDBK/ FP2
      DATA GCONST / 9.810 /
      DATA IBLANK / 3H /
      DATA IFUL / 3HFUL /
      DATA MKLABL(1) / 3HLHS /
      DATA MKLABL(2) / 3HLTO /
      DATA MKLABL(3) / 3HRHS /
      DATA MKLABL(4) / 3HRT0 /
100 CALL INPCON(BH,BM,D67,D78,DB6,IDENT(1),NEXTID)
      WRITE (6,110) IDENT(1)
110 FORMAT(40H'PATIENT CONSTANTS READ FROM DECK',A9,1H.)
      BWT=BM*GCONST
120 CALL INFPD(FP2,NFPSET,IDENT(2),NEXTID,BM,EVNTPT(1))
      WRITE (6,130) IDENT(2),EVNTPT(1)
130 FORMAT (40H'FIRST FORCE-PLATE DATA READ FROM DECK',A9,1H.,10X,
1  16HEVENT POINTER =,F8.2)
      IF (NFPSET.LE.0) CALL ABORT
      DO 140 J=1,3000
      FP1(J)=FP2(J)
140 CONTINUE
      CALL INFPD(FP2,NFPSET,IDENT(3),NEXTID,BM,EVNTPT(2))
      WRITE (6,150) IDENT(3),EVNTPT(2)
150 FORMAT (40H'SECOND FORCE-PLATE DATA READ FROM DECK',A9,1H.,10X,
1  16HEVENT POINTER =,F8.2)
      IF (NFPSET.LE.0) CALL ABORT
      CALL INPKMK(MARK(1),MARK(2),MARK(3),MARK(4),NF,IDENT(4),NEXTID)
      WRITE (6,160) IDENT(4),MARK,NF
160 FORMAT (40H'FRAME NUMBERS READ FROM DECK',A9,1H.,10X,
1  5I8)
      FUL=QIDENT(IDENT(2),6,8,IFUL)
      IF (FUL) GOTO 170
      NSYNCH(1)=NEARST(EVNTPT(1)+0.5)-MARK(1)
      NSYNCH(2)=NEARST(EVNTPT(2)+0.5)-MARK(4)
      GOTO 180
170 NSYNCH(1)=NEARST(EVNTPT(1)+0.5)-MARK(2)
      NSYNCH(2)=NEARST(EVNTPT(2)+0.5)-MARK(3)
180 LABEL=(IDENT(2).AND.MASK(12)).OR.SHIFT(1R/,42).OR.
1  SHIFT(IDENT(2),AND,77 7777 7700B,12)
      WRITE (6,190) LABEL,BM,BWT
190 FORMAT (1H1/6(1H /),1H ,35X,5H'CASE',A7,8X,18H'MASS OF PATIENT =,
1  F7.2,4H KG.,7X,9H'WEIGHT =,F7.1,8H NEWTONS/1H )
      WRITE (6,200)
200 FORMAT (1H0,35X,45HCINE ***** FORCE PLATE 1 *****
1  35H ***** FORCE PLATE 2 *****/1H ,35X,11H'FRAME EVENT,
2  2(3(9H 'FORCE'),8H MOMENT )/1H ,35X,10H NO.
3  2(35H X Y Z Y )/1H )
      LINES=14
      DO 250 J=1,NF
      IMARK=IBLANK
      DO 210 K=1,4
      IF (J.EQ.MARK(K)) IMARK=MKLABL(K)
210 CONTINUE
      J1=J+NSYNCH(1)
      FIDDL90
      FIDDL100
      FIDDL110
      FIDDL120
      FIDDL130
      FIDDL140
      FIDDL150
      FIDDL160
      FIDDL170
      FIDDL180
      FIDDL190
      FIDDL200
      FIDDL210
      FIDDL220
      FIDDL230
      FIDDL240
      FIDDL250

      FPDTBL10
      FPDTBL20
      FPDTBL30
      FPDTBL40
      FPDTBL50
      FPDTBL60
      FPDTBL70
      FPDTBL80
      FPDTBL90
      FPDTBL100
      FPDTBL110
      FPDTBL120
      FPDTBL130
      FPDTBL140
      FPDTBL150
      FPDTBL160
      FPDTBL170
      FPDTBL180
      FPDTBL190
      FPDTBL200
      FPDTBL210
      FPDTBL220
      FPDTBL230
      FPDTBL240
      FPDTBL250
      FPDTBL260
      FPDTBL270
      FPDTBL280
      FPDTBL290
      FPDTBL300
      FPDTBL310
      FPDTBL320
      FPDTBL330
      FPDTBL340
      FPDTBL350
      FPDTBL360
      FPDTBL370
      FPDTBL380
      FPDTBL390
      FPDTBL400
      FPDTBL410
      FPDTBL420
      FPDTBL430
      FPDTBL440
      FPDTBL450
      FPDTBL460
      FPDTBL470
      FPDTBL480
      FPDTBL490
      FPDTBL500
      FPDTBL510
      FPDTBL520
      FPDTBL530
      FPDTBL540
      FPDTBL550
      FPDTBL560
      FPDTBL570
      FPDTBL580
      FPDTBL590
      FPDTBL600
      FPDTBL610
      FPDTBL620
      FPDTBL630
      FPDTBL640

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      J2=J+NSYNCH(2)
      WRITE (6,220) J,IMARK,FP1(J1),FP1(J1+500),FP1(J1+1000),
1      FP1(J1+2000),FP2(J2),FP2(J2+500),FP2(J2+1000),FP2(J2+2000)
220  FORMAT (1H ,35X,14,3X,A3,2(3(F8.1,1X),F8.3))
      IF (MOD(J,5).NE.0) GOTO 250
      WRITE (6,230)
230  FORMAT (1H )
      LINES=LINES+6
      IF (J.GE.(NF-1)) GOTO 250
      IF (LINES.LE.85) GOTO 250
      WRITE (6,240) LABEL
240  FORMAT (1H1/6(1H /),1H ,35X,5HCASE ,A7,10H CONTINUED/1H )
      WRITE (6,200)
      LINES=14
250  CONTINUE
      IF (LINES.LT.67) WRITE (6,260)
260  FORMAT (1H1)
      IF (NEXTID.NE.0) GOTO 270
      WRITE (6,260)
      STOP
270  IF (NEWMAN(IDENT(1),NEXTID)) GOTO 100
      WRITE (6,280) IDENT(1)
280  FORMAT (40HPATIENT CONSTANT> RETAINED FROM DECK   ,A9,1H.)
      GOTO 120
      END

      PROGRAM KINCHK(INPUT,OUTPUT,TAPES=INPUT,TAPE6=OUTPUT)
C
C USES INPKIN TO READ DECK> OF KINEMATIC DATA AND THEN LISTS THEM WITH
C CO-ORDINATE PAIR> FOR EACH MARKER ARRANGED IN COLUMNS.
C
C KINSMT AND KINREG ARE THEN CALLED TO SHOW UP DEVIANT POINTS IN THE
C DATA SET.
C
C USES SUBROUTINES INPKIN, KINREG, KINSMT, AND QIDENT.
C
      DIMENSION IDENT(2),X(2000),Y(2000)
      INTEGER VALUES
      LOGICAL QIDENT,STATIC
      DATA IBLANK / 3H /
      DATA IX / 2H X /
      DATA IXNEG / 2H-X /
      DATA IY / 2H Y /
      DATA IZ / 2H Z /
      DATA VALUES / 10H VALUES /
100  CALL SIMKIN(X,Y,N,IDENT,NEXTID)
      STATIC=QIDENT(IDENT,6,9,4HSTAT)
      NCOLS=11
      IF (STATIC) NCOLS=8
      L1=IX
      L2=IY
      IF (.NOT.QIDENT(IDENT,3,5,3HXR2)) GOTO 110
      L1=IXNEG
      GOTO 120
110  IF (.NOT.QIDENT(IDENT,3,5,3HXR3)) GOTO 120
      L1=IZ
      NCOLS=13
      IF (STATIC) NCOLS=11
120  NFRAME=N/NCOLS
      WRITE (6,130) IDENT(1)
130  FORMAT (1H1/10H DECKNAME ,A9/1H )
      WRITE (6,140) N,NFRAME
140  FORMAT (25HNUMBER OF POINT> READ =,16,15X,
      * 33HCORRESPONDING NUMBER OF FRAMES =,15)
      IF ((NFRAME*NCOLS).NE.N) WRITE (6,150)
150  FORMAT (1H,98X,33HWARNING = PRODUCT IS NOT EXACT.)
      NF=1
      NFIRST=1
      NLAST=8
160  NLines=8
      JFIRST=NFIRST
      JLAST=NLAST
170  WRITE (6,180) (IBLANK,J,J=NFIRST,NLAST)
180  FORMAT (6HOFRAME,8(A3,9H* MARKER ,12,2H *))
      WRITE (6,190) (L1,L2,J=NFIRST,NLAST)
190  FORMAT (6H NO. ,8(5X,A2,4X,A2,3X))
      WRITE (6,200)
200  FORMAT (1H )
210  WRITE (6,220) NF,(X(J),Y(J),J=JFIRST,JLAST)
220  FORMAT (1H ,14,8(14X,2F6.0))
      IF (MOD(NF,5).NE.0) GOTO 230
      WRITE (6,200)
      KINCHK10
      KINCHK20
      KINCHK30
      KINCHK40
      KINCHK50
      KINCHK60
      KINCHK70
      KINCHK80
      KINCHK90
      KINCHK100
      KINCHK110
      KINCHK120
      KINCHK130
      KINCHK140
      KINCHK150
      KINCHK160
      KINCHK170
      KINCHK180
      KINCHK190
      KINCHK200
      KINCHK210
      KINCHK220
      KINCHK230
      KINCHK240
      KINCHK250
      KINCHK260
      KINCHK270
      KINCHK280
      KINCHK290
      KINCHK300
      KINCHK310
      KINCHK320
      KINCHK330
      KINCHK340
      KINCHK350
      KINCHK360
      KINCHK370
      KINCHK380
      KINCHK390
      KINCHK400
      KINCHK410
      KINCHK420
      KINCHK430
      KINCHK440
      KINCHK450
      KINCHK460
      KINCHK470
      KINCHK480
      KINCHK490
      KINCHK500
      KINCHK510
      KINCHK520
      KINCHK530
      KINCHK540
      KINCHK550
      KINCHK560

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NLINES=NLINES+6
230 NF=NF+1
    JFIRST=JFIRST+NCOLS
    IF (JFIRST.GT.N) GOTO 260
    JLAST=JLAST+NCOLS
    IF (JLAST.GT.N) JLAST=N
    IF (NLINES.LT.59) GOTO 210
240 WRITE (6,130) IDENT(1)
    NLINES=6
    IF (NF.NE.1) GOTO 170
    WRITE (6,250)
250 FORMAT (1H0)
    GOTO 160
260 IF (NLAST.EQ.NCOLS) GOTO 280
    NF=1
    NFIRST=9
    NLAST=NCOLS
    IF (.NOT.>STATIC) GOTO 240
    WRITE (6,270) IDENT(1)
270 FORMAT (5(1H0/),10H DECKNAME ,A9/1H )
    GOTO 160
280 WRITE (6,130) IDENT(1)
    IDENT(2)=SHIFT(((L1.AND.MASK(12)).OR.(VALUES.AND.
1 (.NOT.MASK(12))))),54)
    CALL KIN>MT(IDENT,NCOLS,NFRAME,X,10)
    IDENT(2)=SHIFT(((L2.AND.MASK(12)).OR.(VALUES.AND.
1 (.NOT.MASK(12))))),54)
    CALL KIN>MT(IDENT,NCOLS,NFRAME,Y,10)
    IF (NEXTID.EQ.0) STOP
    GOTO 100
END

PROGRAM KINREF(INPUT,OUTPUT,TAPES=INPUT,TAPE6=OUTPUT)
C
C MEAN VALUES FOR REFERENCE MARKERS. FOR USE ON P1/FULO.
C
    DIMENSION X(1600),Y(1600),SX(3),SY(3)
    LOGICAL QIDENT
100 CALL INPKIN(X,Y,N,IDENT,NEXTID)
    N>STEP=11
    IF (QIDENT(IDENT,4,5,2HF3)) N>STEP=13
    DO 110 J=1,3
        SX(J)=0.
        SY(J)=0.
110 CONTINUE
    NPNTS=0
    DO 130 K=1,N,N>STEP
        DO 120 J=1,3
            SX(J)=SX(J)+X(K+J-1)
            SY(J)=SY(J)+Y(K+J-1)
120 CONTINUE
        NPNTS=NPNTS+1
130 CONTINUE
    WRITE (6,140) IDENT, (SX(J),SY(J),J=1,3)
140 FORMAT (1H0/1H0,A9,3(2F12.1,6X))
    FACTOR=1./FLOAT(NPNTS)
    DO 150 J=1,3
        SX(J)=FACTOR*SX(J)
        SY(J)=FACTOR*SY(J)
150 CONTINUE
    WRITE (6,160) N, (SX(J),SY(J),J=1,3),NPNTS
160 FORMAT (1H0,19,1X,3(2F12.2,6X),110)
    IF (NEXTID.NE.0) GOTO 100
    STOP
END

SUBROUTINE KINREG(ND>BD1,ND,YEXT,NK)
    DIMENSION YEXT(ND>BD1,ND)
    DIMENSION SUMCY(30),SUMSY(30)
    DIMENSION A(30),B(30),SUMSOR(31)
    REAL ICPEXT
    COMMON /SMOOTH/ A,B,C,COVERT,GRAD,GRDEXT,ICPEXT,STEP,SUMSOR,YM,YO
    DATA T / 0.02000000 /
    DATA TWOPI / 6.283185307 /
    N=ND-1
    RINT=FLOAT(N)
    NA=NK
    C=TWOPI/RINT
    COVERT=C/T
    GRAD=(YEXT(1,ND)-YEXT(1,1))/RINT
    >STEP=(YEXT(1,ND)-YEXT(1,1))

```

KINCH570  
KINCH580  
KINCH590  
KINCH600  
KINCH610  
KINCH620  
KINCH630  
KINCH640  
KINCH650  
KINCH660  
KINCH670  
KINCH680  
KINCH690  
KINCH700  
KINCH710  
KINCH720  
KINCH730  
KINCH740  
KINCH750  
KINCH760  
KINCH770  
KINCH780  
KINCH790  
KINCH800  
KINCH810  
KINCH820  
KINCH830  
KINCH840  
KINCH850  
KINCH860  
KINCH870

KINREF10  
KINREF20  
KINREF30  
KINREF40  
KINREF50  
KINREF60  
KINREF70  
KINREF80  
KINREF90  
KINRE100  
KINRE110  
KINRE120  
KINRE130  
KINRE140  
KINRE150  
KINRE160  
KINRE170  
KINRE180  
KINRE190  
KINRE200  
KINRE210  
KINRE220  
KINRE230  
KINRE240  
KINRE250  
KINRE260  
KINRE270  
KINRE280  
KINRE290  
KINRE300  
KINRE310  
KINRE320  
KINRE330

KINREG10  
KINREG20  
KINREG30  
KINREG40  
KINREG50  
KINREG60  
KINREG70  
KINREG80  
KINREG90  
KINRE100  
KINRE110  
KINRE120  
KINRE130  
KINRE140  
KINRE150

```

GRAD=STEP/RINT
YO=YEXT(1,1)-GRAD
SUMY=0.
SUMSQ=0.
DO 100 K=1,NA
SUMCY(K)=0.
SUMSY(K)=0.
100 CONTINUE
DO 120 I=1,N
YI=YEXT(1,I)-YO-GRAD*FLOAT(I)
SUMY=SUMY+YI
SUMSQ=SUMSQ+YI*YI
XI=C*FLOAT(I-1)
DO 110 K=1,NA
ARG=K*XI
SUMCY(K)=SUMCY(K)+COS(ARG)*YI
SUMSY(K)=SUMSY(K)+SIN(ARG)*YI
110 CONTINUE
120 CONTINUE
YM=SUMY/RINT
CYY=SUMSQ-SUMY*YM
SUMSQR(1)=CYY
DO 130 K=1,NA
A(K)=SUMCY(K)*(2./RINT)
B(K)=SUMSY(K)*(2./RINT)
CYY=CYY-A(K)*SUMCY(K)-B(K)*SUMSY(K)
SUMSQR(K+1)=CYY
130 CONTINUE
ICPEXT=YEXT(1,1)+YM
GRDEXT=GRAD/T
RETURN
END

```

KINRE160  
KINRE170  
KINRE180  
KINRE190  
KINRE200  
KINRE210  
KINRE220  
KINRE230  
KINRE240  
KINRE250  
KINRE260  
KINRE270  
KINRE280  
KINRE290  
KINRE300  
KINRE310  
KINRE320  
KINRE330  
KINRE340  
KINRE350  
KINRE360  
KINRE370  
KINRE380  
KINRE390  
KINRE400  
KINRE410  
KINRE420  
KINRE430  
KINRE440  
KINRE450  
KINRE460  
KINRE470

```

SUBROUTINE KIN>MT(LABEL,ND>BD1,ND,Y,NK)
C
C PROVIDES AN INTERFACE THROUGH WHICH THE HARMONIC ANALYSIS ROUTINE
C KINREG IS CALLED, TO PROVIDE CHECKING OF KINEMATIC DATA.
C
DIMENSION LABEL(2),Y(ND>BD1,ND)
DIMENSION A(30),B(30),SUMSQR(31)
REAL ICPEXT
COMMON /SMOOTH/ A,B,C,COVERT,GRAD,GRDEXT,ICPEXT,STEP,SUMSQR,YM,YO
C
WRITE (6,90)
90 FORMAT (1H0)
WRITE (6,100) LABEL
100 FORMAT (52H SMOOTHING AND DIFFERENTIATION BY FOURIER REGRESSION,
1 16H - DECKNAME ,2A10)
IF (NK.EQ.0) NK=NEAREST(FLOAT(ND-1)/20.)
WRITE (6,160)
160 FORMAT (1H0/50H FRAME MARKER INPUT FITTED,
1 33H RESIDUAL RESID. //22H NO. NO.
2 51H VALUE VALUE DIFFERENCE
3 13H>D.DEVIATION/1H )
DO 200 JCOLS=1,ND>BD1
CALL KINREG(ND>BD1,ND,Y(JCOLS,1),NK)
YOYM=YO+YM
STDEV=SQRT(SUMSQR(NK+1)/FLOAT(ND-NK-NK-3))
DO 190 I=1,ND
YCHECK=YOYM+GRAD*FLOAT(I)
CII=C*FLOAT(I-1)
DO 170 J=1,NK
RJCII=FLOAT(J)*CII
YCHECK=YCHECK+A(J)*COS(RJCII)+B(J)*SIN(RJCII)
170 CONTINUE
YDIFF=Y(JCOLS,I)-YCHECK
RATIO=YDIFF/STDEV
IF (ABS(RATIO).GT.2.3)
1 WRITE (6,180) I,JCOLS,Y(JCOLS,I),YCHECK,YDIFF,RATIO
180 FORMAT (1H ,I4,I10,3X,E18.5,2E16.5,F13.2)
190 CONTINUE
200 CONTINUE
RETURN
END

```

KIN>MT10  
KIN>MT20  
KIN>MT30  
KIN>MT40  
KIN>MT50  
KIN>MT60  
KIN>MT70  
KIN>MT80  
KIN>MT90  
KIN>M100  
KIN>M110  
KIN>M120  
KIN>M130  
KIN>M140  
KIN>M150  
KIN>M160  
KIN>M170  
KIN>M180  
KIN>M190  
KIN>M200  
KIN>M210  
KIN>M220  
KIN>M230  
KIN>M240  
KIN>M250  
KIN>M260  
KIN>M270  
KIN>M280  
KIN>M290  
KIN>M300  
KIN>M310  
KIN>M320  
KIN>M330  
KIN>M340  
KIN>M350  
KIN>M360  
KIN>M370  
KIN>M380  
KIN>M390  
KIN>M400  
KIN>M410

```

PROGRAM KMKCHK(TAPES,OUTPUT,TAPE6=OUTPUT)
C
LOGICAL FUL,OIDENT
C
WRITE (6,100)
LINES=0

```

KMKCHK10  
KMKCHK20  
KMKCHK30  
KMKCHK40  
KMKCHK50  
KMKCHK60

```

100 FORMAT (50H) IDENT          LHS      LTO      RHS      RTO,      KMKCHK70
      * 13H      NFRAMES /1H )      KMKCHK80
110 CALL INPKMK(LHS,LTO,NHS,NTD,NF,ID,NEXTID)      KMKCHK90
      FUL=QIDENT(ID,6,8,3HFUL)      KMKCH100
      WRITE (6,120) ID,LHS,LTO,NHS,NTD,NF      KMKCH110
120 FORMAT (1H ,A9,5I10)      KMKCH120
      LINES=LINES+1      KMKCH130
      IF (MOD(LINES,5).EQ.0) WRITE (6,120)      KMKCH140
      IF (LHS.LT.0) WRITE (6,130)      KMKCH150
130 FORMAT (1H,60X,6(10H*****))      KMKCH160
      IF (NHS.LE.NTD) WRITE (6,130)      KMKCH170
      IF (LHS.LE.LTO) WRITE (6,130)      KMKCH180
      IF (FUL) GOTO 140      KMKCH190
      IF (NTD.LE.LHS) WRITE (6,130)      KMKCH200
      IF (NF.LE.NHS) WRITE (6,130)      KMKCH210
      GOTO 150      KMKCH220
140 IF (LTO.LE.NHS) WRITE (6,130)      KMKCH230
      IF (NF.LE.LHS) WRITE (6,130)      KMKCH240
150 IF (NEXTID.NE.0) GOTO 110      KMKCH250
      STOP      KMKCH260
      END      KMKCH270

      SUBROUTINE LISFPD(X,NSETS,IDENT,NPNTS)      LISFPD10
C      C LISFPD FORCE PLATE DATA FROM INPPFD      LISFPD20
C      C      DIMENSION X(NPNTS)      LISFPD30
C      C      J=1      LISFPD40
100 WRITE (6,110) IDENT      LISFPD50
110 FORMAT (17H1***** DECKNAME ,A9,7H ***** )      LISFPD60
      IF (J.NE.1) WRITE (6,120)      LISFPD70
120 FORMAT (1H,33X,10HCONTINUED.)      LISFPD80
      WRITE (6,130)      LISFPD90
130 FORMAT (52H0POINT ***** FORCES (NEWTONS) ***** ,      LISFP100
      1 46H ***** MOMENTS (NEWTON METRE) *****/7H NO. ,      LISFP110
      2 2(46H X-COMPONENT Y-COMPONENT Z-COMPONENT )/1H )      LISFP120
      NLINES=5      LISFP130
140 WRITE (6,150) J,(X(K),K=J,NPNTS,NSETS)      LISFP140
150 FORMAT (1H ,14,2(3X,3(F12.5,1X)))      LISFP150
      J=J+1      LISFP160
      IF (J.GT.NSETS) RETURN      LISFP170
      IF (MOD(J,5).NE.1) GOTO 140      LISFP180
      NLINES=NLINES+6      LISFP190
      IF (NLINES.GT.57) GOTO 100      LISFP200
      WRITE (6,160)      LISFP210
160 FORMAT (1H )      LISFP220
      GOTO 140      LISFP230
      END      LISFP240
      LISFP250
      LISFP260
      LISFP270

      PROGRAM LISKIN(INPUT,OUTPUT,TAPES=INPUT,TAPE6=OUTPUT)      LISKN 10
C      C      C USES INPKIN TO READ DECKS OF KINEMATIC DATA AND THEN LISTS THEM WITH      LISKN 20
C      C      C CO-ORDINATE PAIRS FOR EACH MARKER ARRANGED IN COLUMNS.      LISKN 30
C      C      C USES SUBROUTINES QIDENT AND INPKIN.      LISKN 40
C      C      C      DIMENSION X(2000),Y(2000)      LISKN 50
C      C      C      LOGICAL QIDENT,STATIC      LISKN 60
C      C      C      DATA IBLANK / 3H /      LISKN 70
C      C      C      DATA IX / 2H X /      LISKN 80
C      C      C      DATA IXNEG / 2H-X /      LISKN 90
C      C      C      DATA IY / 2H Y /      LISKN100
C      C      C      DATA IZ / 2H Z /      LISKN110
100 CALL INPKIN(X,Y,N,IDENT,NEXTID)      LISKN120
      STATIC=QIDENT(IDENT,6,9,4H,TAT)      LISKN130
      NCOLS=11      LISKN140
      IF (STATIC) NCOLS=8      LISKN150
      L1=IX      LISKN160
      L2=IY      LISKN170
      IF (.NOT.QIDENT(IDENT,3,5,3HKR2)) GOTO 110      LISKN180
      L1=IXNEG      LISKN190
      GOTO 120      LISKN200
110 IF (.NOT.QIDENT(IDENT,3,5,3HKF3)) GOTO 120      LISKN210
      L1=IZ      LISKN220
      NCOLS=13      LISKN230
      IF (STATIC) NCOLS=11      LISKN240
120 NFRAME=N/NCOLS      LISKN250
      WRITE (6,130) IDENT      LISKN260
130 FORMAT (1H1/10H DECKNAME ,A9/1H )      LISKN270
      WRITE (6,140) N,NFRAME      LISKN280
      LISKN290
      LISKN300
      LISKN310

```

```

140 FORMAT (25HNUMBER OF POINTS READ =,I6,15X,
* 33HCORRESPONDING NUMBER OF FRAMES =,I5)
IF ((NFRAME*NCOLS).NE.N) WRITE (6,150)
150 FORMAT (1H+,98X,33HWARNING - PRODUCT IS NOT EXACT.)
NF=1
NFIRST=1
NLA5T=8
160 NLINE5=8
JFIR5T=NFIRST
JLA5T=NLA5T
170 WRITE (6,180) (IBLANK,J,J=NFIRST,NLA5T)
180 FORMAT (6H0FRAME,8(A3,9H* MARKER ,I2,2H *))
WRITE (6,190) (L1,L2,J=NFIR5T,NLA5T)
190 FORMAT (6H NO. ,8(5X,A2,4X,A2,3X))
WRITE (6,200)
200 FORMAT (1H )
210 WRITE (6,220) NF,(X(J),Y(J),J=JFIR5T,JLA5T)
220 FORMAT (1H ,I4,8(4X,2F6.0))
IF (MOD(NF,5).NE.0) GOTO 230
WRITE (6,200)
NLINE5=NLINE5+6
230 NF=NF+1
JFIR5T=JFIR5T+NCOL5
IF (JFIR5T.GT.N) GOTO 260
JLA5T=JLA5T+NCOL5
IF (JLA5T.GT.N) JLA5T=N
IF (NLINE5.LT.59) GOTO 210
240 WRITE (6,130) IDENT
NLINE5=6
IF (NF.NE.1) GOTO 170
WRITE (6,250)
250 FORMAT (1H0)
GOTO 160
260 IF (NLA5T.EQ.NCOL5) GOTO 280
NF=1
NFIRST=9
NLA5T=NCOL5
IF (.NOT.5TATIC) GOTO 240
WRITE (6,270) IDENT
270 FORMAT (5(1H/),10H DECKNAME ,A9/1H )
GOTO 160
280 IF (NEXTID.EQ.0) 5TOP
GOTO 100
END

```

LISK320  
LISK330  
LISK340  
LISK350  
LISK360  
LISK370  
LISK380  
LISK390  
LISK400  
LISK410  
LISK420  
LISK430  
LISK440  
LISK450  
LISK460  
LISK470  
LISK480  
LISK490  
LISK500  
LISK510  
LISK520  
LISK530  
LISK540  
LISK550  
LISK560  
LISK570  
LISK580  
LISK590  
LISK600  
LISK610  
LISK620  
LISK630  
LISK640  
LISK650  
LISK660  
LISK670  
LISK680  
LISK690  
LISK700  
LISK710  
LISK720  
LISK730  
LISK740  
LISK750

```

SUBROUTINE SIMKIN(X,Y,N,IDENT,NEXTID)
C READ5 X AND Y CO-ORDINATE5 COMPRISING KINETIC DATA, FROM UPDATE
C COMPILE FILE. DATA ARE READ IN SEQUENCE X(1),Y(1),X(2),Y(2),
C . . . X(N),Y(N). X AND Y DATA ARE ON 5TREAM 5 IN FORMAT
C J(15,1X,15,1X) WHERE 0.LE.J.LE.6. DECK NAME IS READ FROM COL5,
C 74 TO 82 AND IS RETURNED IN A9 FORMAT AS IDENT. READING 5TOP5
C WHEN A NEW DECK IDENTIFIER IS FOUND AND THIS IS RETURNED AS
C NEXTID. N CONTAIN5 NUMBER OF PAIR5 READ. TO AVOID LO55 OF
C DATA AND OTHER PROBLE55 THE FIR5T LINE OF EACH DECK 5HOULD BE
C BLANK. IF END-OF-FILE IS READ NEXTID IS SET TO ZERO.
C NOTE THAT THIS IS AN EARLY AND 5IMPLE VERSION OF INPKIN.
C
C DIMENSION X(1400),Y(1400),LINE(12),LNCH(6)
C LOGICAL FIR5T,5IDENT
C DATA IBLANK / 6H /
C
C NLOC=0
C FIR5T=.TRUE.
C IDENT=0
C
100 READ (5,110) LNCH,LINE,NXTLOC
110 FORMAT (6(6X,A6),T1,I2(15,1X),1X,A9)
IF (EOF(5).NE.0.) GOTO 140
IF (.NOT.FIR5T) GOTO 120
FIR5T=.FALSE.
IDLOC=NXTLOC
5IDENT=NXTLOC
120 IF (NXTLOC.EQ.IDLOC) GOTO 124
IF (.NOT.5IDENT(NXTLOC,1,5,5H5CORR)) GOTO 150
124 DO 130 K=1,6
IF (LNCH(K).EQ.5BLANK) GOTO 100
NLOC=NLOC+1
X(NLOC)=FLOAT(LINE(2*K-1))
Y(NLOC)=FLOAT(LINE(2*K))
130 CONTINUE

```

SIMKIN10  
SIMKIN20  
SIMKIN30  
SIMKIN40  
SIMKIN50  
SIMKIN60  
SIMKIN70  
SIMKIN80  
SIMKIN90  
SIMK1100  
SIMK1110  
SIMK1120  
SIMK1130  
SIMK1140  
SIMK1150  
SIMK1160  
SIMK1170  
SIMK1180  
SIMK1190  
SIMK1200  
SIMK1210  
SIMK1220  
SIMK1230  
SIMK1240  
SIMK1250  
SIMK1260  
SIMK1270  
SIMK1280  
SIMK1290  
SIMK1300  
SIMK1310  
SIMK1320  
SIMK1330  
SIMK1340  
SIMK1350  
SIMK1360  
SIMK1370

```

      GOTO 100
C
140 NXTLOC=0
150 NEXTID=NXTLOC
    N=NLOC
    RETURN
    END
      SIMKI380
      SIMKI390
      SIMKI400
      SIMKI410
      SIMKI420
      SIMKI430
      SIMKI440

      PROGRAM TESTFPD(INPUT,OUTPUT,TAPE7,TAPES=INPUT,TAPE6=OUTPUT)
C
C TESTS INPFPD.
C
      DIMENSION X(1920)
C
      CALL CONNED(7)
100 CALL INPFPD(X,N,ID,NX)
      WRITE (6,110) N, ID, NX
110 FORMAT (1H1/1H0,15,33H SETS OF 6 VALUES READ FROM DECK ,A9,1H.,
+ 10X,14H(NEXT DECK IS ,A9,2H.)/1H0)
      IF (N.GT.0) GOTO 140
      WRITE (7,120) ID
120 FORMAT (15HOERROR IN DECK ,A9,1H./1H )
      WRITE (6,130)
130 FORMAT (16H ERROR FLAG SET./1H0)
      GOTO 190
C
140 WRITE (6,150)
150 FORMAT (1H ,3X,4HF(X),6X,4HF(Y),6X,4HF(Z),6X,4HM(X),6X,4HM(Y),
+ 6X,4HM(Z)/1H0)
      NV=6*N
      DO 170 J=1,N
      WRITE (6,160) (X(K),K=J,NV,N)
160 FORMAT (1H ,6(F8.0,2X))
170 CONTINUE
      WRITE (7,180) ID
180 FORMAT (6HODECK ,A9,20H READ WITHOUT ERROR./1H )
190 IF (NX.NE.0) GOTO 100
      STOP
      END
      TESFPD10
      TESFPD20
      TESFPD30
      TESFPD40
      TESFPD50
      TESFPD60
      TESFPD70
      TESFPD80
      TESFPD90
      TESFP100
      TESFP110
      TESFP120
      TESFP130
      TESFP140
      TESFP150
      TESFP160
      TESFP170
      TESFP180
      TESFP190
      TESFP200
      TESFP210
      TESFP220
      TESFP230
      TESFP240
      TESFP250
      TESFP260
      TESFP270
      TESFP280
      TESFP290
      TESFP300
      TESFP310

      PROGRAM TESTKIN(INPUT,OUTPUT,TAPES=INPUT,TAPE6=OUTPUT)
C
C TESTS INPKIN.
C
      DIMENSION A(1400),B(1400)
      COMMON A,B
100 CALL INPKIN(A,B,NPAIRS, ID, NEXT)
      WRITE (6,110) NPAIRS, ID, NEXT
110 FORMAT (1H1/1H0,15,26H PAIRS X,Y READ FROM DECK ,A9,1H.,10X,
+ 15H(NEXT IDENT IS ,A9,2H.)/1H0)
      NTOP=NPAIRS
      IF (NTOP.GT.36) NTOP=18
      WRITE (6,120) (A(J),B(J),J=1,NTOP)
120 FORMAT (6(1H ,2F8.0,2X))
      IF (NTOP.EQ.NPAIRS) GOTO 140
      WRITE (6,130)
130 FORMAT (20H0 ETCETERA, TO -/1H )
      NLOW=6*(NPAIRS/6)-5
      WRITE (6,120) (A(J),B(J),J=NLOW,NPAIRS)
140 IF (NEXT.NE.0) GOTO 100
      STOP
      END
      TESKIN10
      TESKIN20
      TESKIN30
      TESKIN40
      TESKIN50
      TESKIN60
      TESKIN70
      TESKIN80
      TESKIN90
      TESKI100
      TESKI110
      TESKI120
      TESKI130
      TESKI140
      TESKI150
      TESKI160
      TESKI170
      TESKI180
      TESKI190
      TESKI200
      TESKI210
      TESKI220

      PROGRAM TRYDEV(QEVDAT,OUTPUT,TAPES=QEVDAT,TAPE6=OUTPUT)
C
C TESTS SUBROUTINE QEVENT.
C
      DIMENSION X(15),Y(15),Z(15,6)
      LOGICAL FORWRD
      IDENT=9H**FP1BDT*
      FORWRD=.TRUE.
100 READ (5,110) X
110 FORMAT (15F5.0)
      IF (EOF(5).EQ.0.) GOTO 120
      IF (.NOT.FORWRD) STOP
      FORWRD=.FALSE.
      IDENT=9H**FP1FUL*
      REWIND 5
      GOTO 100
120 DO 140 J=1,15

```

```

JJ=J
IF (.NOT.FORWRD) JJ=16-J
Y(J)=X(JJ)
DO 130 K=1,6
Z(J,K)=Y(J)
130 CONTINUE
140 CONTINUE
WRITE (6,150)
150 FORMAT (1H0/1H )
CALL QEVENT(Z,15,IDENT,2.000000001,EVNTPT)
WRITE (6,160) IDENT,EVNTPT
160 FORMAT(1H0,A9,F12.3)
WRITE (6,170) Y,Z
170 FORMAT (1H0,15F8.4)
GOTO 100
END

```

TRYQE180  
TRYQE190  
TRYQE200  
TRYQE210  
TRYQE220  
TRYQE230  
TRYQE240  
TRYQE250  
TRYQE260  
TRYQE270  
TRYQE280  
TRYQE290  
TRYQE300  
TRYQE310  
TRYQE320  
TRYQE330

```

PROGRAM UPEDBK(TAPE1,TAPE2,OUTPUT,TAPE6=OUTPUT)
C
C EDITS AN UPDATE INPUT FILE TO ENSURE THAT THE FIRST TWO LINES OF EACH
C DECK ARE BLANK, BLANK LINES BEING INSERTED IF NECESSARY. THE
C ORIGINAL SOURCE FILE IS TAPE1 AND THE EDITED VERSION IS TAPE2.
C ADDITIONAL BLANK LINES IMMEDIATELY FOLLOWING A *DECK CARD ARE
C ELIMINATED. BLANK LINES ELSEWHERE REMAIN UNCHANGED. THE
C LINE LENGTH PROCESSED IS 72 CHARACTERS.
C
DIMENSION LINE(9)
LOGICAL NUDECK
DATA IBLANK / 8H /
DATA IDECK / 5H*DECK /
DATA ND / 0 /
DATA NI / 0 /
DATA NL / 0 /
DATA NUDECK / .FALSE. /
C
100 READ (1,110) LTEST,LINE
110 FORMAT (A5,T1,9A8)
IF (EOF(1).NE.0.) GOTO 200
IF (NUDECK) GOTO 140
120 IF (LTEST.NE.IDECK) GOTO 170
WRITE (2,130) LINE
130 FORMAT (9A8/1H /1H )
NUDECK=.TRUE.
ND=ND+1
NI=NI+2
NL=NL+3
GOTO 100
140 DO 150 J=1,9
IF (LINE(J).NE.IBLANK) GOTO 160
150 CONTINUE
NI=NI-1
GOTO 100
160 NUDECK=.FALSE.
GOTO 120
170 WRITE (2,180) LINE
180 FORMAT (9A8)
NL=NL+1
GOTO 100
C
200 REWIND 1
REWIND 2
WRITE (6,210) NL,ND,NI
210 FORMAT (1H0,16,40H LINES WRITTEN TO EDITED FILE, INCLUDING/
1 1H ,16,33H LINES WITH *DECK DIRECTIVES, AND/
2 1H ,16,50H BLANK LINES NEWLY INSERTED, LESS REDUNDANT BLANK ,
3 14HLINES DELETED./1H )
STOP
END

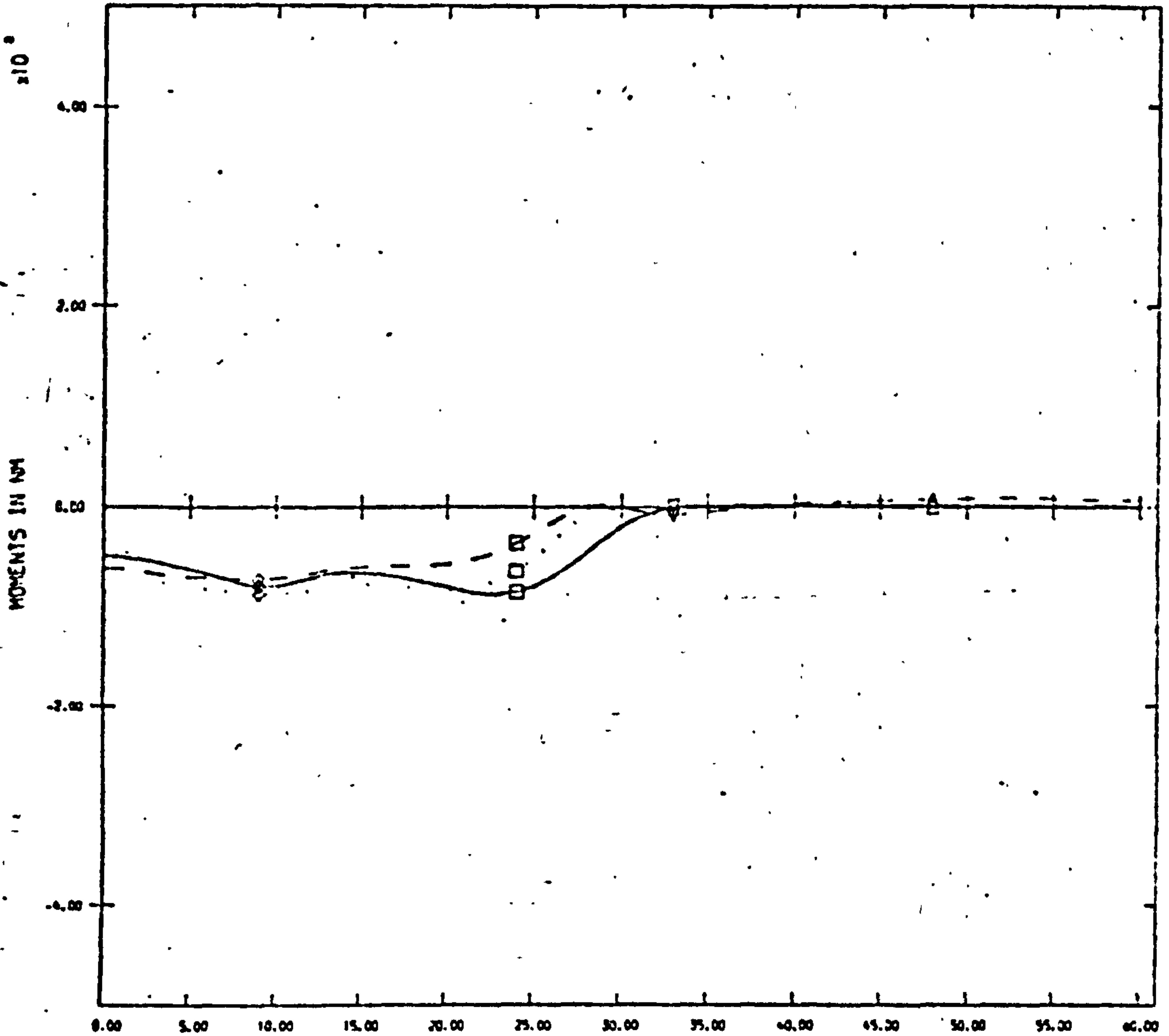
```

UPEDBK10  
UPEDBK20  
UPEDBK30  
UPEDBK40  
UPEDBK50  
UPEDBK60  
UPEDBK70  
UPEDBK80  
UPEDBK90  
UPEDB100  
UPEDB110  
UPEDB120  
UPEDB130  
UPEDB140  
UPEDB150  
UPEDB160  
UPEDB170  
UPEDB180  
UPEDB190  
UPEDB200  
UPEDB210  
UPEDB220  
UPEDB230  
UPEDB240  
UPEDB250  
UPEDB260  
UPEDB270  
UPEDB280  
UPEDB290  
UPEDB300  
UPEDB310  
UPEDB320  
UPEDB330  
UPEDB340  
UPEDB350  
UPEDB360  
UPEDB370  
UPEDB380  
UPEDB390  
UPEDB400  
UPEDB410  
UPEDB420  
UPEDB430  
UPEDB440  
UPEDB450  
UPEDB460  
UPEDB470  
UPEDB480  
UPEDB490  
UPEDB500  
UPEDB510



## **8.2 Intersegmental Moments for all Subjects and Patients**

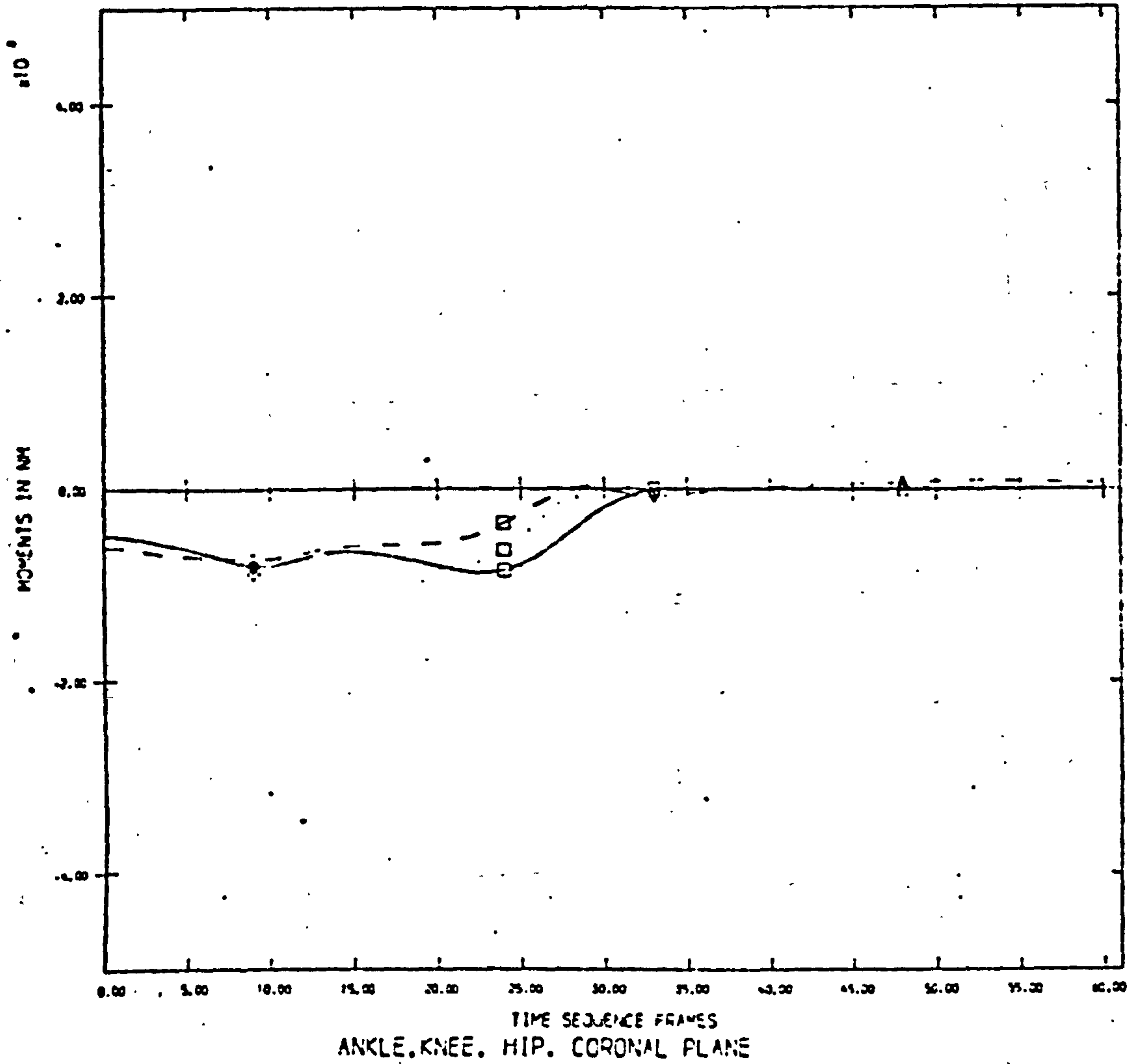
P1/L/FULO



ANKLE, KNEE, HIP, CORONAL PLANE

LEFT HEEL STRIKE	△	CONTINUOUS	ANKLE
LEFT TOE OFF	▽	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	◇		

PI/L/FULO



LEFT HEEL STRIKE  $\blacktriangle$

CONTINUOUS

ANKLE

LEFT TOE OFF  $\blacktriangledown$

DASHED

KNEE

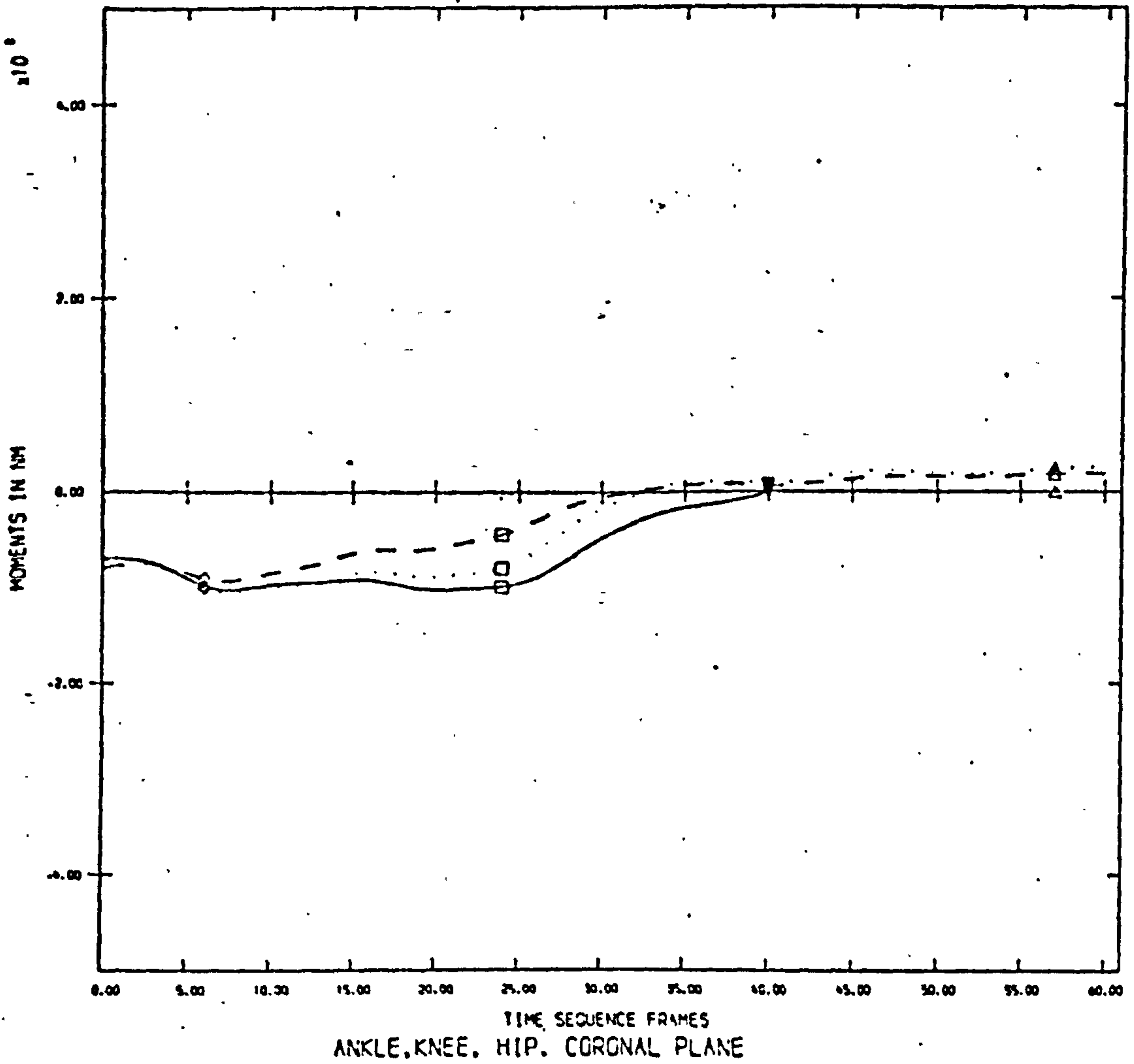
RIGHT HEELSTRIKE  $\square$

DOTTED

HIP

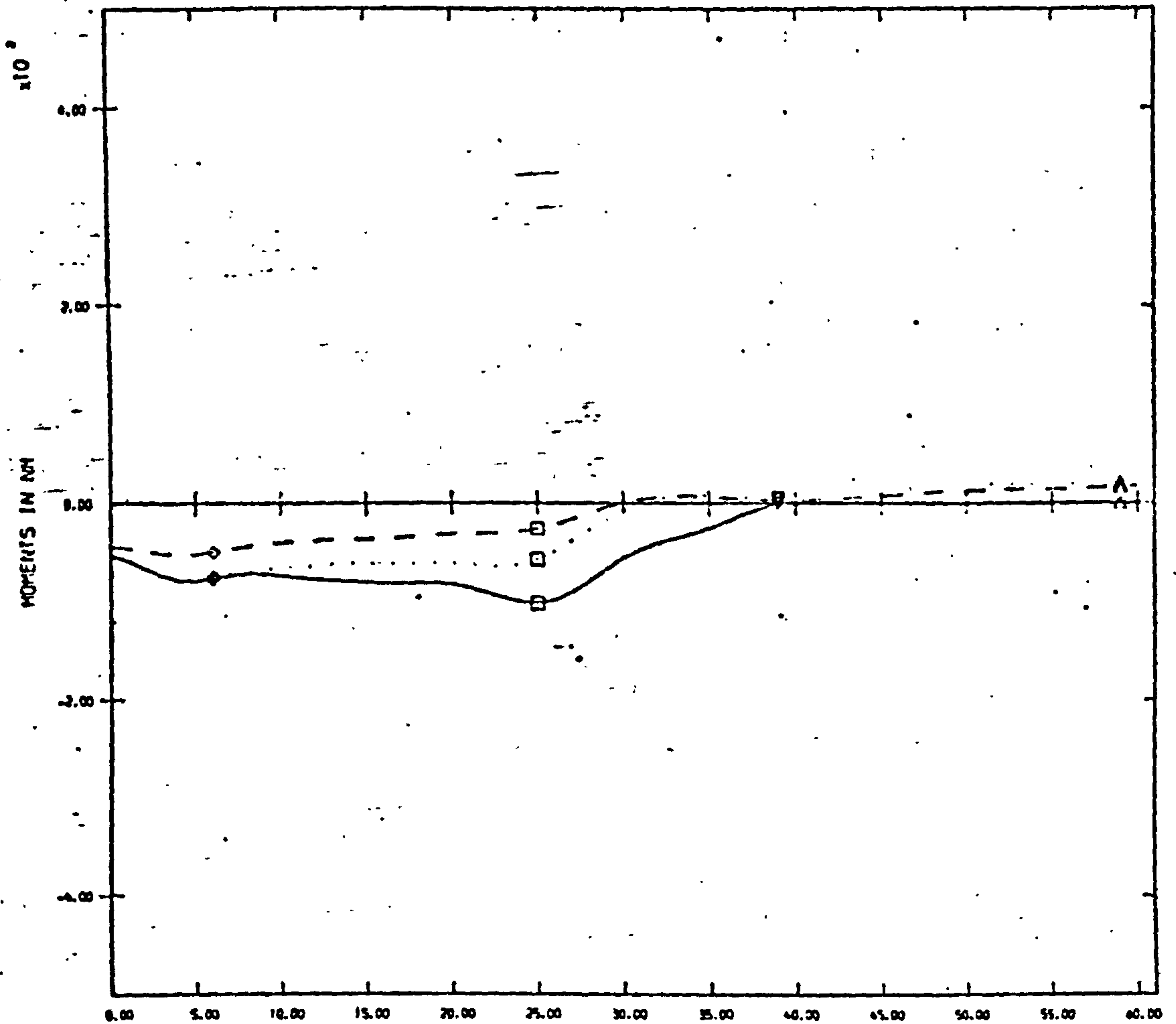
RIGHT TOE OFF  $\circ$

P4/L/FUL0



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

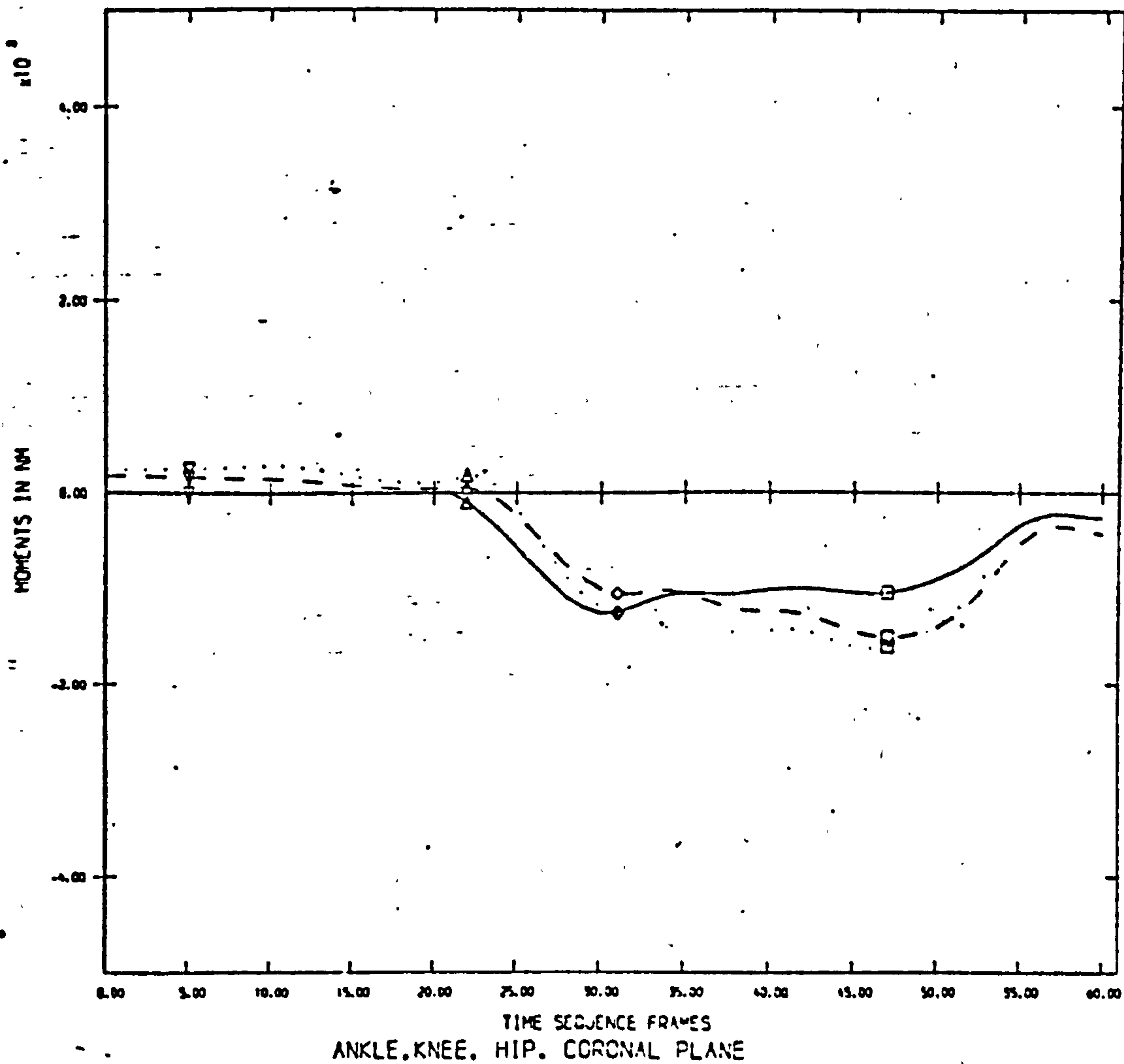
P6/L/FULO



TIME SEQUENCE FRAMES  
ANKLE, KNEE, HIP, CORONAL PLANE

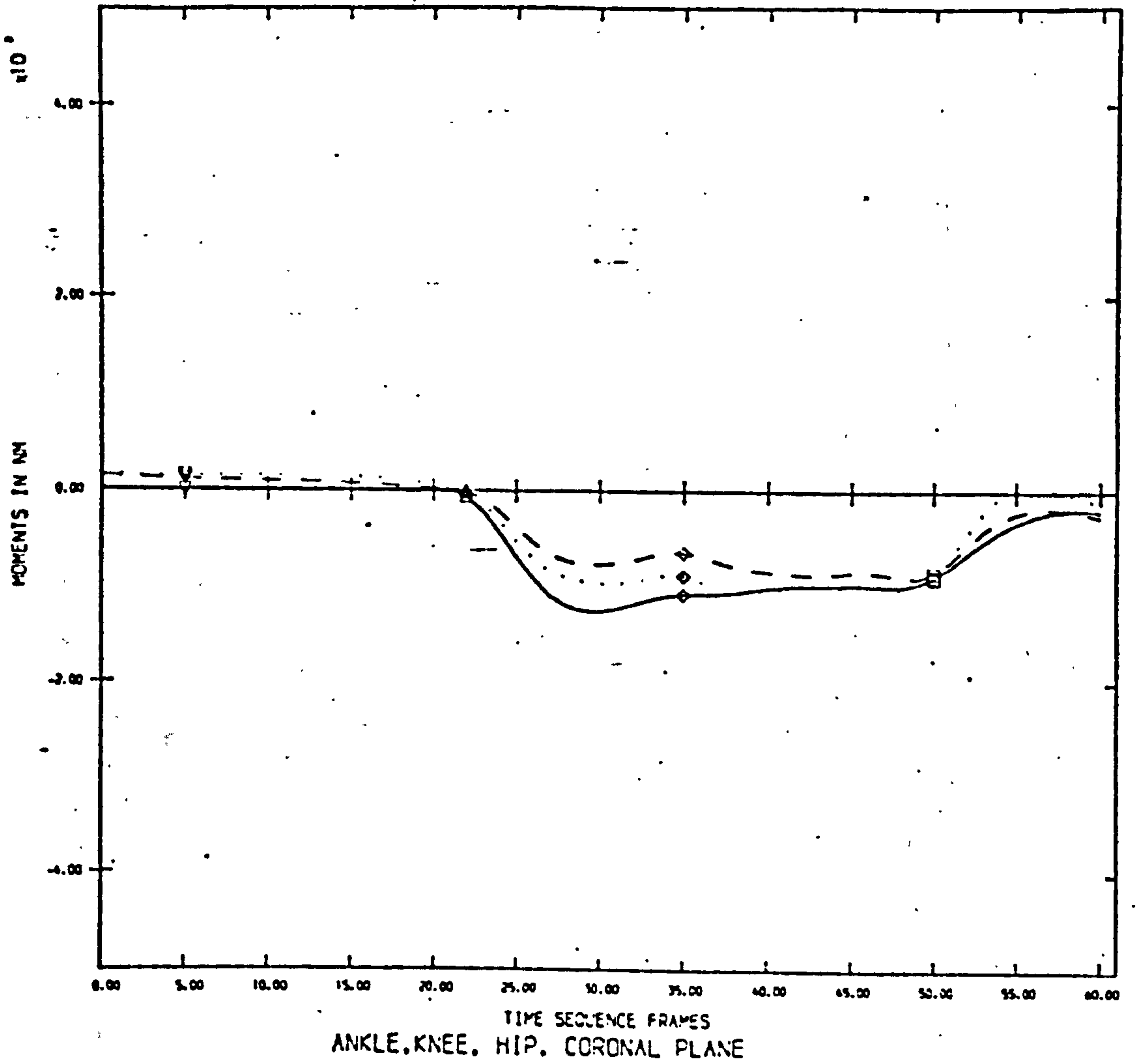
LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◆		

P3/L/B0T0



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

P4/L/BDT0



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

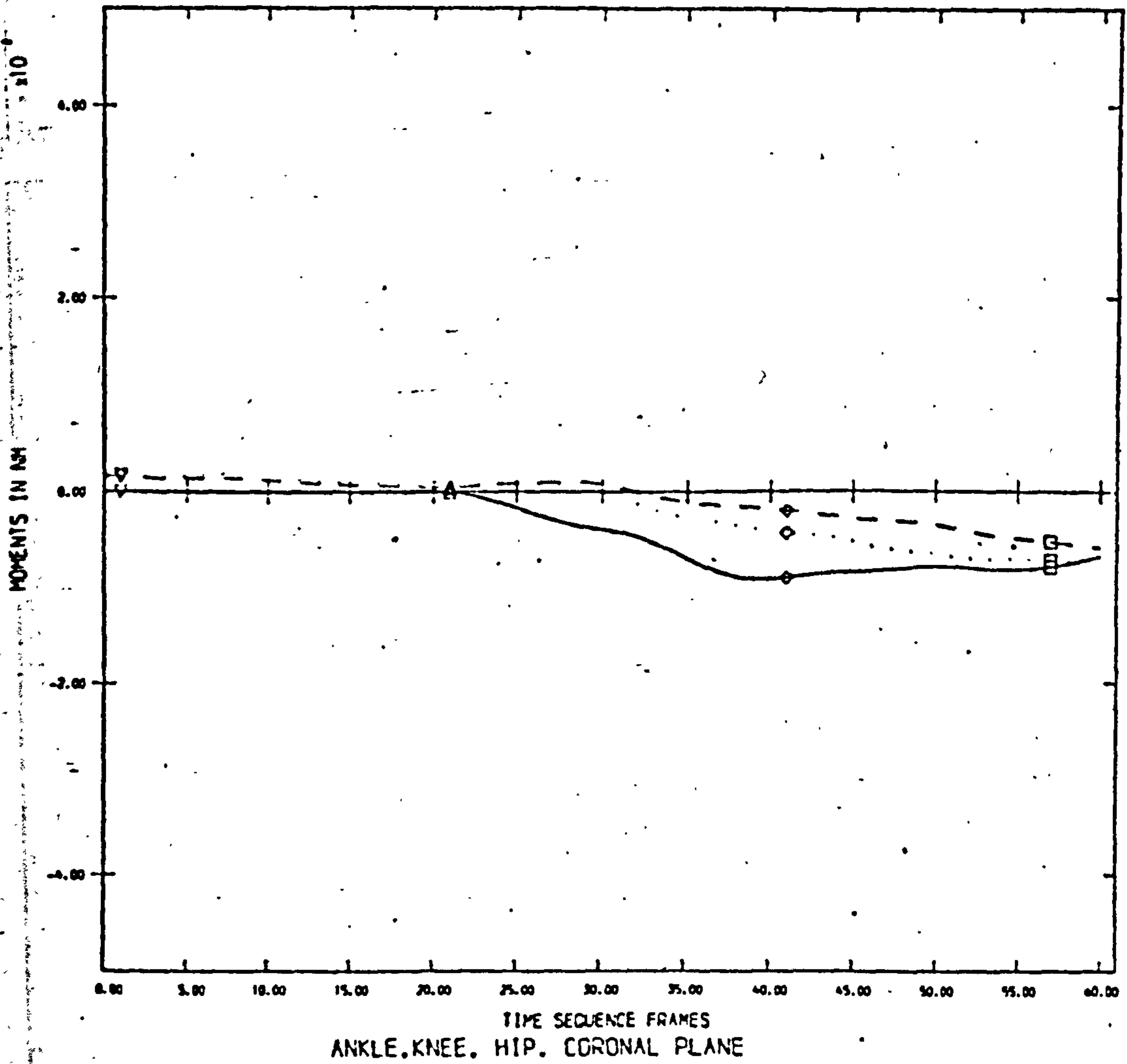
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\circ$

P6/L/BDTO



LEFT HEEL STRIKE ▲

CONTINUOUS ANKLE

LEFT TOE OFF ▼

DASHED KNEE

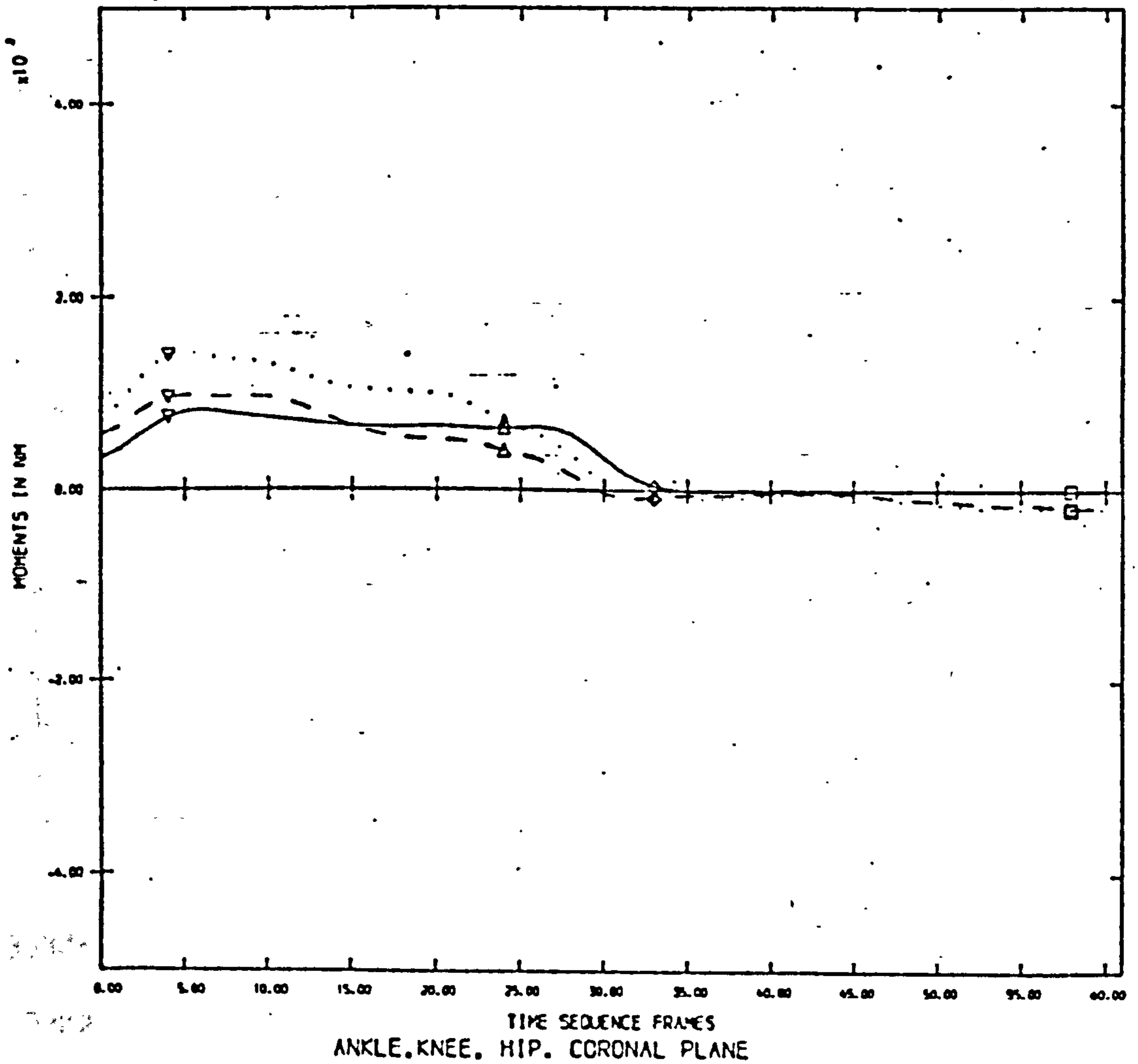
RIGHT HEELSTRIKE □

DOTTED HIP

RIGHT TOE OFF ◆



P1/R/BOT0



LEFT HEEL STRIKE ▲

CONTINUOUS ANKLE

LEFT TOE OFF ▼

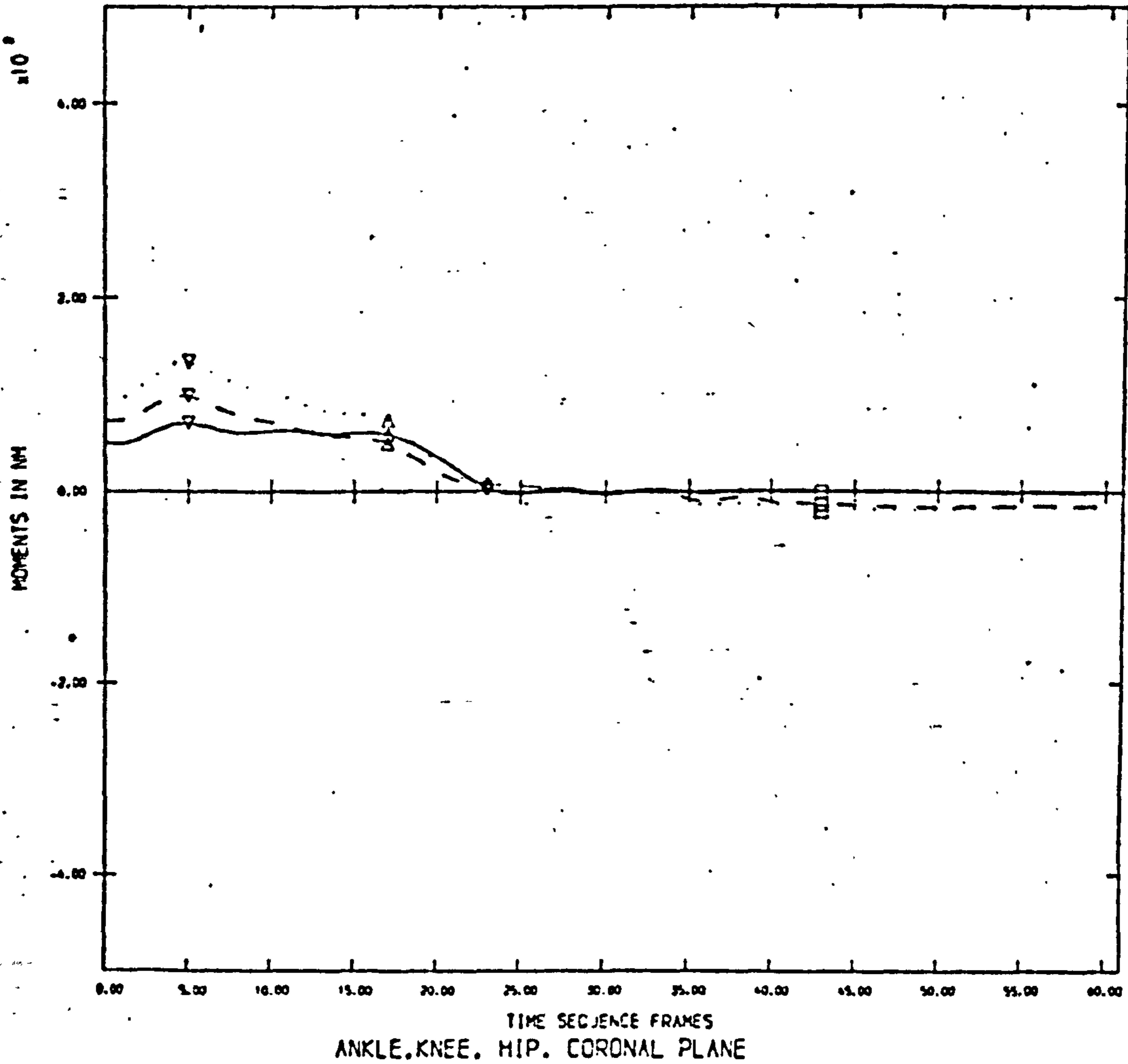
DASHED KNEE

RIGHT HEELSTRIKE □

DOTTED HIP

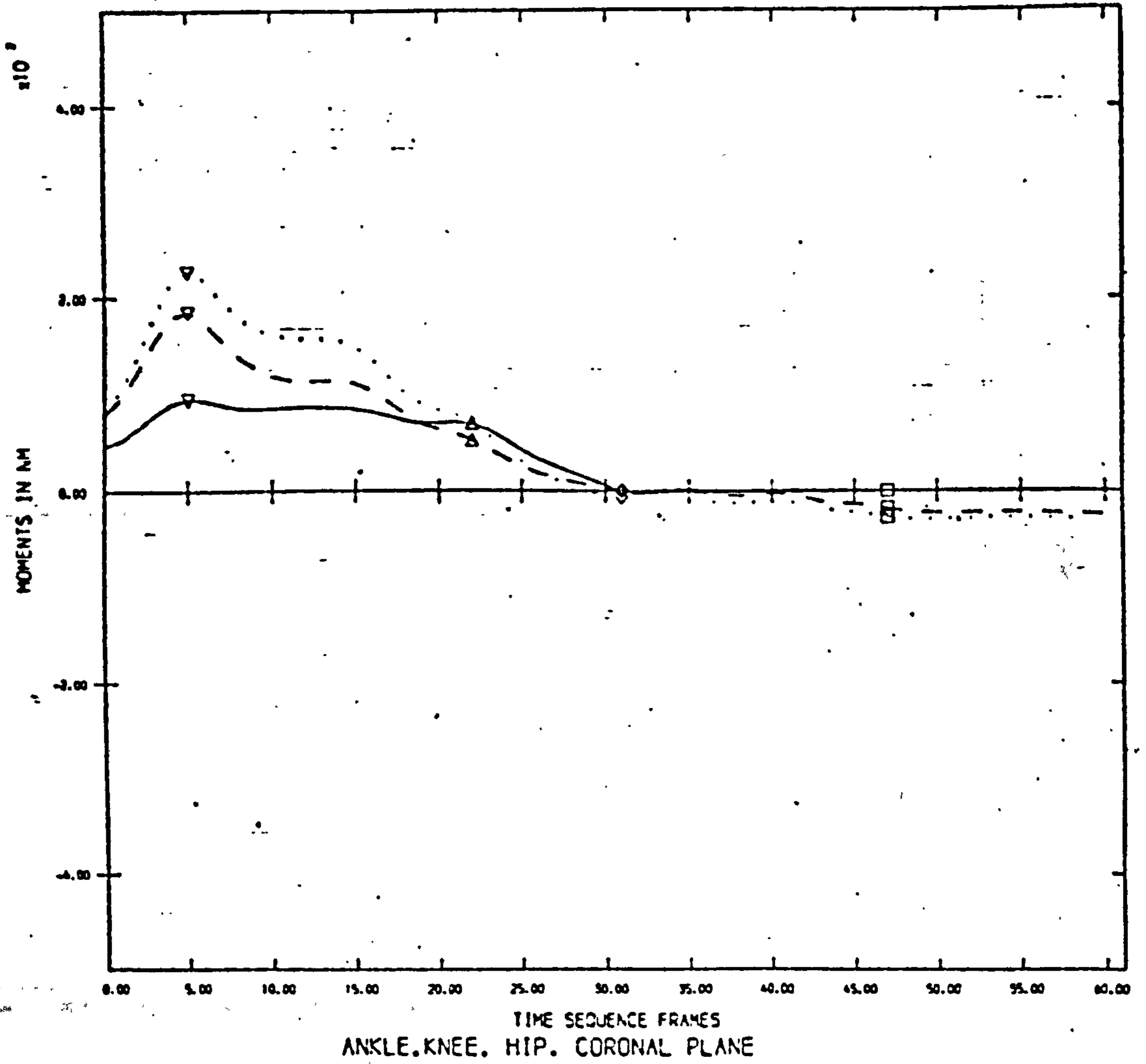
RIGHT TOE OFF ◆

P2/R/B0T0



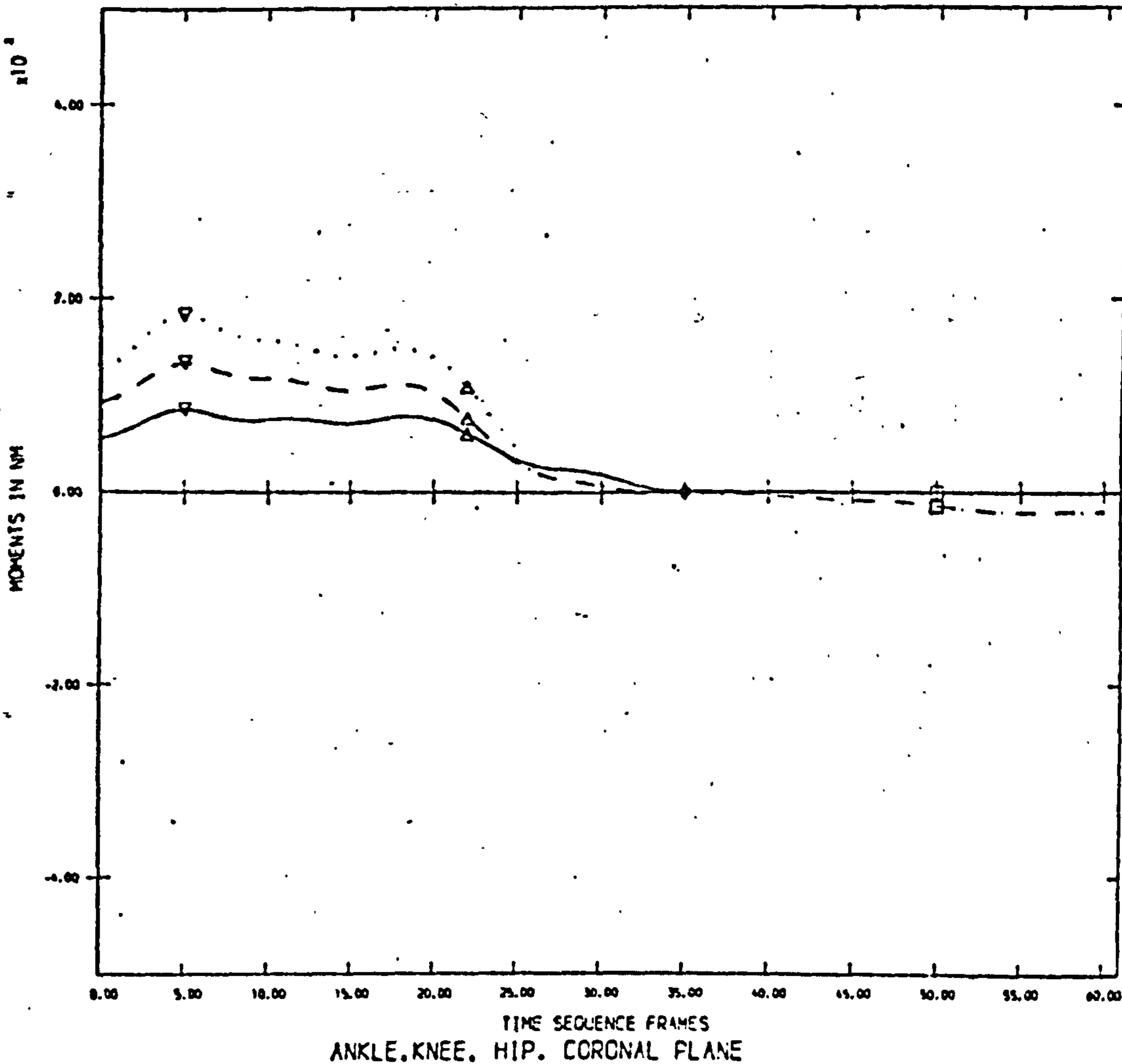
LEFT HEEL STRIKE $\Delta$	CONTINUOUS	ANKLE
LEFT TOE OFF $\nabla$	DASHED	KNEE
RIGHT HEELSTRIKE $\square$	DOTTED	HIP
RIGHT TOE OFF $\diamond$		

P3/R/8DT0



LEFT HEEL STRIKE	△	CONTINUOUS	ANKLE
LEFT TOE OFF	▽	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	○		

P4/R/BOTO



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

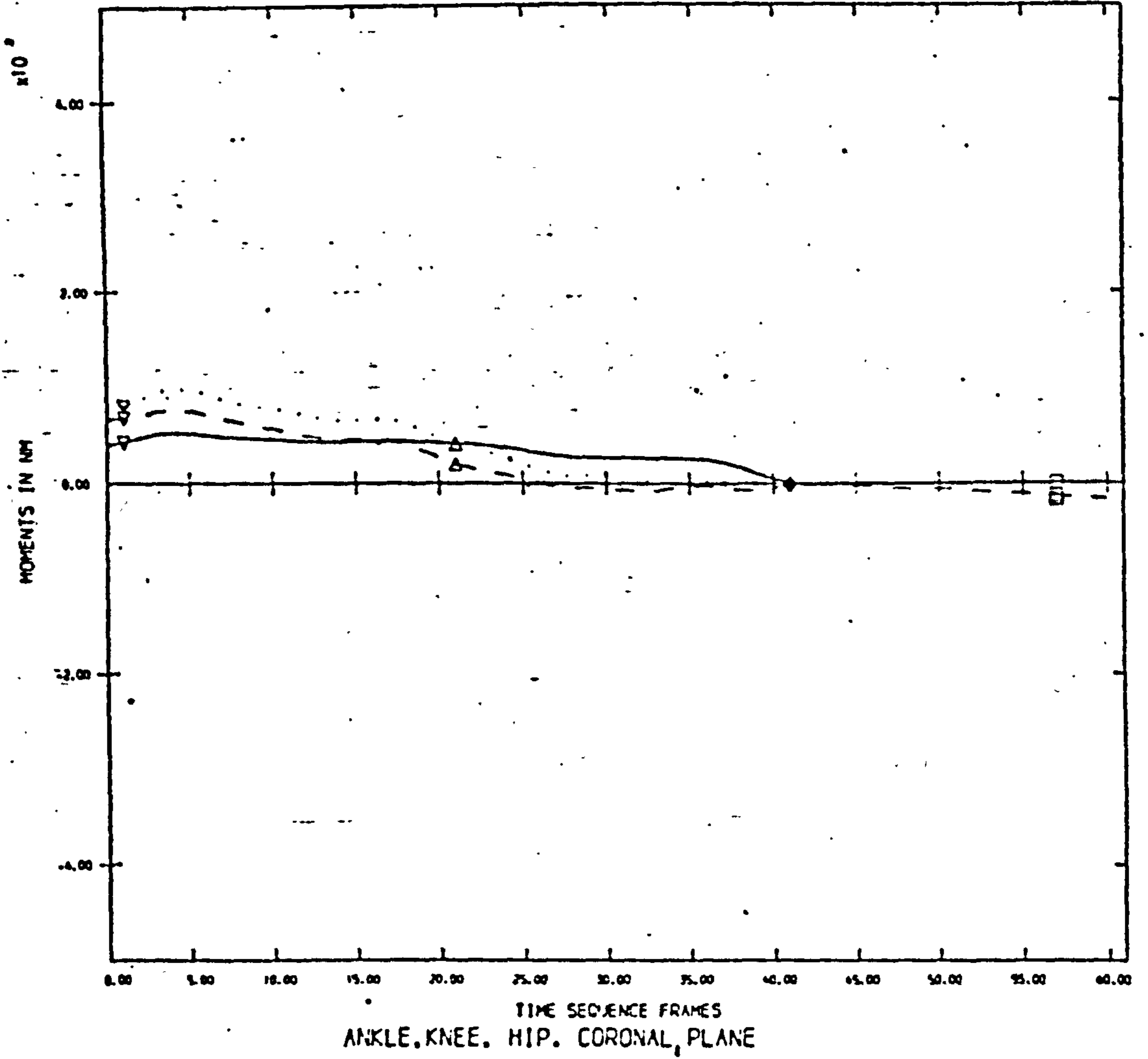
LEFT TOE OFF  $\nabla$

DASHED KNEE

RIGHT HEELSTRIKE  $\square$

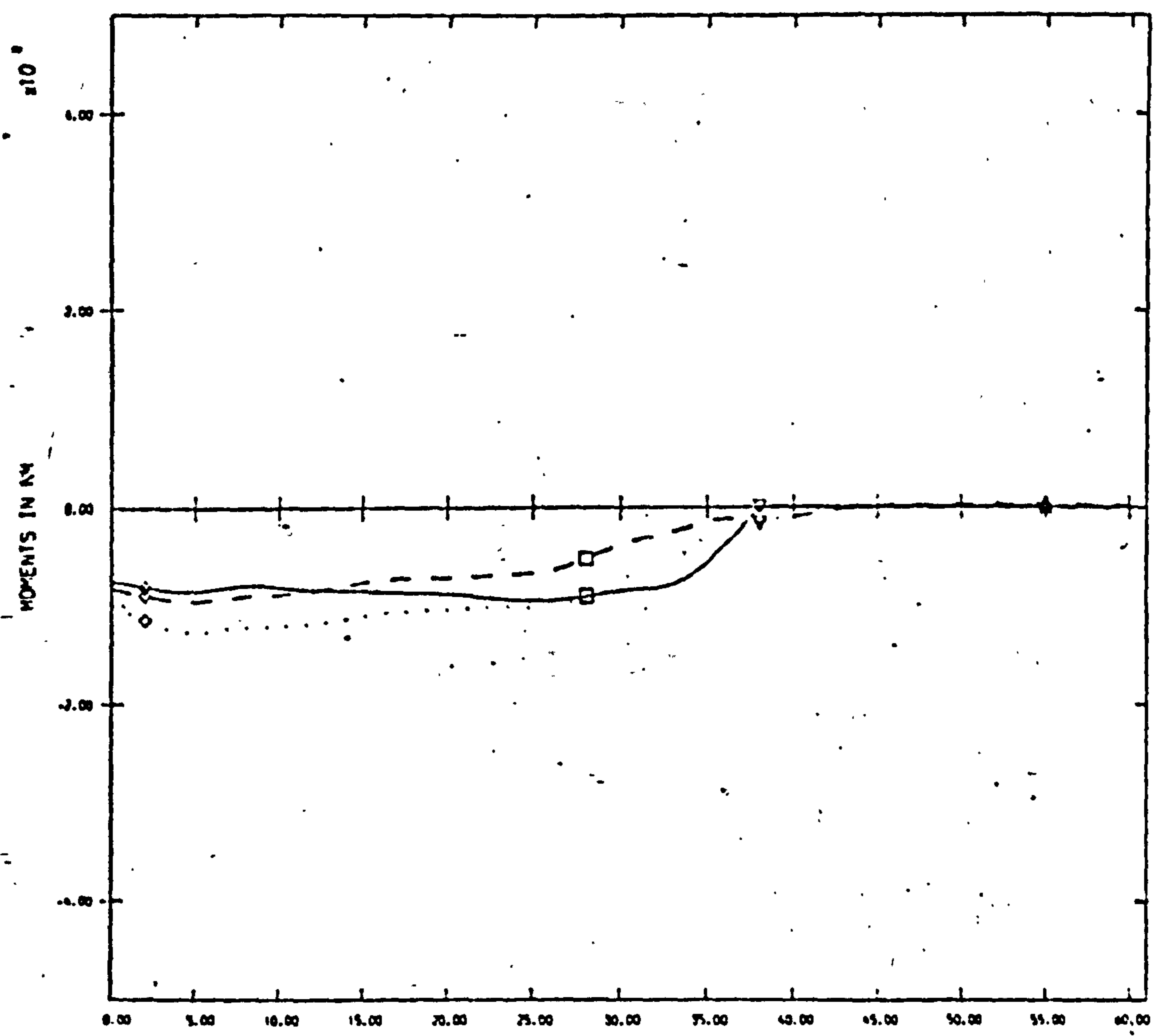
DOTTED HIP

RIGHT TOE OFF  $\diamond$



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

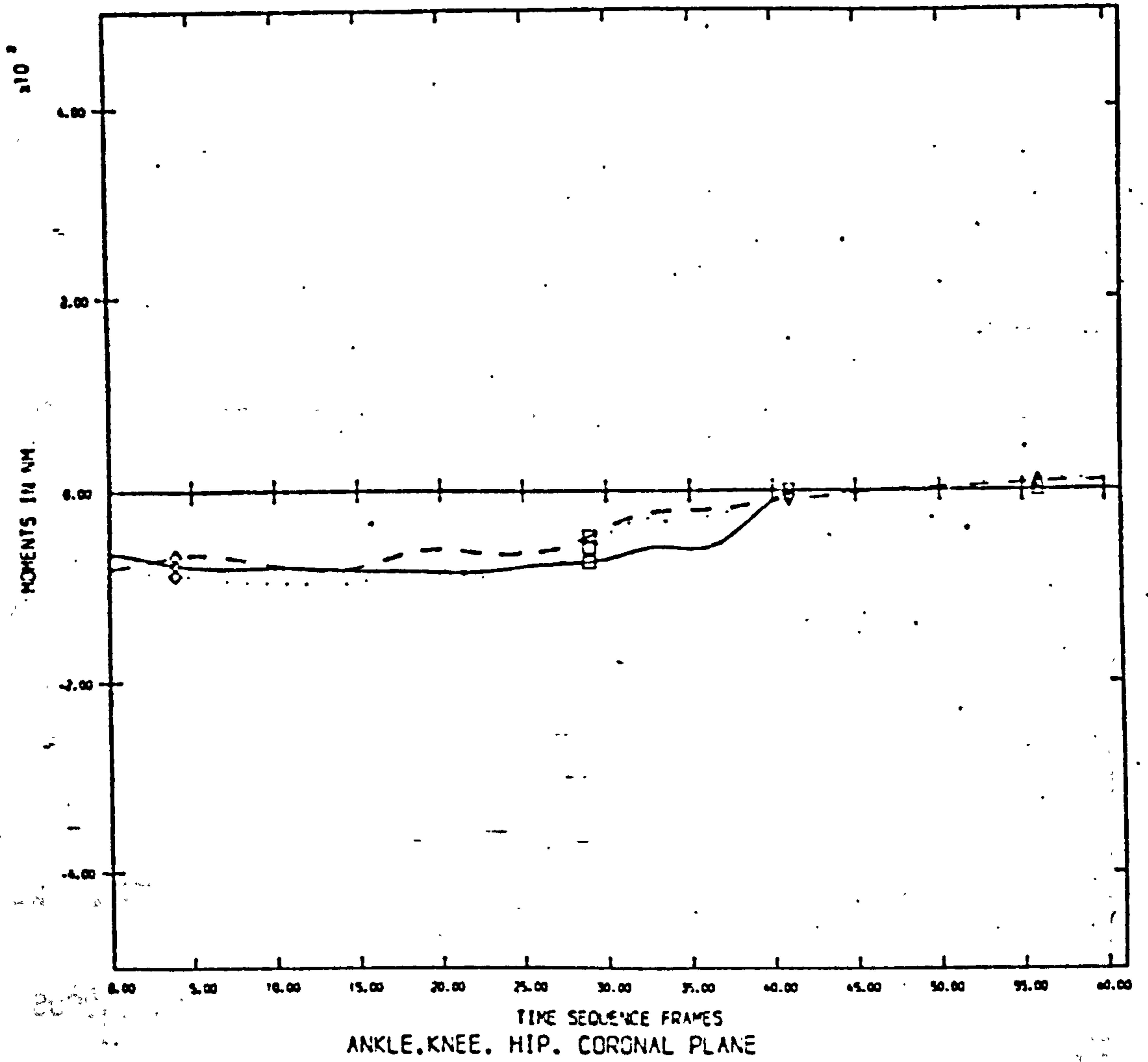
P1/L/FUL1



ANKLE, KNEE, HIP, CORONAL PLANE

- LEFT HEEL STRIKE  $\blacktriangle$  CONTINUOUS ANKLE
- LEFT TOE OFF  $\blacktriangledown$  DASHED KNEE
- RIGHT HEELSTRIKE  $\square$  DOTTED HIP
- RIGHT TOE OFF  $\diamond$

P2/L/FUL1



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

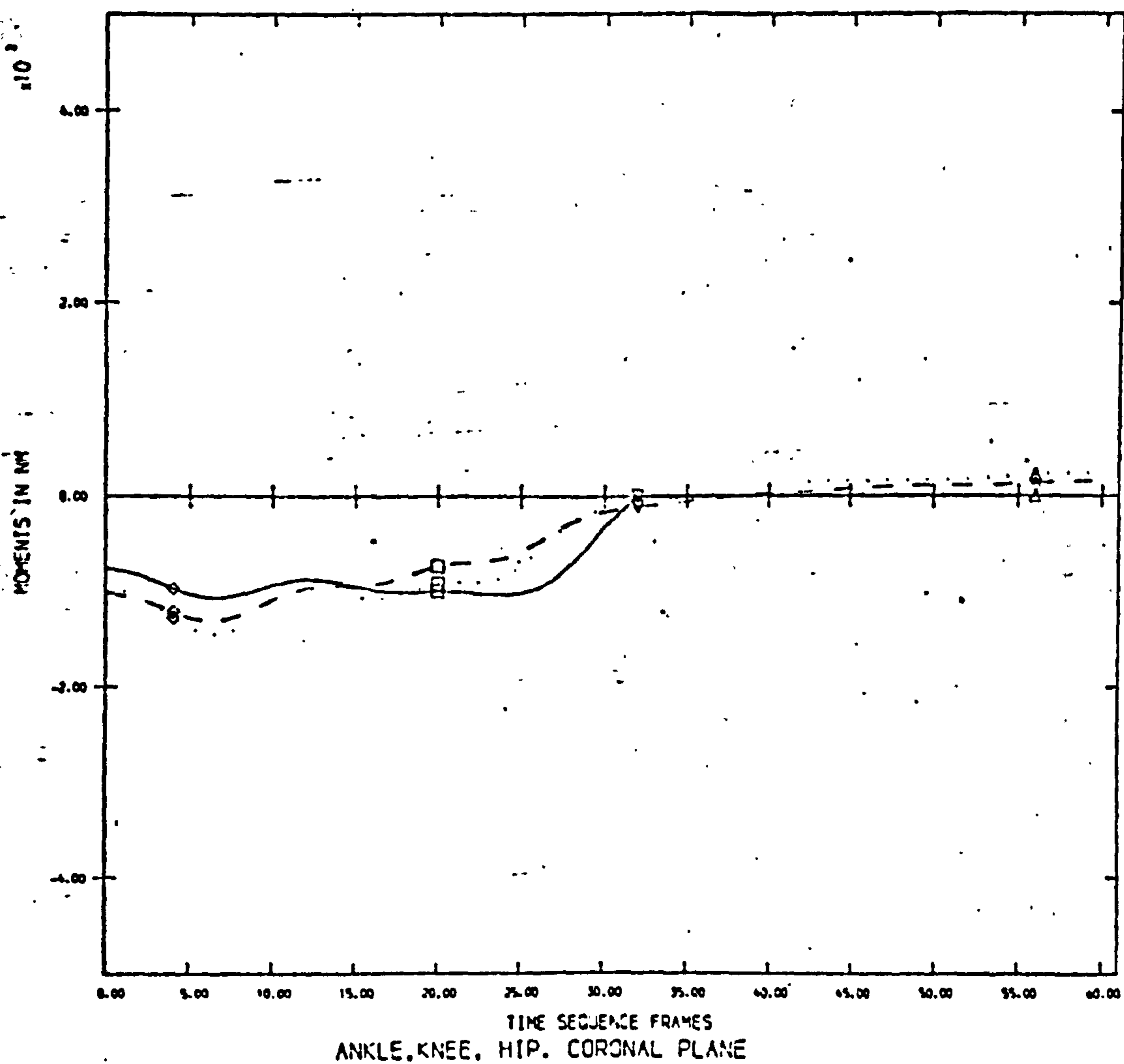
DASHED KNEE

RIGHT HEEL STRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\diamond$

P3/L/FUL1

LEFT HEEL STRIKE  $\blacktriangle$ 

CONTINUOUS ANKLE

LEFT TOE OFF  $\blacktriangledown$ 

DASHED KNEE

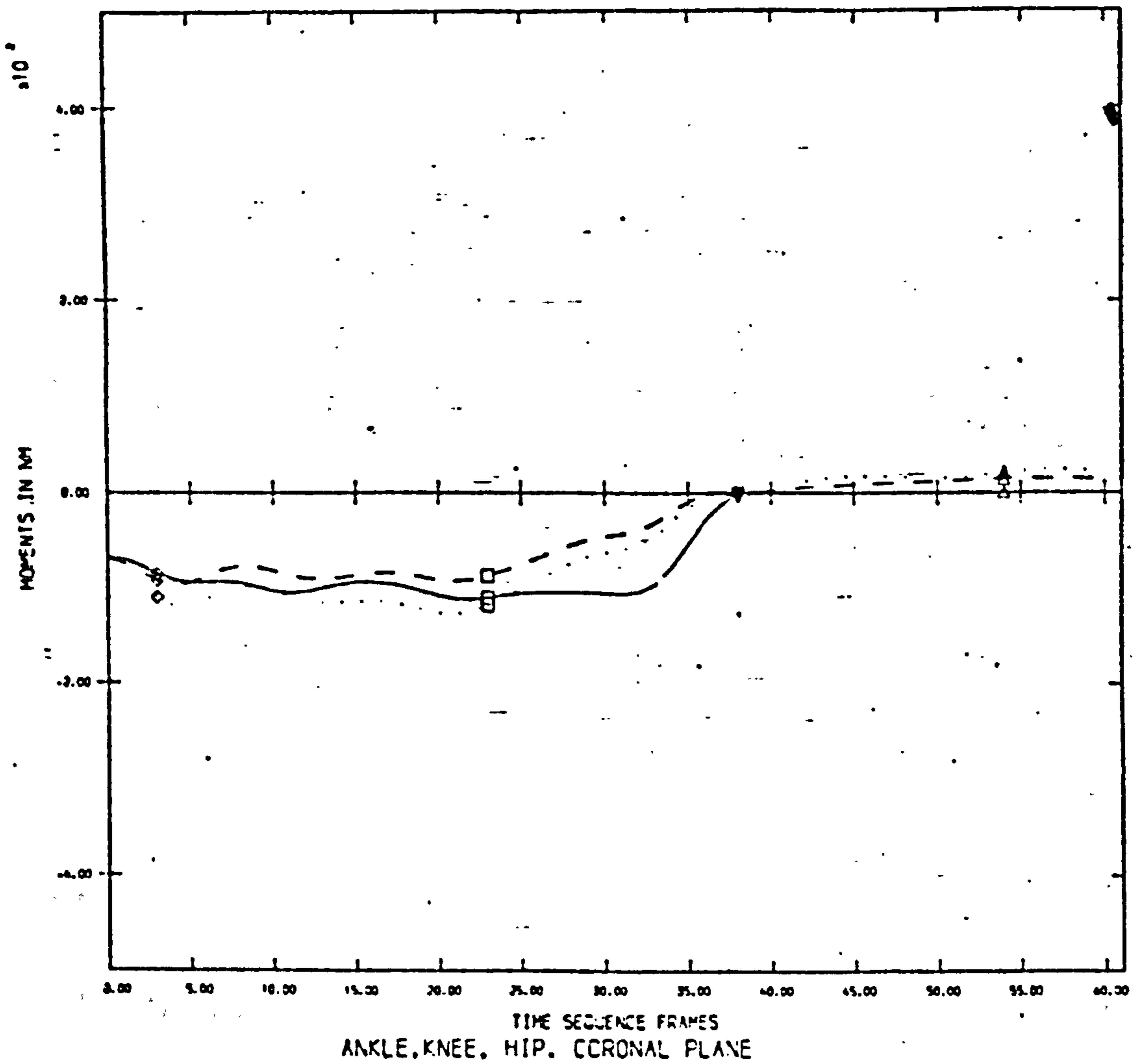
RIGHT HEELSTRIKE  $\square$ 

DOTTED HIP

RIGHT TOE OFF  $\diamond$

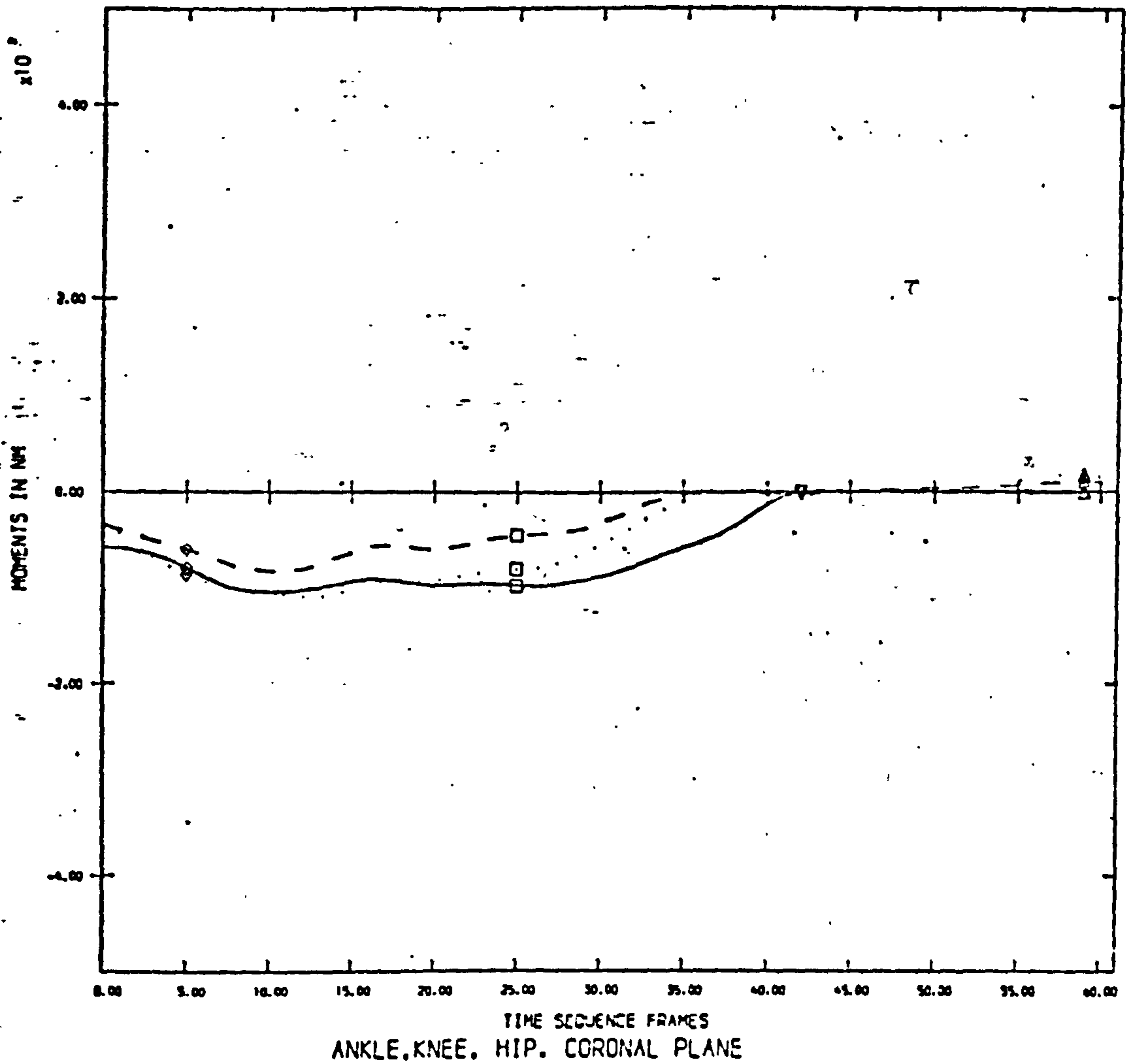


P4/L/FUL1



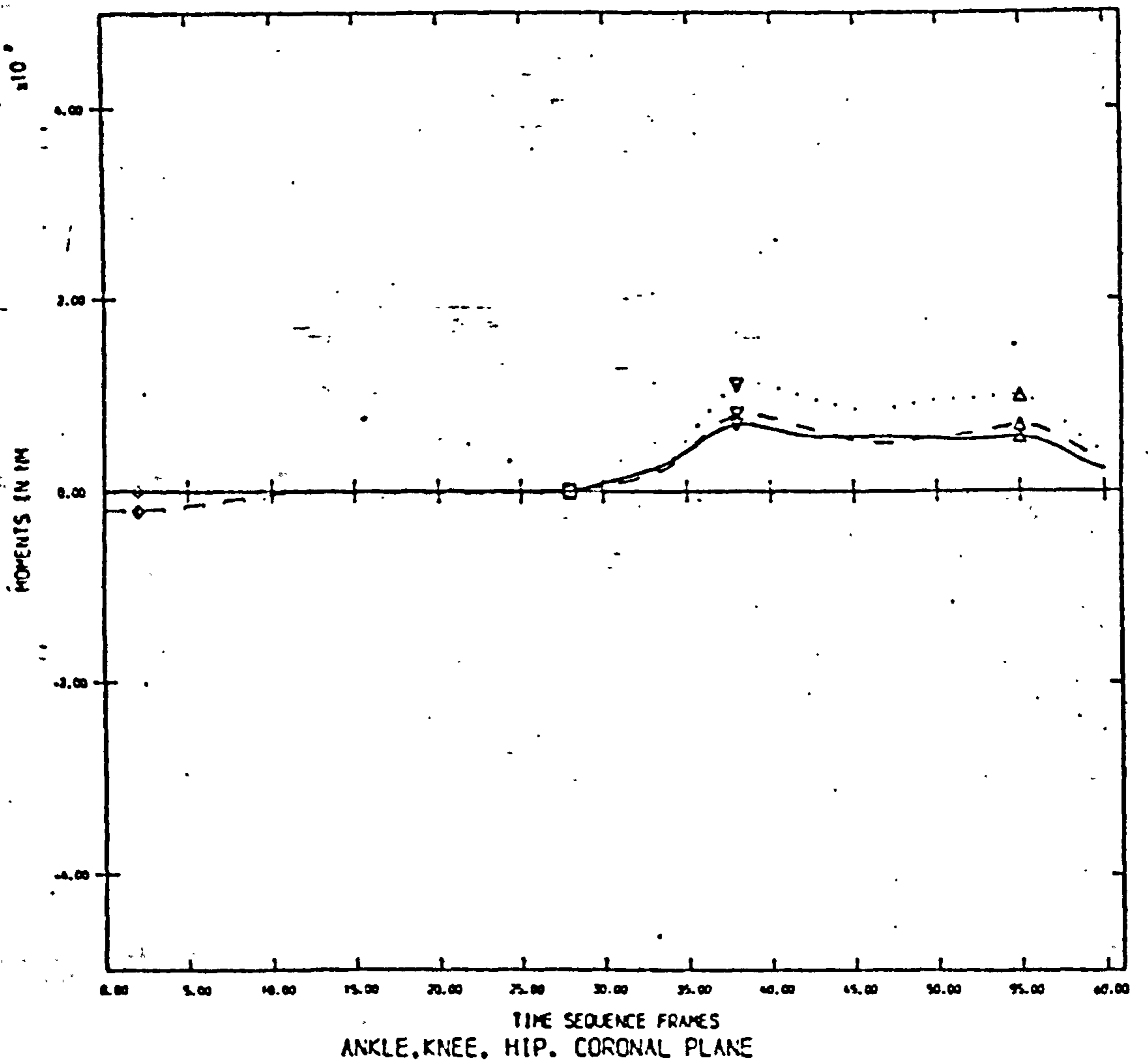
LEFT HEEL STRIKE ▲	CONTINUOUS	ANKLE
LEFT TOE OFF ▼	DASHED	KNEE
RIGHT HEELSTRIKE □	DOTTED	HIP
RIGHT TOE OFF ◆		

P6/L/FUL1



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	○		

P1/R/FUL1



LEFT HEEL STRIKE.  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

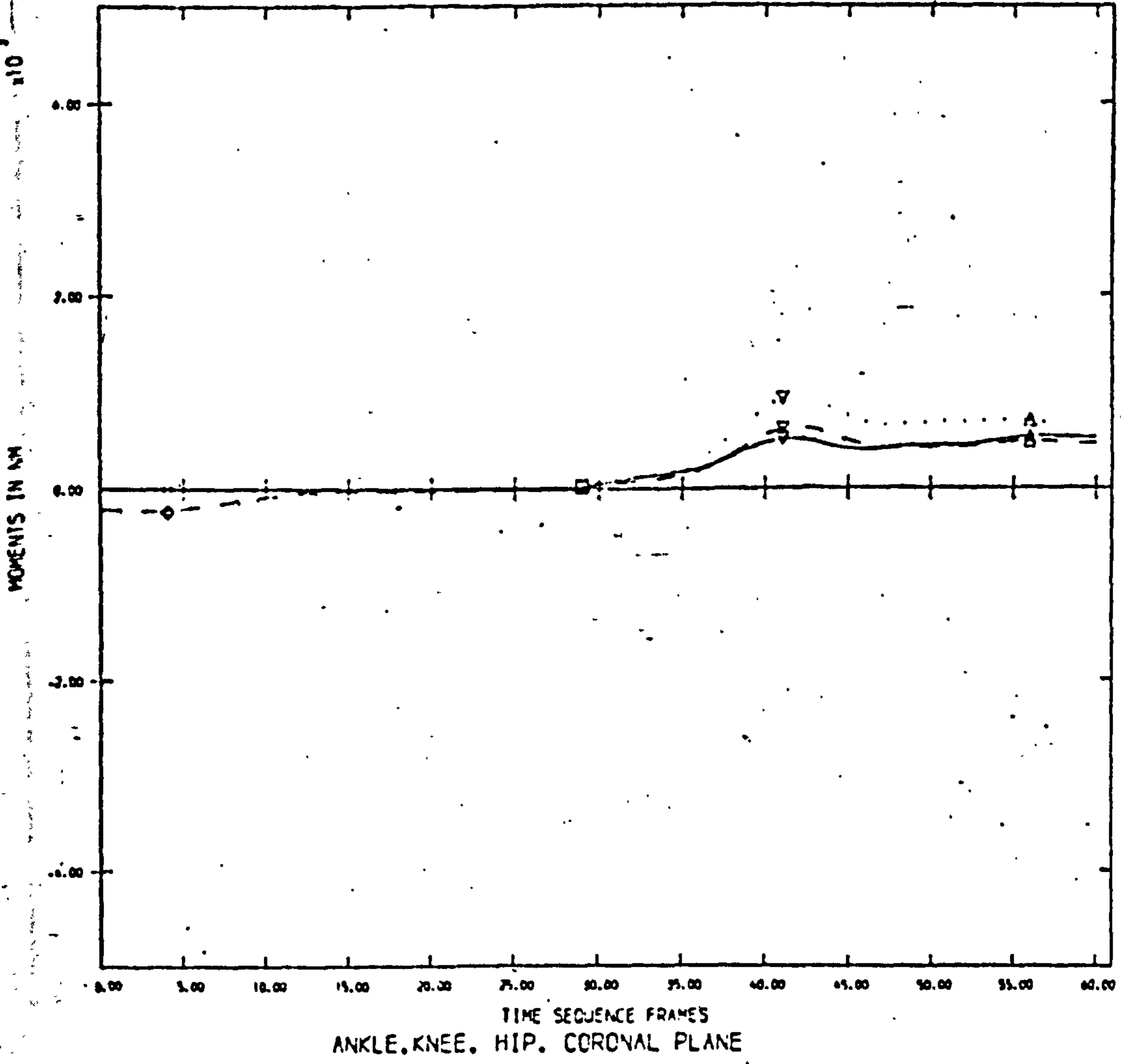
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

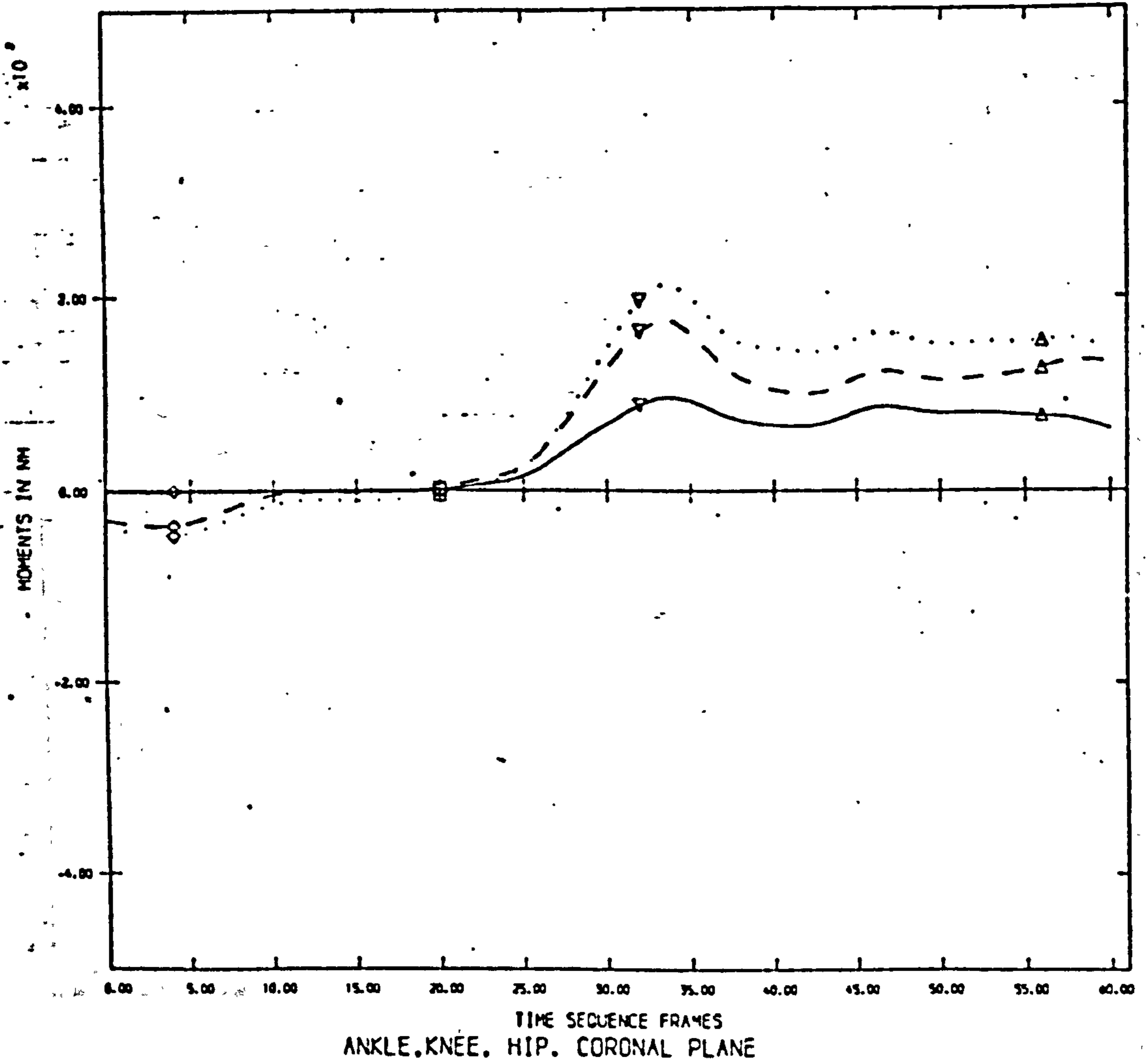
RIGHT TOE OFF  $\diamond$

P2/R/FUL1



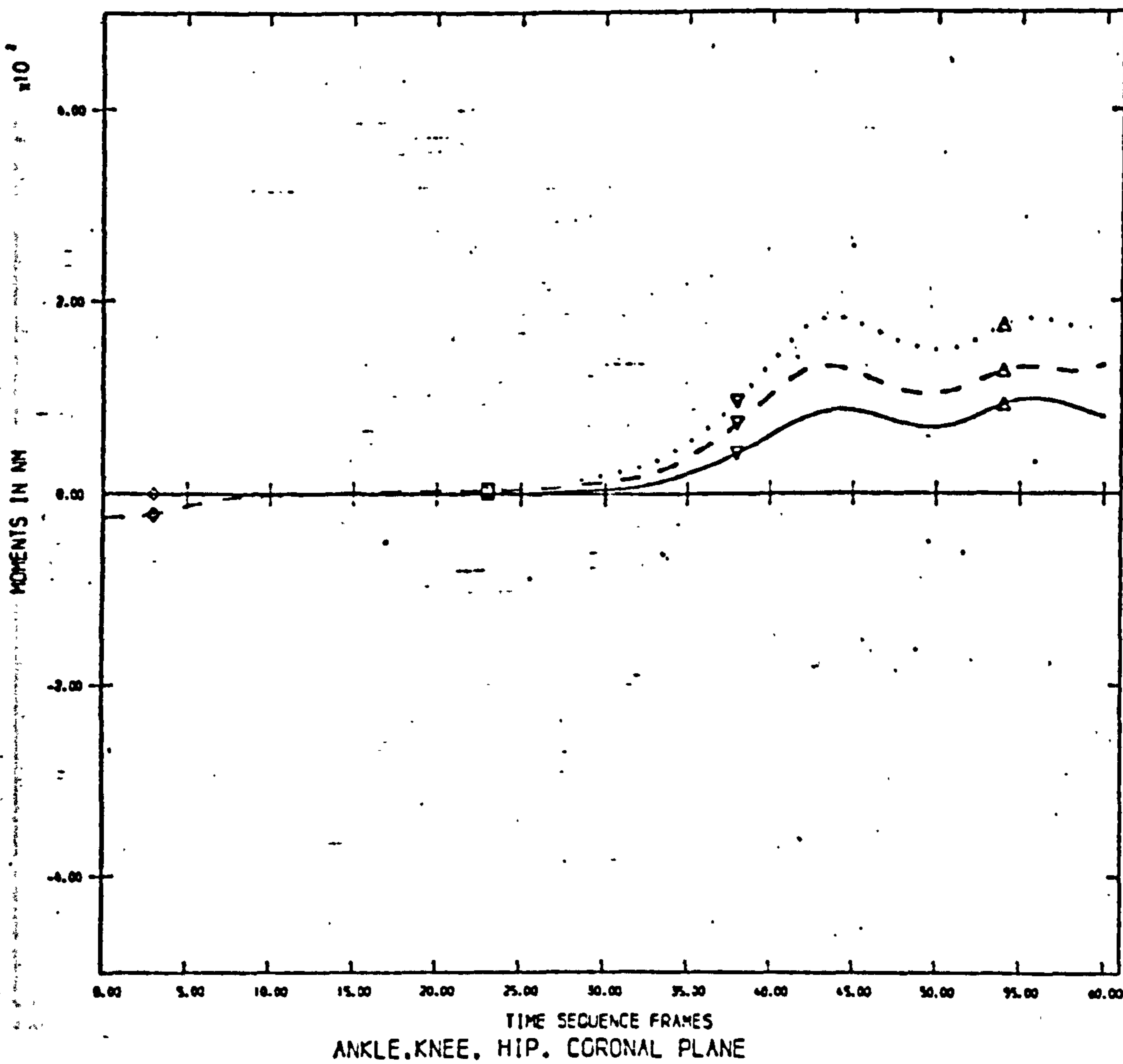
LEFT HEEL STRIKE	△	CONTINUOUS	ANKLE
LEFT TOE OFF	▽	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	◇		

P3/R/FUL1



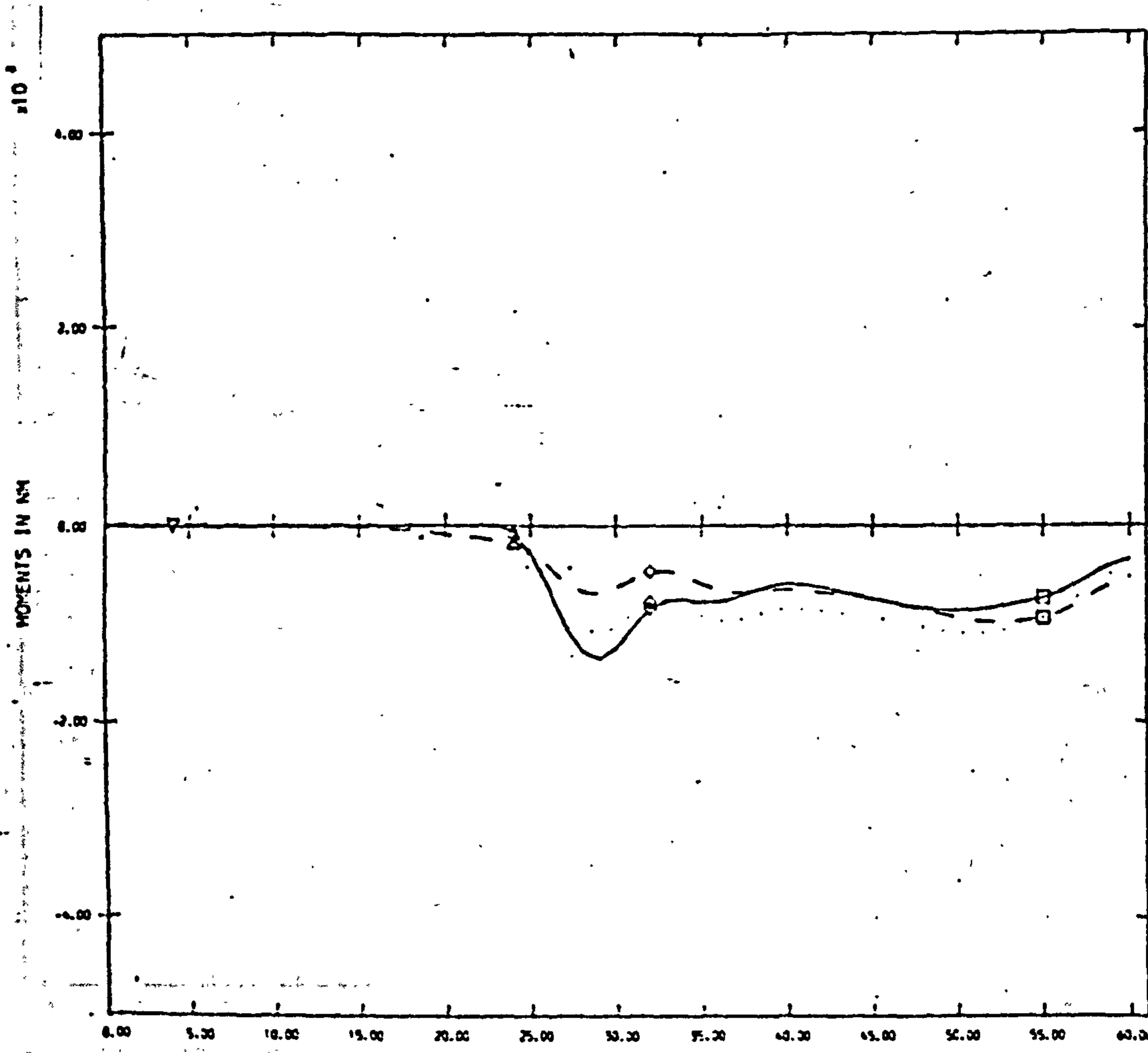
LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

P4/R/FUL1



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

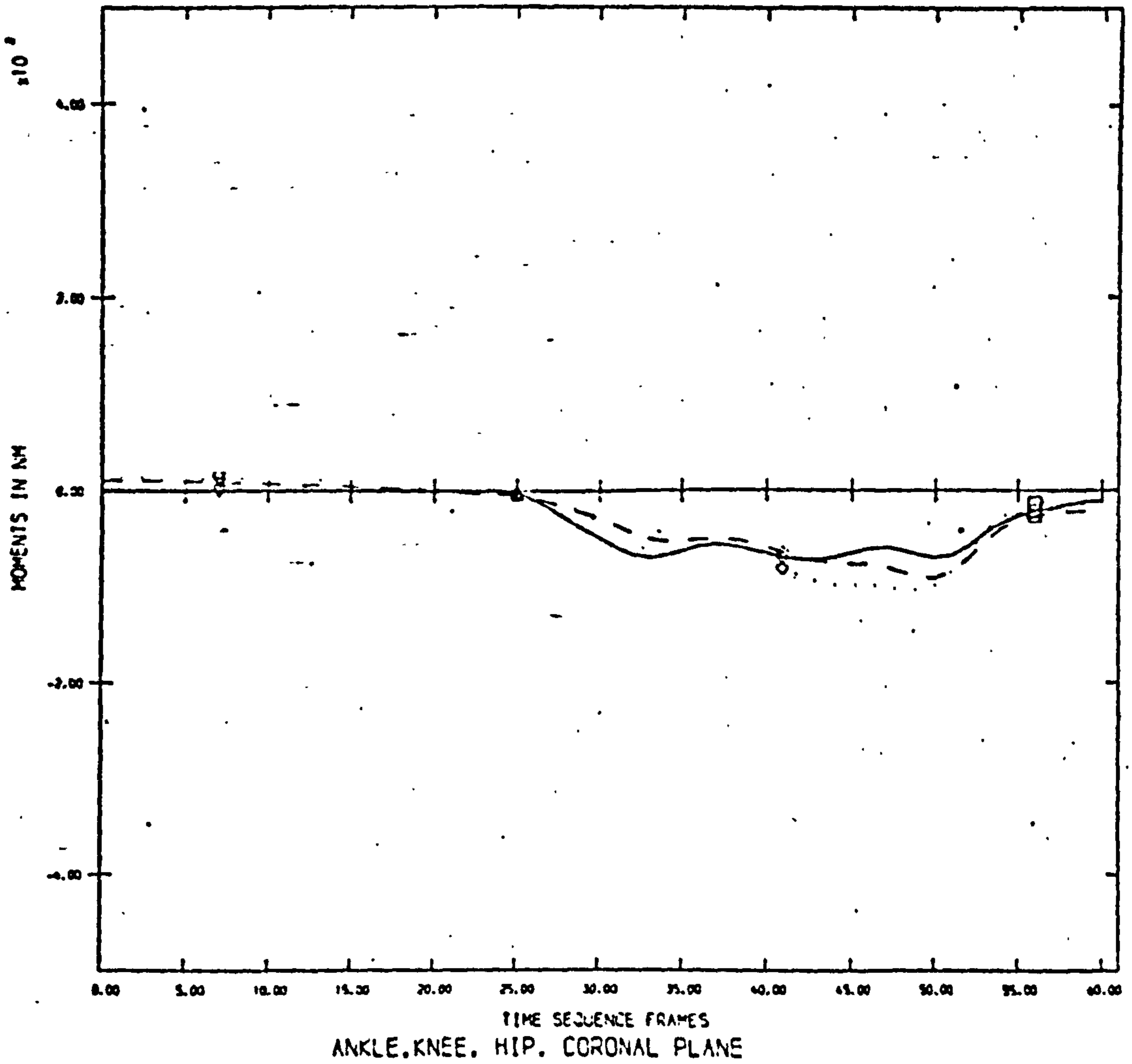
PI/L/BDT1



TIME SEQUENCE FRAMES  
ANKLE, KNEE, HIP, CORONAL PLANE

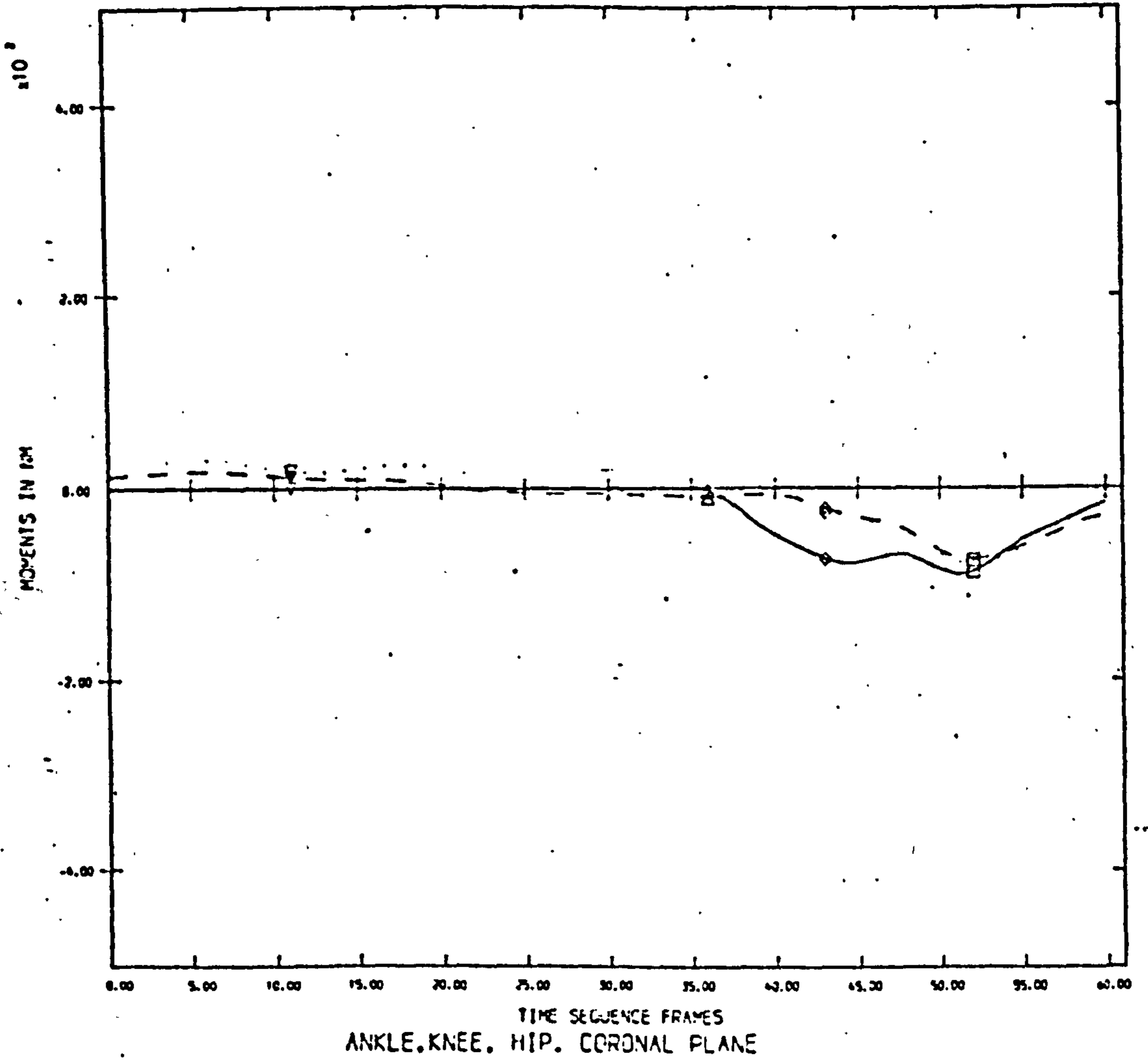
- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▼ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | □ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ○ |            |       |

P2/L/80T1



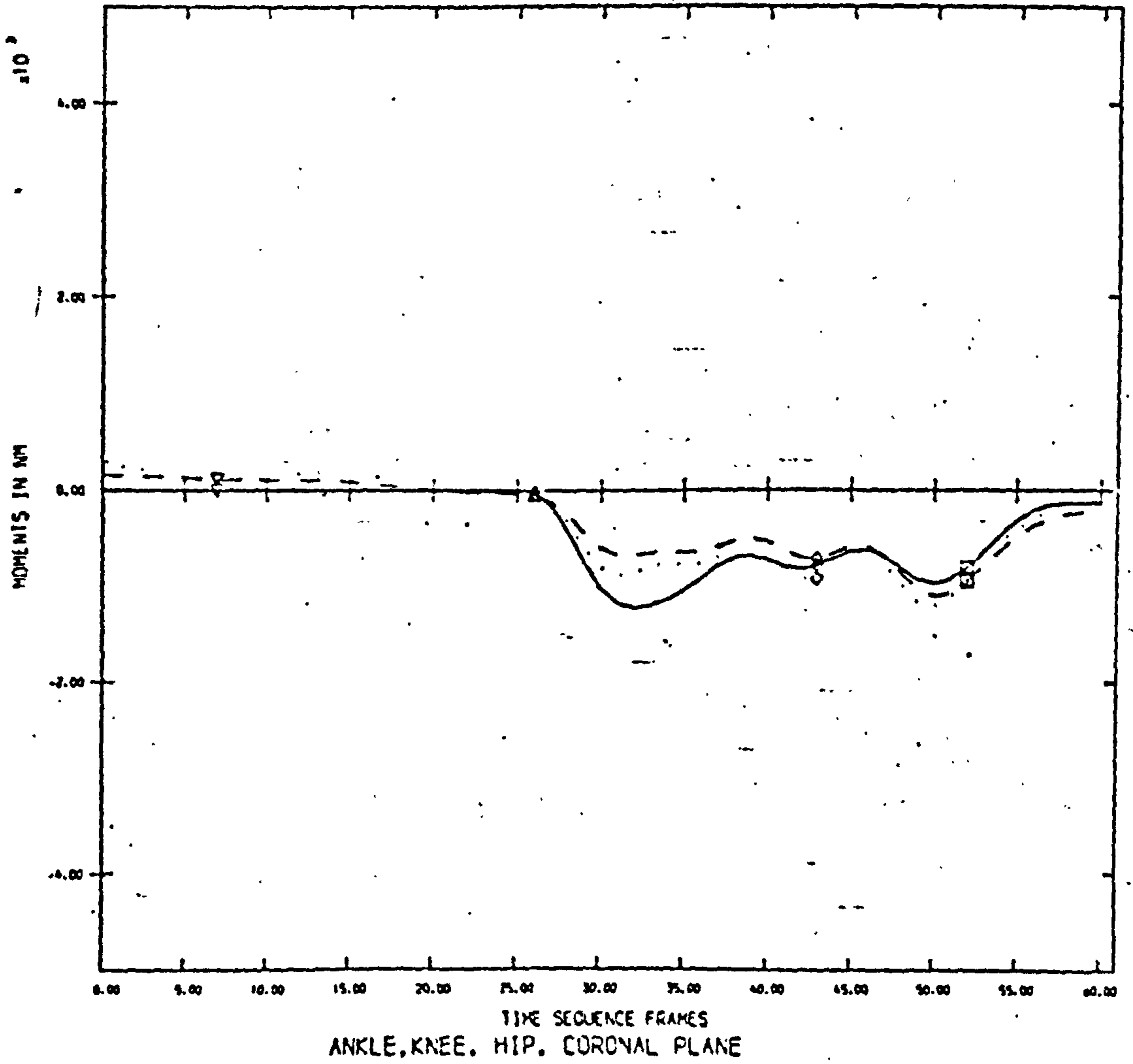
LEFT HEEL STRIKE $\Delta$	CONTINUOUS	ANKLE
LEFT TOE OFF $\nabla$	DASHED	KNEE
RIGHT HEEL STRIKE $\square$	DOTTED	HIP
RIGHT TOE OFF $\circ$		





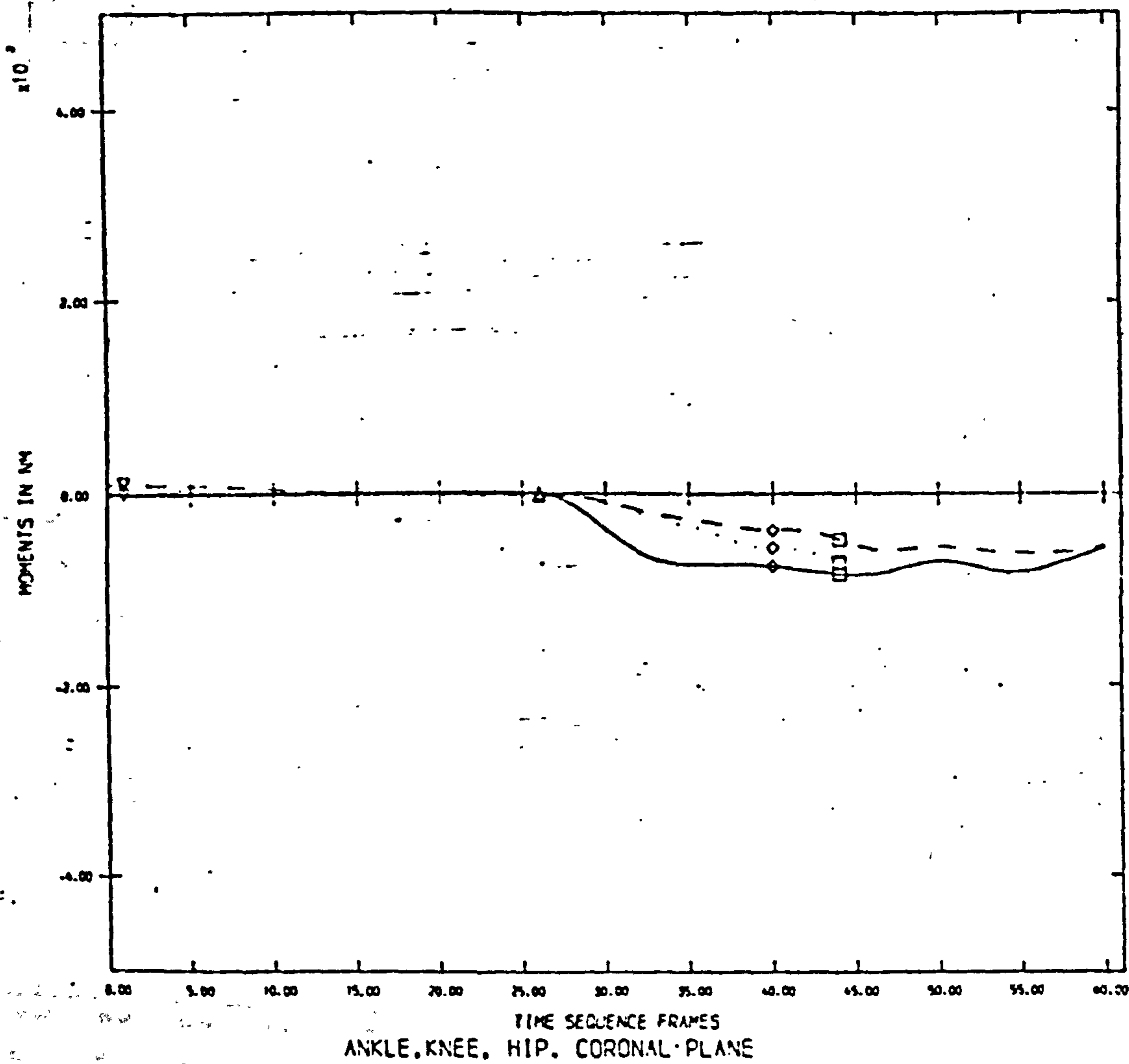
LEFT HEEL STRIKE	△	CONTINUOUS	ANKLE
LEFT TOE OFF	▽	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	◇		

P4/L/BOT1



LEFT HEEL STRIKE $\Delta$	CONTINUOUS	ANKLE
LEFT TOE OFF $\nabla$	DASHED	KNEE
RIGHT HEELSTRIKE $\square$	DOTTED	HIP
RIGHT TOE OFF $\circ$		

P6/L/BDT1



7-21-73

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303

LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

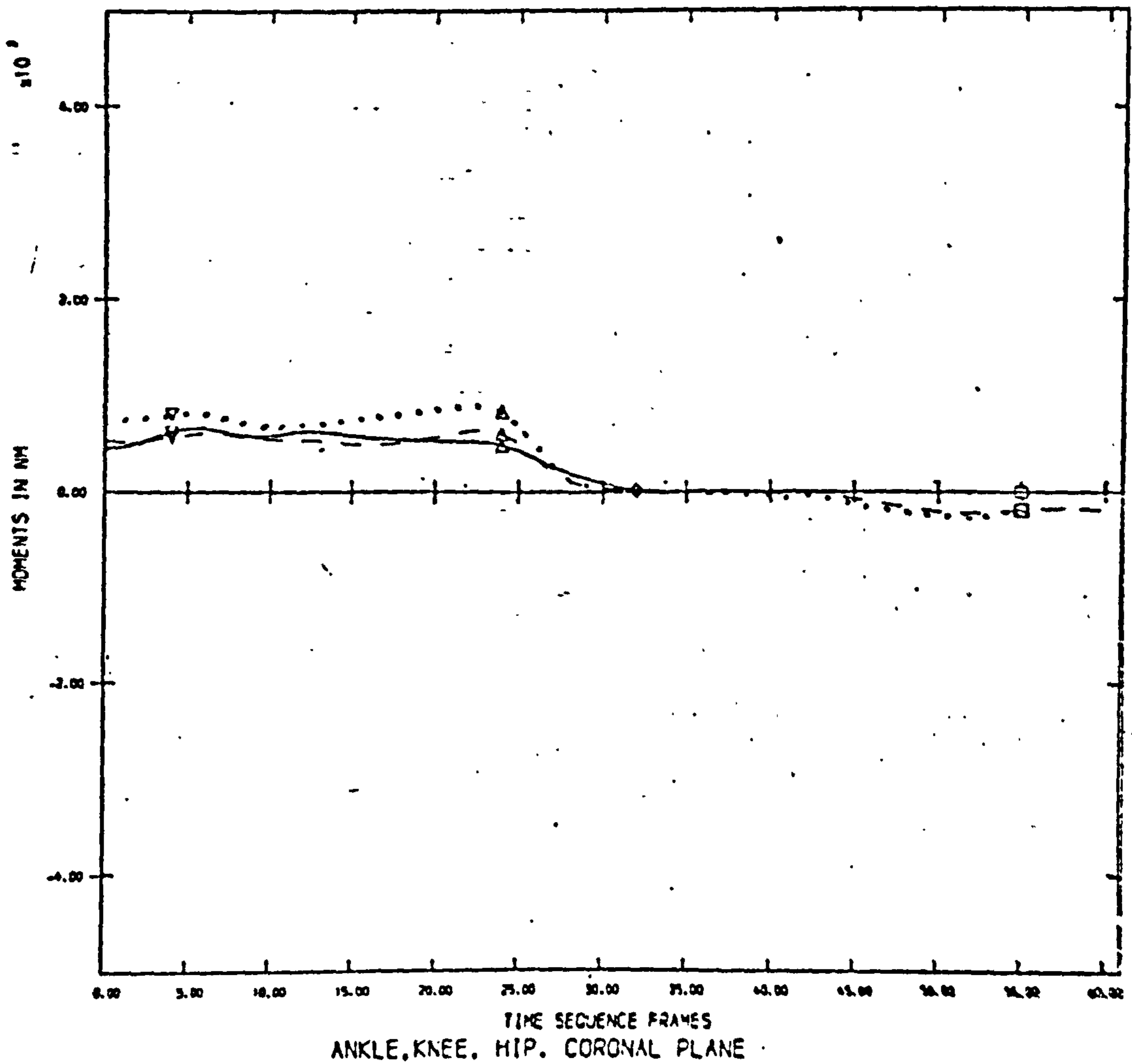
DASHED KNEE

RIGHT HEEL STRIKE  $\square$

DOTTED HIP

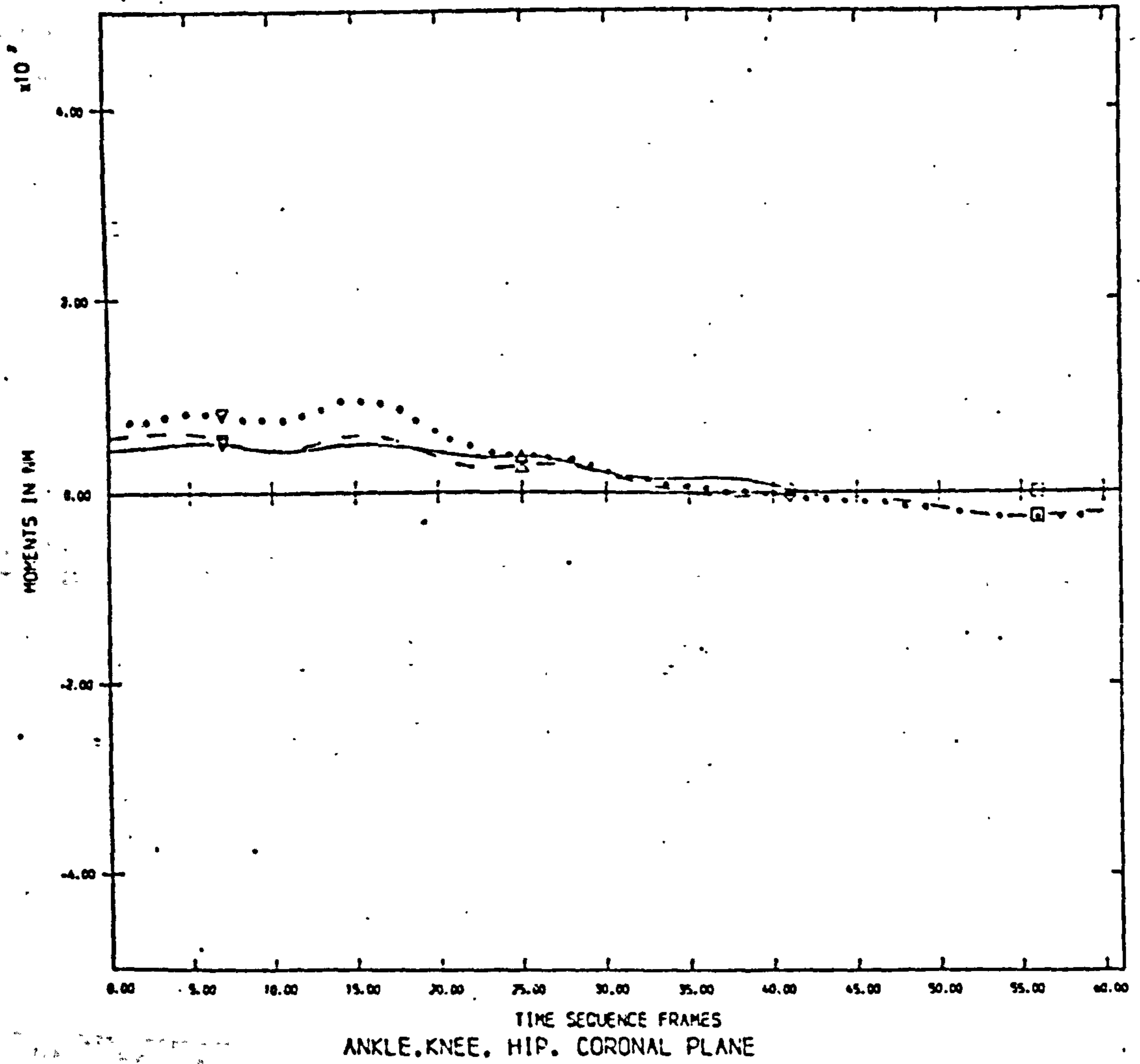
RIGHT TOE OFF  $\diamond$

PI/R/BOT1



LEFT HEEL STRIKE $\Delta$	CONTINUOUS	ANKLE
LEFT TOE OFF $\nabla$	DASHED	KNEE
RIGHT HEELSTRIKE $\square$	DOTTED	HIP
RIGHT TOE OFF $\diamond$		

P2/R/BOT1



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

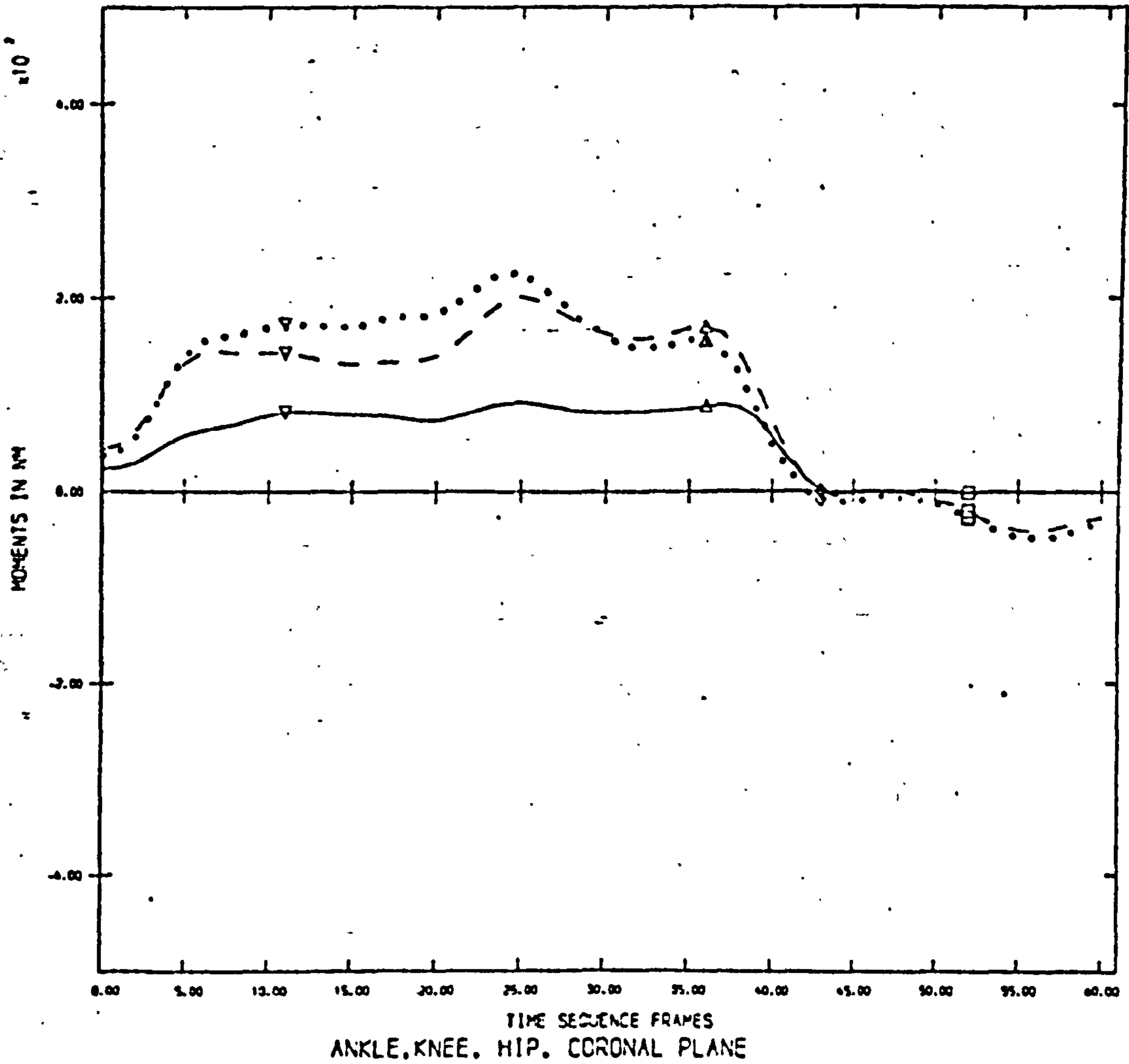
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

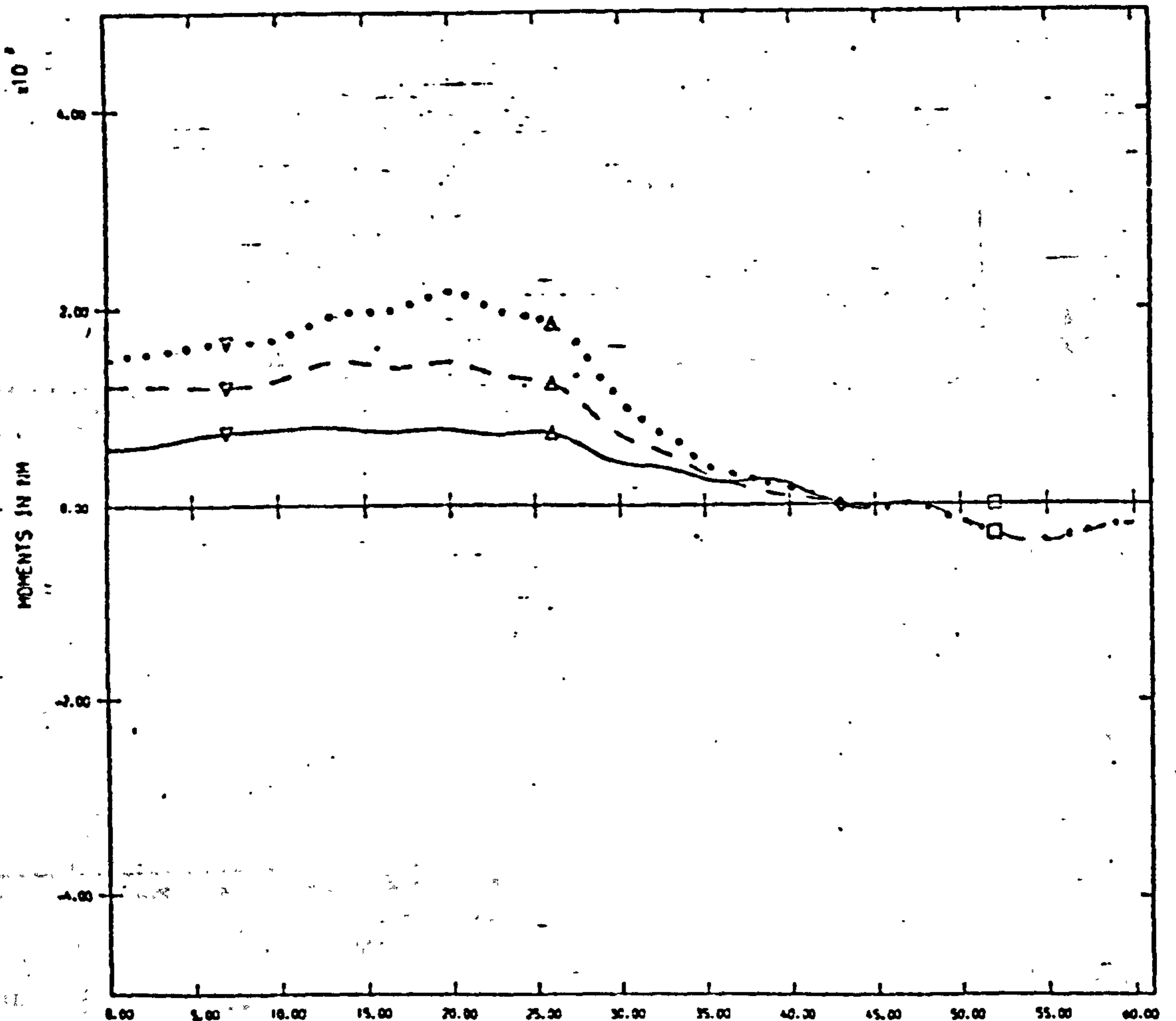
RIGHT TOE OFF  $\diamond$

P3/R/8DT1



LEFT HEEL STRIKE $\Delta$	CONTINUOUS	ANKLE
LEFT TOE OFF $\nabla$	DASHED	KNEE
RIGHT HEELSTRIKE $\square$	DOTTED	HIP
RIGHT TOE OFF $\diamond$		

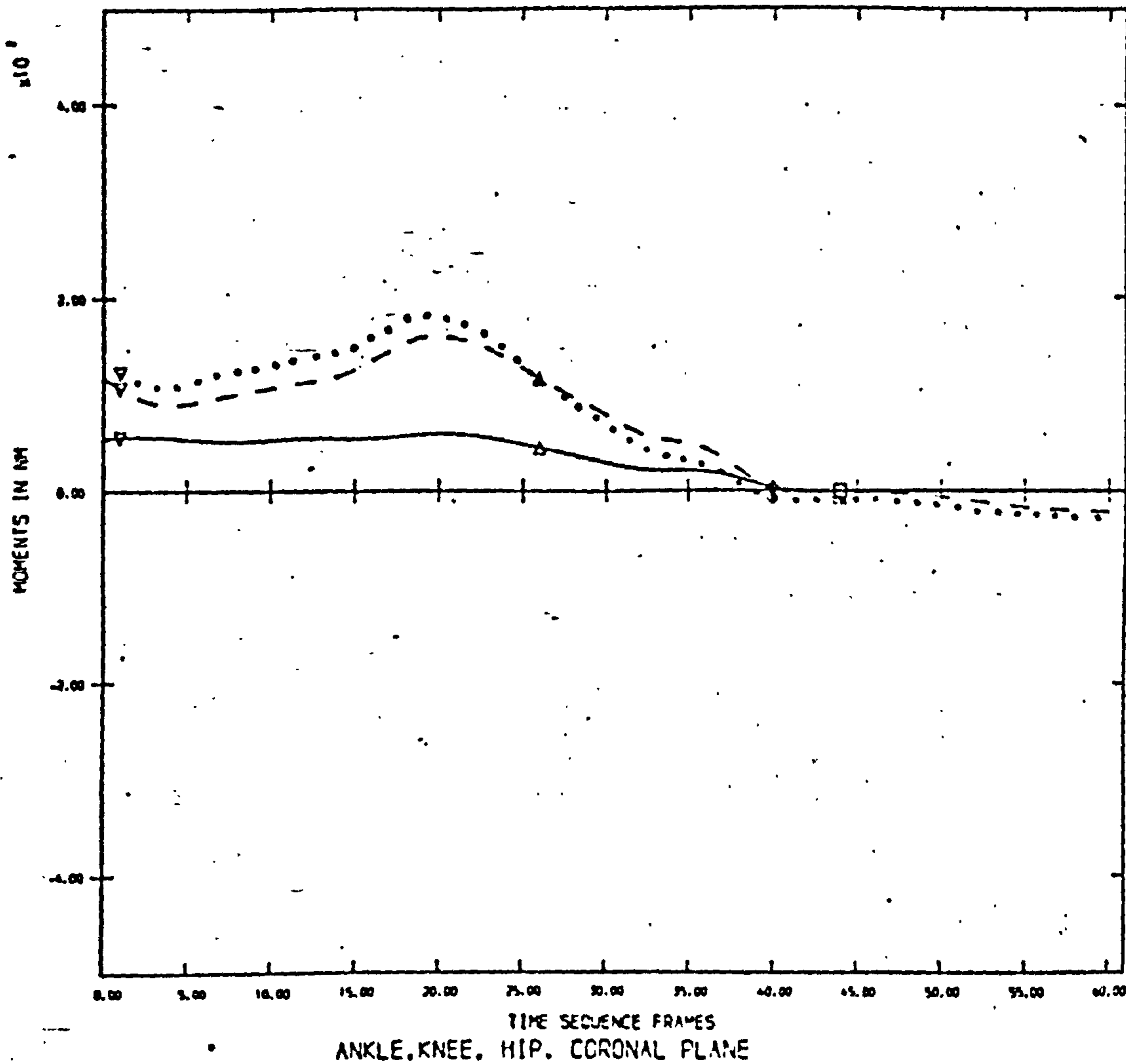
P4/R/BDT1



ANKLE, KNEE, HIP, CORONAL PLANE

- |                   |   |            |       |
|-------------------|---|------------|-------|
| LEFT HEEL STRIKE  | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF      | ▼ | DASHED     | KNEE  |
| RIGHT HEEL STRIKE | ◻ | DOTTED     | HIP   |
| RIGHT TOE OFF     | ◊ |            |       |

P6/R/BOT1



LEFT HEEL STRIKE  $\blacktriangle$

CONTINUOUS ANKLE

LEFT TOE OFF  $\blacktriangledown$

DASHED KNEE

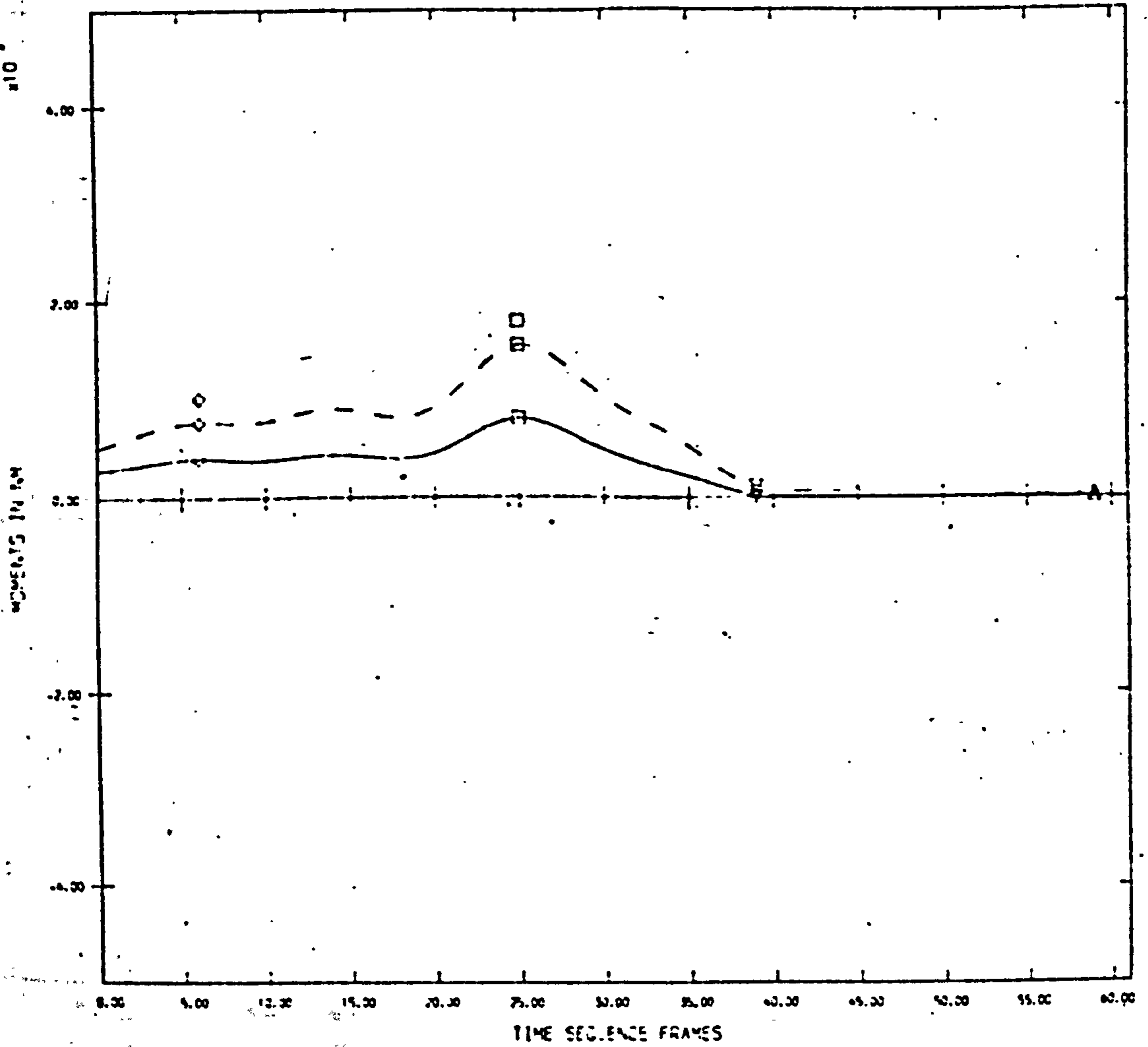
RIGHT HEELSTRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\diamond$



P6/L/FULO



ANKLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE ▲

CONTINUOUS ANKLE

LEFT TOE OFF ▼

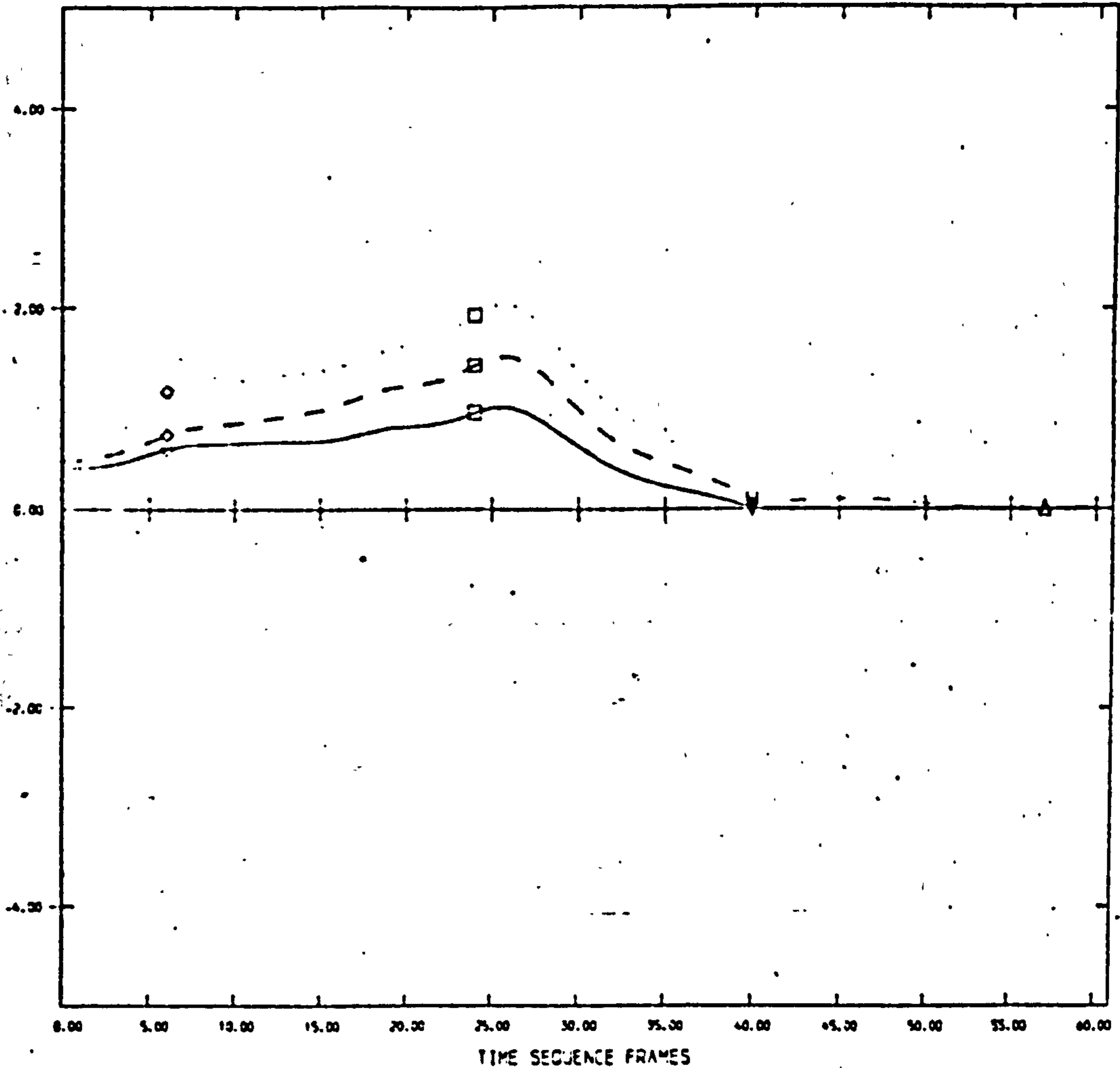
DASHED KNEE

RIGHT HEEL STRIKE □

DOTTED HIP

RIGHT TOE OFF ○

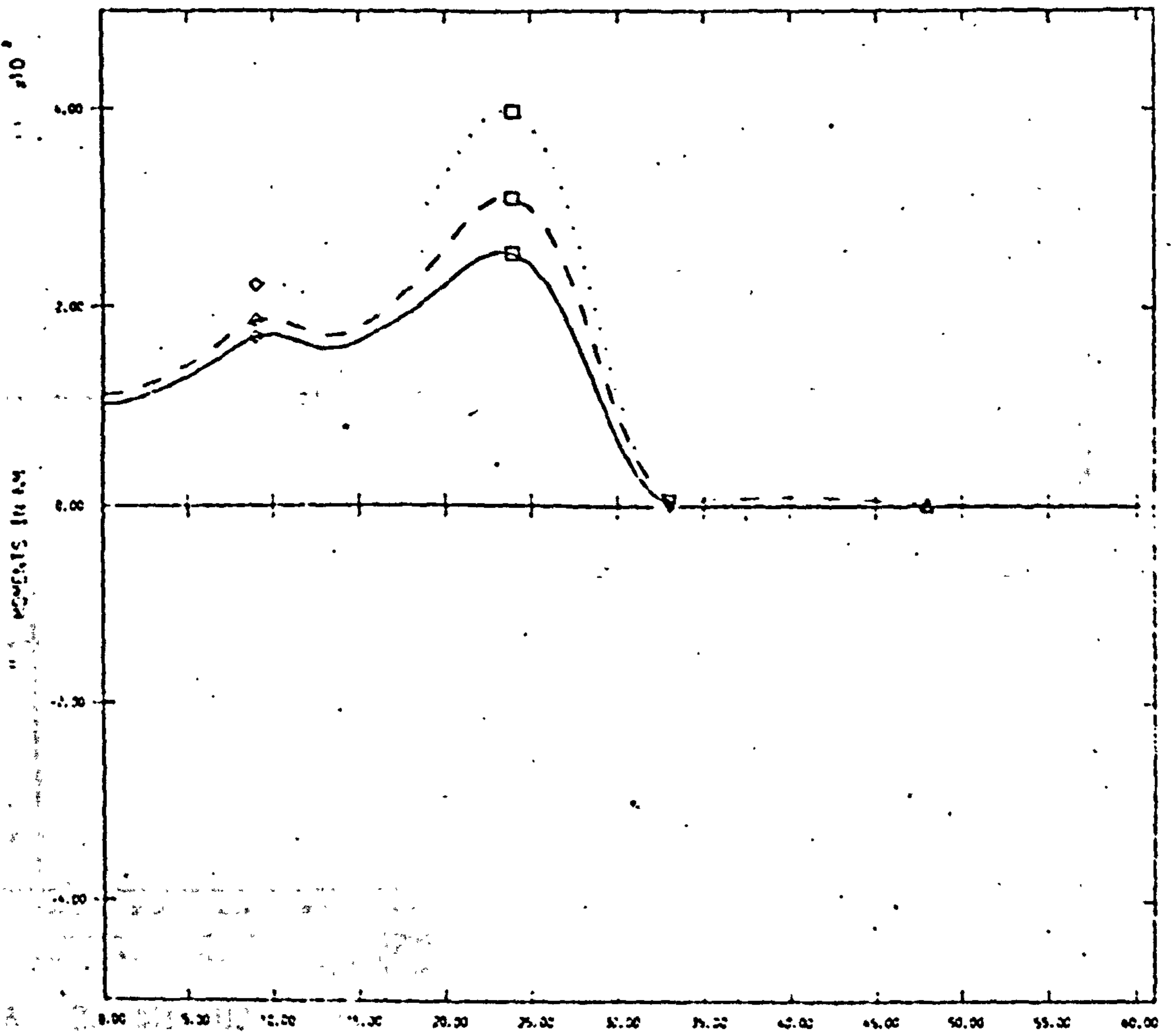
P4/L/FULO



ANKLE, KNEE, HIP, SAGITTAL PLANE

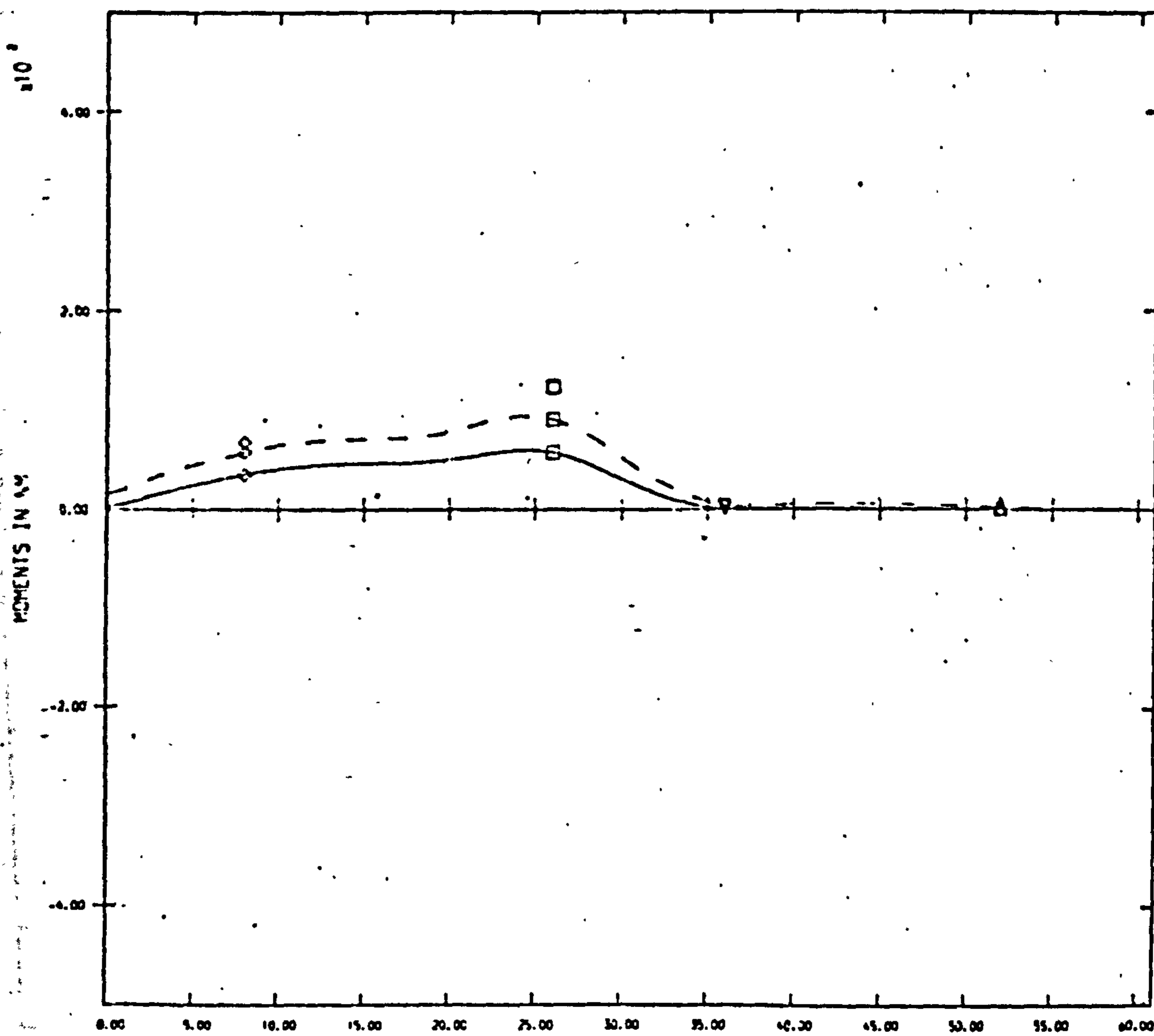
- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▼ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | □ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ◇ |            |       |

PI/L/FULO



01:10 08:00 09:30 11:00 12:30 14:00 15:30 17:00 18:30 20:00 21:30 23:00 24:30 26:00 27:30 29:00 30:30 32:00 33:30 35:00 36:30 38:00 39:30 41:00 42:30 44:00 45:30 47:00 48:30 50:00 51:30 53:00 54:30 56:00 57:30 59:00 60:00  
 ANKLE, KNEE, HIP, SAGITTAL PLANE  
 LEFT HEEL STRIKE ▲ CONTINUOUS ANKLE  
 LEFT TOE OFF ▼ DASHED KNEE  
 RIGHT HEEL STRIKE □ DOTTED HIP  
 RIGHT TOE OFF ◇

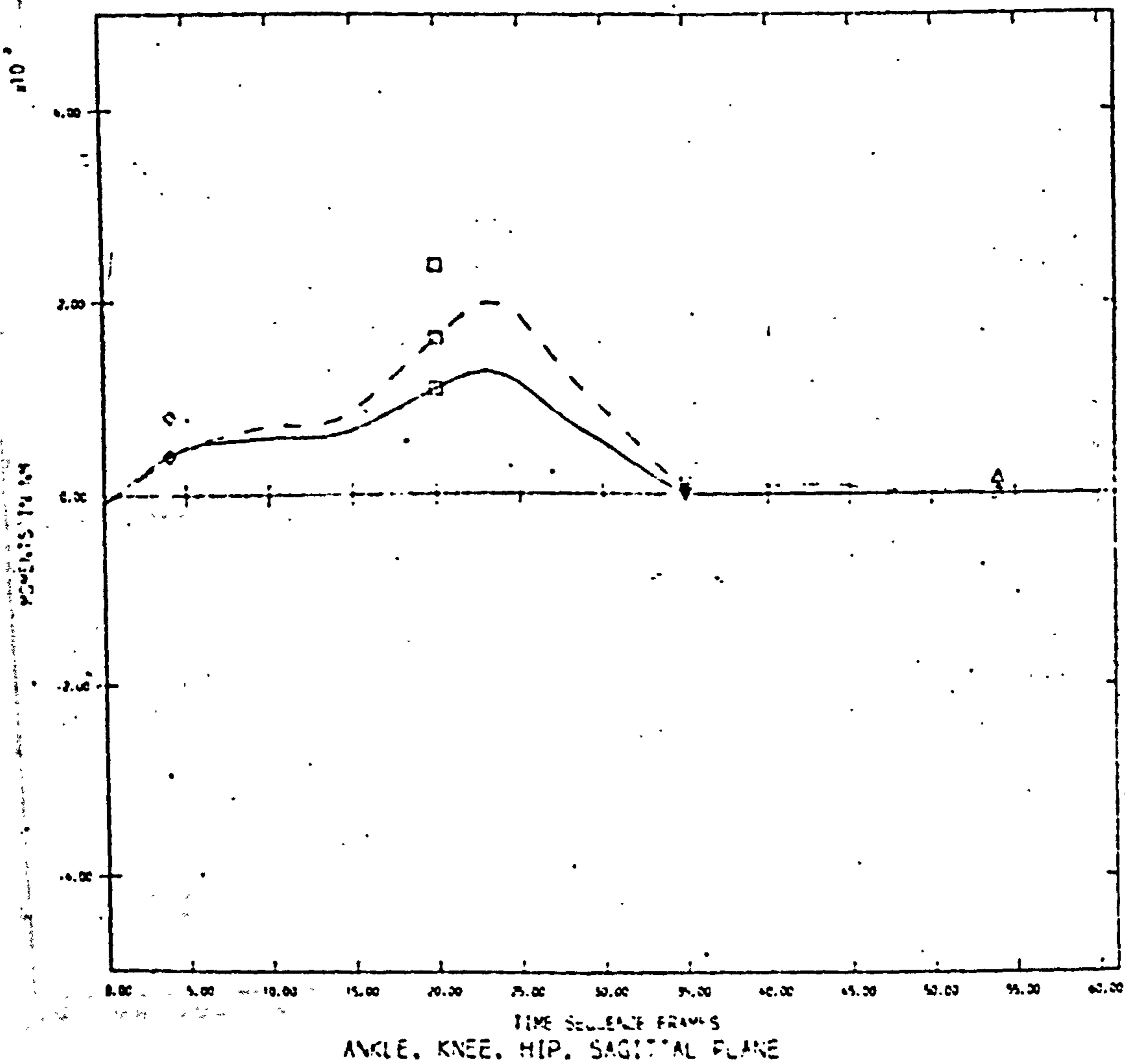
P2/L/FULO



ANKLE, KNEE, HIP. SAGITTAL PLANE

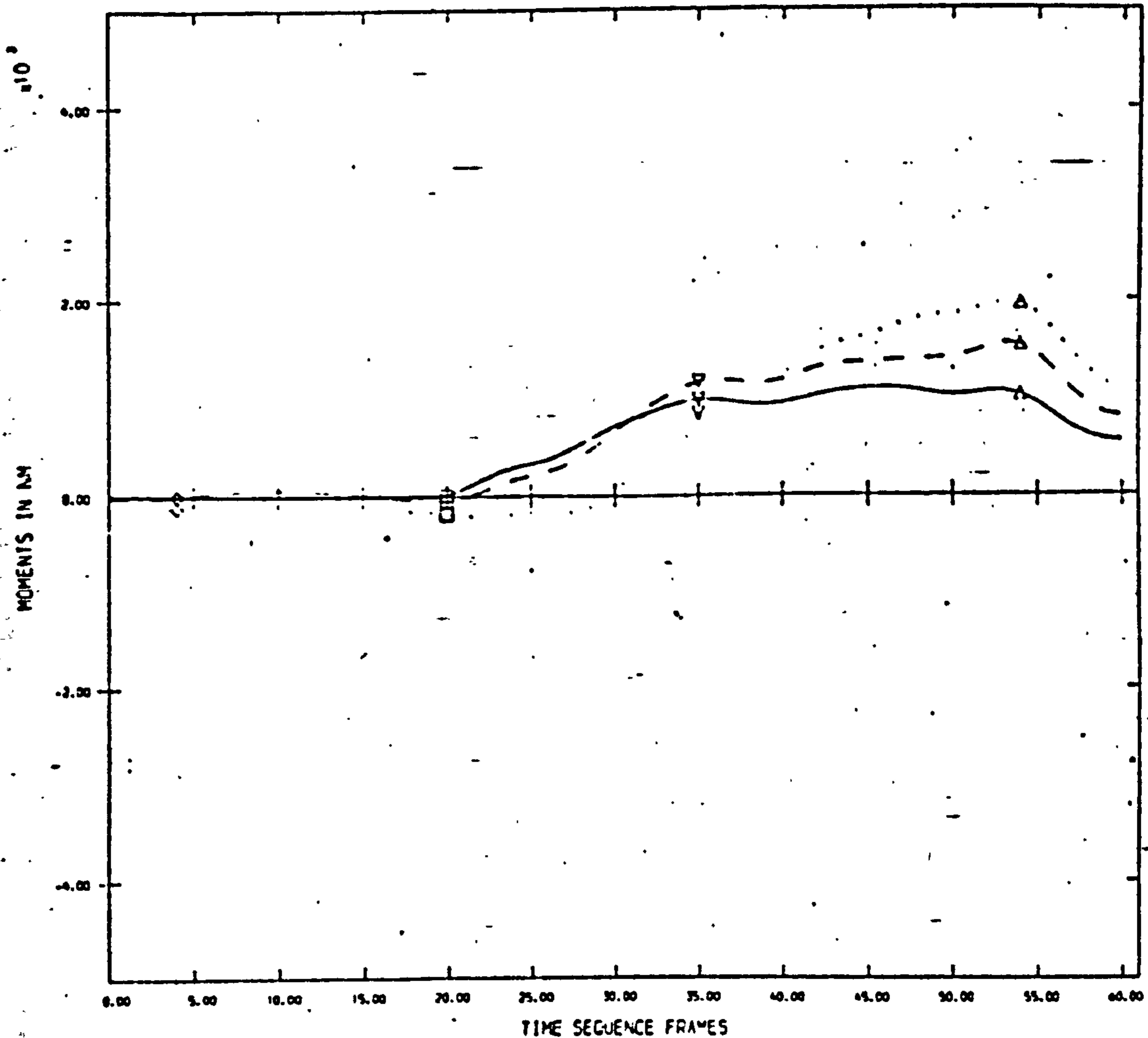
- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | △ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▽ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | □ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ○ |            |       |

P3/L/FULO



- LEFT HEEL STRIKE  $\Delta$  CONTINUOUS ANKLE
- LEFT TOE OFF  $\nabla$  DASHED KNEE
- RIGHT HEELSTRIKE  $\square$  DOTTED HIP
- RIGHT TOE OFF  $\diamond$

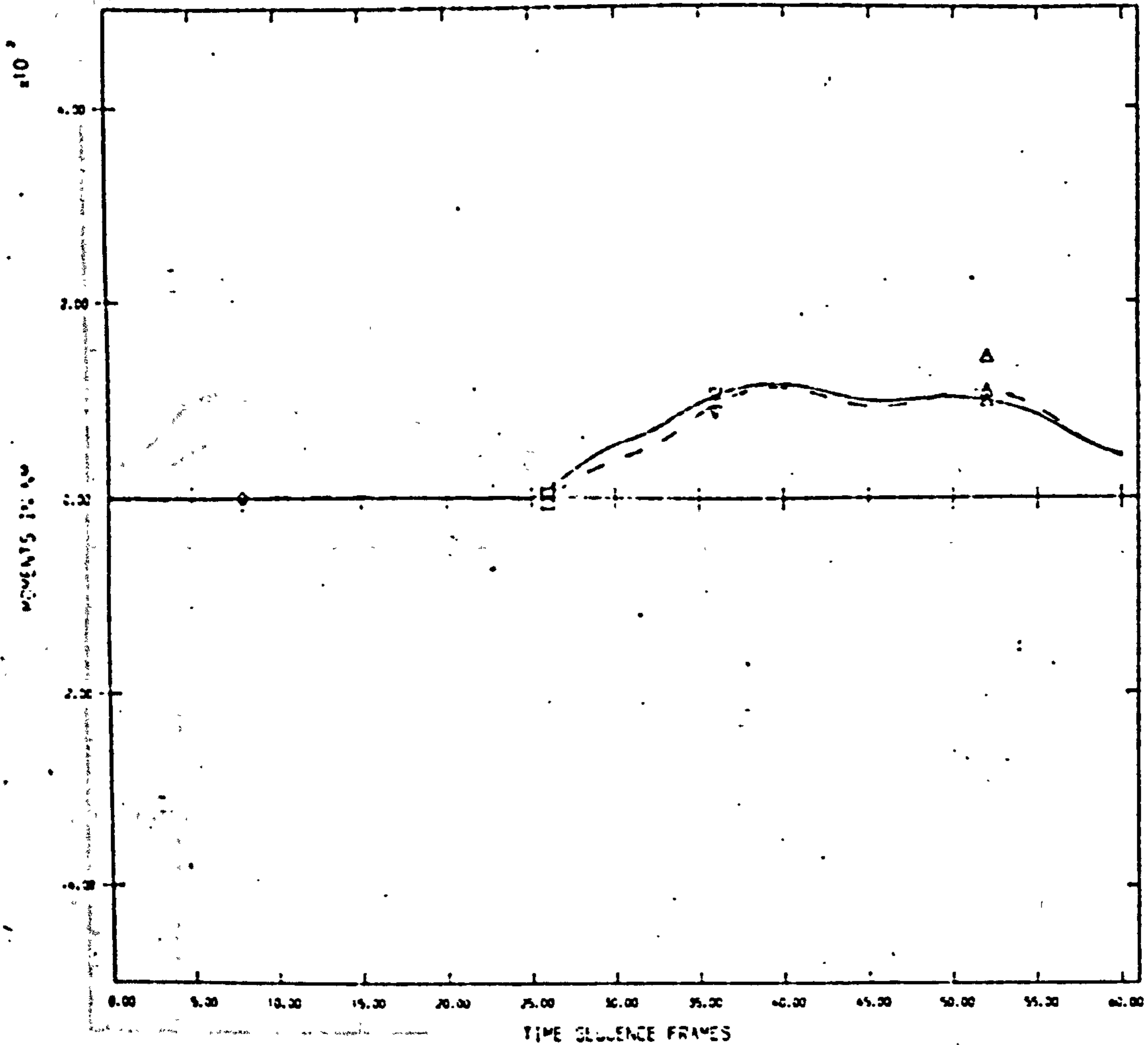
P3/R/FULO



ANKLE, KNEE, HIP, SAGITTAL PLANE

- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | △ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▽ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | □ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ◇ |            |       |

P2/R/FUL0



ANGLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

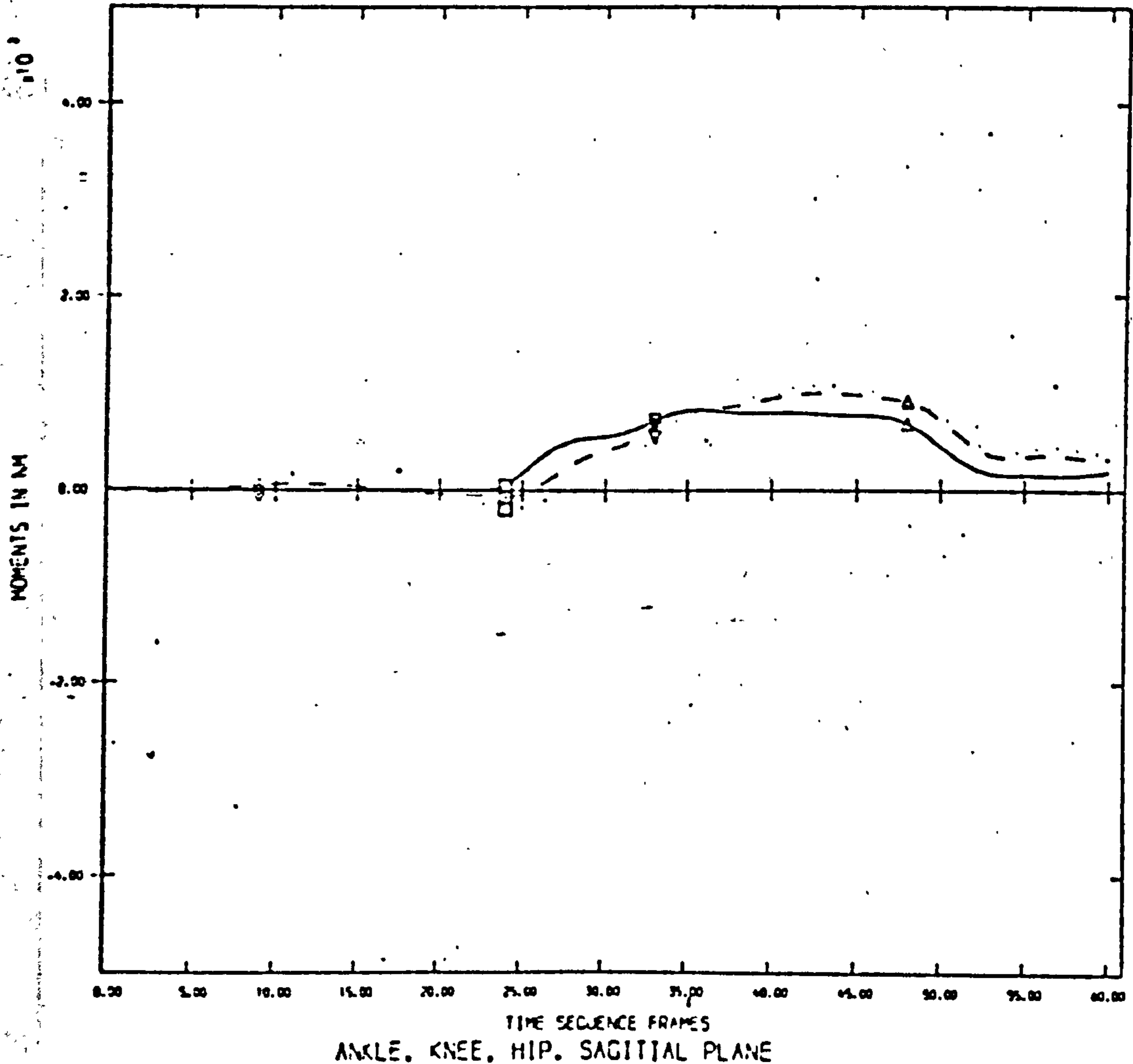
DASHED KNEE

RIGHT HEEL STRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\diamond$

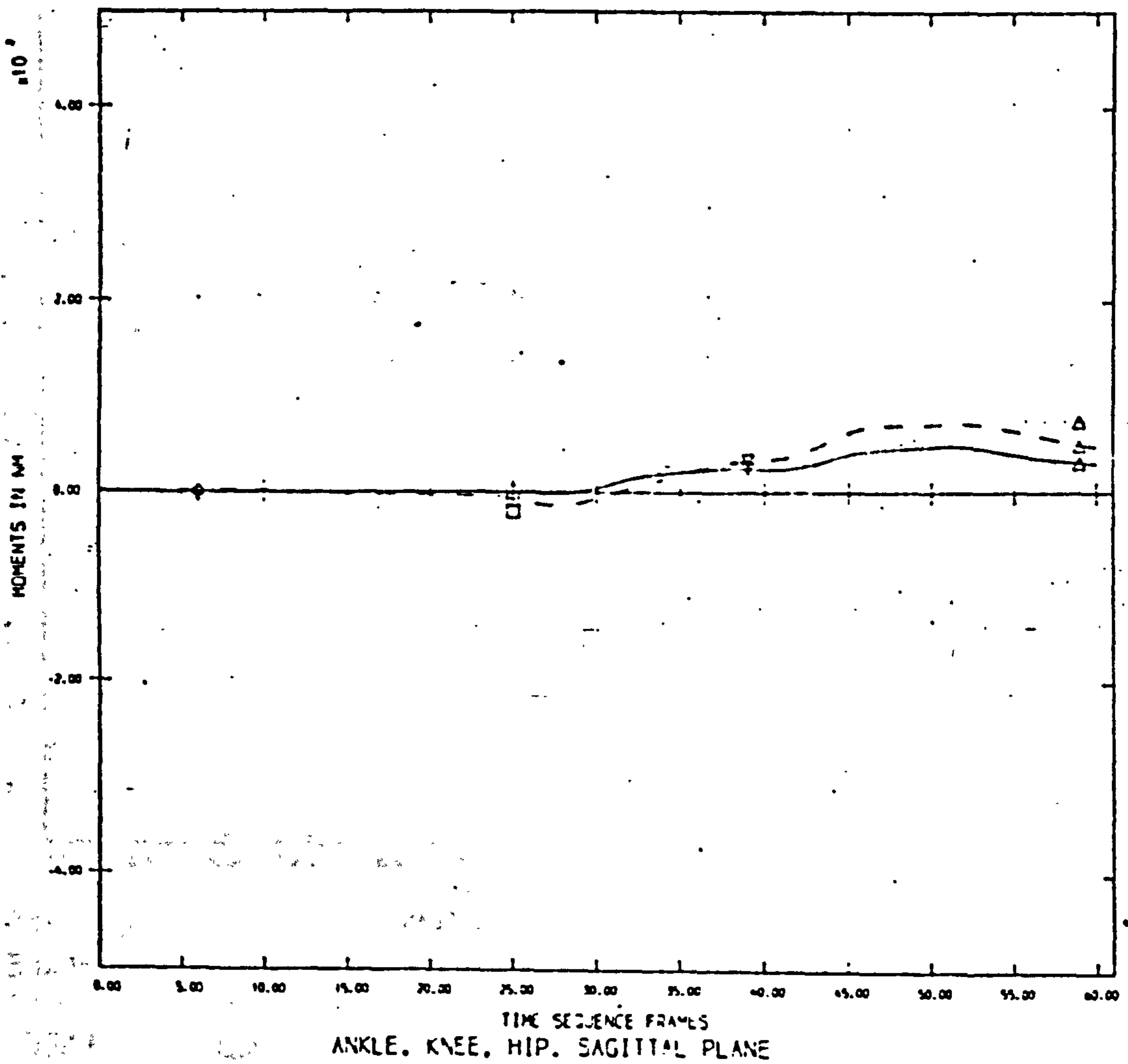
PI/R/FULO



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRKE	□	DOTTED	HIP
RIGHT TOE OFF	○		

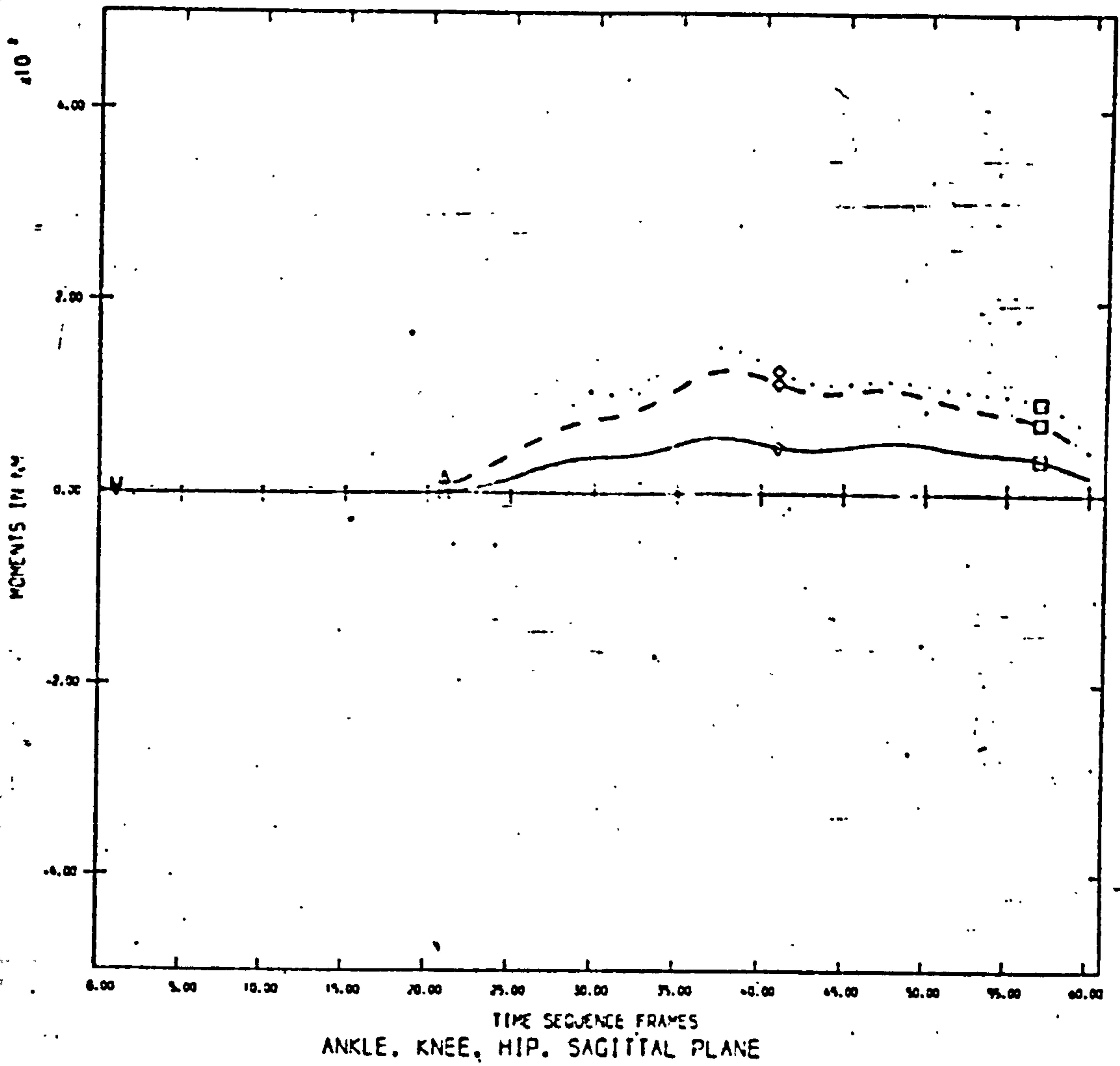


P6/R/FULO



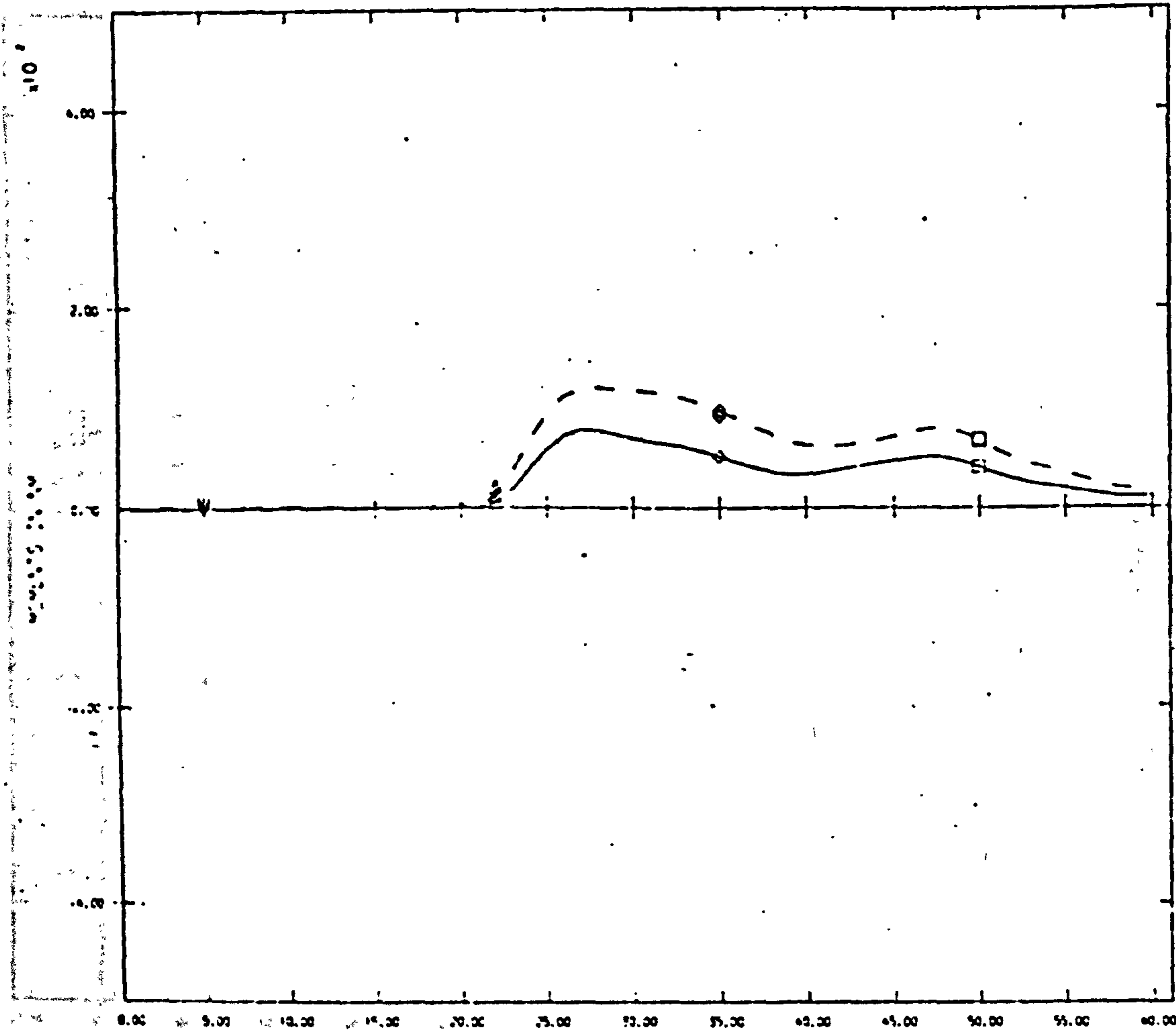
LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEEL STRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

P6/L/BDTO



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	○		

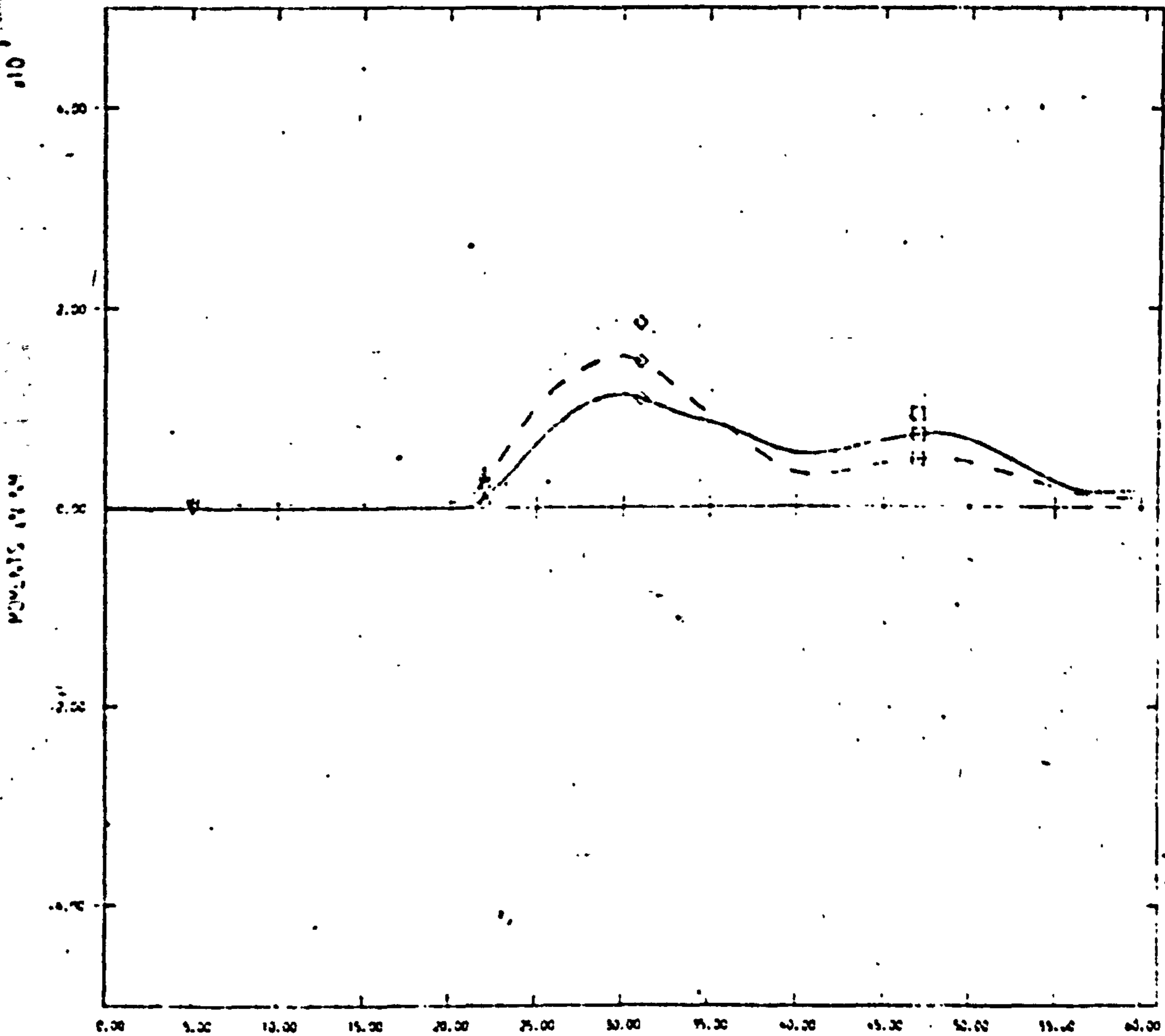
P4/L/B0T0



ANKLE, KNEE, HIP, SAGITTAL PLANE

0.00	LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
25.00	LEFT TOE OFF	▼	DASHED	KNEE
35.00	RIGHT HEEL STRIKE	□	DOTTED	HIP
55.00	RIGHT TOE OFF	○		

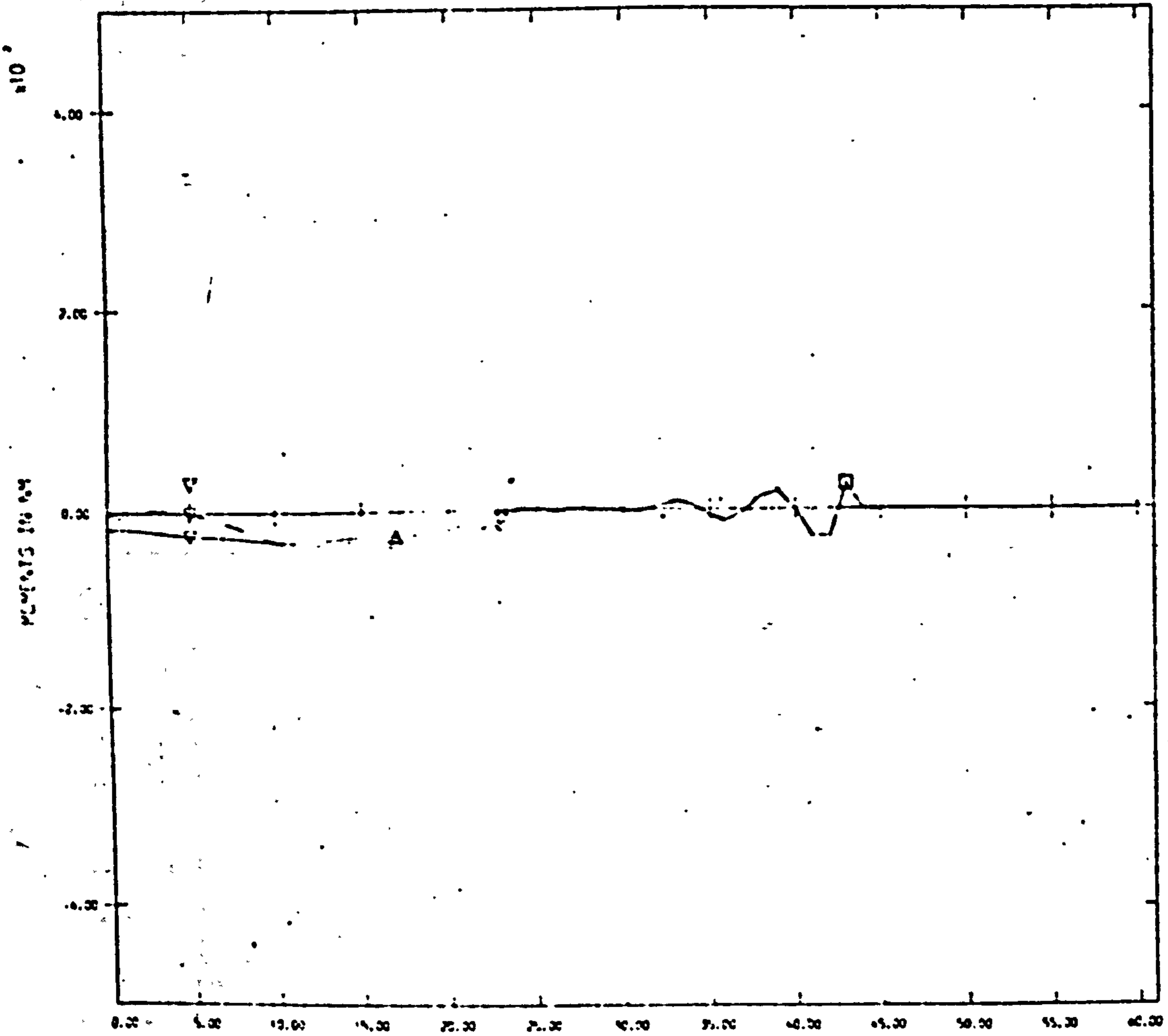
P3/L/B010



ANGLE. KNEE. HIP. SAGITTAL PLANE

- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▼ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | □ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ◇ |            |       |

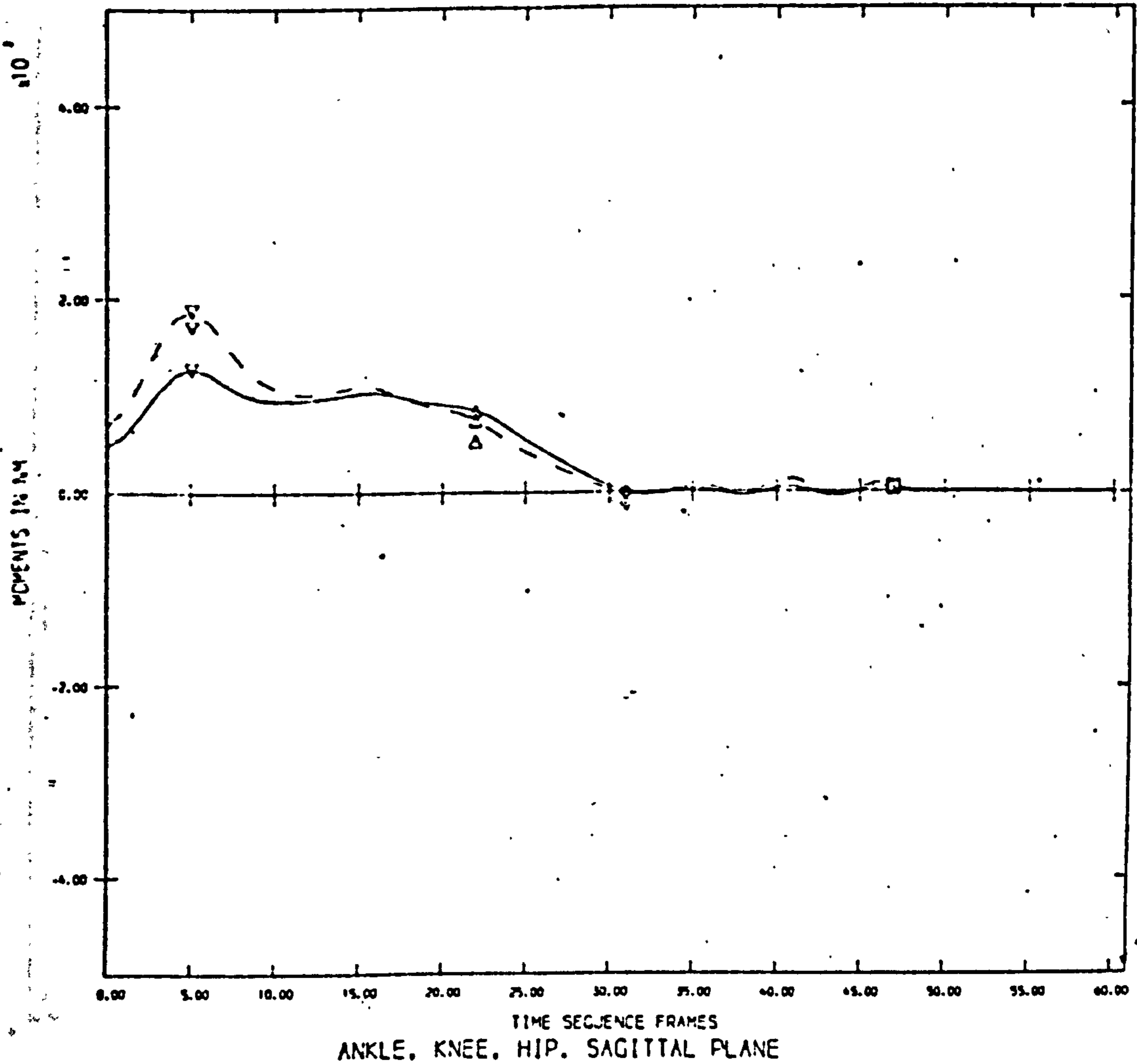
P2/R/BOT0



ANKLE, KNEE, HIP, SAGITTAL PLANE

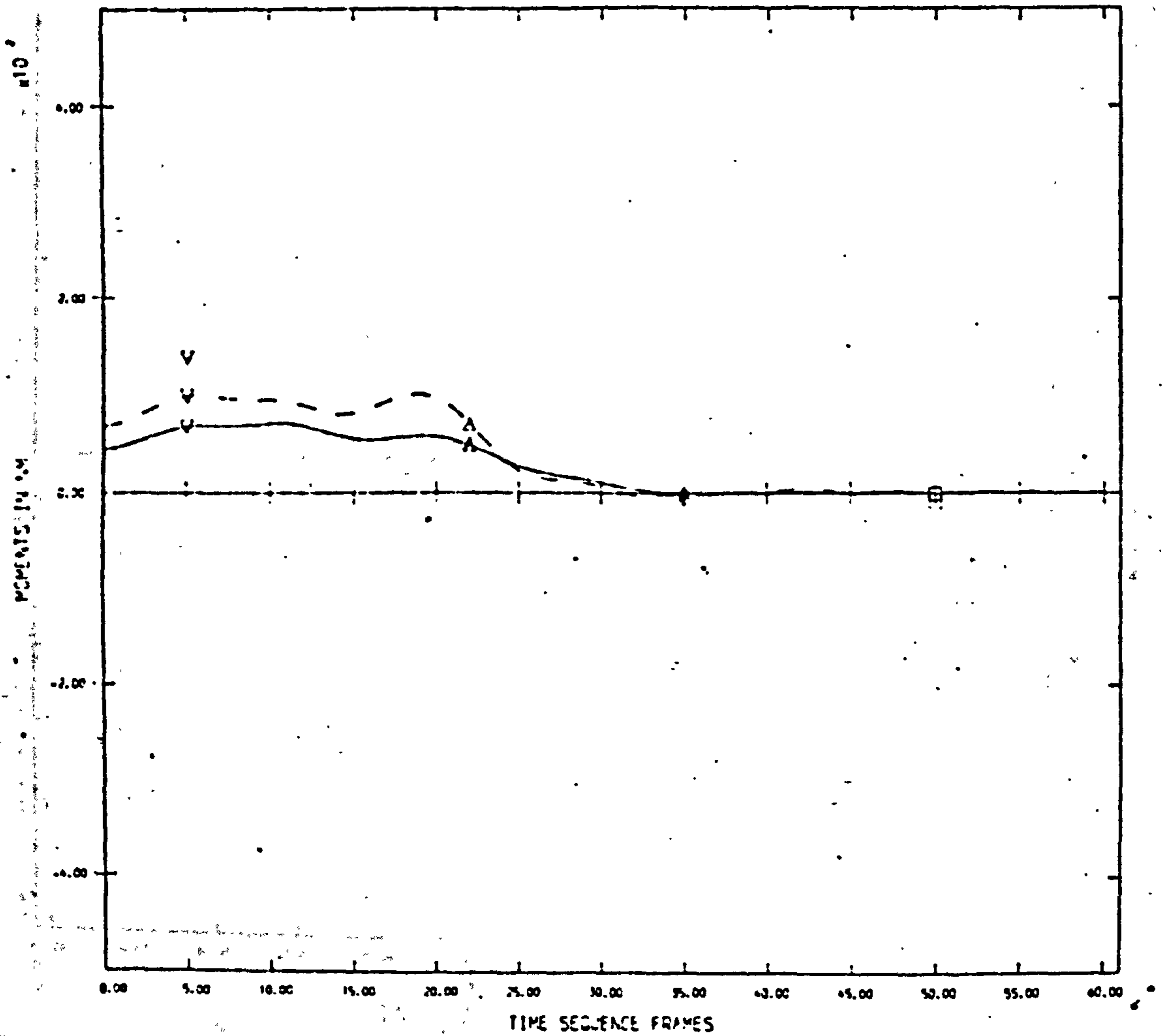
- |                   |   |            |       |
|-------------------|---|------------|-------|
| LEFT HEEL STRIKE  | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF      | ▼ | DASHED     | KNEE  |
| RIGHT HEEL STRIKE | ◻ | DOTTED     | HIP   |
| RIGHT TOE OFF     | ◊ |            |       |

P3/R/BD10



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	◇		

P4/R/BDT0



ANKLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE ▲

CONTINUOUS ANKLE

LEFT TOE OFF ▼

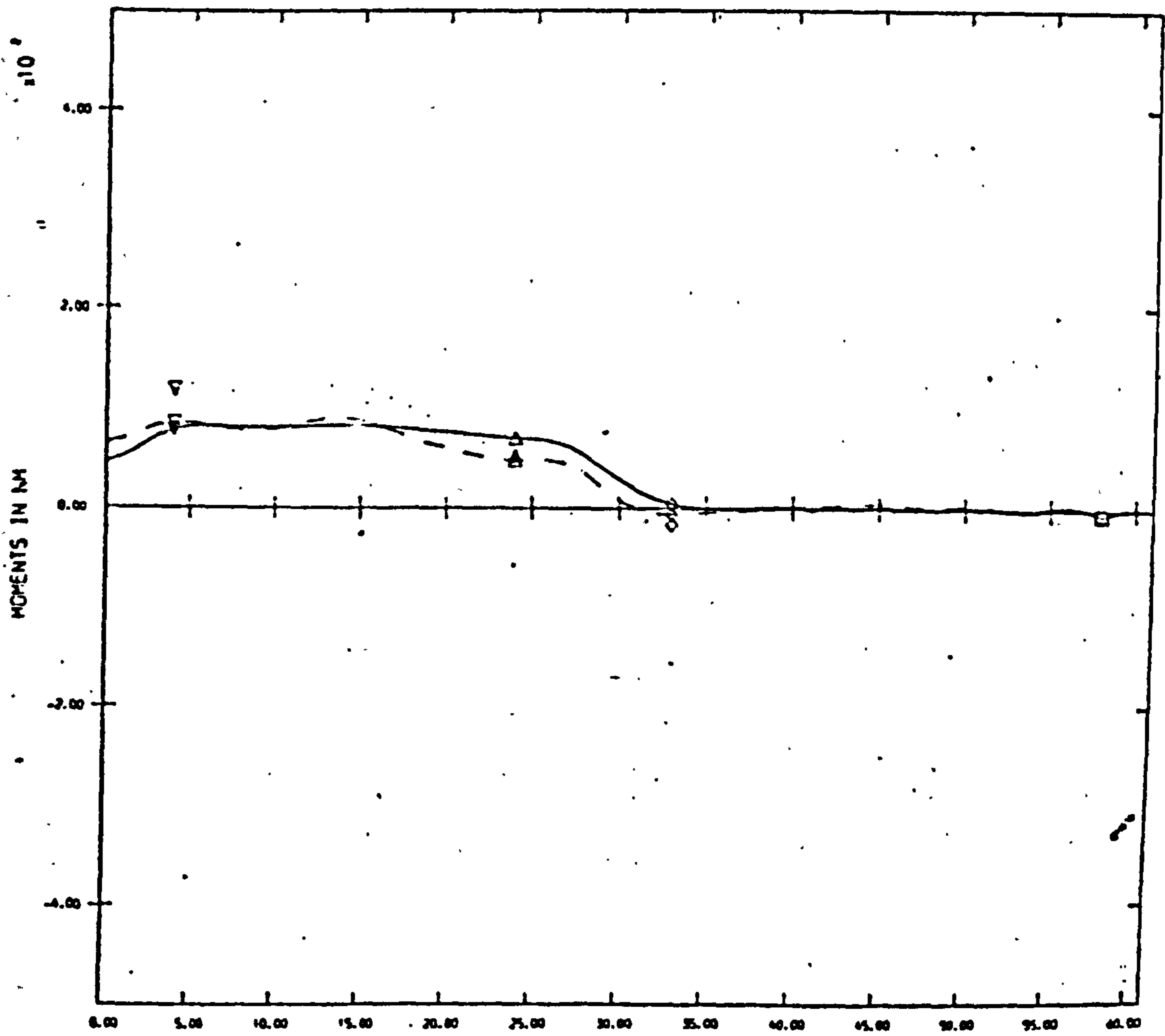
DASHED KNEE

RIGHT HEELSTRIKE □

DOTTED HIP

RIGHT TOE OFF ◇

PI/R/BDTO



ANKLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE  $\Delta$

LEFT TOE OFF  $\nabla$

RIGHT HEELSTRIKE  $\square$

RIGHT TOE OFF  $\diamond$

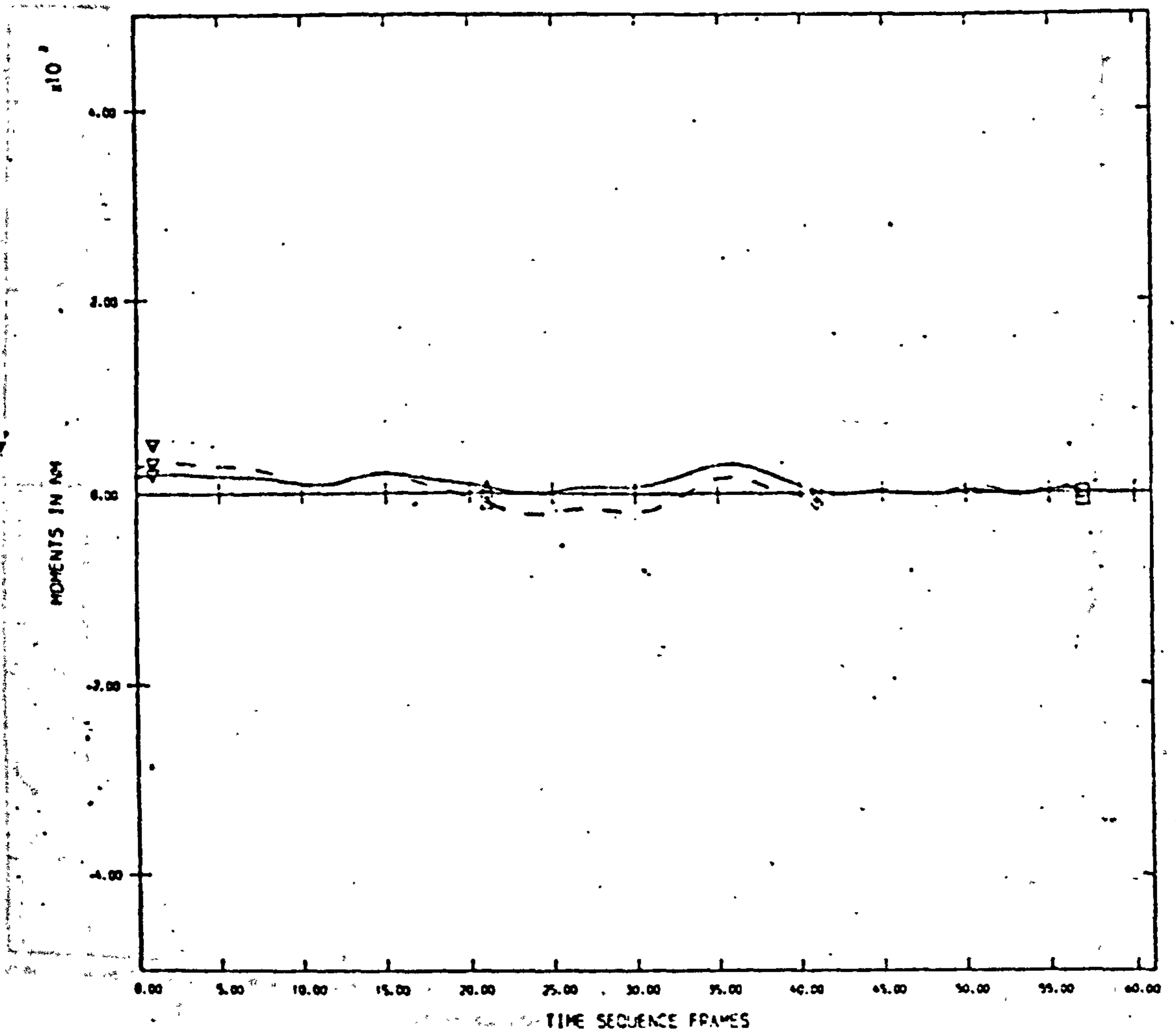
CONTINUOUS ANKLE

DASHED KNEE

DOTTED HIP



P6/R/BDTO



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

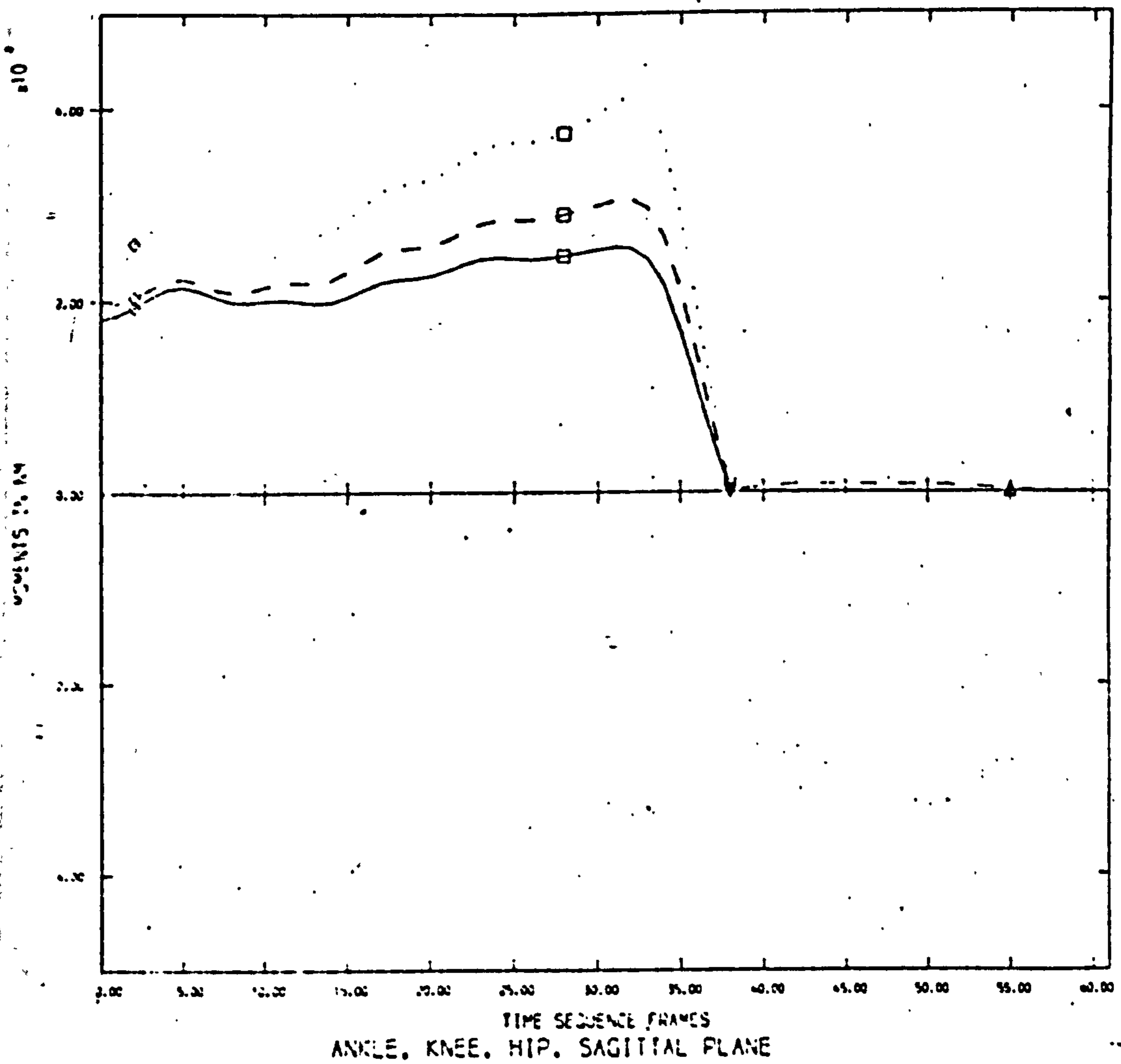
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

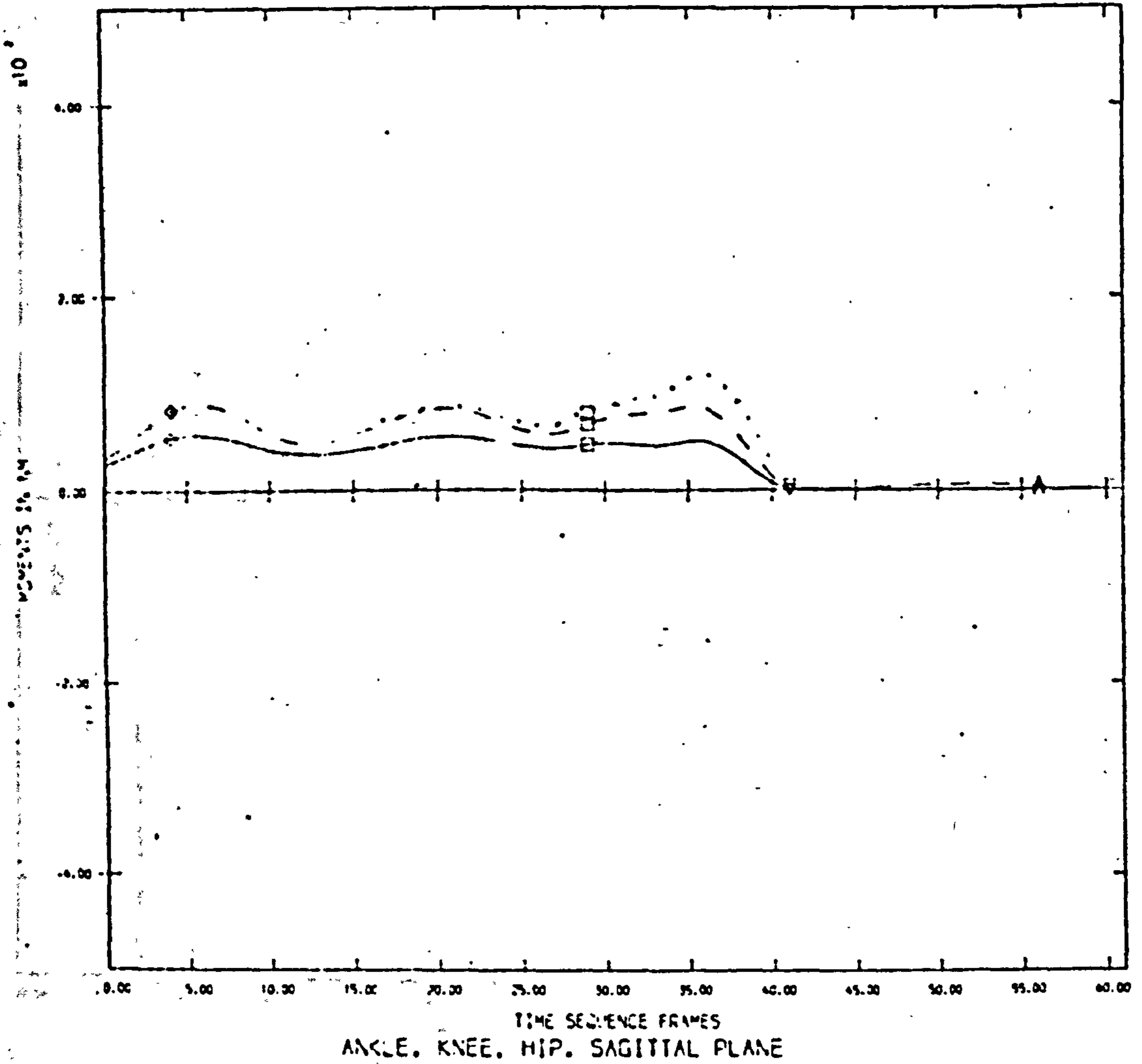
RIGHT TOE OFF  $\diamond$

PI/L/FUL1



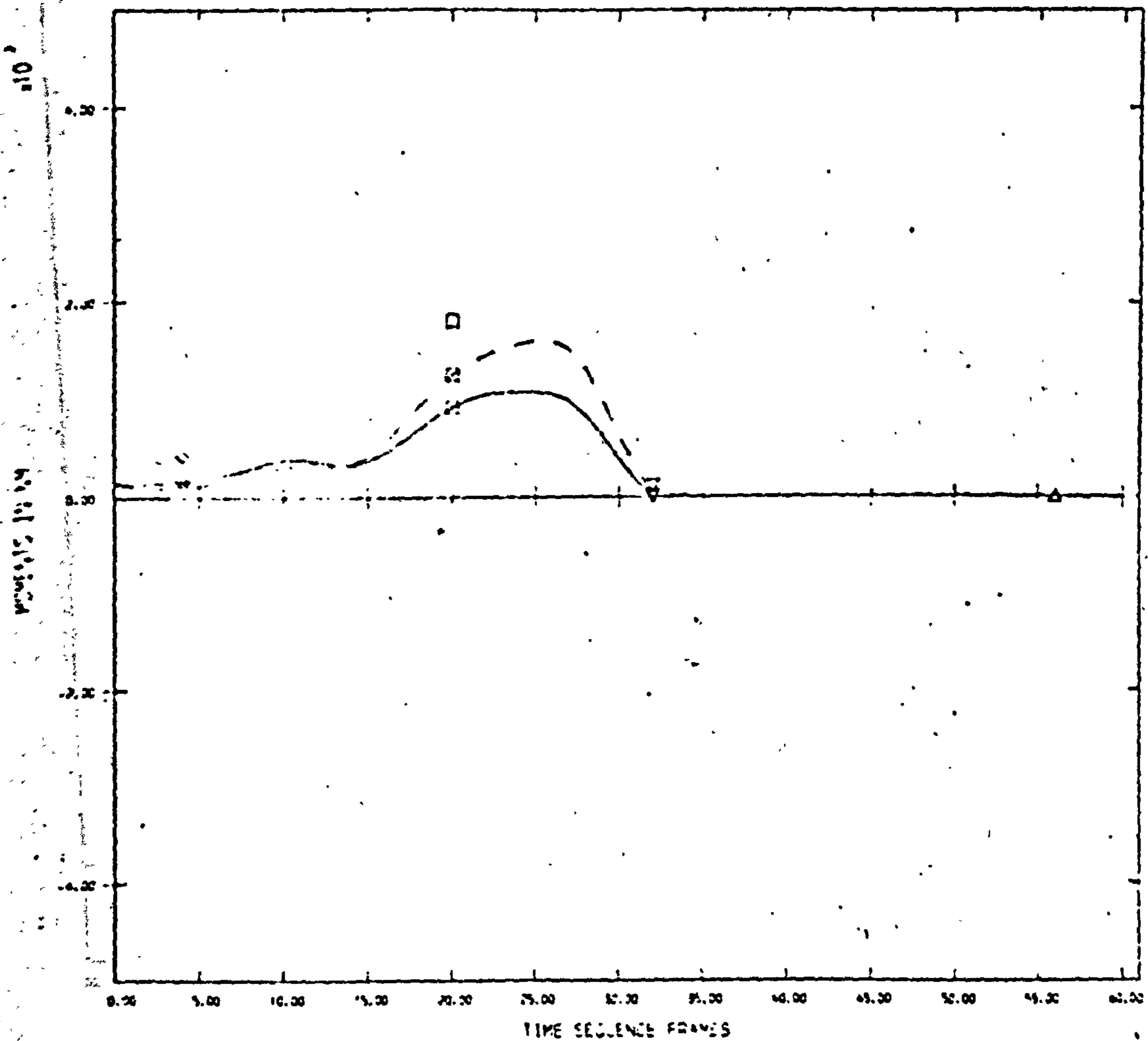
LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	○		

P2/L/FUL1



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEEL STRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

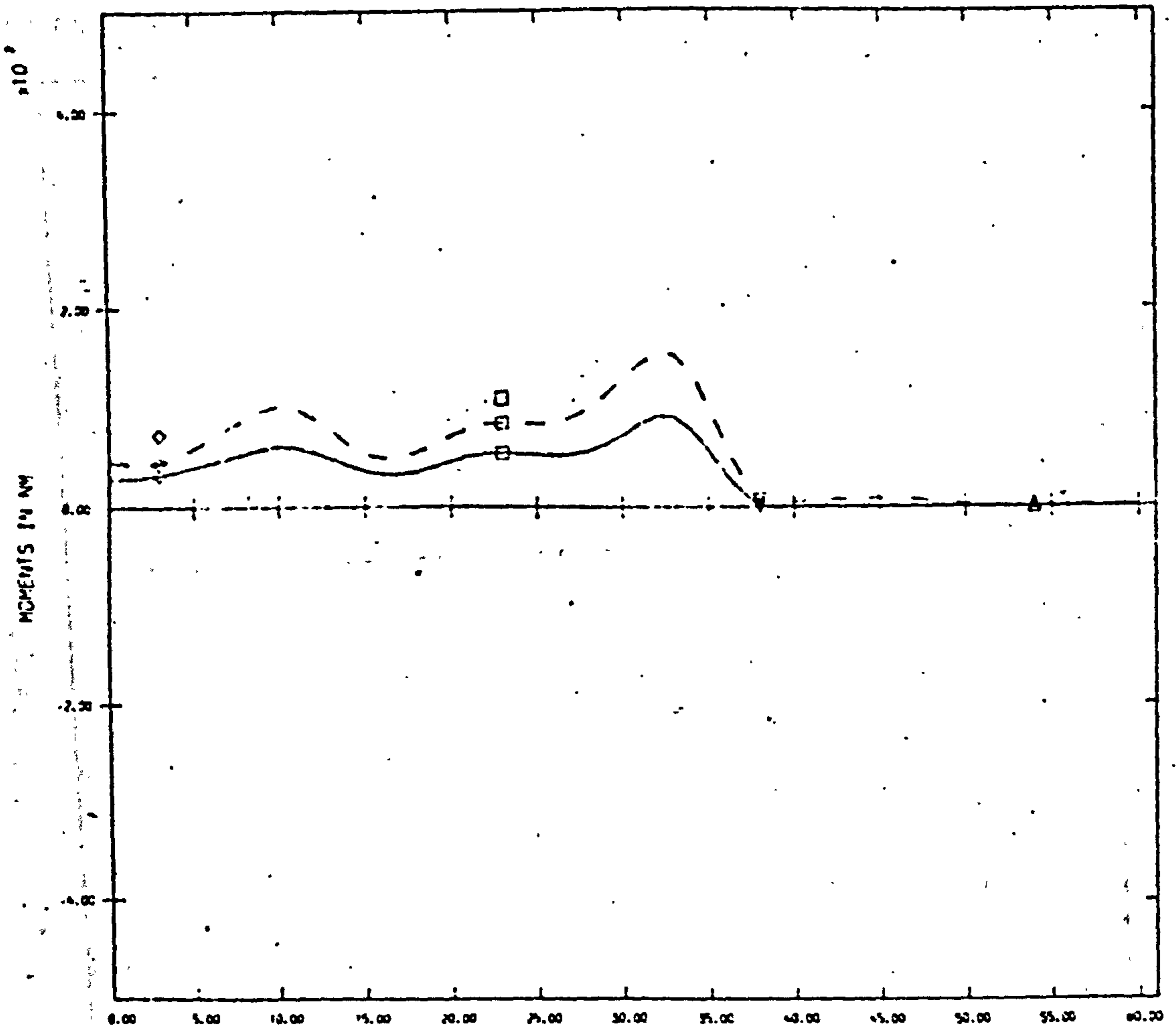
P3/L/FUL1



ANKLE, KNEE, HIP, SAGITTAL PLANE

- LEFT HEEL STRIKE ▲ CONTINUOUS ANKLE
- LEFT TOE OFF ▼ DASHED KNEE
- RIGHT HEELSTRIKE □ DOTTED HIP
- RIGHT TOE OFF ○

P4/L/FUL1



ANKLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE  $\Delta$

LEFT TOE OFF  $\nabla$

RIGHT HEELSTRIKE  $\square$

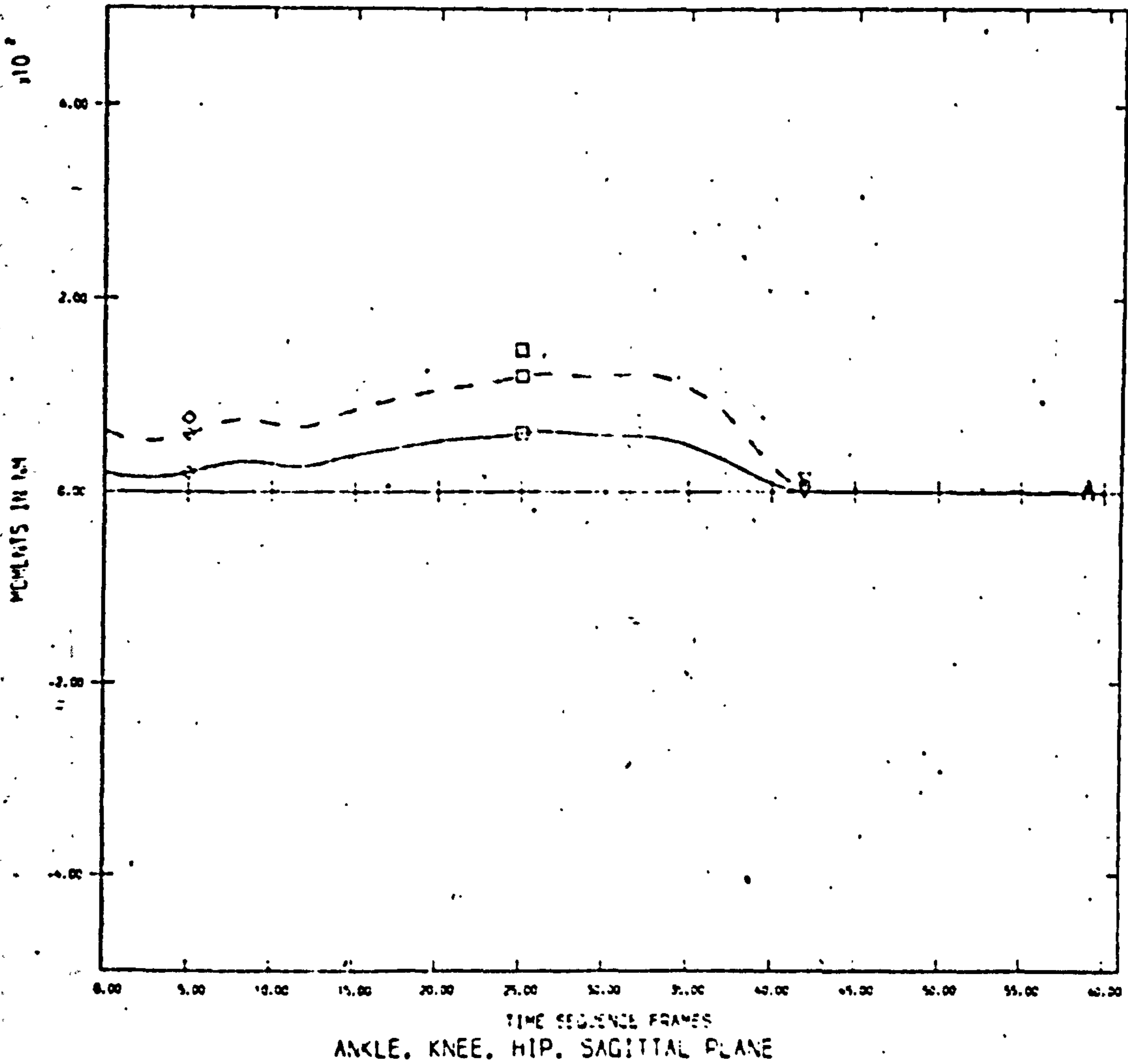
RIGHT TOE OFF  $\diamond$

CONTINUOUS ANKLE

DASHED KNEE

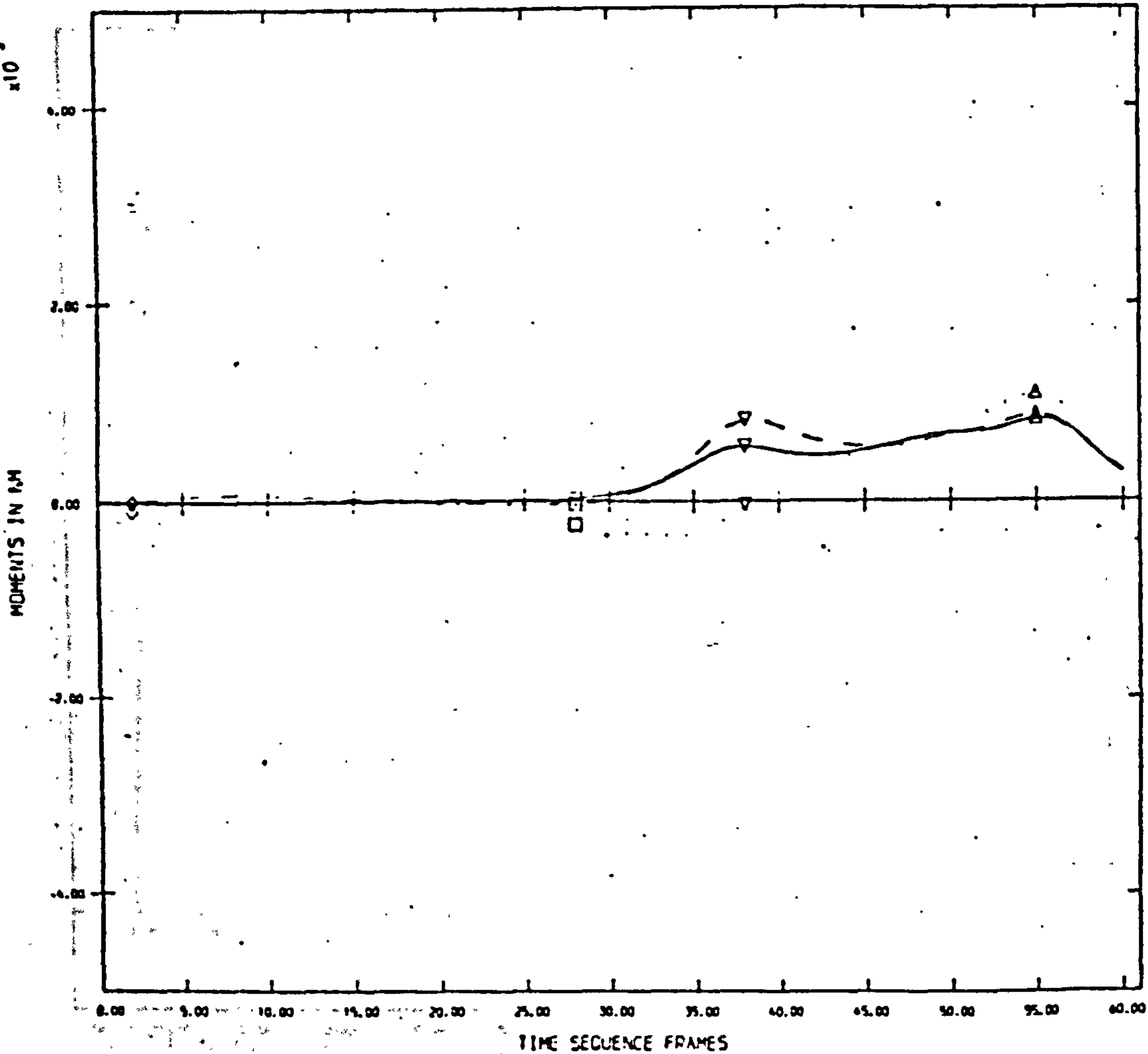
DOTTED HIP

P6/L/FUL1



LEFT HEEL STRIKE $\Delta$	CONTINUOUS	ANKLE
LEFT TOE OFF $\nabla$	DASHED	KNEE
RIGHT HEEL STRIKE $\square$	DOTTED	HIP
RIGHT TOE OFF $\diamond$		

P1/R/FUL1

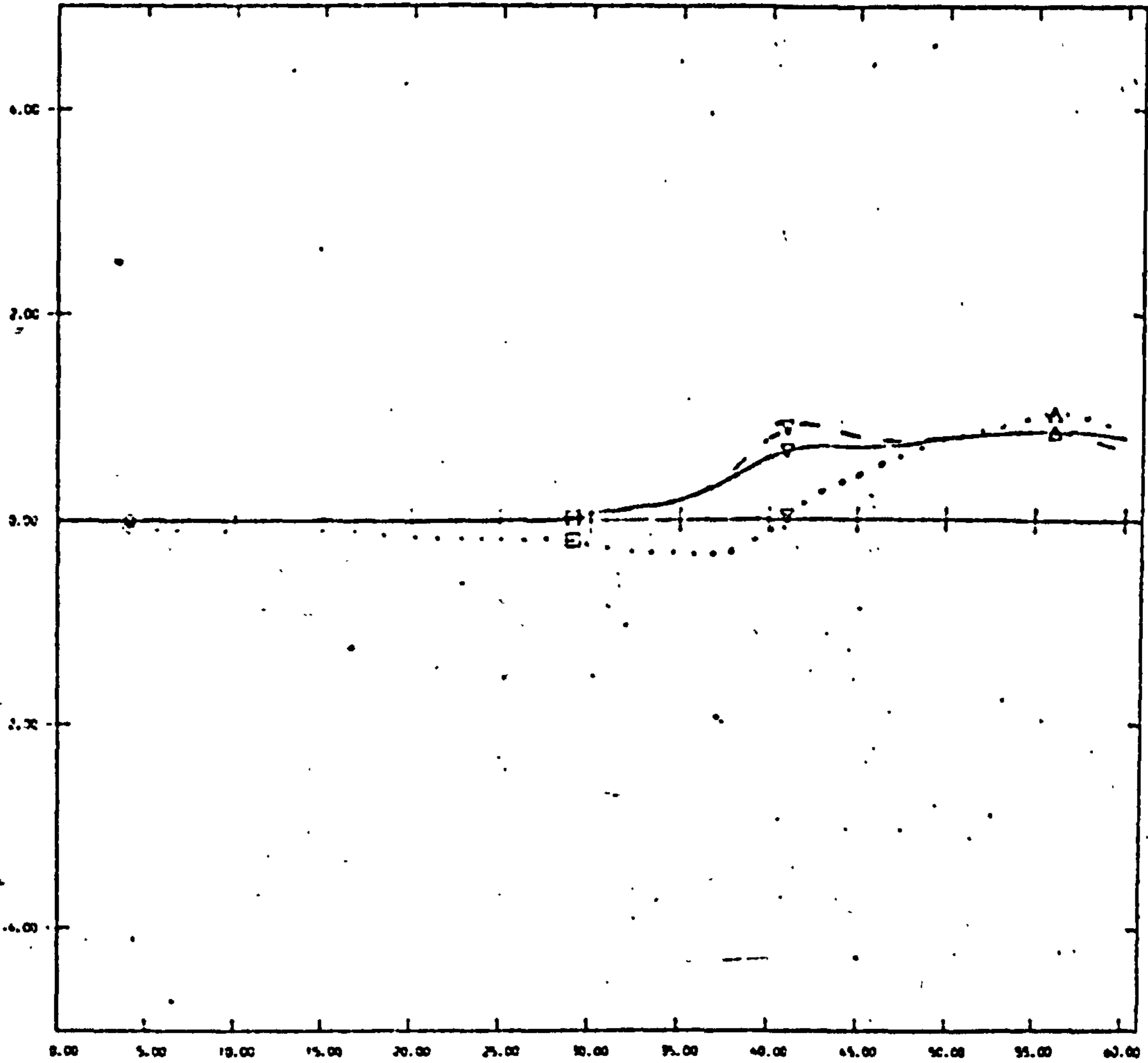


ANKLE, KNEE, HIP, SAGITTAL PLANE

- LEFT HEEL STRIKE ▲ CONTINUOUS ANKLE
- LEFT TOE OFF ▼ DASHED KNEE
- RIGHT HEEL STRIKE □ DOTTED HIP
- RIGHT TOE OFF ◇

P2/R/FUL1

MOMENTS IN NM

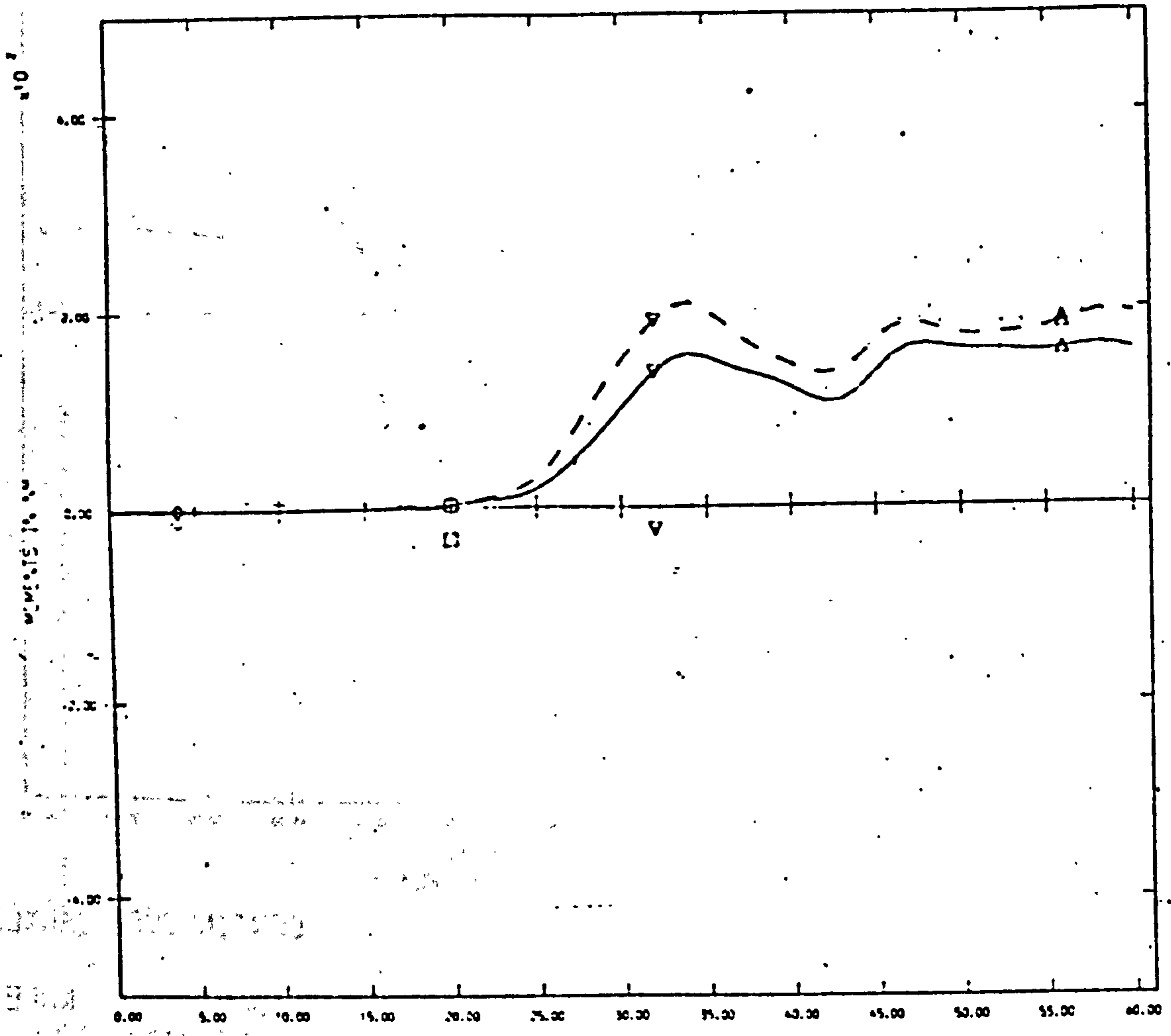


TIME SEQUENCE FRAMES  
ANKLE, KNEE, HIP, SAGITTAL PLANE

- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▼ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | □ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ◇ |            |       |



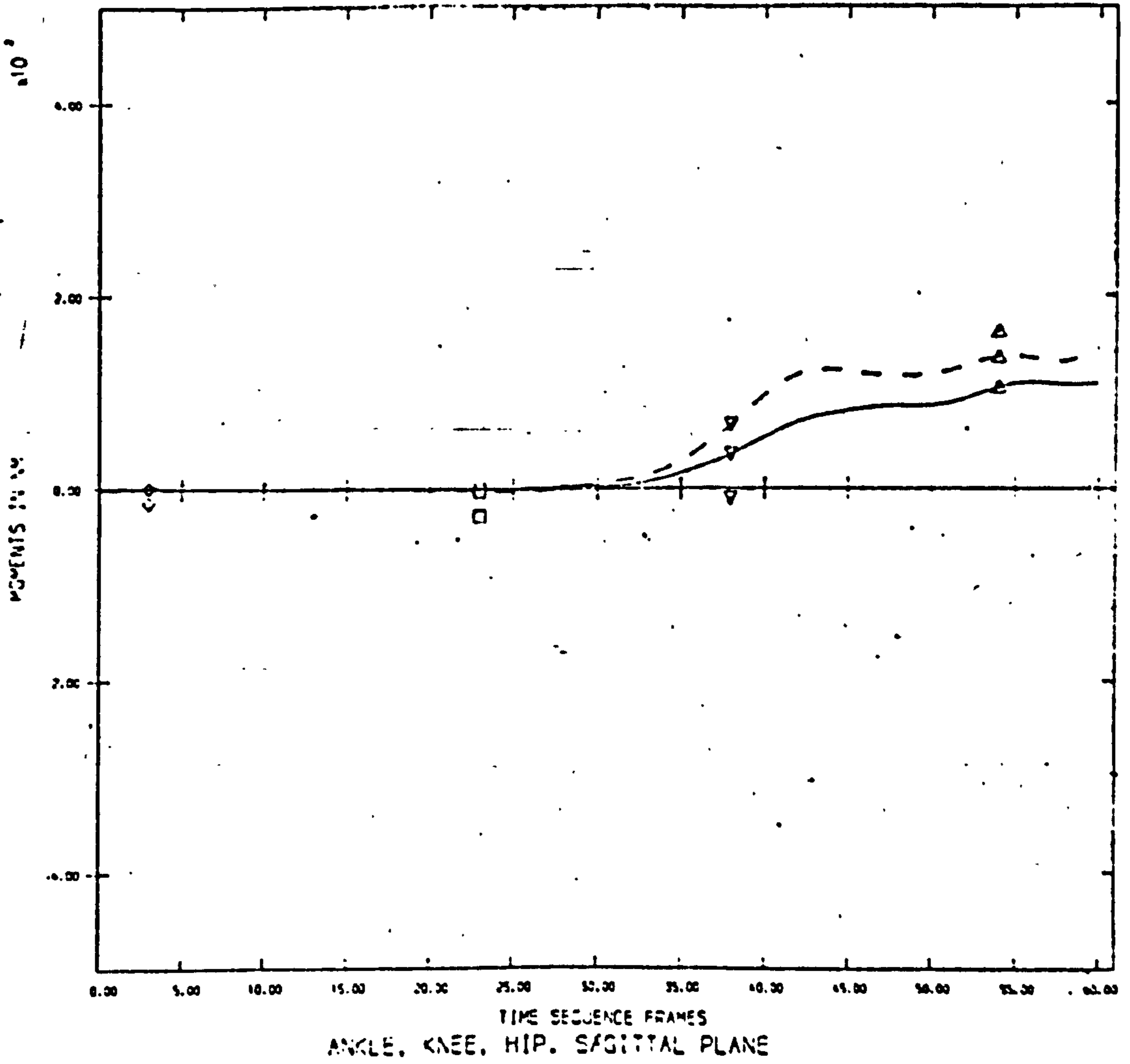
P3/R/FUL1



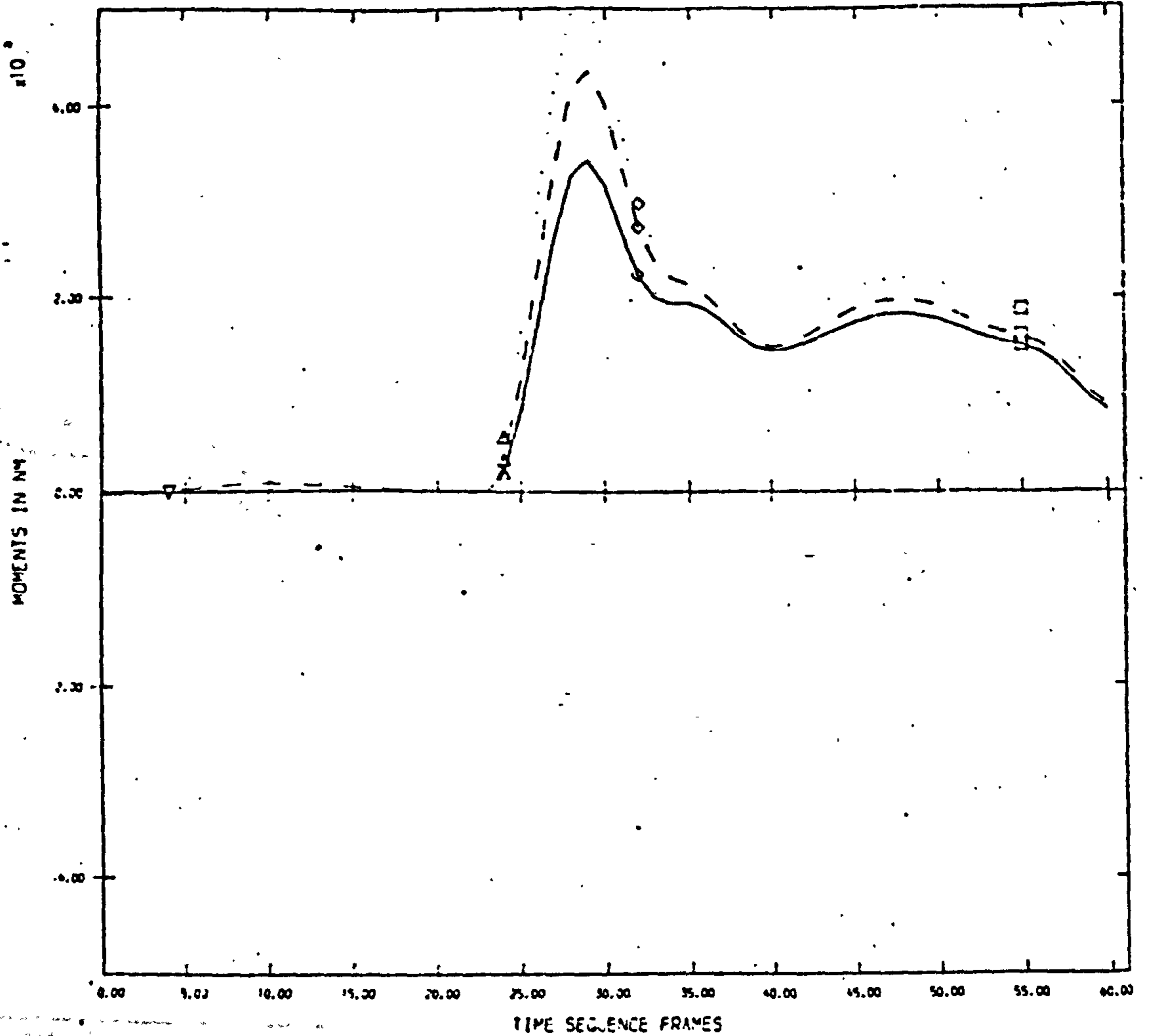
ANKLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE $\Delta$	CONTINUOUS	ANKLE
LEFT TOE OFF $\nabla$	DASHED	KNEE
RIGHT HEELSTRIKE $\square$	DOTTED	HIP
RIGHT TOE OFF $\diamond$		

P4/R/FUL1



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	◇		



ANKLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

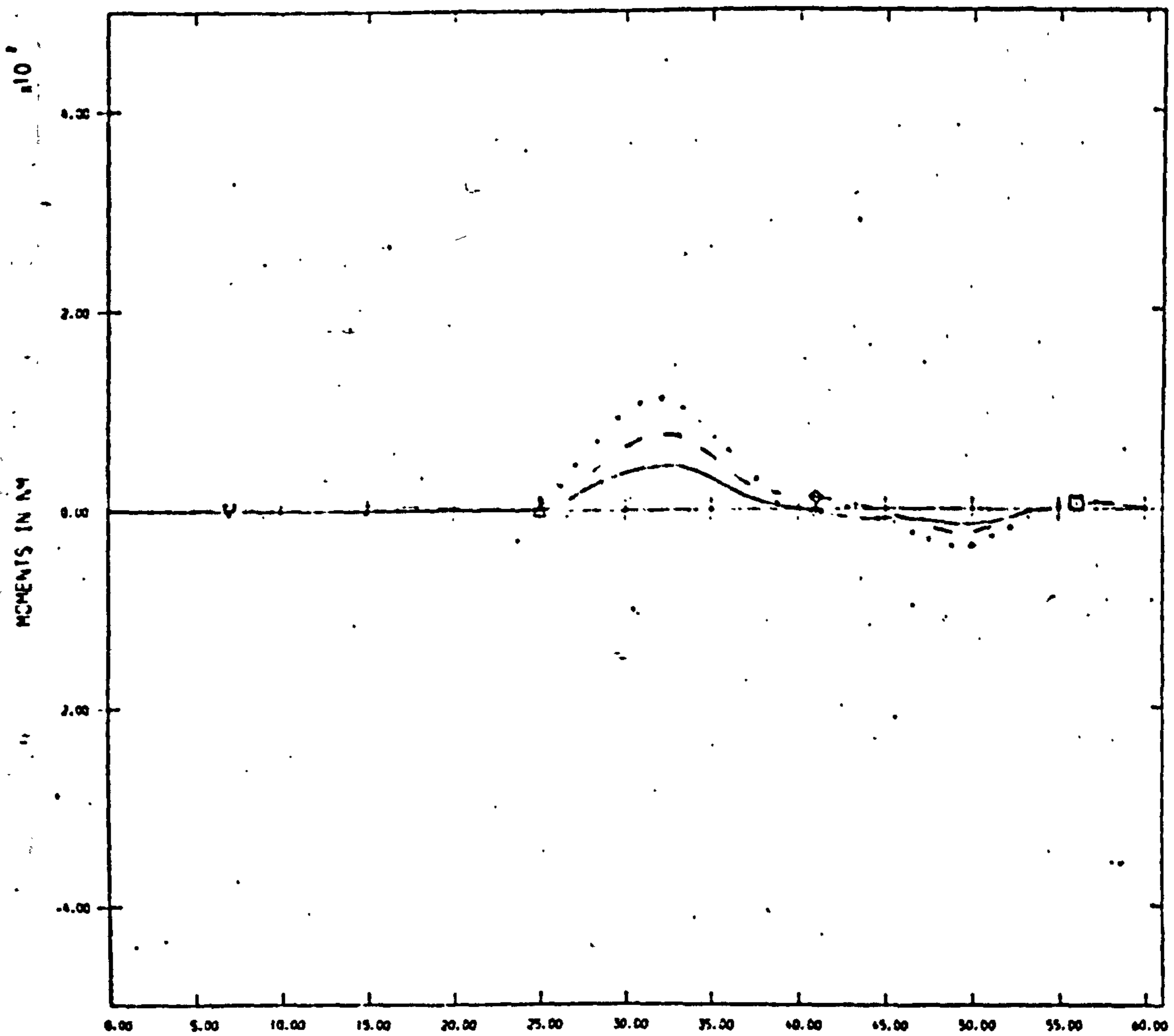
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\circ$

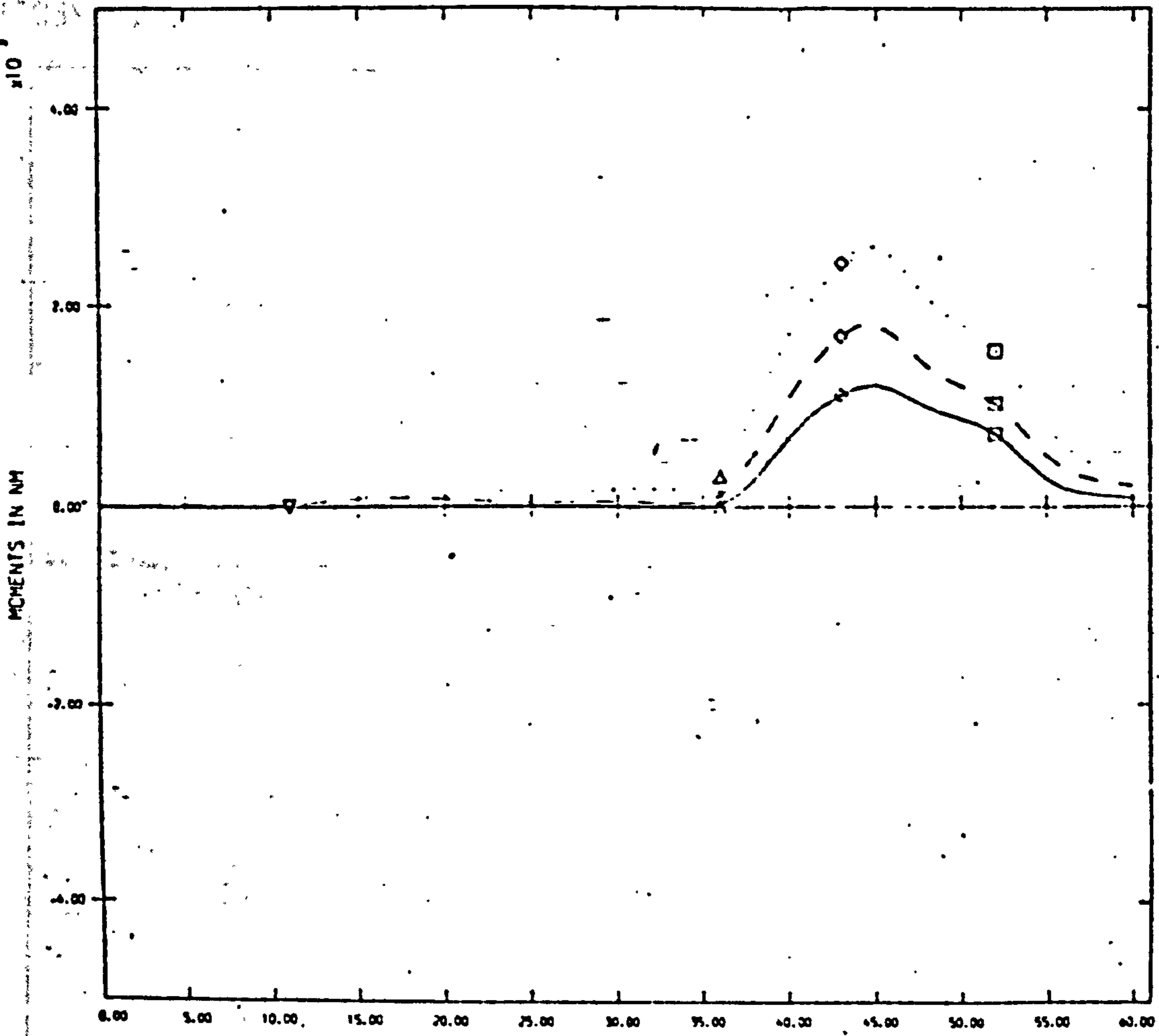
P2/L/BDT1



ANKLE, KNEE, HIP, SAGITTAL PLANE

- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | △ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▽ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | □ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ◇ |            |       |

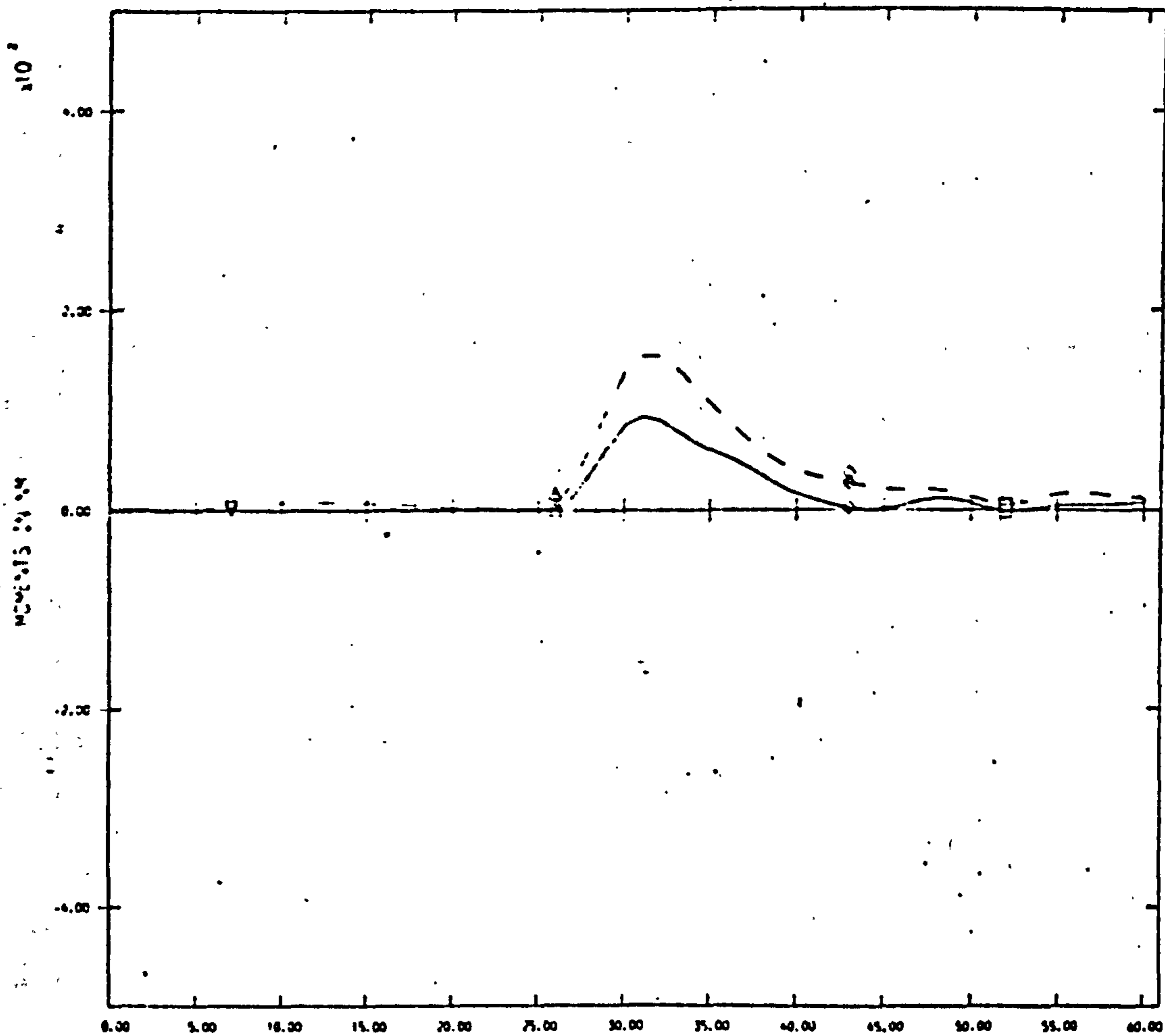
P3/L/BOT1



ANKLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE $\Delta$	CONTINUOUS	ANKLE
LEFT TOE OFF $\nabla$	DASHED	KNEE
RIGHT HEELSTRIKE $\square$	DOTTED	HIP
RIGHT TOE OFF $\diamond$		

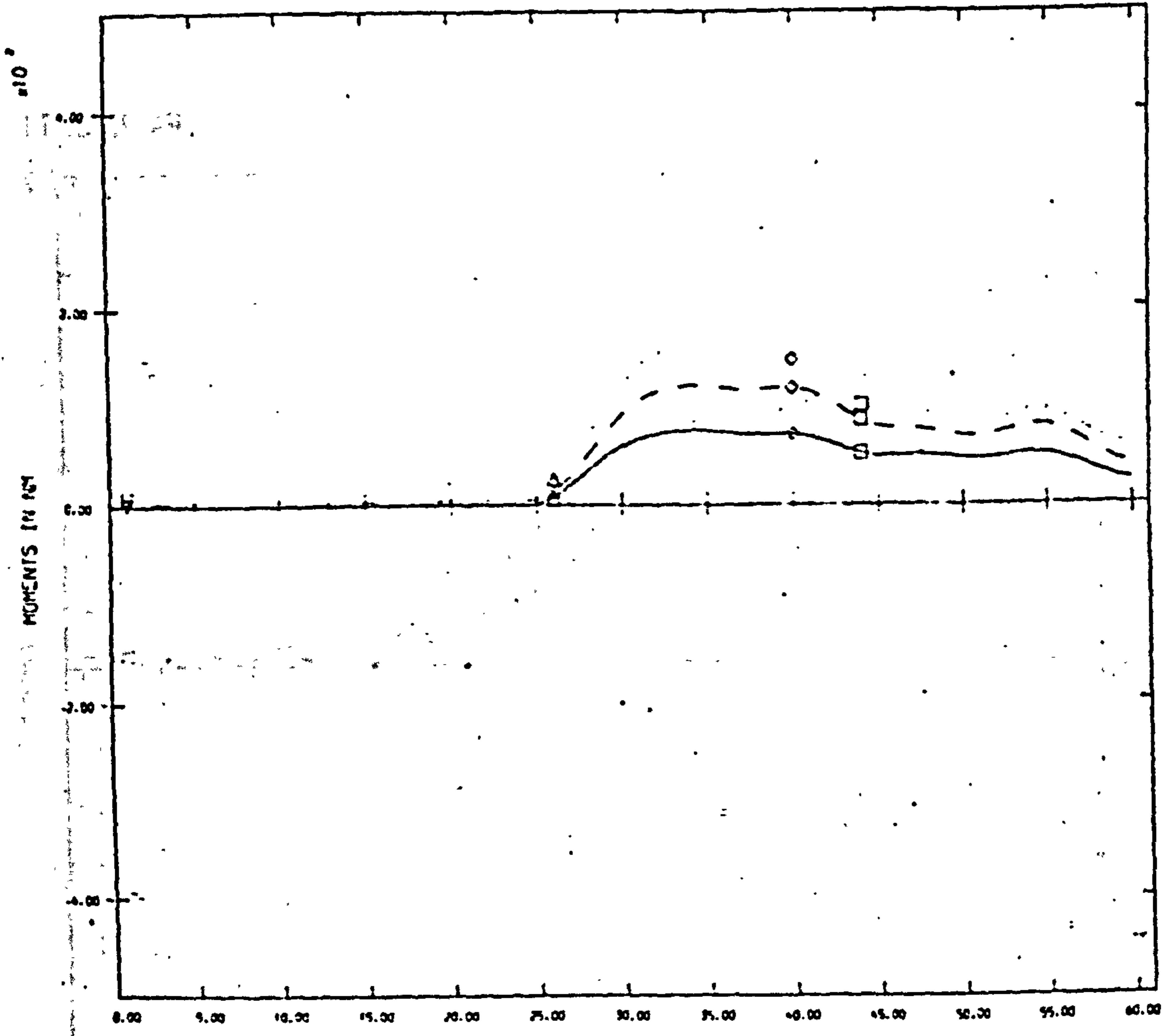
P4/L/BOT1



ANKLE, KNEE, HIP, SAGITTAL PLANE

- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▼ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | □ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ◇ |            |       |

P6/L/BOT1

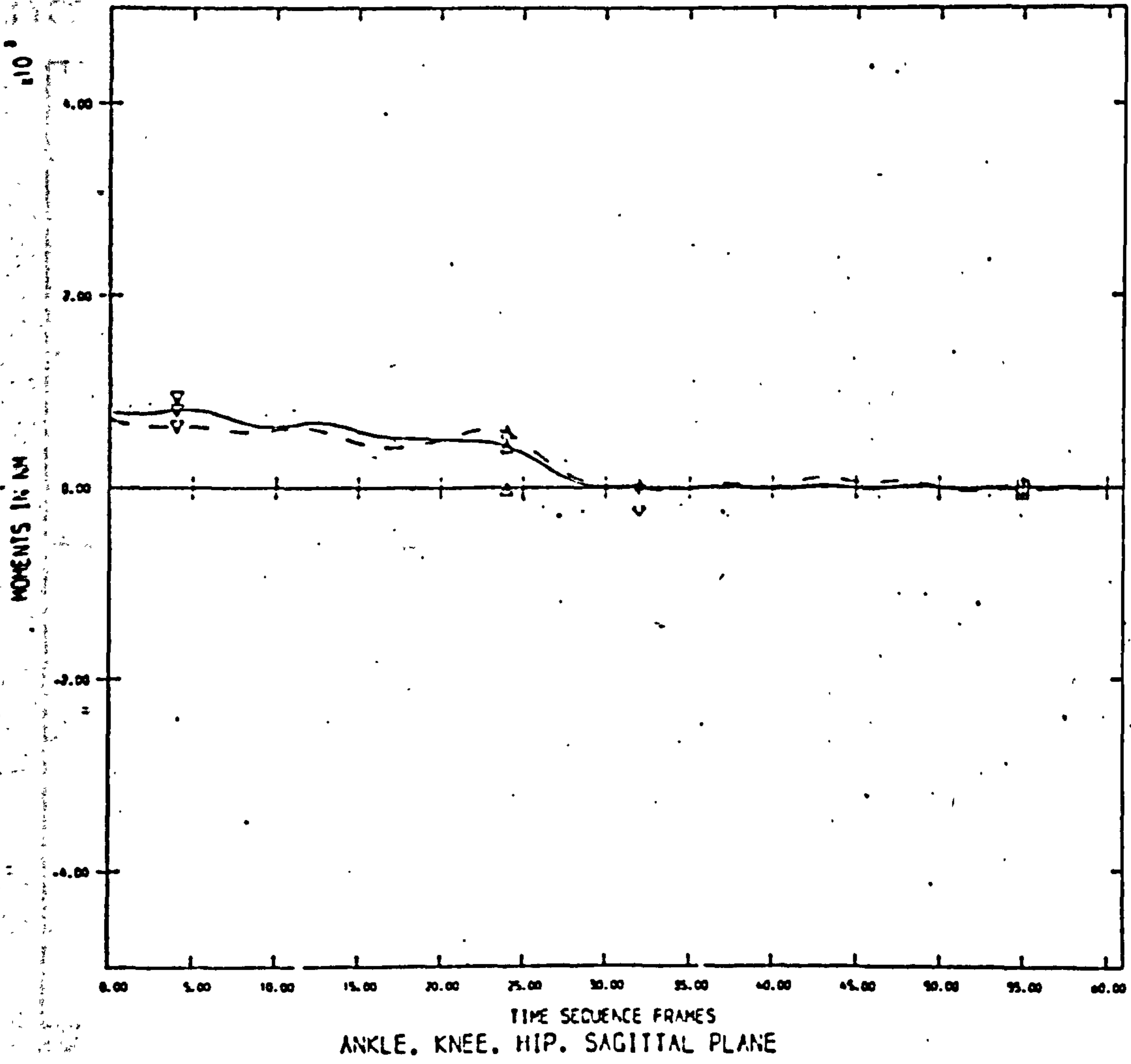


ANKLE, KNEE, HIP, SAGITTAL PLANE

- |                   |   |            |       |
|-------------------|---|------------|-------|
| LEFT HEEL STRIKE  | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF      | ▼ | DASHED     | KNEE  |
| RIGHT HEEL STRIKE | □ | DOTTED     | HIP   |
| RIGHT TOE OFF     | ○ |            |       |

911 00100

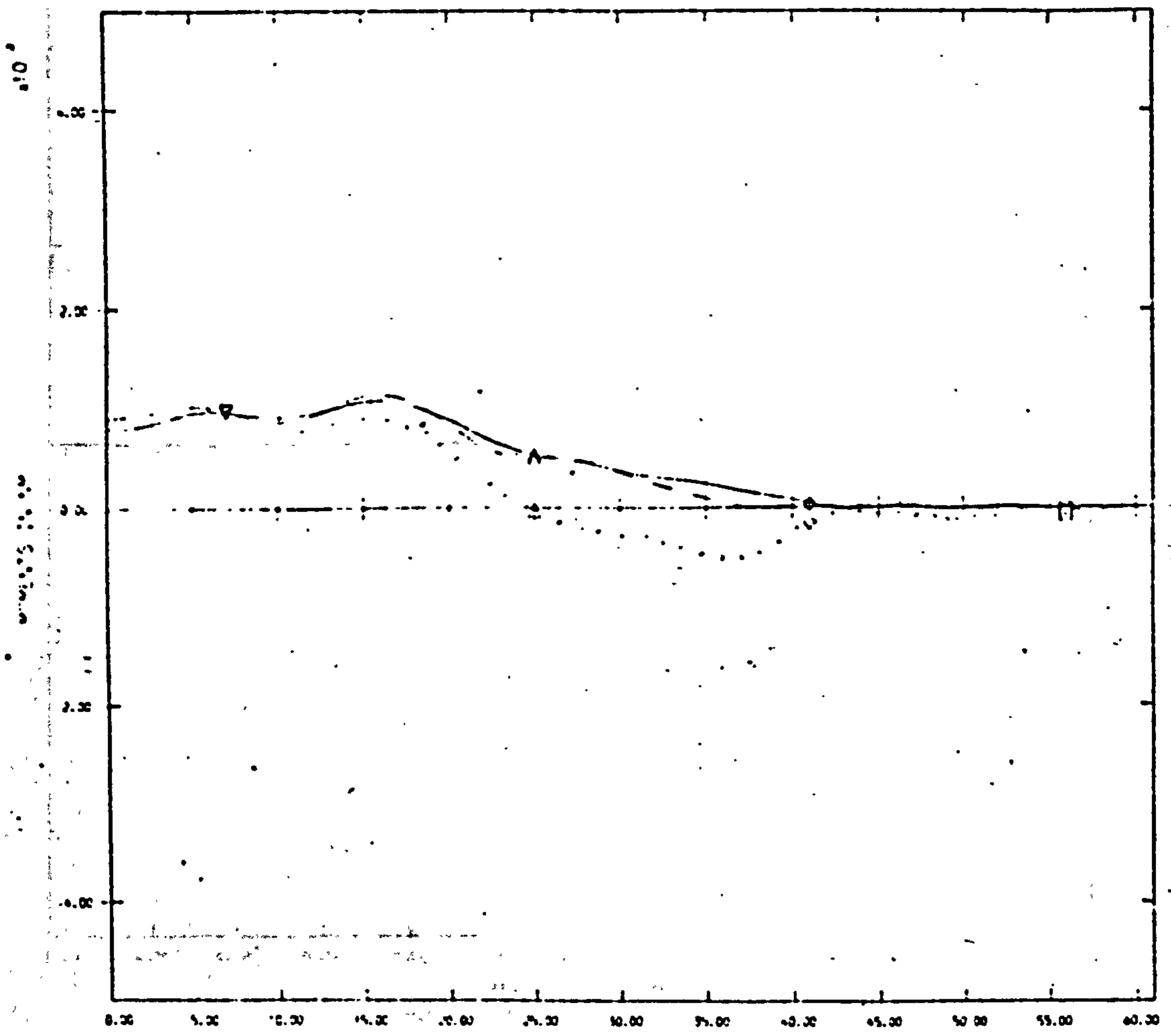
P1/R/BOT1



LEFT HEEL STRIKE	△	CONTINUOUS	ANKLE
LEFT TOE OFF	▽	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	◇		



P2/R/BDT1



ANGLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE ▲

CONTINUOUS ANKLE

LEFT TOE OFF ▼

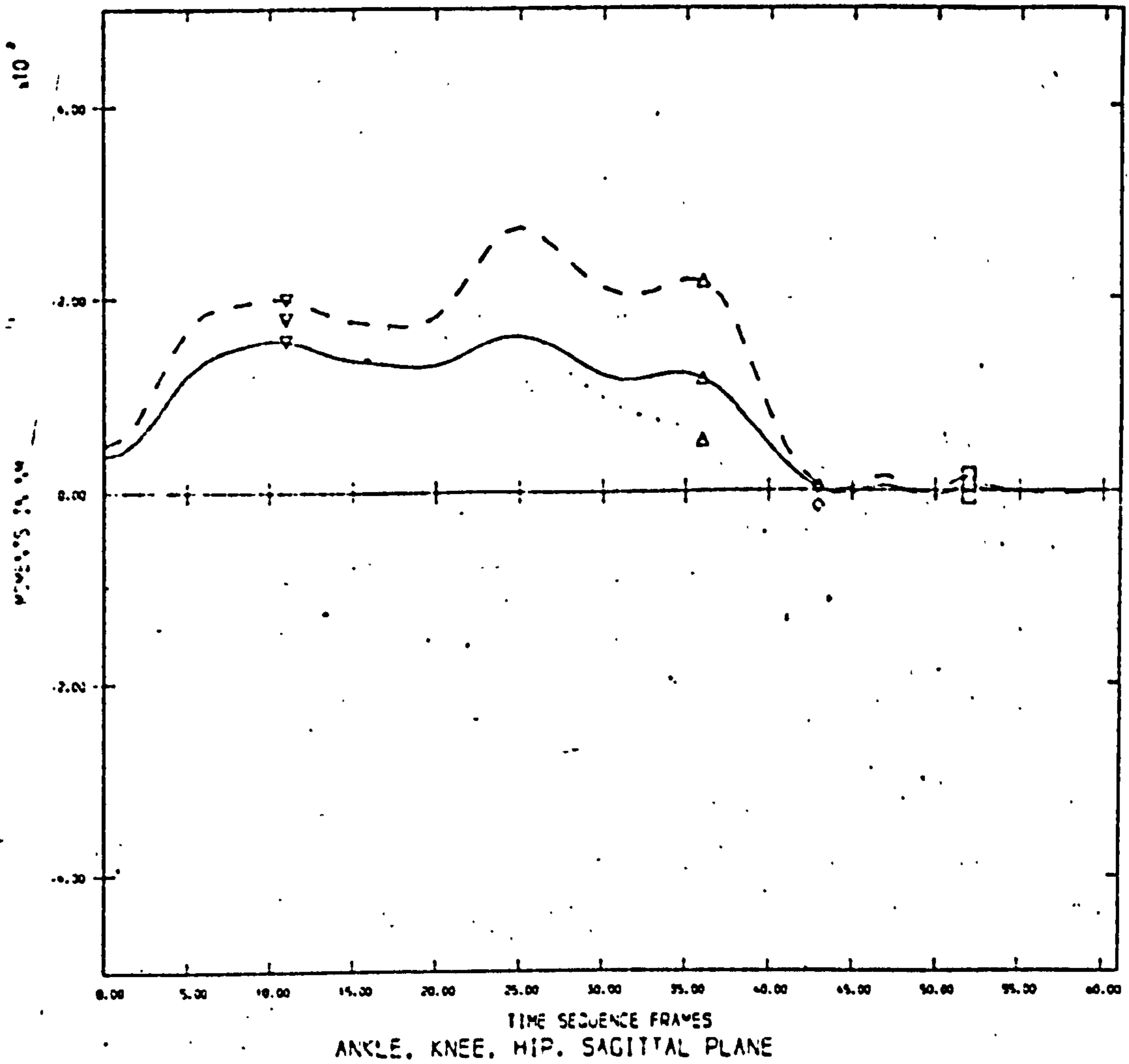
DASHED KNEE

RIGHT HEEL STRIKE ◻

DOTTED HIP

RIGHT TOE OFF ◊

P3/R/BOT1



LEFT HEEL STRIKE ▲

CONTINUOUS ANKLE

LEFT TOE OFF ▼

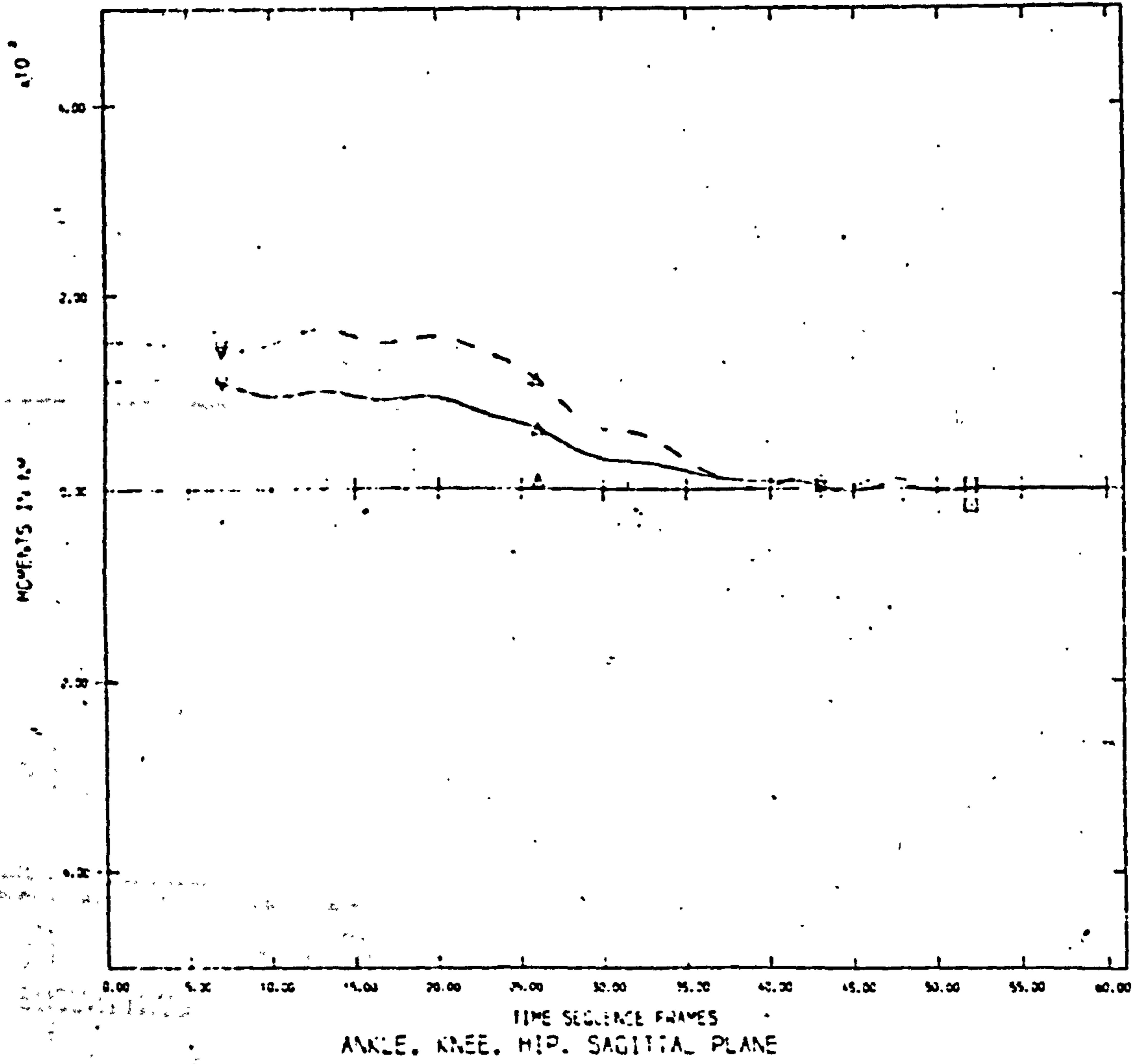
DASHED KNEE

RIGHT HEELSTRIKE ◻

DOTTED HIP

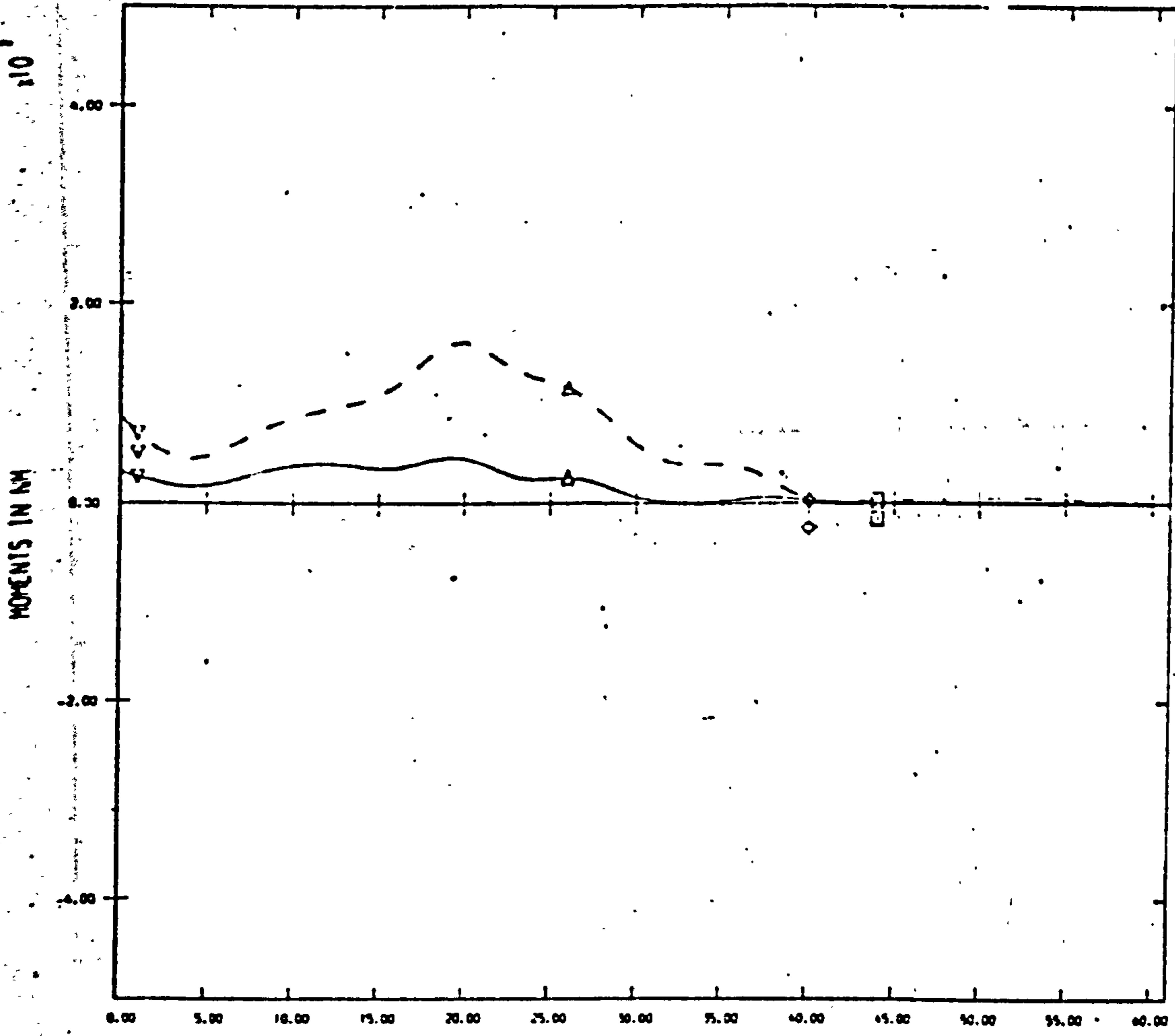
RIGHT TOE OFF ◊

P4/R/BDT1



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEEL STRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

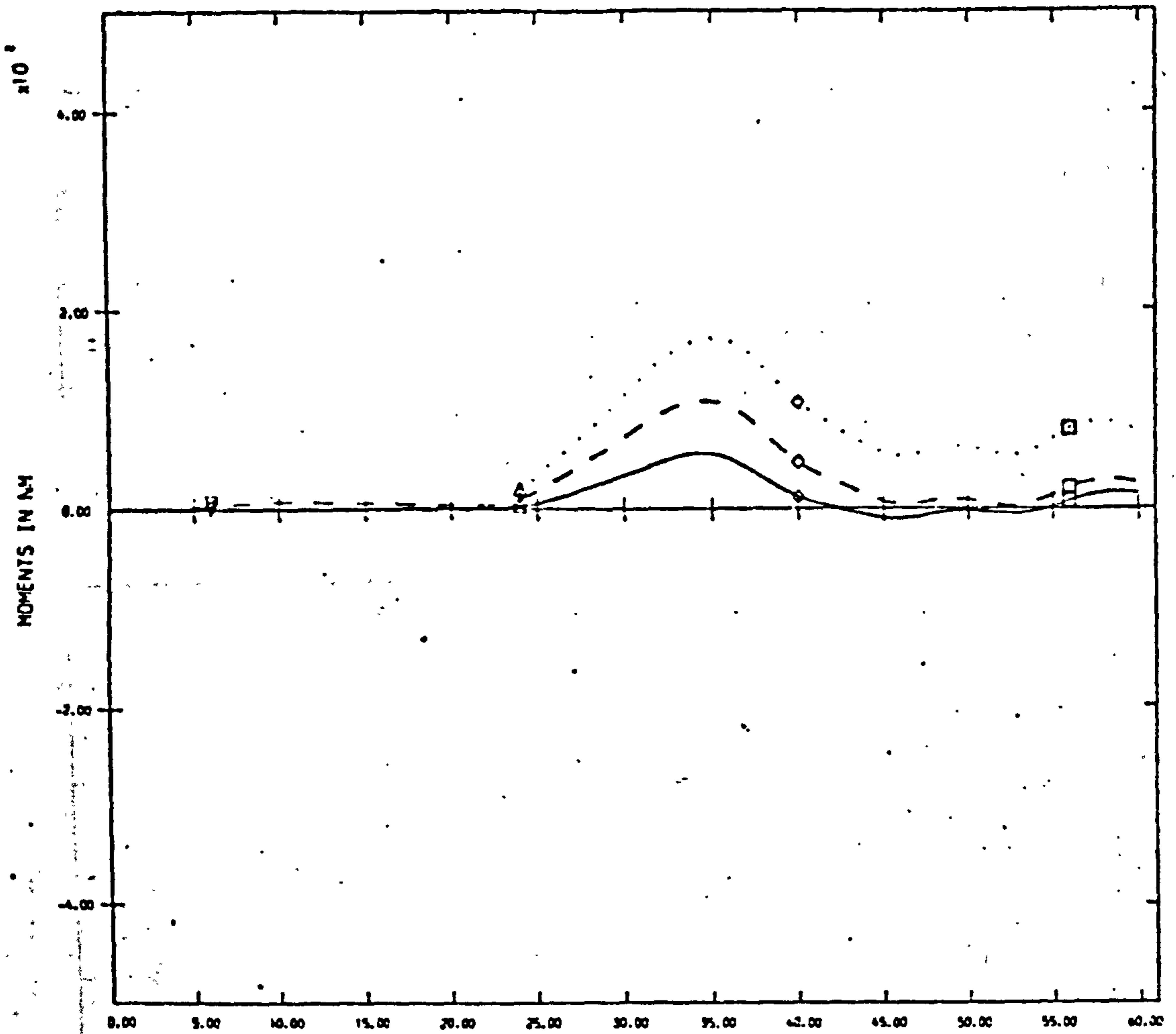
P6/R/BDT1



TIME SEQUENCE FRAMES  
ANKLE, KNEE, HIP, SAGITTAL PLANE

- |                    |            |       |
|--------------------|------------|-------|
| LEFT HEEL STRIKE ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF ▼     | DASHED     | KNEE  |
| RIGHT HEELSTRIKE □ | DOTTED     | HIP   |
| RIGHT TOE OFF ◆    |            |       |

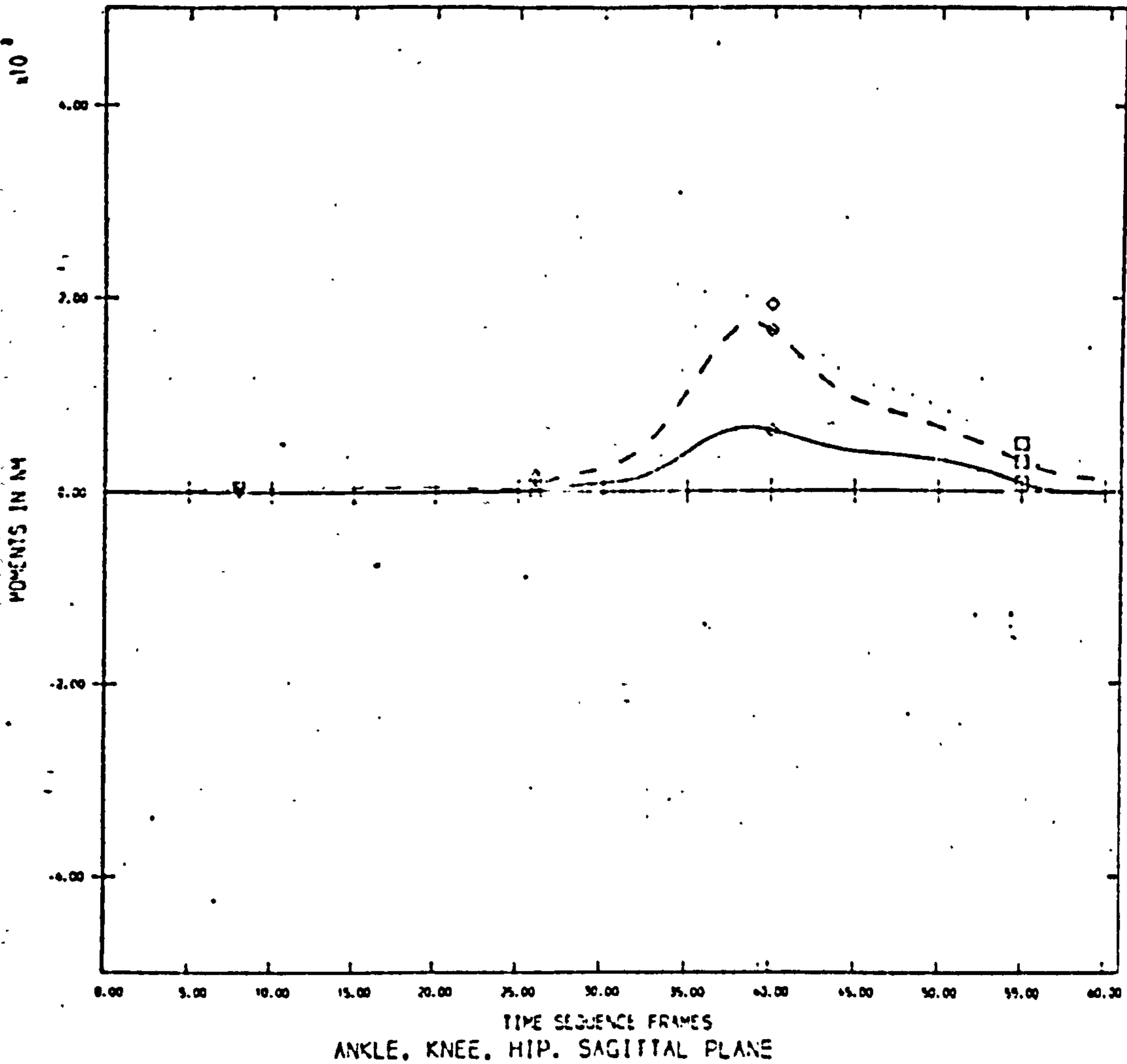
S1/L/BD10



ANKLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE ▲	CONTINUOUS	ANKLE
LEFT TOE OFF ▼	DASHED	KNEE
RIGHT HEELSTRIKE □	DOTTED	HIP
RIGHT TOE OFF ○		

S2/L/B0T0



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

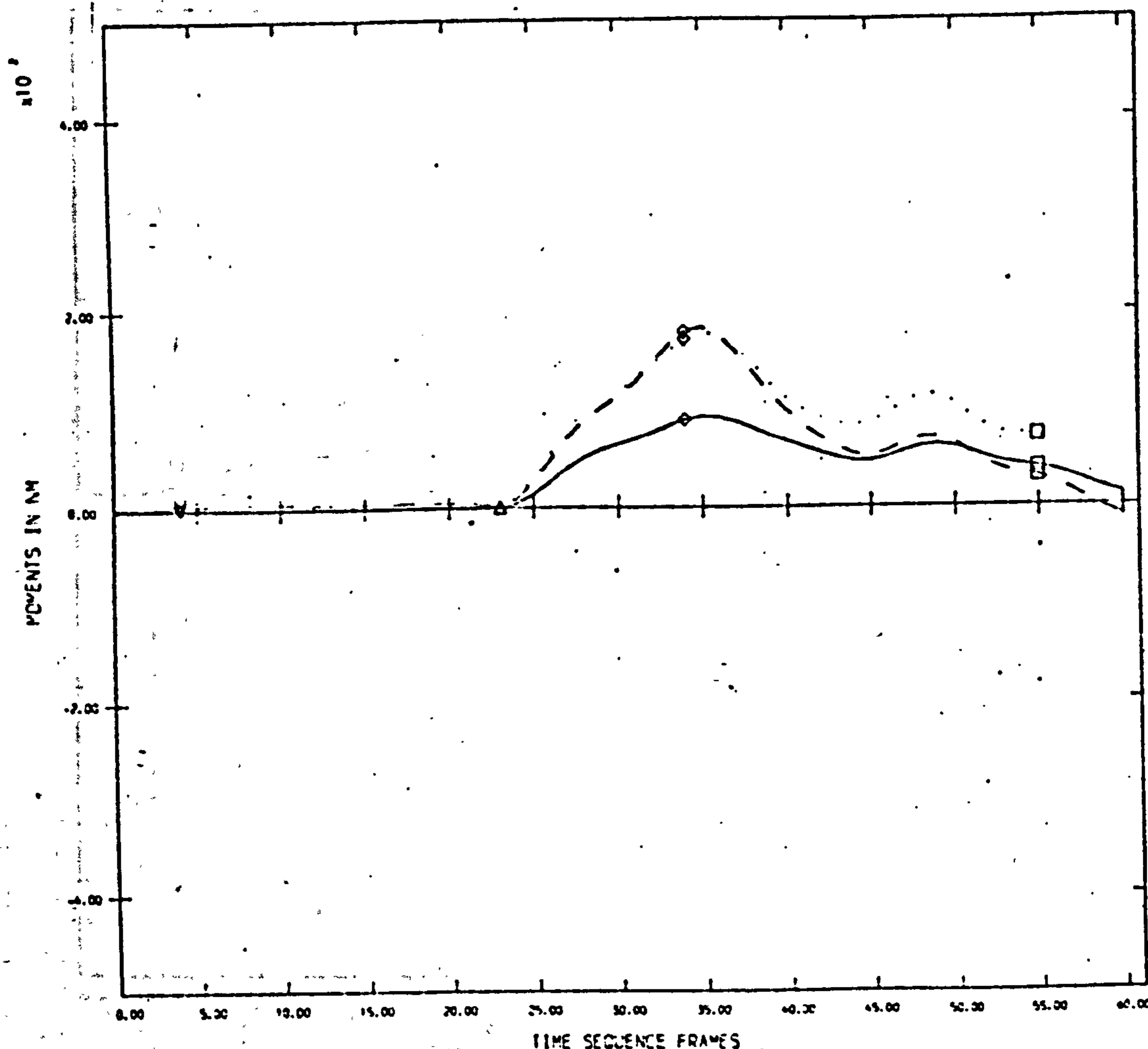
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

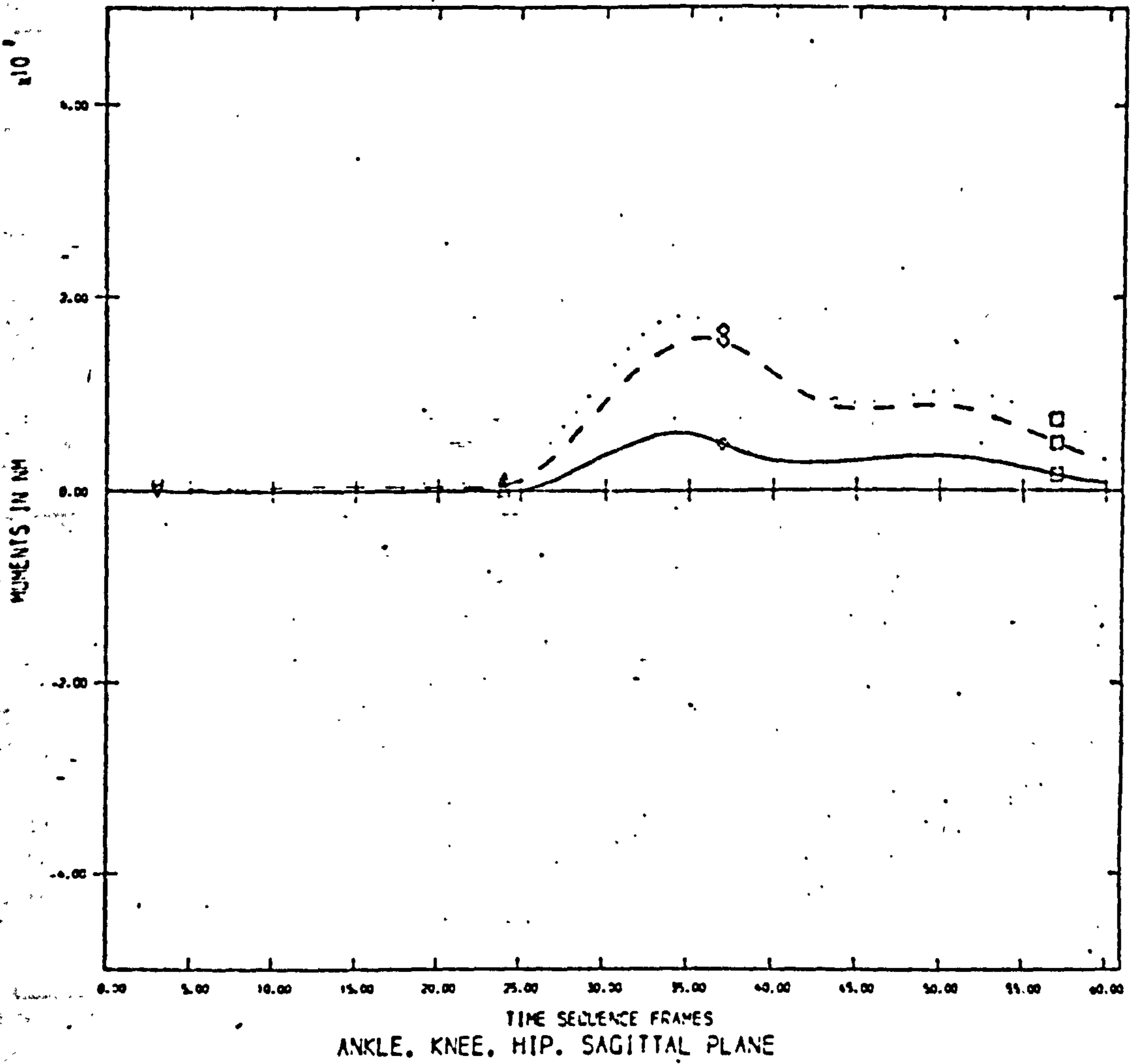
RIGHT TOE OFF  $\diamond$

S5/L/BOTO



LEFT HEEL STRIKE $\Delta$	CONTINUOUS	ANKLE*
LEFT TOE OFF $\nabla$	DASHED	KNEE
RIGHT HEELSTRIKE $\square$	DOTTED	HIP
RIGHT TOE OFF $\diamond$		

S3/L/BOTO



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

DASHED KNEE

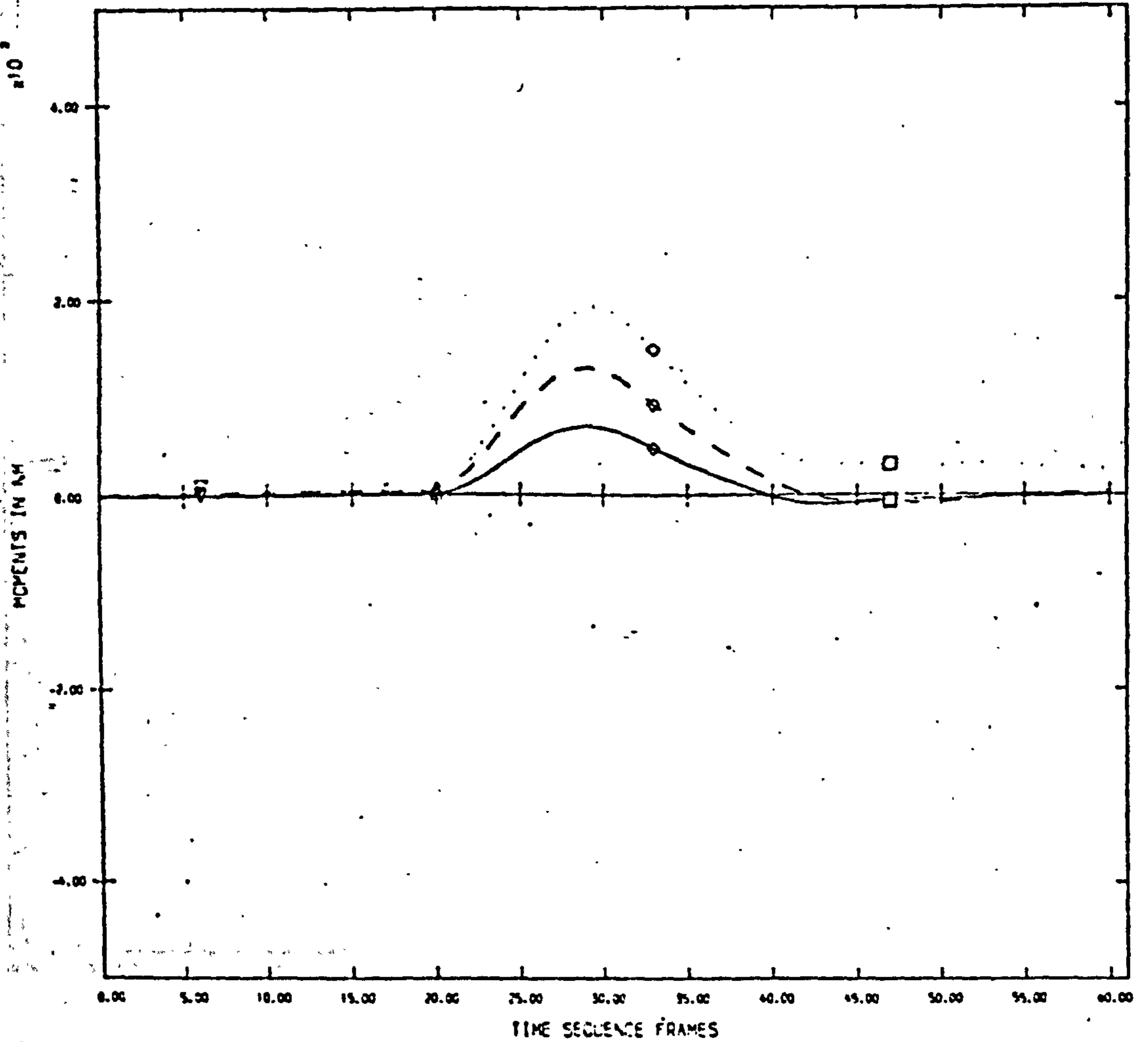
RIGHT HEELSTRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\circ$



S4/L/8070



LEFT HEEL STRIKE ▲

CONTINUOUS ANKLE

LEFT TOE OFF ▼

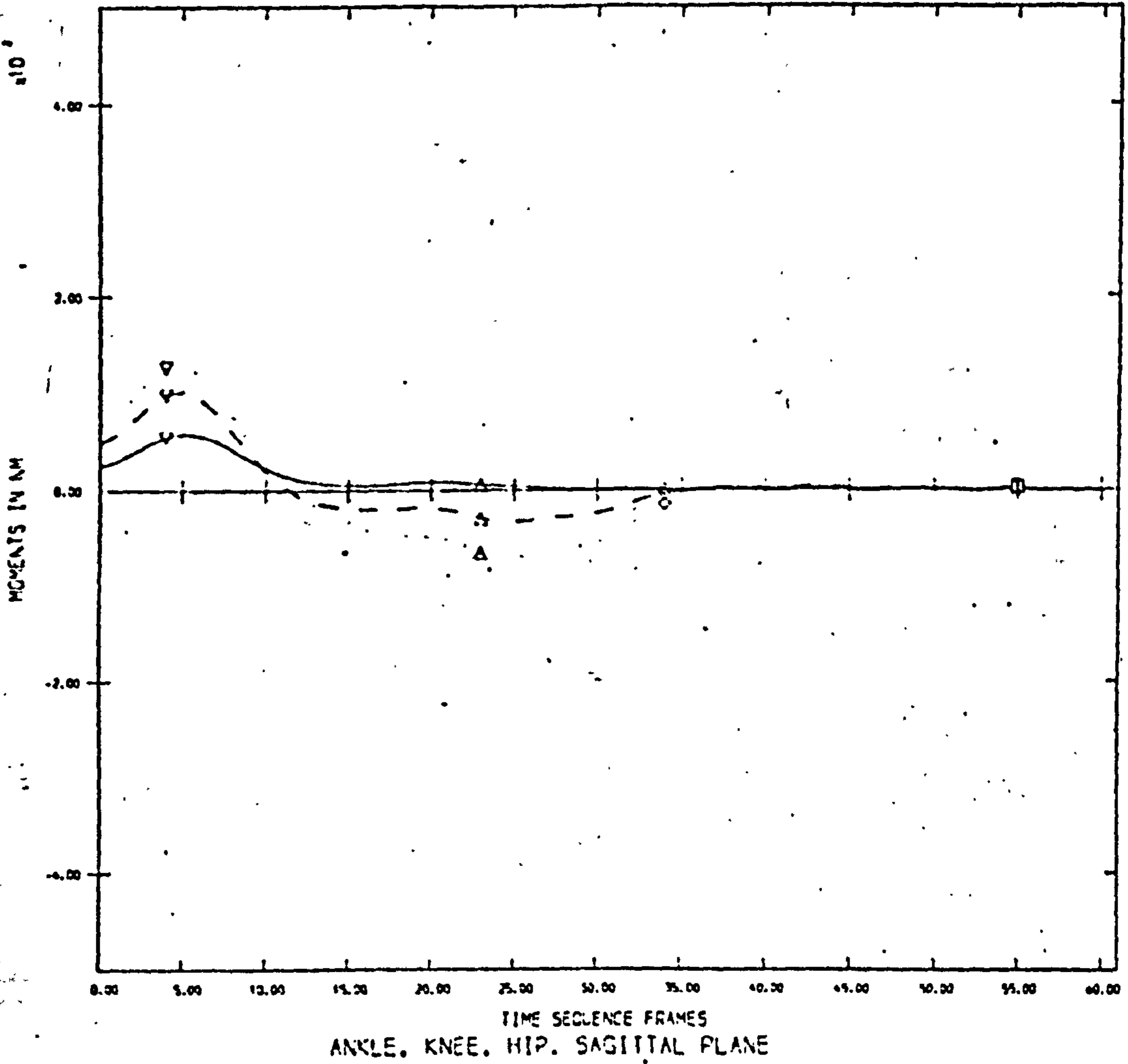
DASHED KNEE

RIGHT HEELSTRIKE ◻

DOTTED HIP

RIGHT TOE OFF ◊

S5/R/B0T0



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

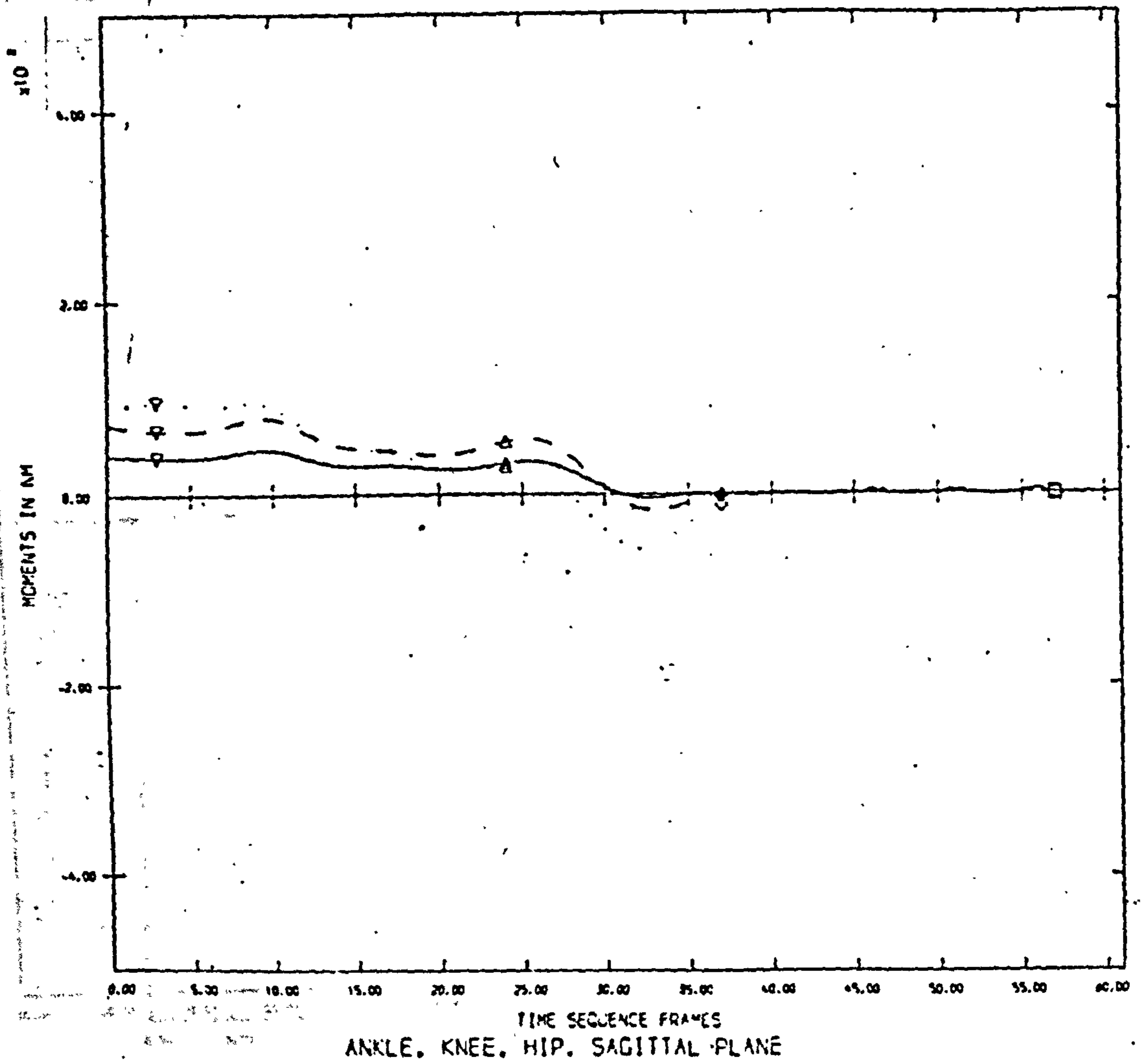
DASHED KNEE

RIGHT HEEL STRIKE  $\square$

DOTTED HIP

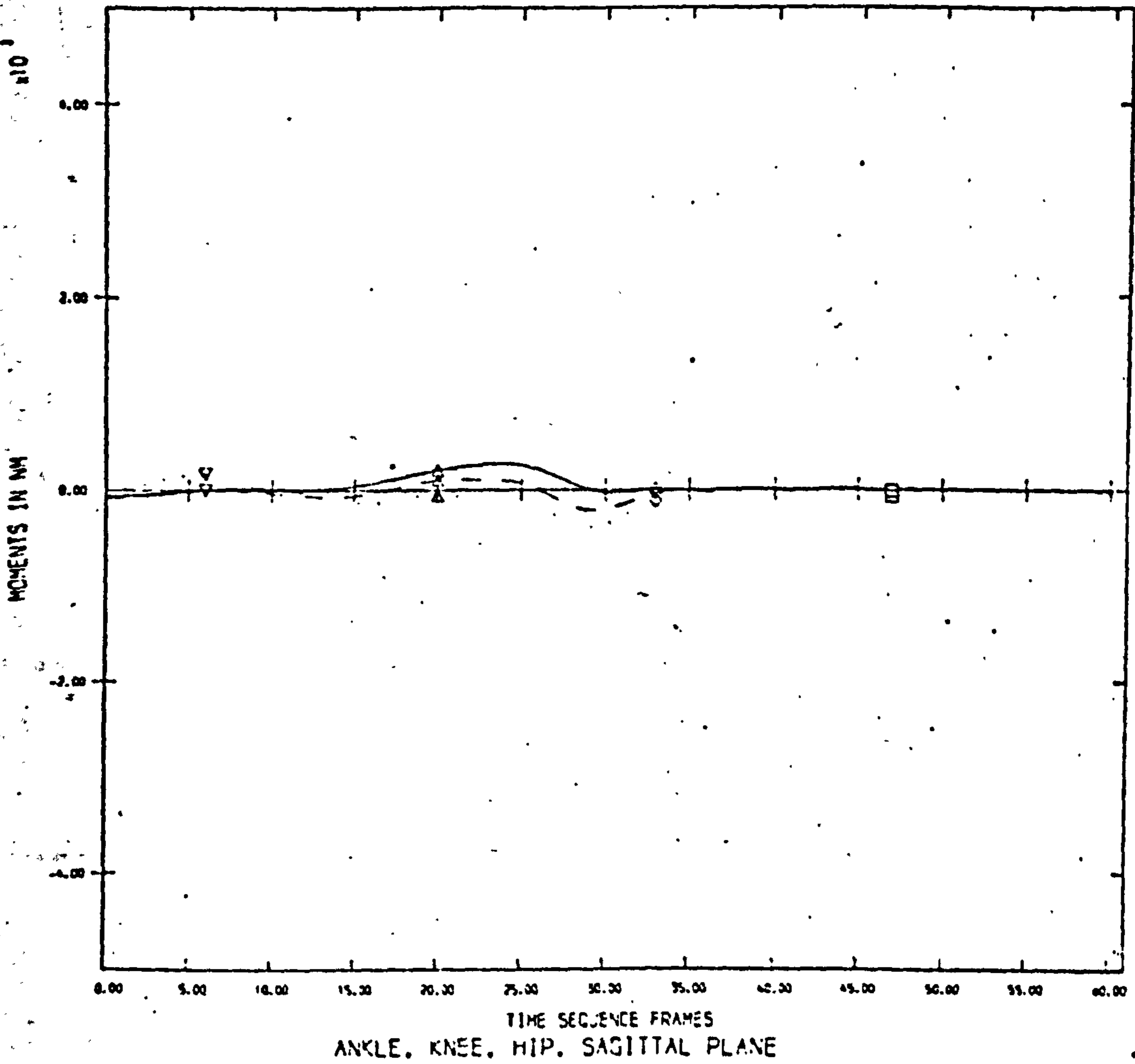
RIGHT TOE OFF  $\diamond$

S3/R/B010



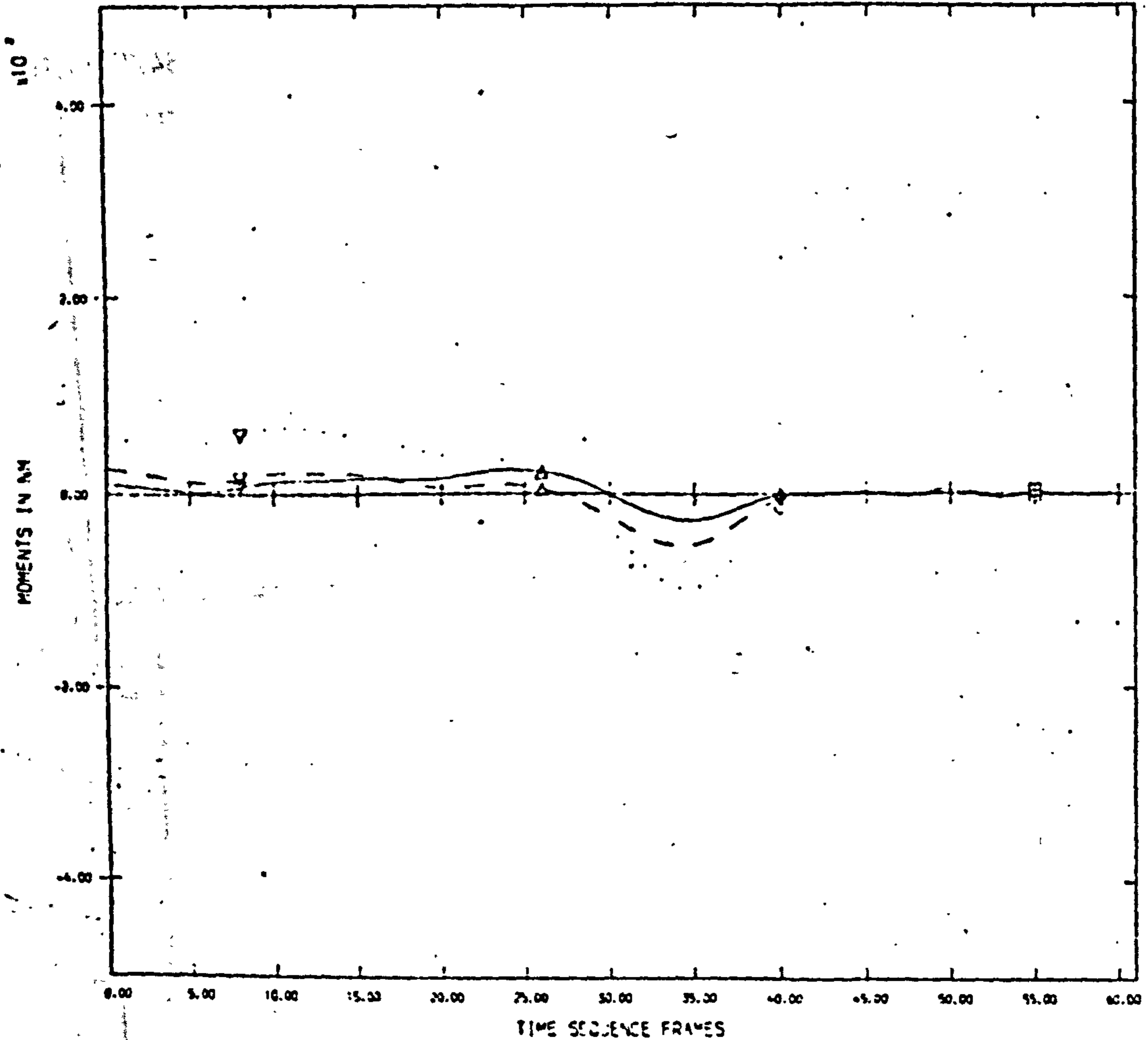
LEFT HEEL STRIKE ▲	CONTINUOUS	ANKLE
LEFT TOE OFF ▼	DASHED	KNEE
RIGHT HEELSTRIKE □	DOTTED	HIP
RIGHT TOE OFF ○		

S4/R/BDT0



- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▼ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | ◻ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ◊ |            |       |

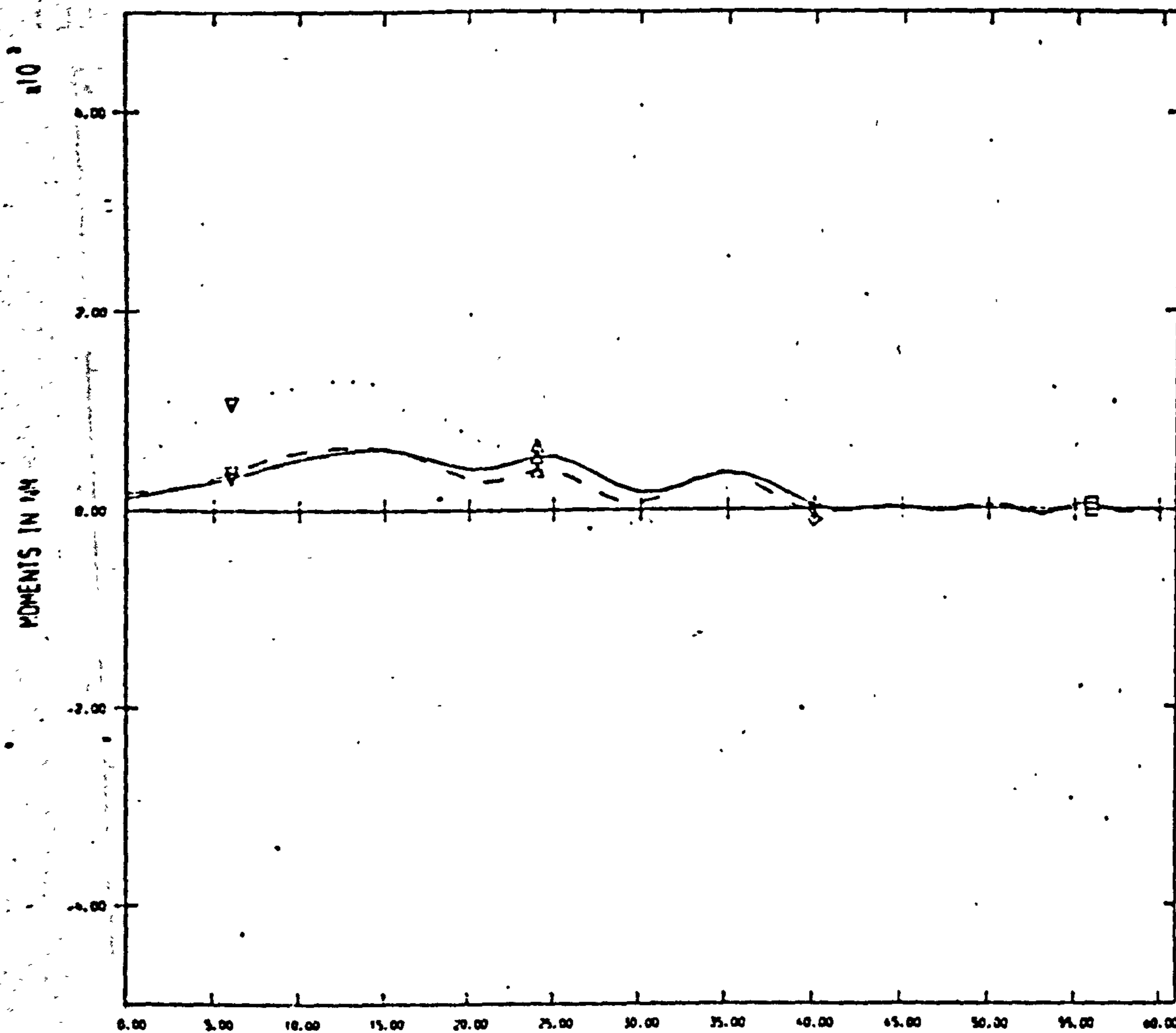
S2/R/BOT0



ANKLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE $\Delta$	CONTINUOUS	ANKLE
LEFT TOE OFF $\nabla$	DASHED	KNEE
RIGHT HEELSTRIKE $\square$	DOTTED	HIP
RIGHT TOE OFF $\diamond$		

SI/R/BDTO



ANKLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

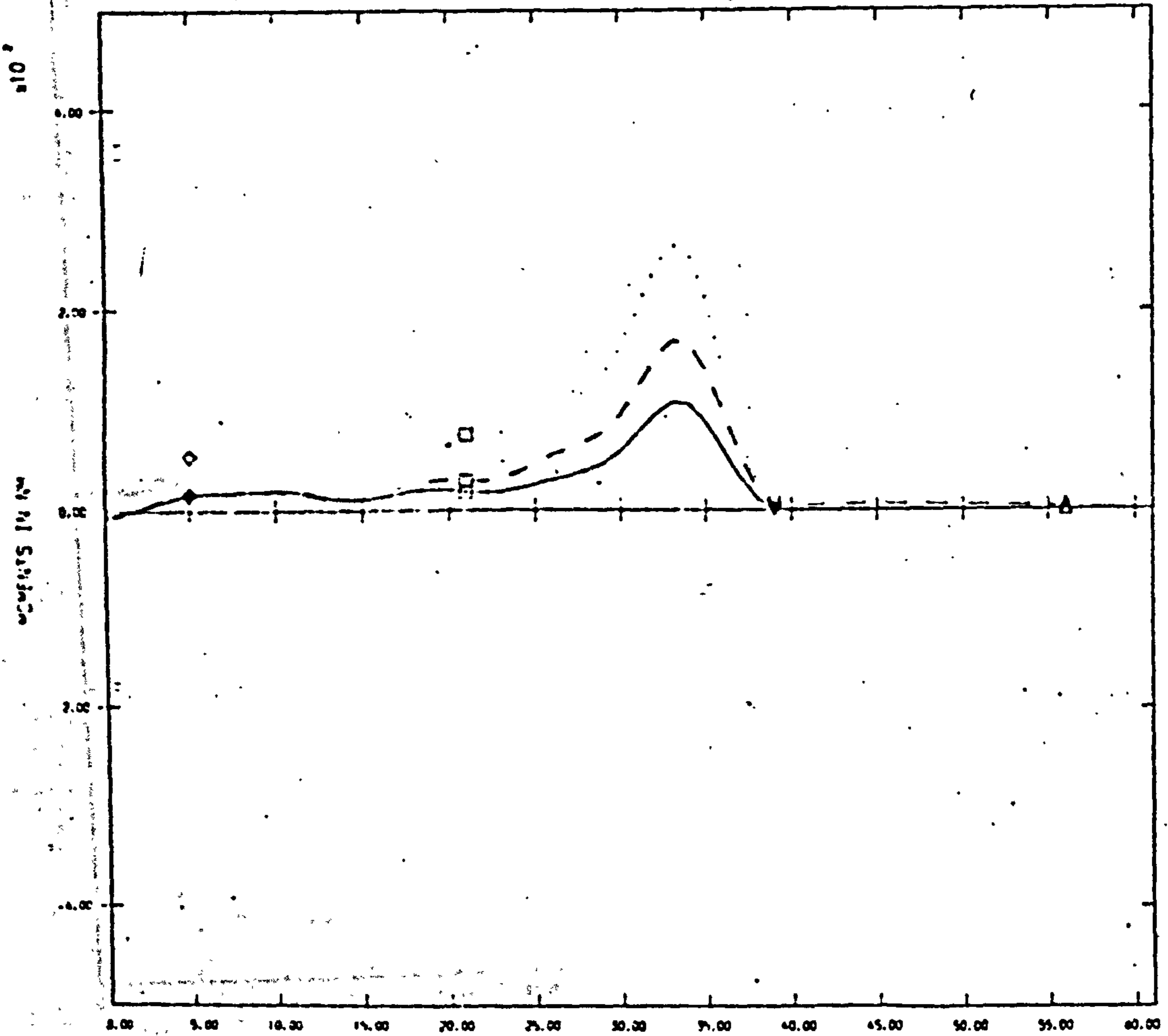
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\diamond$

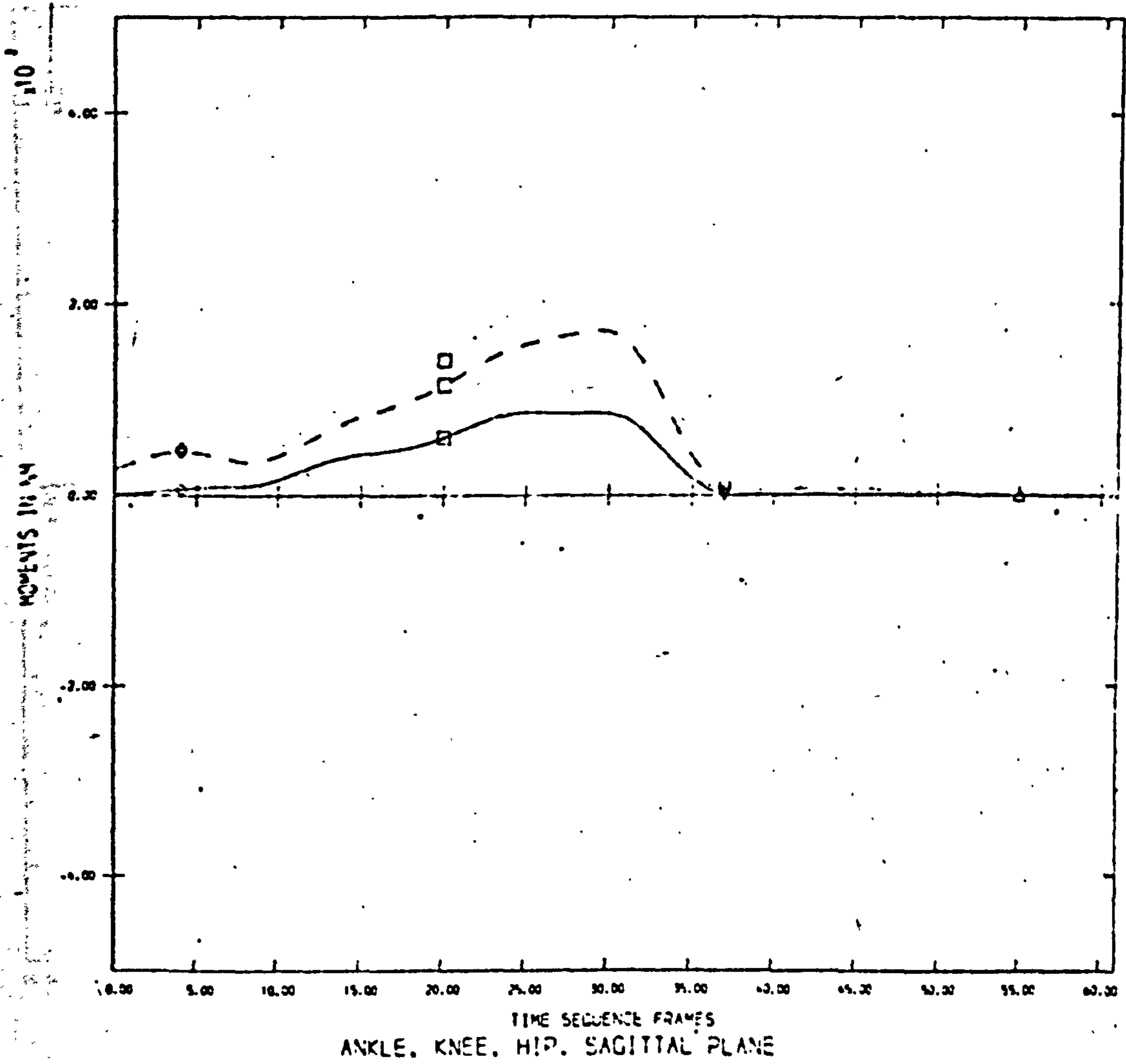
SI/L/FUL1



ANKLE, KNEE, HIP. SAGITTAL PLANE

- |                   |   |            |       |
|-------------------|---|------------|-------|
| LEFT HEEL STRIKE  | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF      | ▼ | DASHED     | KNEE  |
| RIGHT HEEL STRIKE | □ | DOTTED     | HIP   |
| RIGHT TOE OFF     | ◇ |            |       |

S2/L/FUL1



LEFT HEEL STRIKE ▲ CONTINUOUS ANKLE

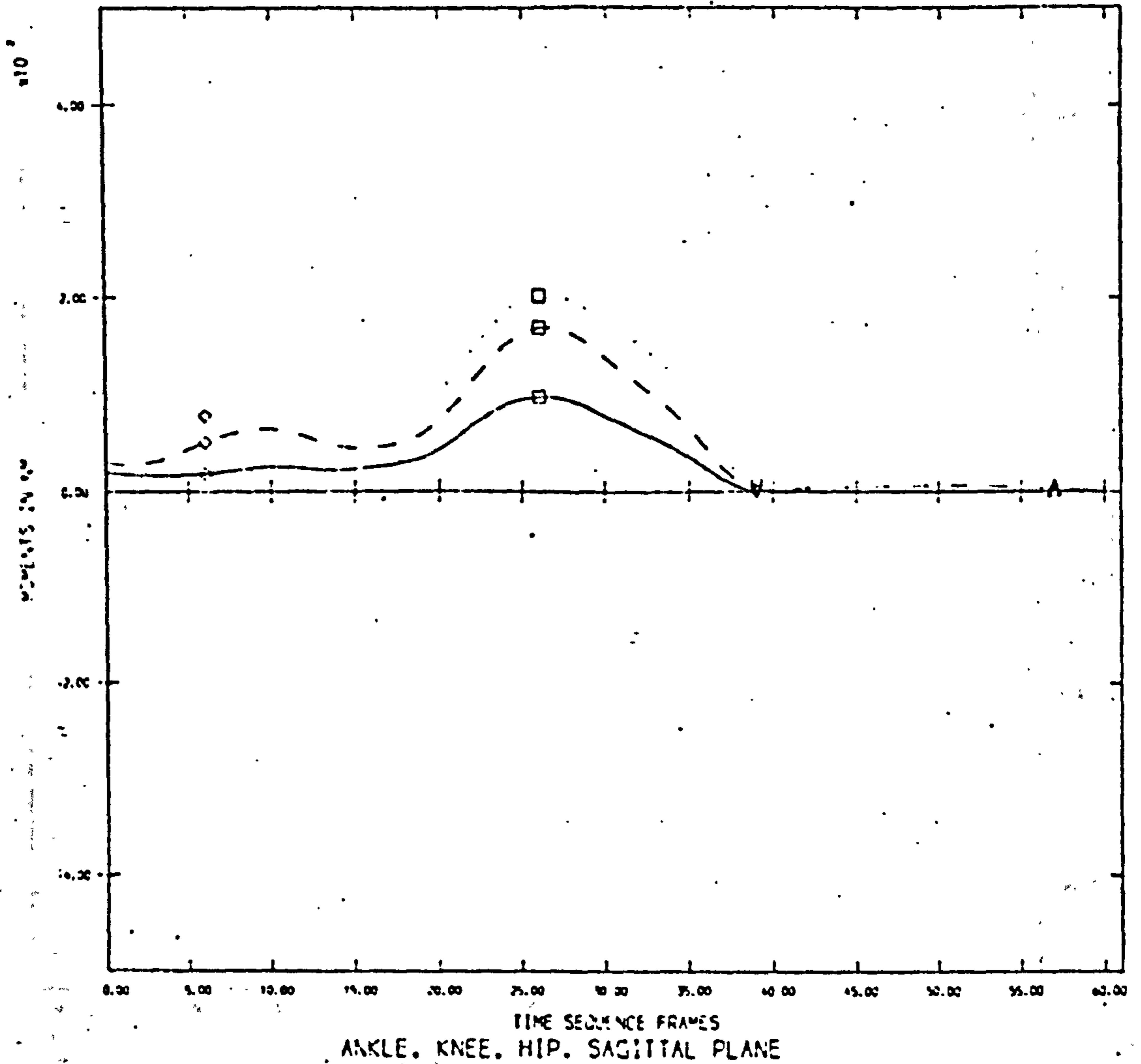
LEFT TOE OFF ▼ DASHED KNEE

RIGHT HEELSTRIKE □ DOTTED HIP

RIGHT TOE OFF ○



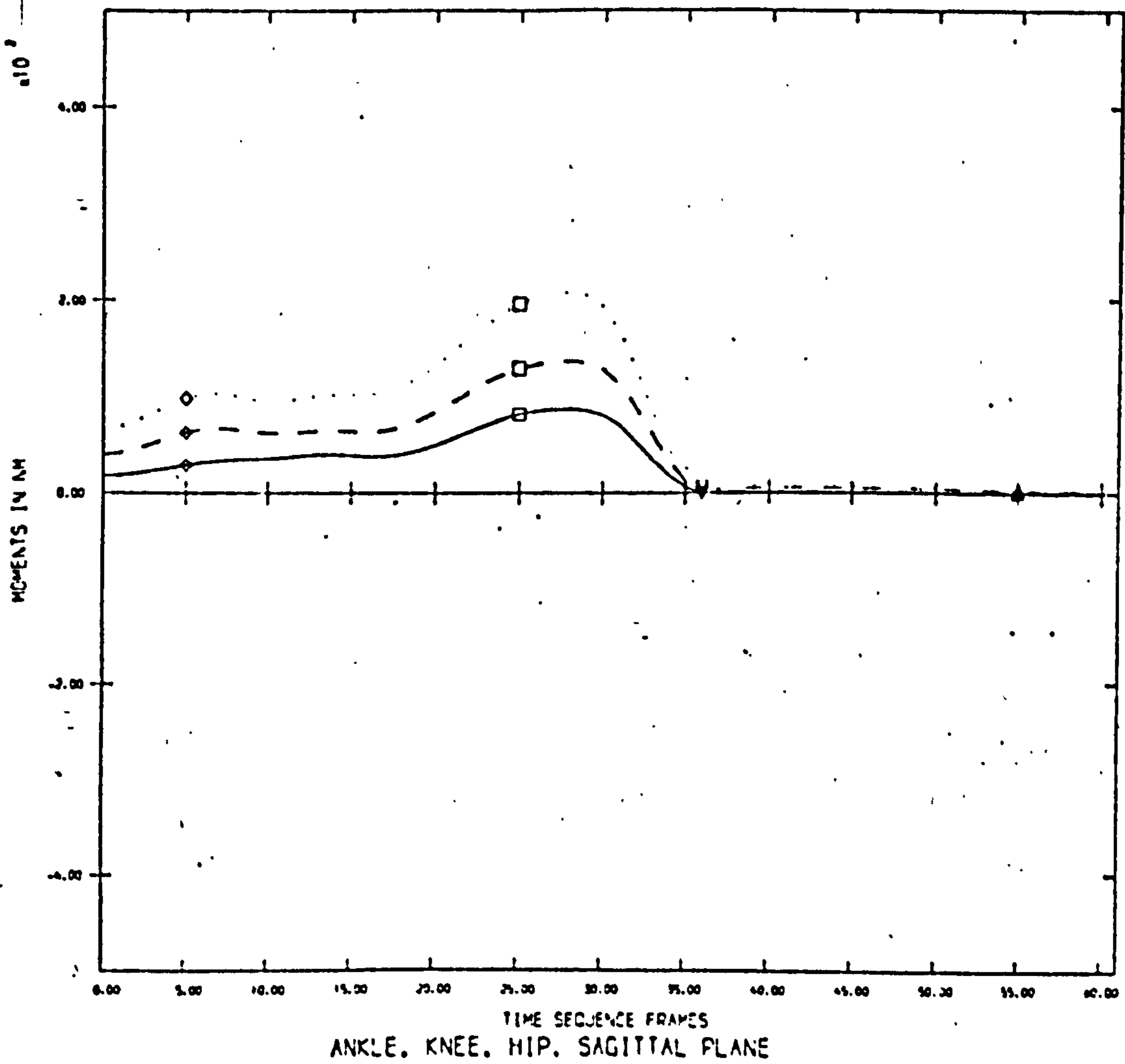
S3/L/FUL1



ANKLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE ▲	CONTINUOUS	ANKLE
LEFT TOE OFF ▼	DASHED	KNEE
RIGHT HEELSTRIKE □	DOTTED	HIP
RIGHT TOE OFF ○		

S4/L/FUL1



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

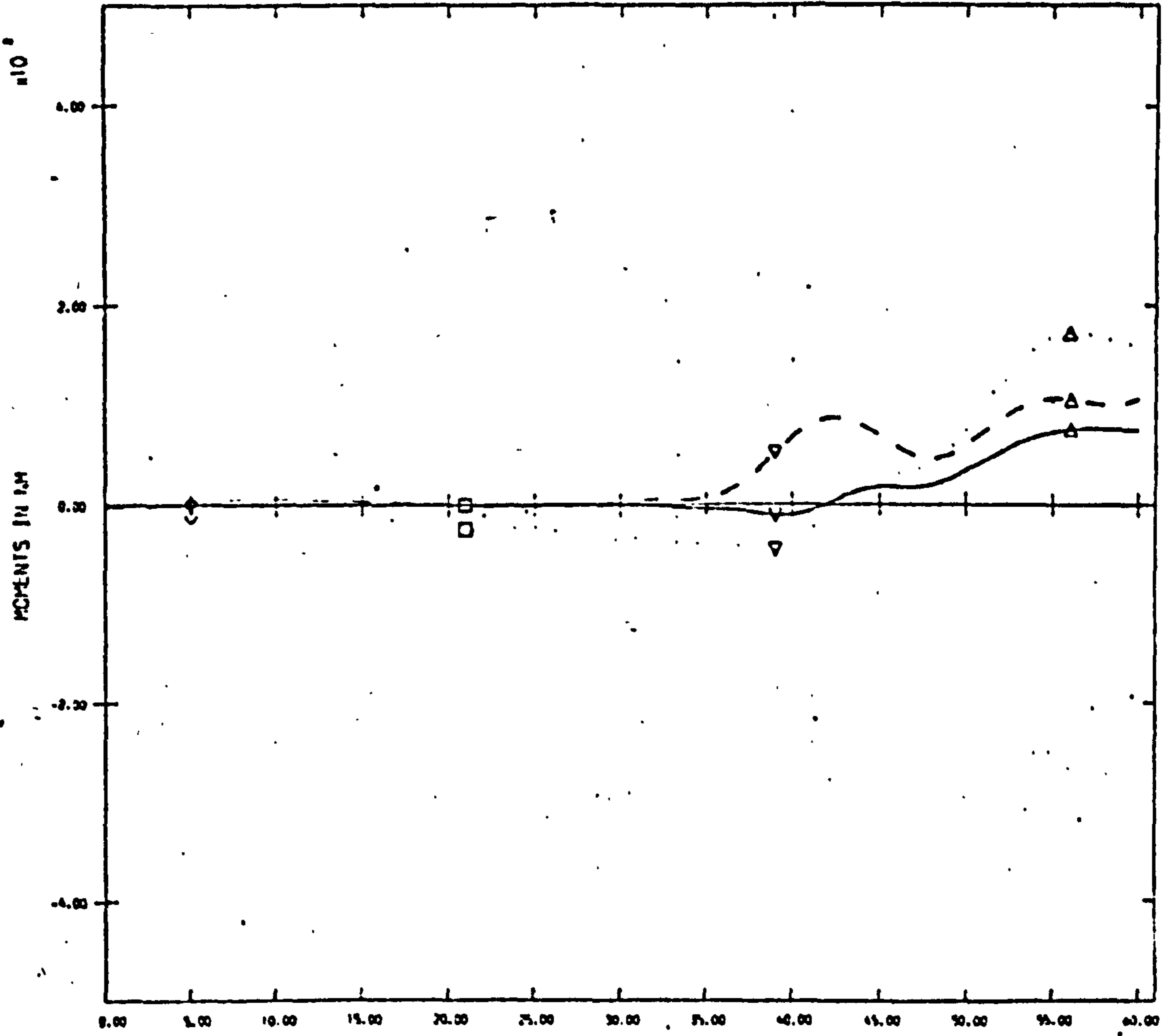
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\circ$

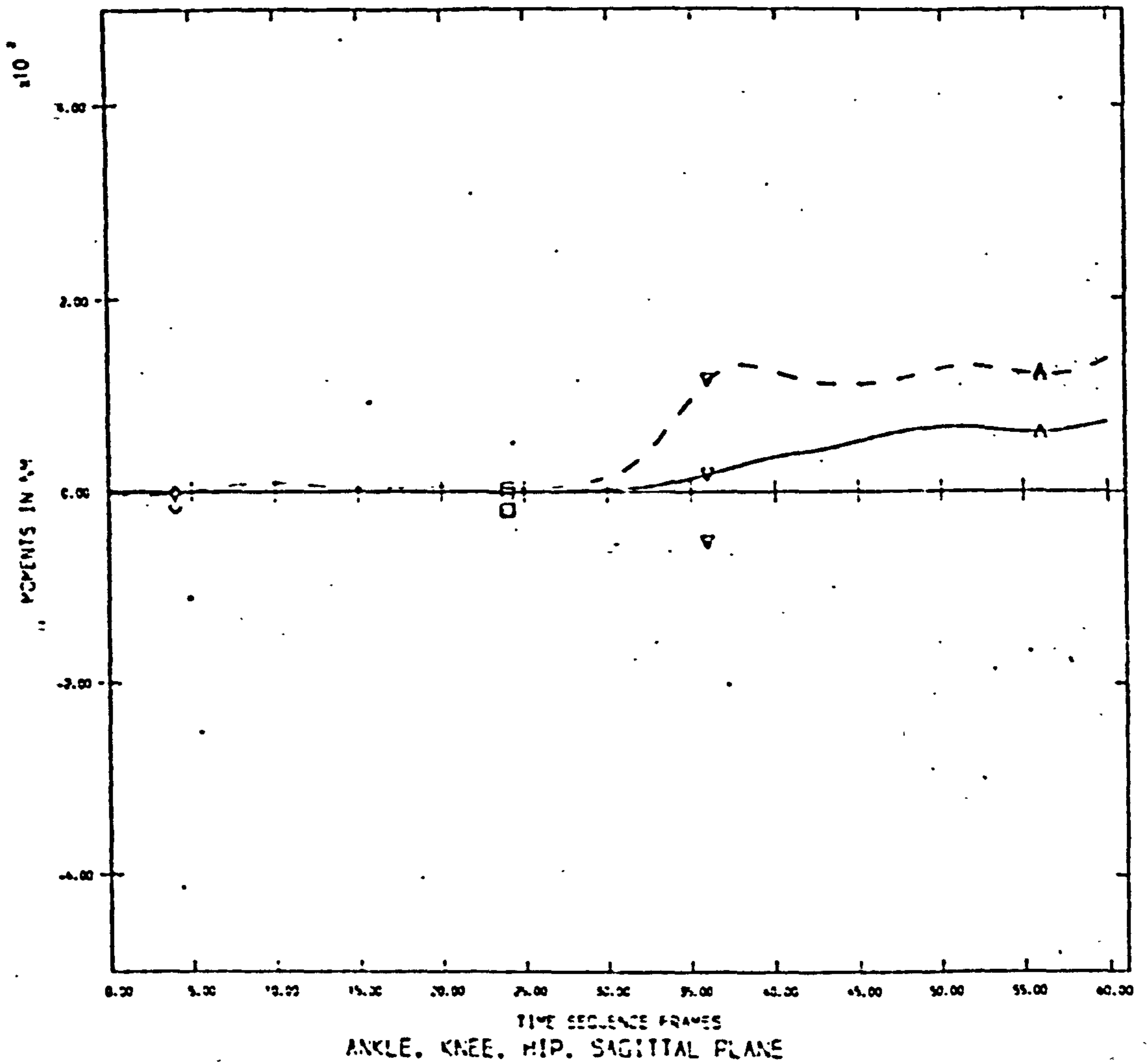
SI/R/FUL1



TIME SEQUENCE FRAMES  
ANKLE, KNEE, HIP, SAGITTAL PLANE

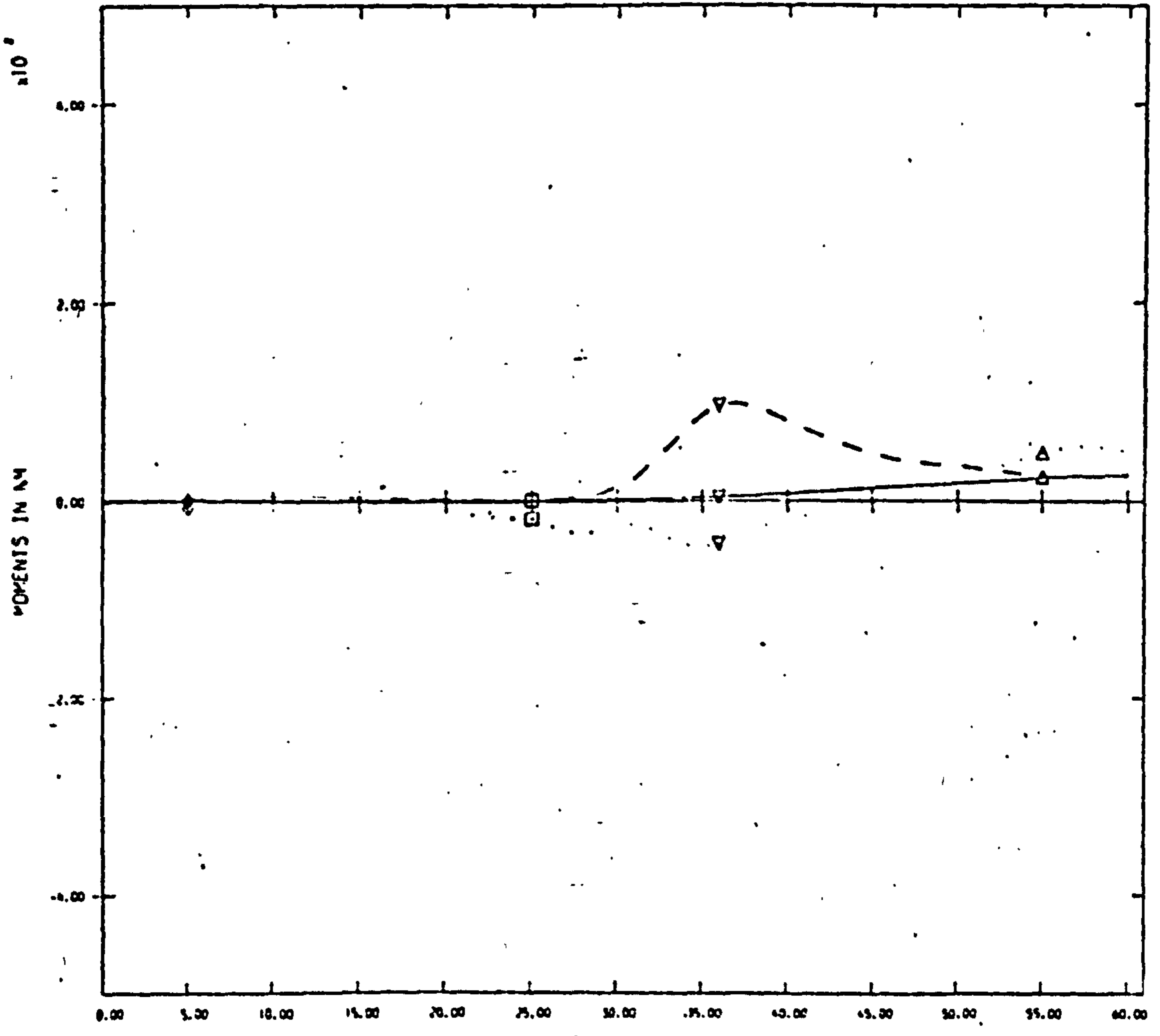
- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▼ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | ◻ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ◊ |            |       |

S5/R/FUL1



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

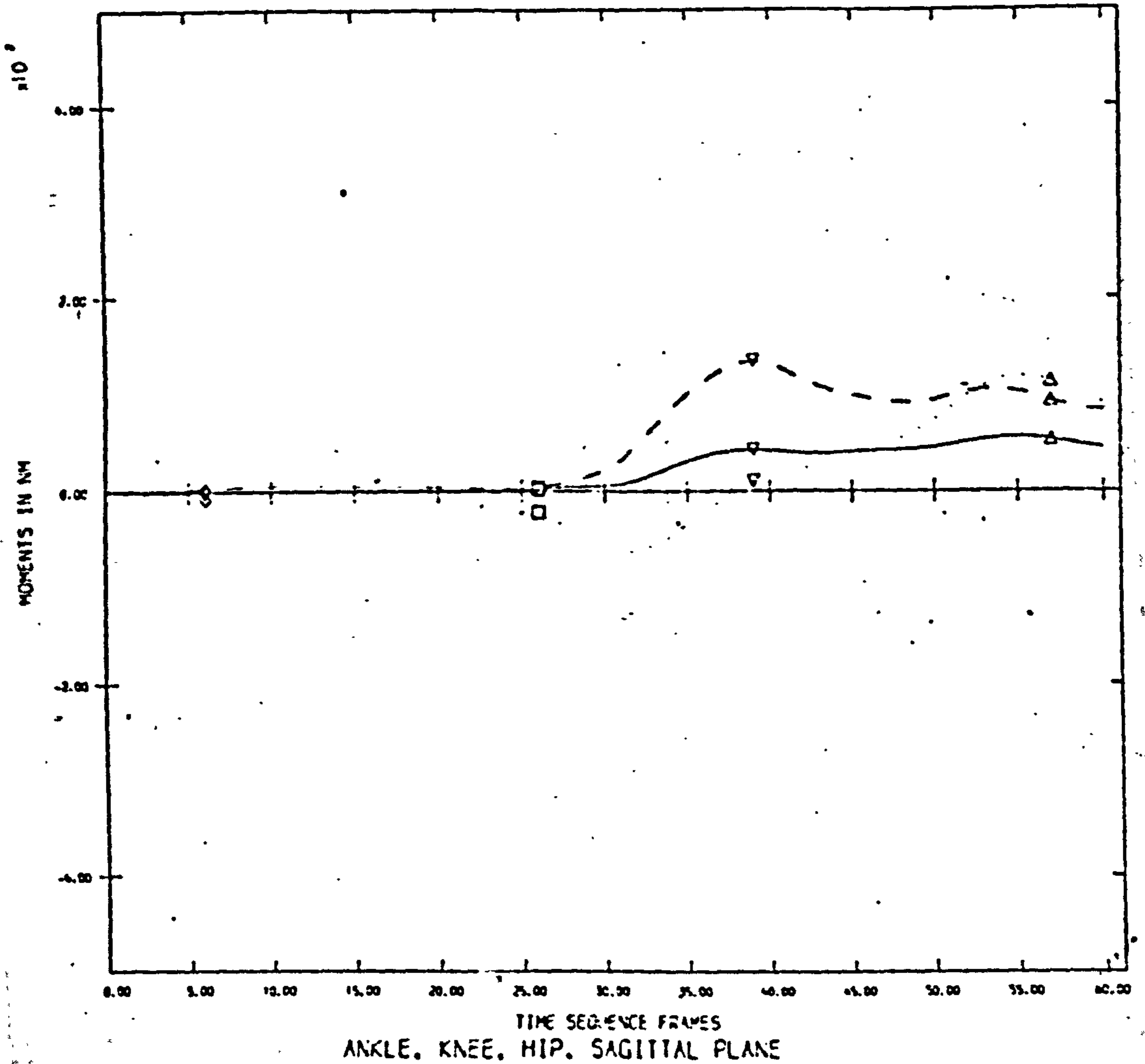
S4/R/FUL1



TIME SEQUENCE FRAMES  
ANKLE, KNEE, HIP, SAGITTAL PLANE

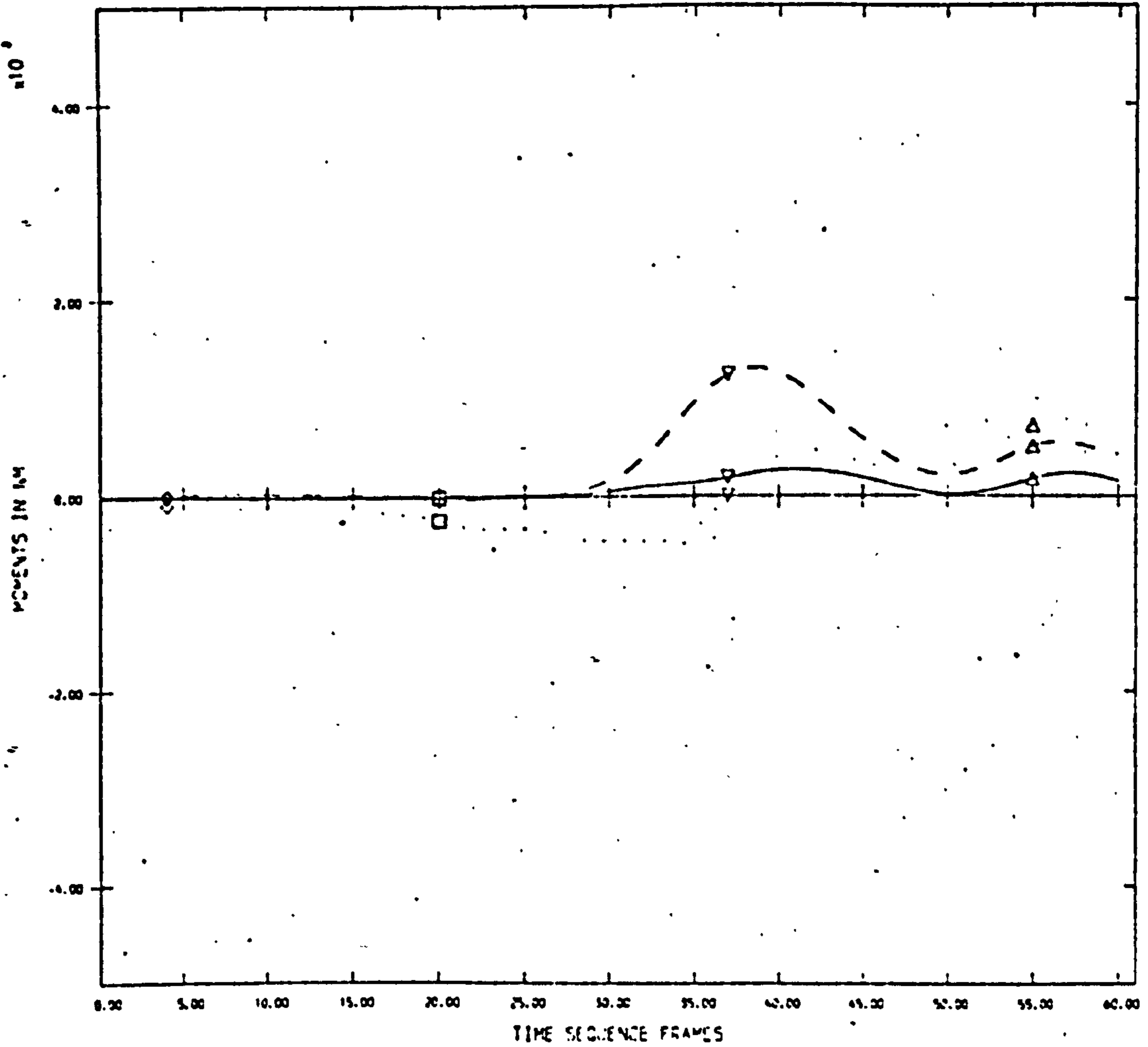
- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▼ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | ◻ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ◊ |            |       |

S3/R/FUL1



LEFT HEEL STRIKE	△	CONTINUOUS	ANKLE
LEFT TOE OFF	▽	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	◇		

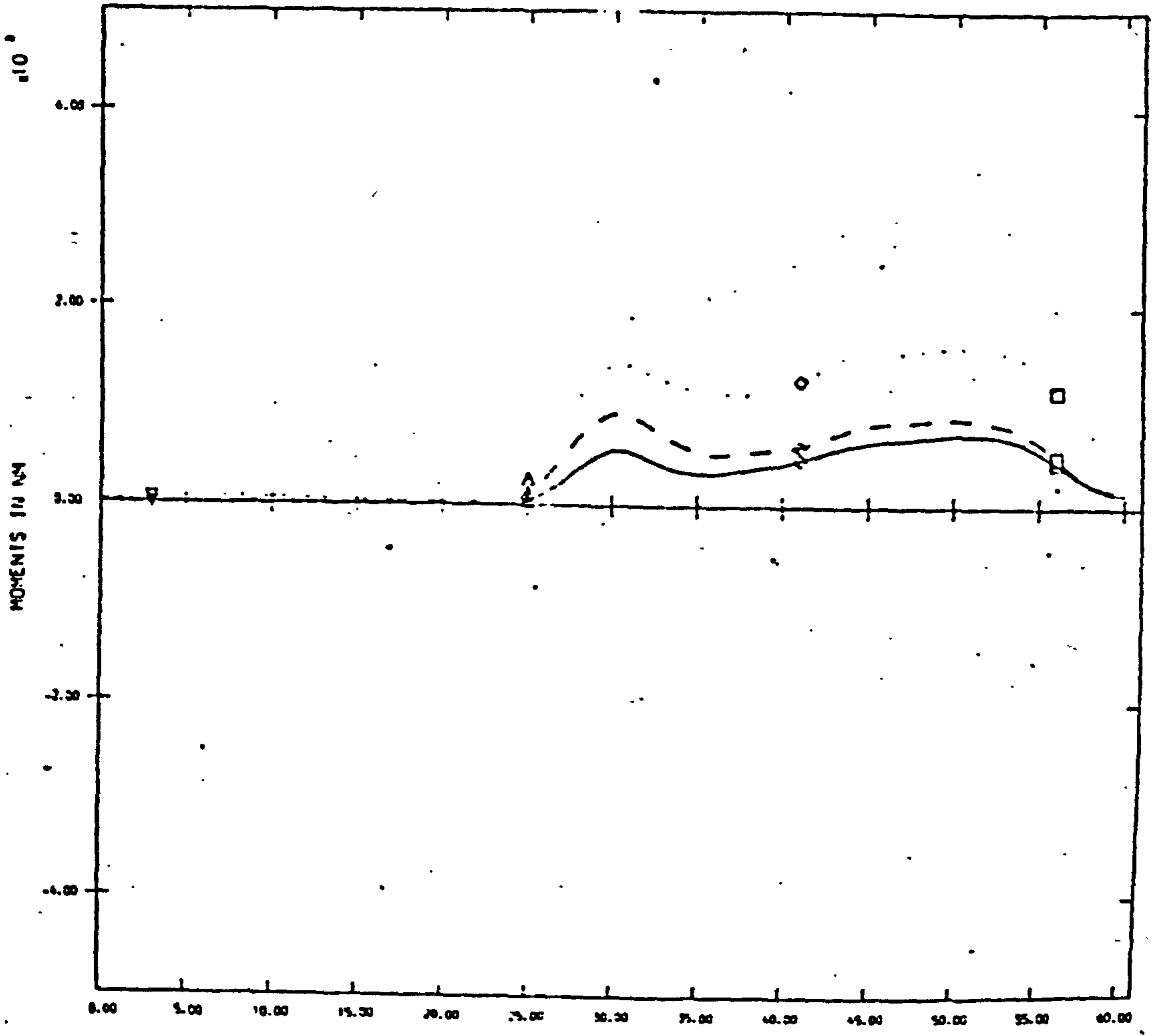
S2/R/FUL1



ANKLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	○		

SI/L/BDT1



ANKLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

DASHED KNEE

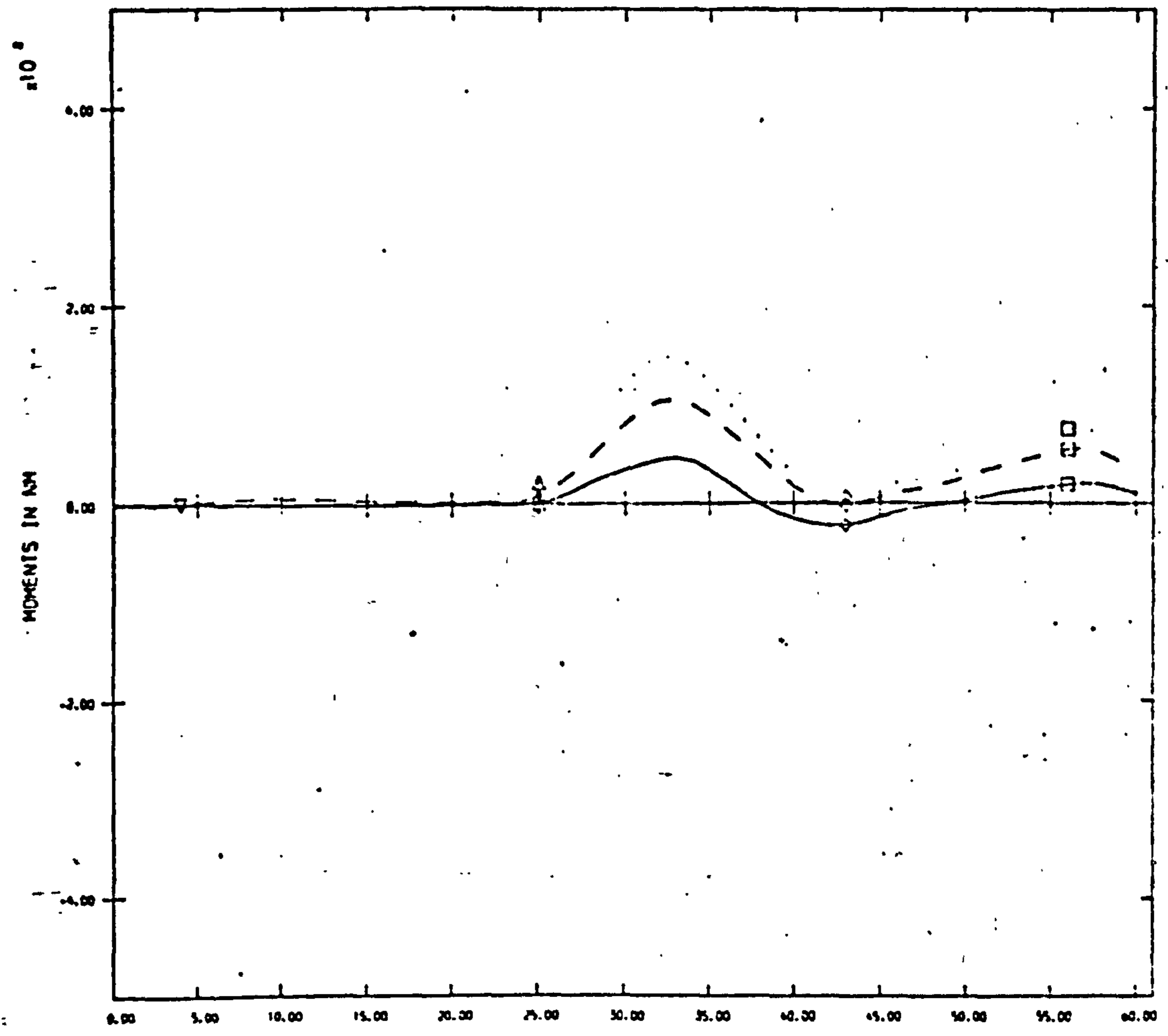
RIGHT HEEL STRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\diamond$



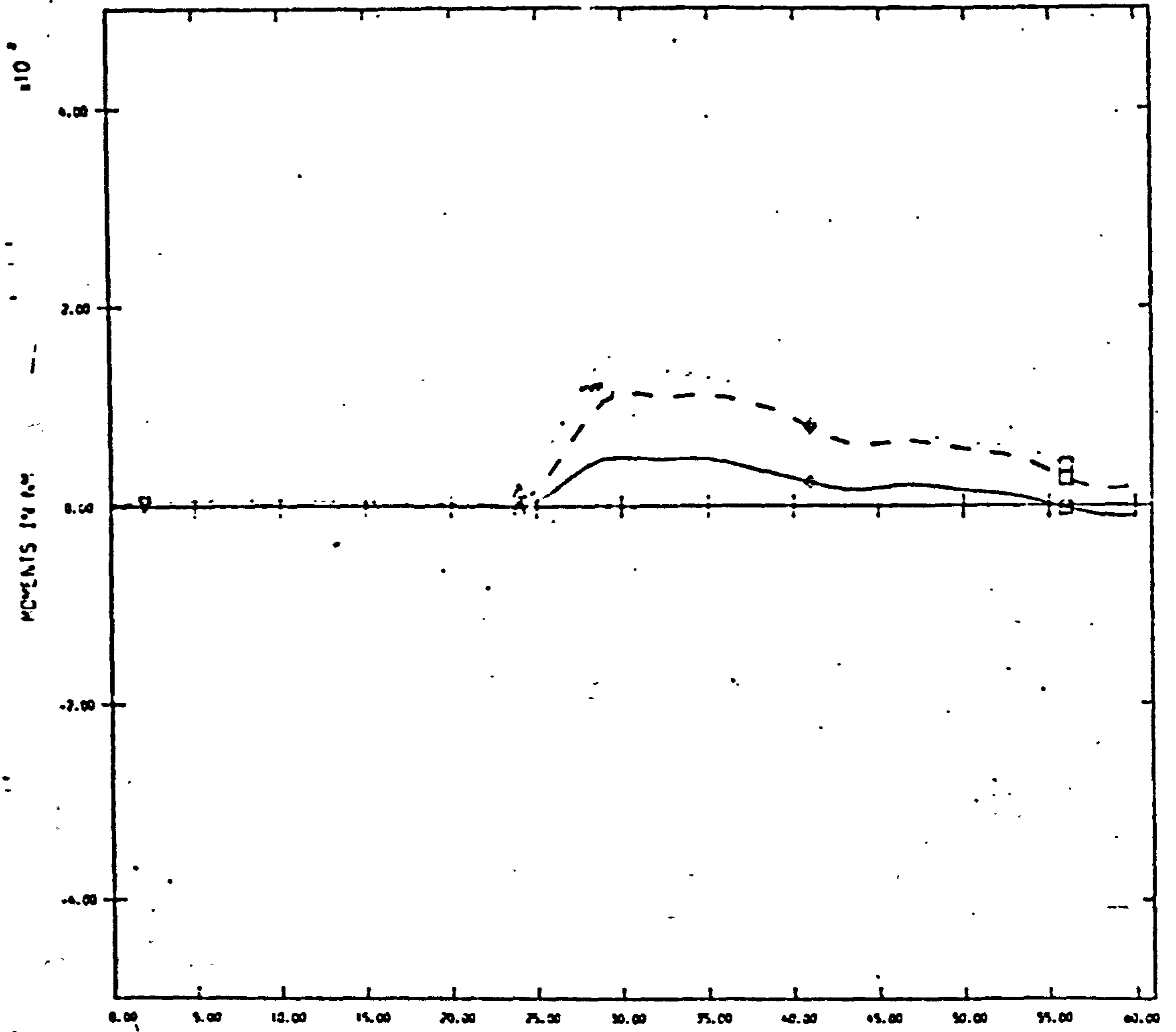
S2/L/BOT1



ANKLE, KNEE, HIP, SAGITTAL PLANE

- |                            |            |       |
|----------------------------|------------|-------|
| LEFT HEEL STRIKE $\Delta$  | CONTINUOUS | ANKLE |
| LEFT TOE OFF $\nabla$      | DASHED     | KNEE  |
| RIGHT HEELSTRIKE $\square$ | DOTTED     | HIP   |
| RIGHT TOE OFF $\diamond$   |            |       |

S3/L/BOT1



ANKLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE  $\Delta$

LEFT TOE OFF  $\nabla$

RIGHT HEELSTRIKE  $\square$

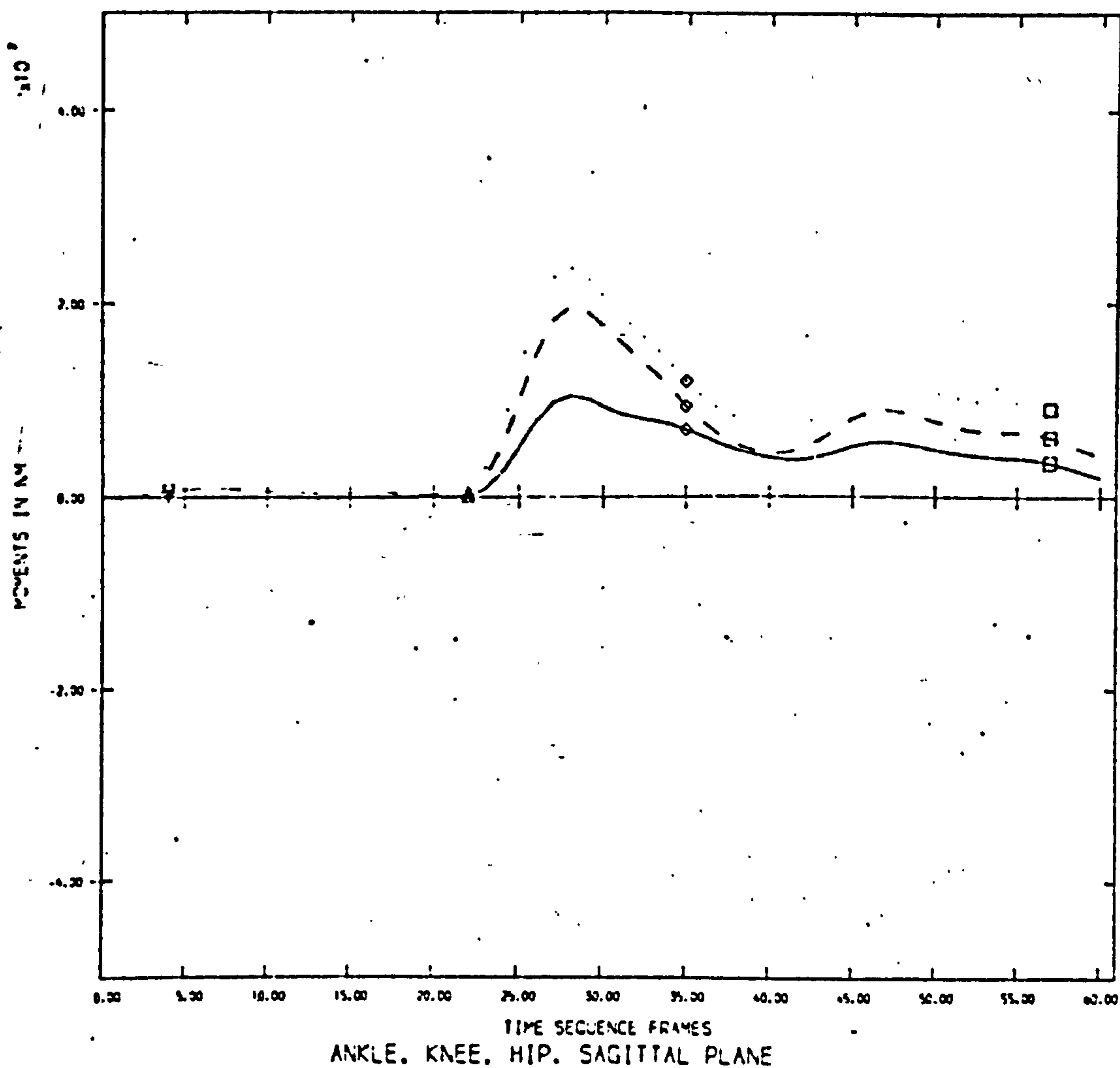
RIGHT TOE OFF  $\diamond$

CONTINUOUS ANKLE

DASHED KNEE

DOTTED HIP

S5/L/BOT1

LEFT HEEL STRIKE  $\Delta$ 

CONTINUOUS. ANKLE

LEFT TOE OFF  $\nabla$ 

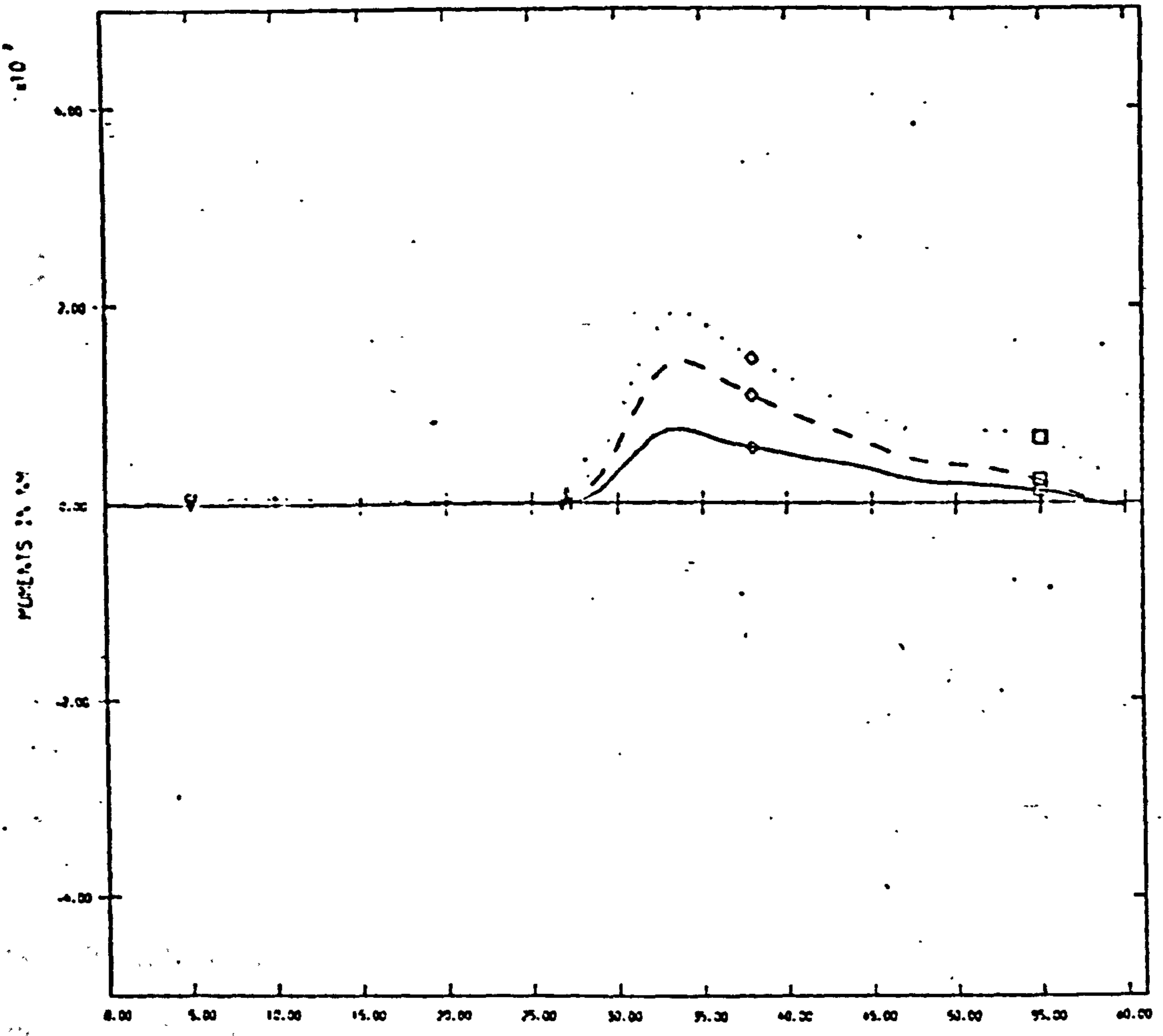
DASHED KNEE

RIGHT HEELSTRIKE  $\square$ 

DOTTED HIP

RIGHT TOE OFF  $\diamond$

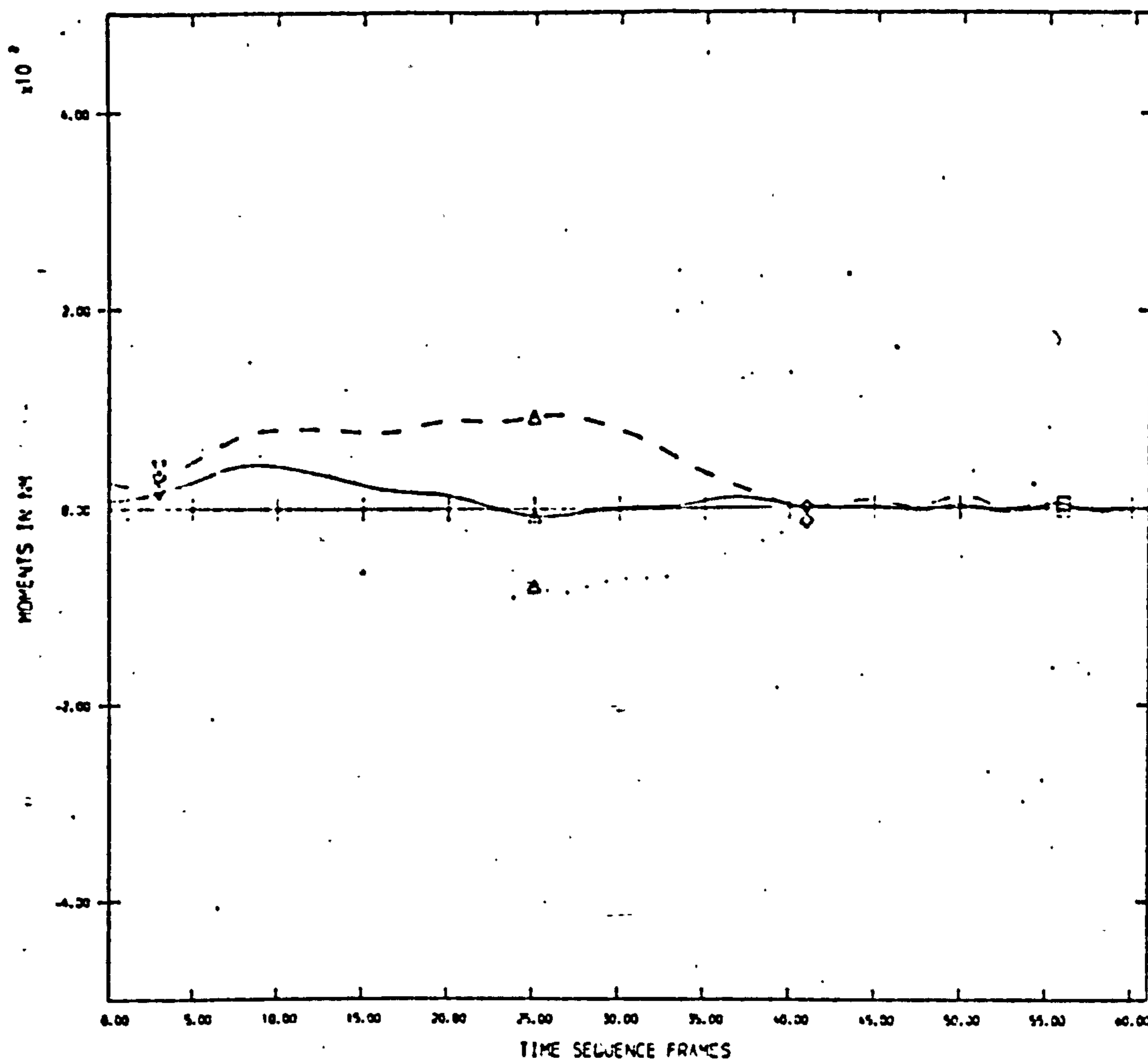
S4/L/BOT1



TIME SEQUENCE FRAMES  
 ANGLE, KNEE, HIP, SAGITTAL PLANE

LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	○		

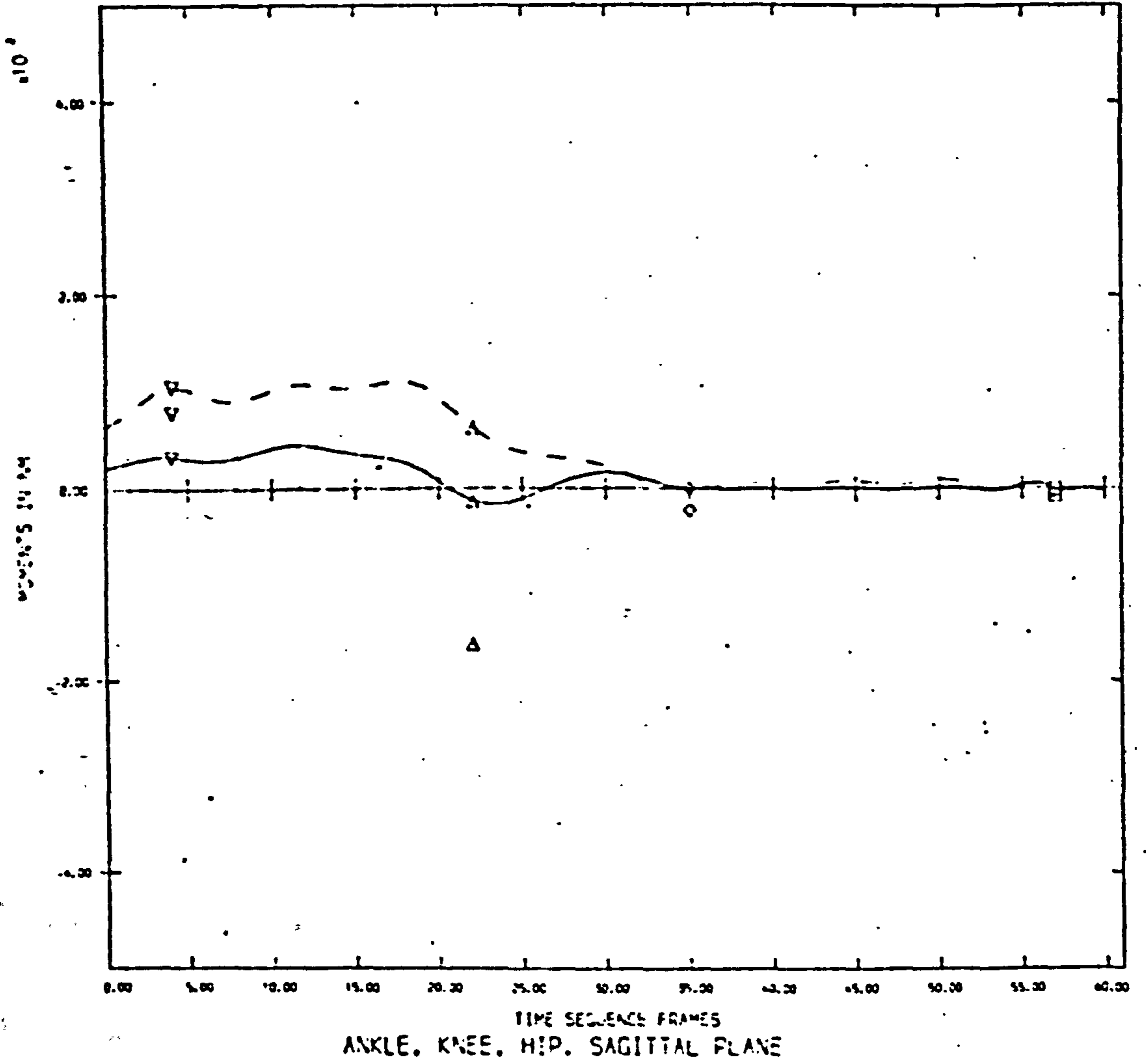
S1/R/BOT1



ANKLE, KNEE, HIP, SAGITTAL PLANE

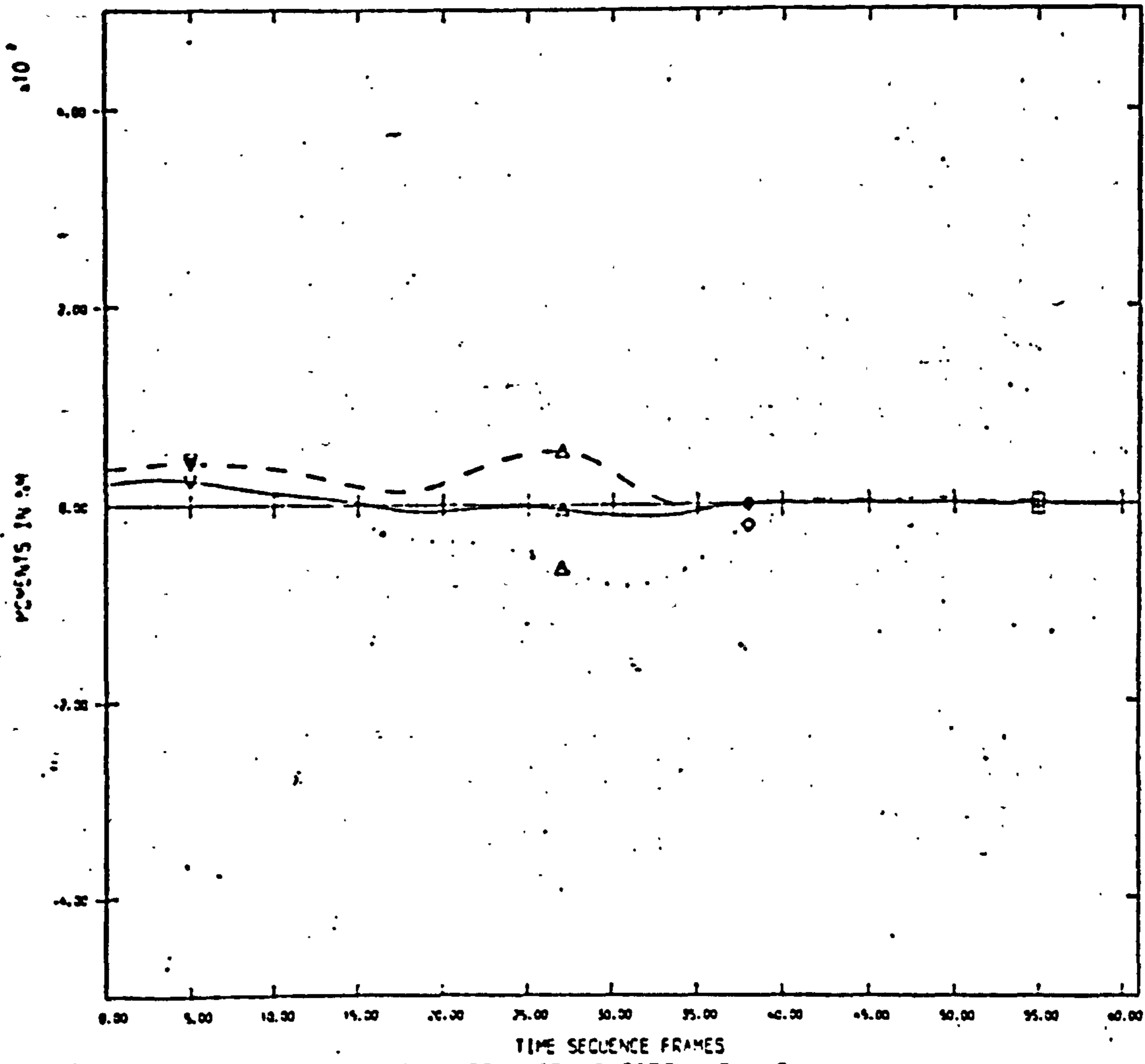
- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | △ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▽ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | □ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ◇ |            |       |

S5/R/BDT1



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

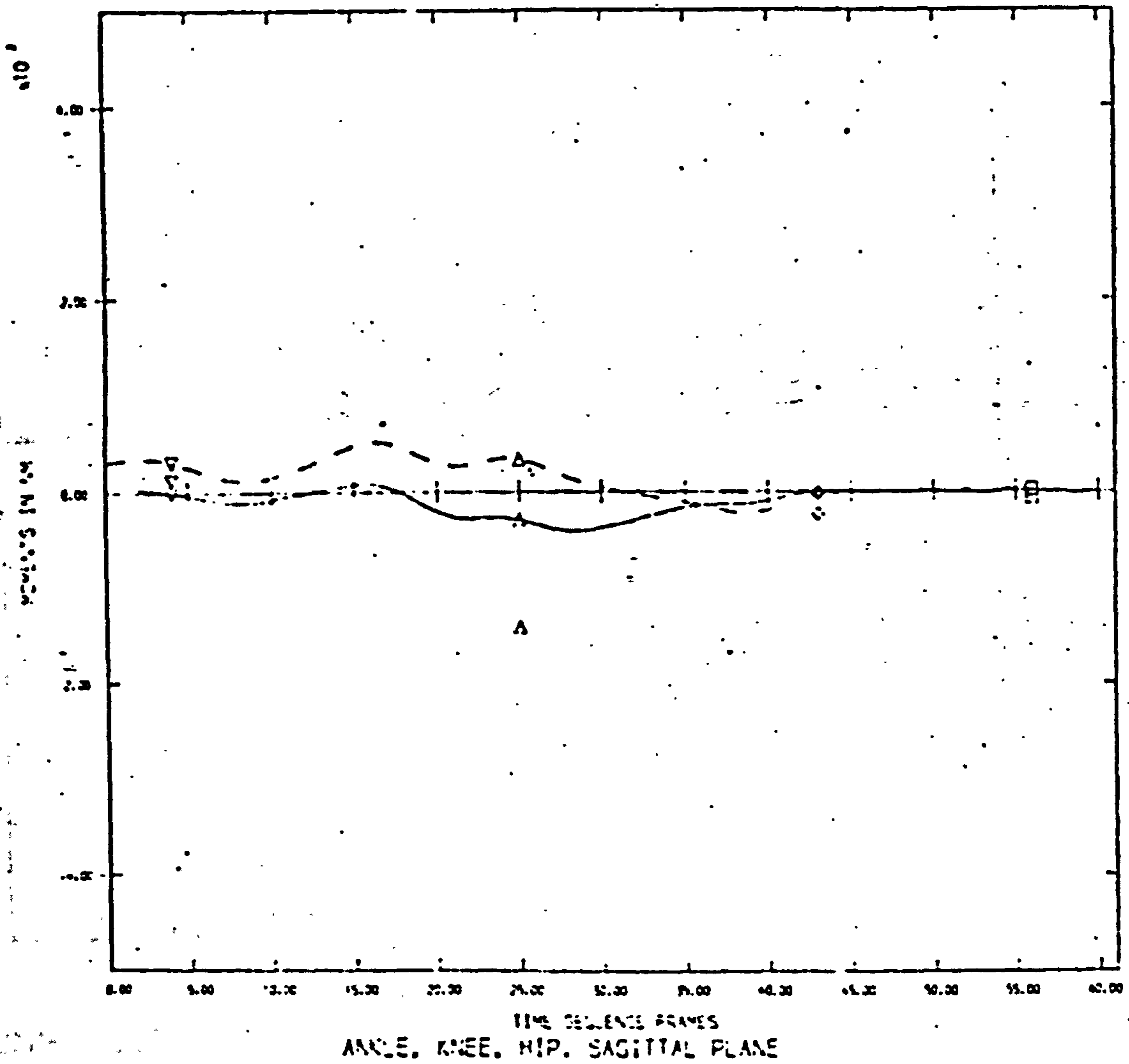
S4/R/BOT 1



TIME SEQUENCE FRAMES  
ANKLE, KNEE, HIP, SAGITTAL PLANE

- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▼ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | ◻ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ◊ |            |       |

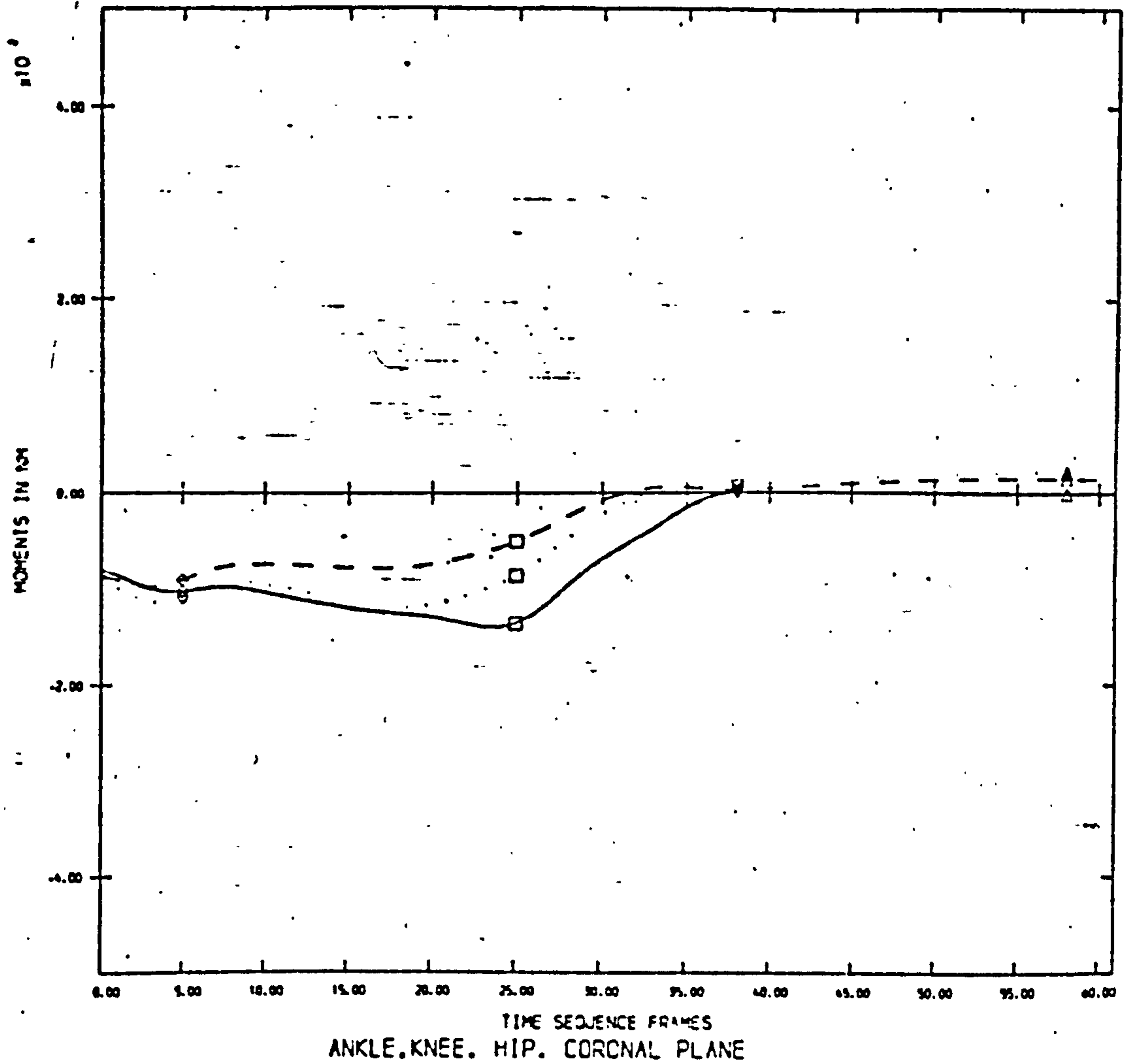
S2/R/BOT1



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	■	DOTTED	HIP
RIGHT TOE OFF	○		

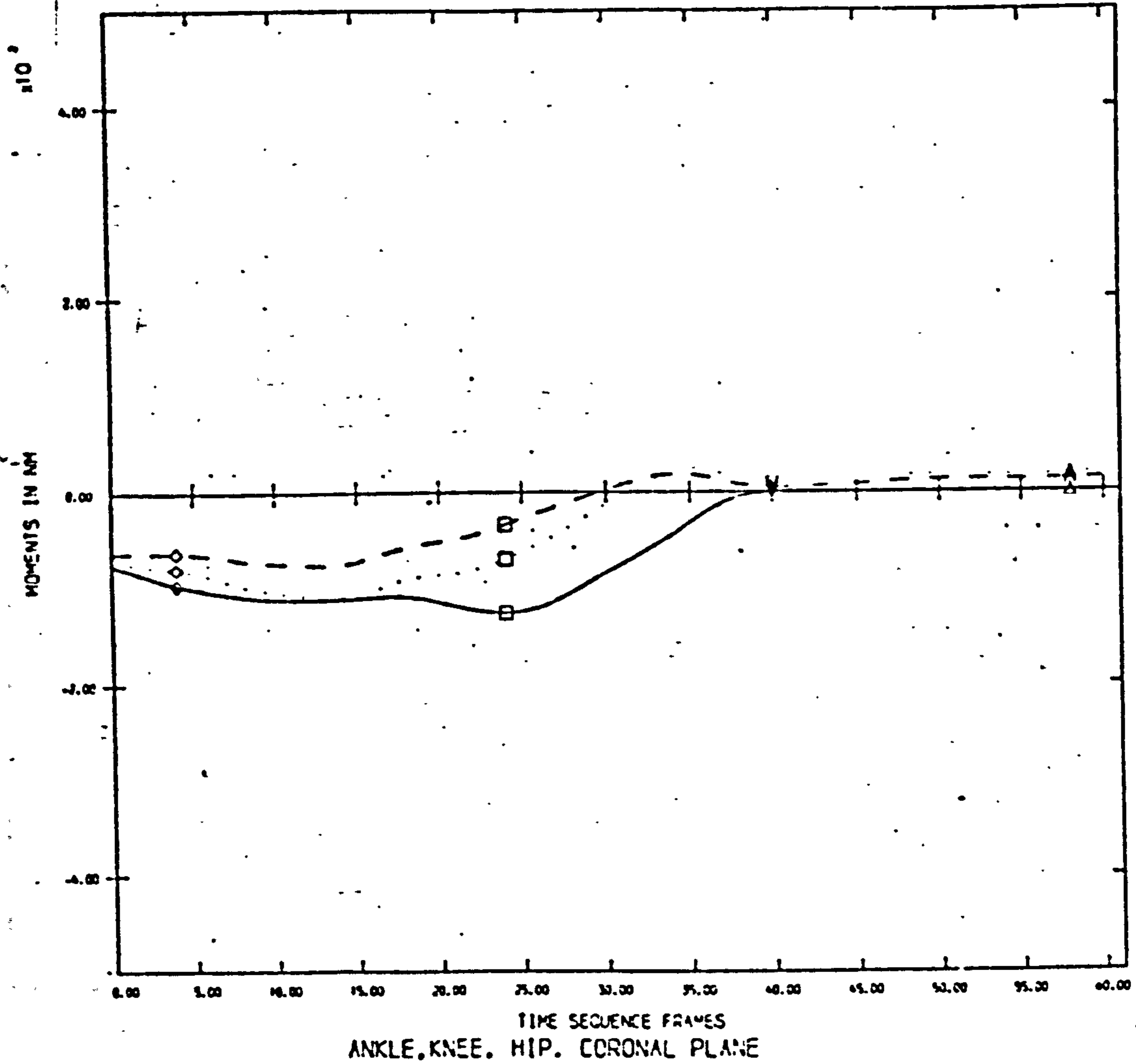


SI/L/FULO



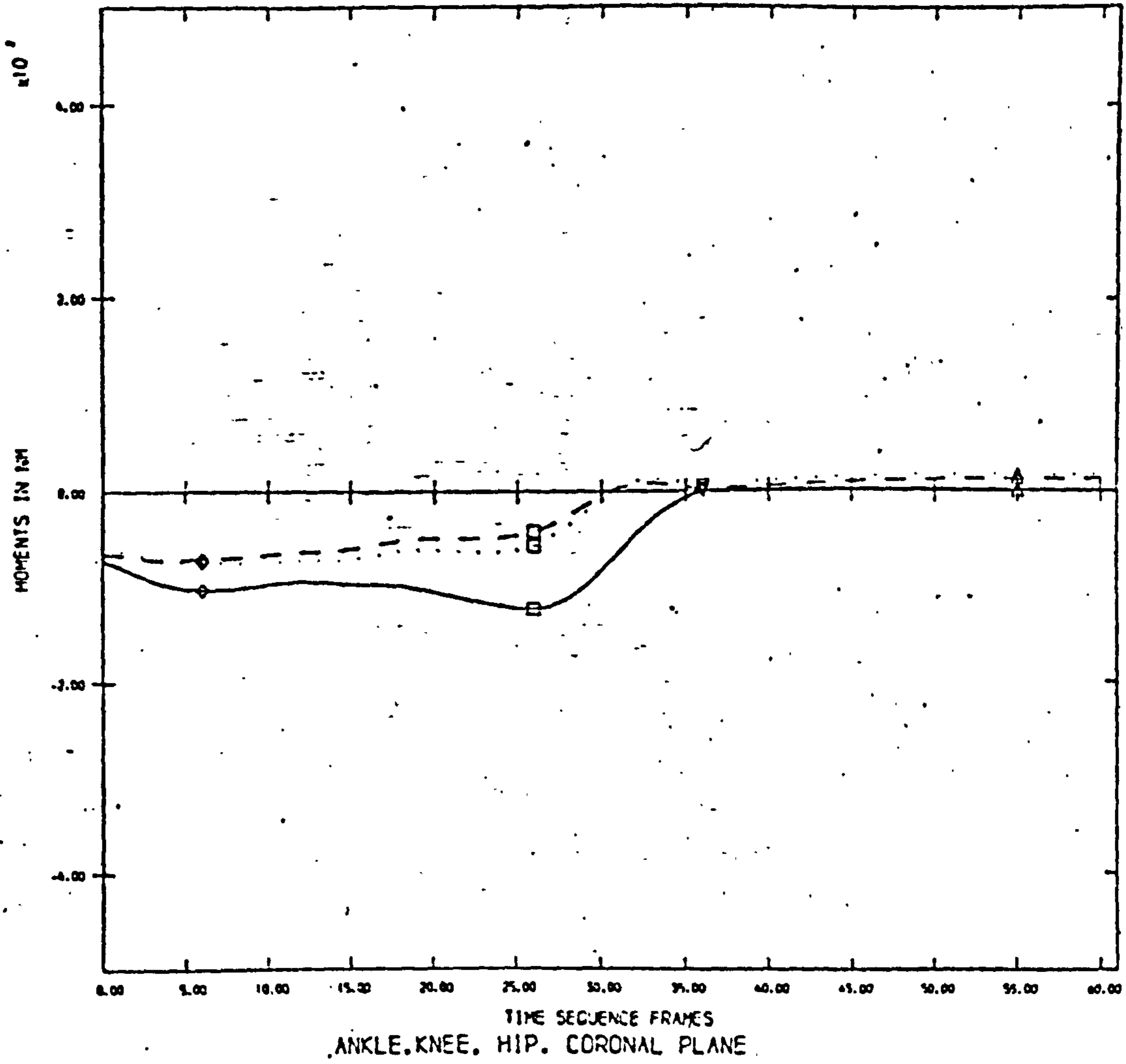
LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	◇		

S2/L/FULO



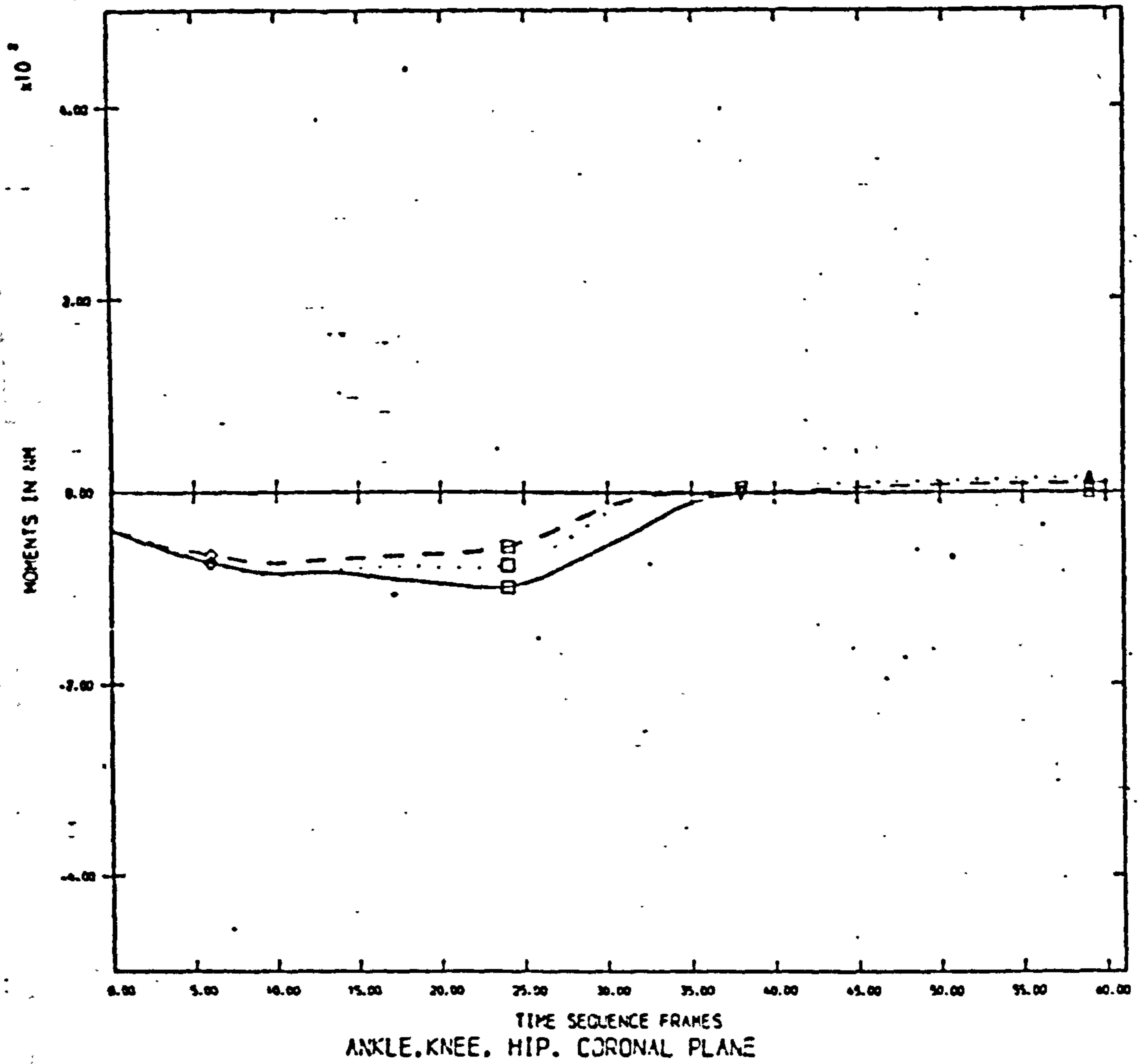
LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	◆		

S3/L/FULO



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

S4/L/FULO



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

DASHED KNEE

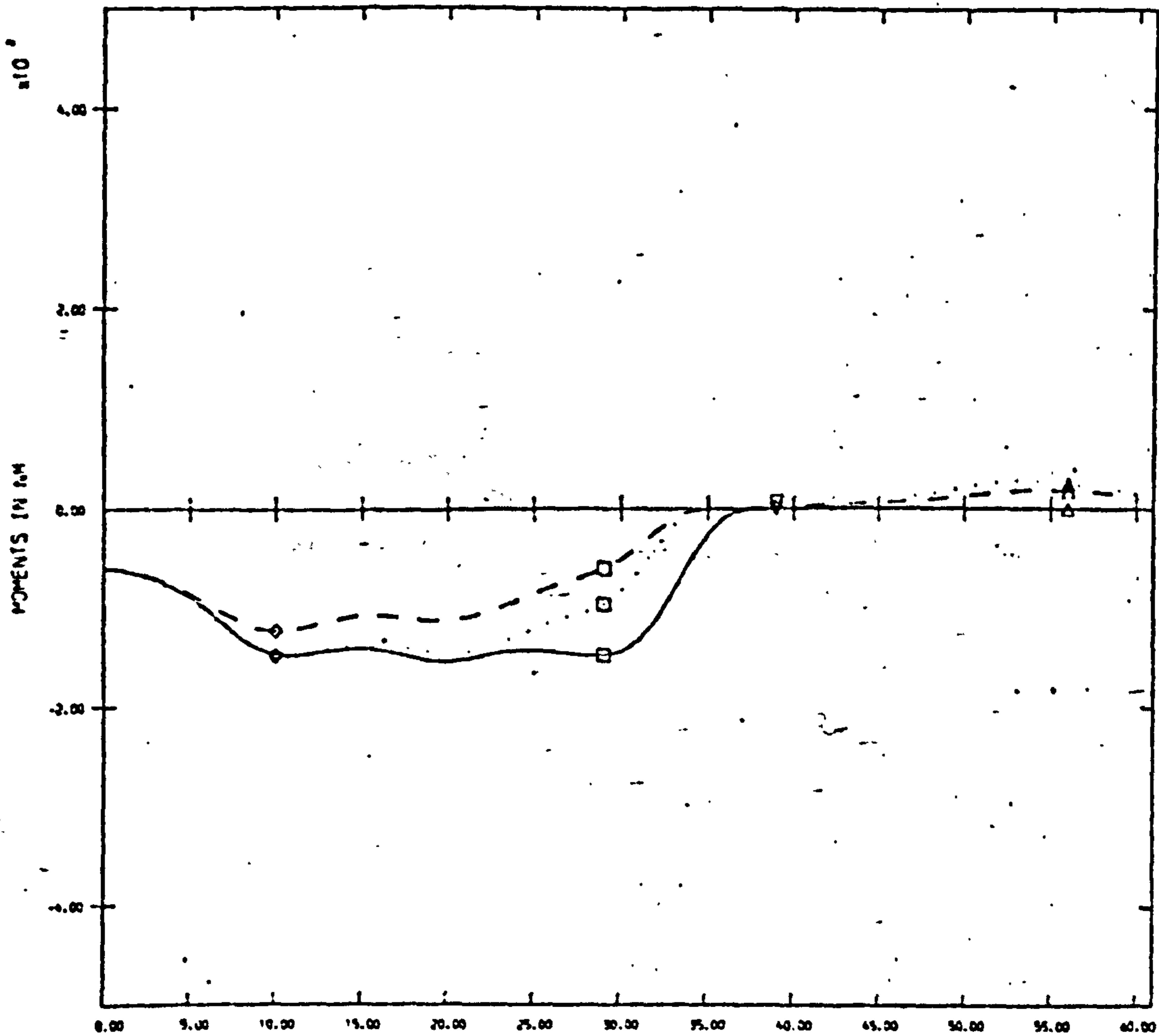
RIGHT HEELSTRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\diamond$

TIME SEQUENCE FRAMES  
ANKLE, KNEE, HIP, CORONAL PLANE

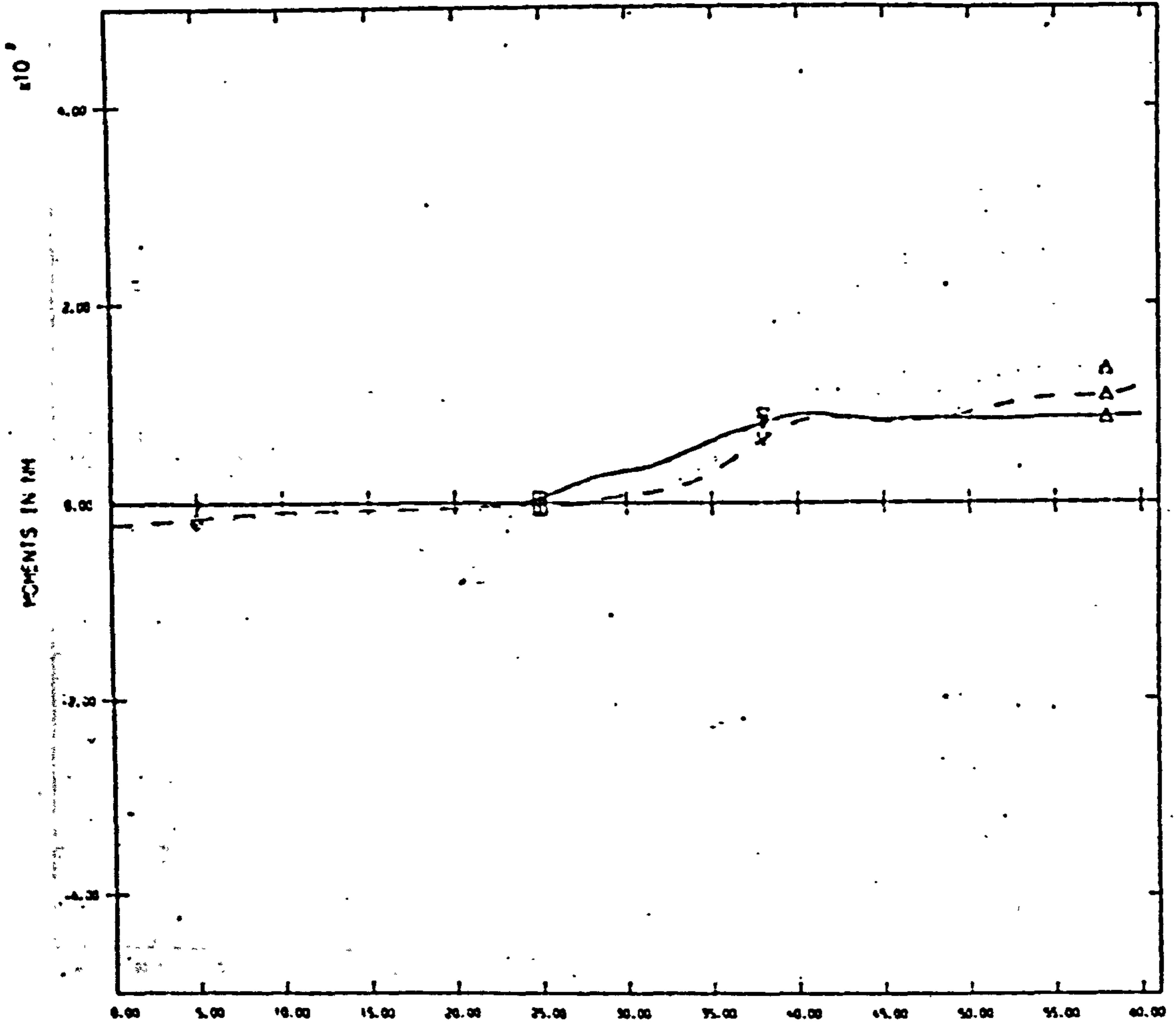
S5/L/FULO



TIME SEQUENCE FRAMES  
ANKLE, KNEE, HIP, CORONAL PLANE

LEFT HEEL STRIKE	△	CONTINUOUS	ANKLE
LEFT TOE OFF	▽	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	◇		

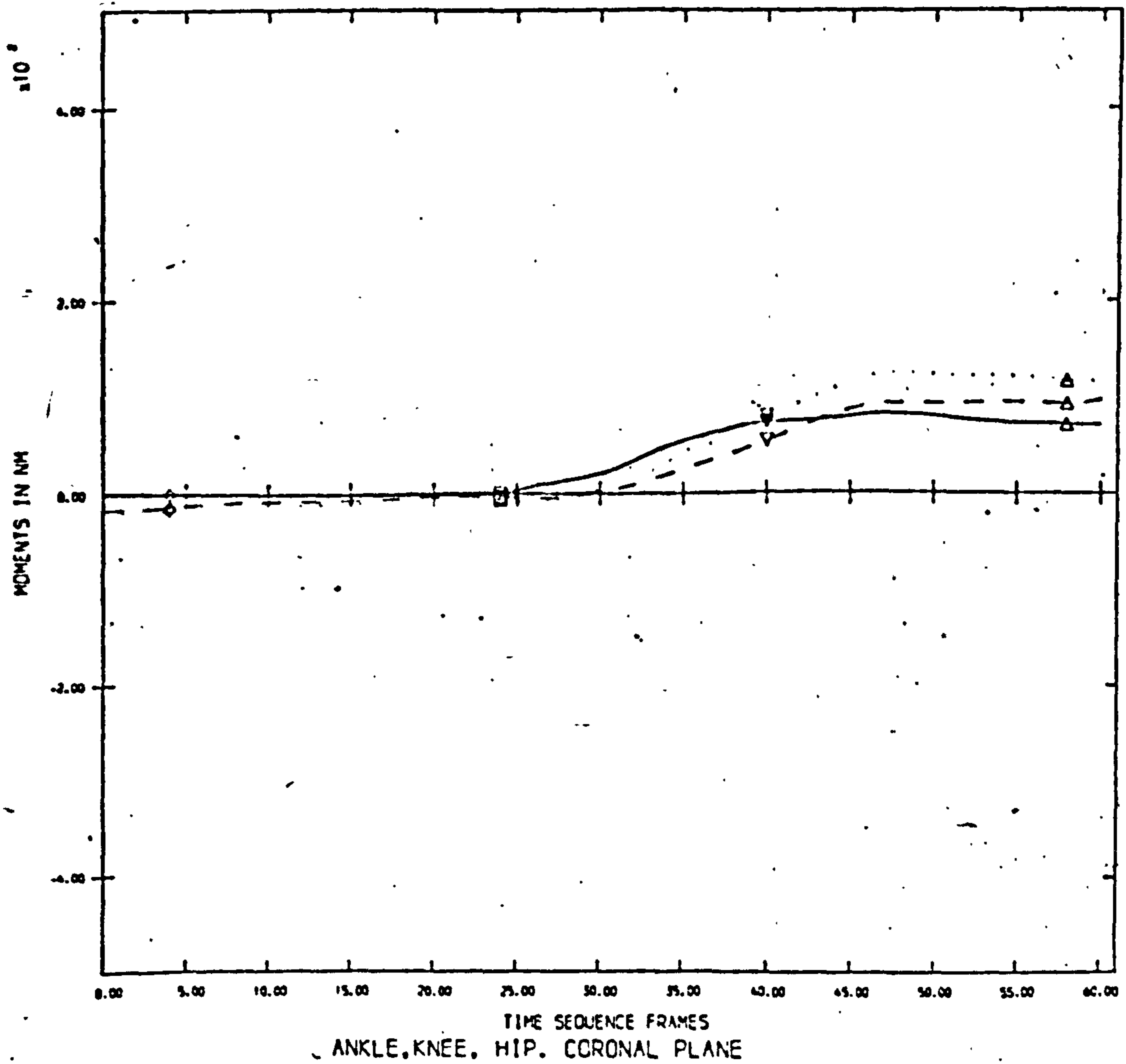
S1/R/FULO



TIME SEQUENCE FRAMES  
ANKLE, KNEE, HIP, CORONAL PLANE

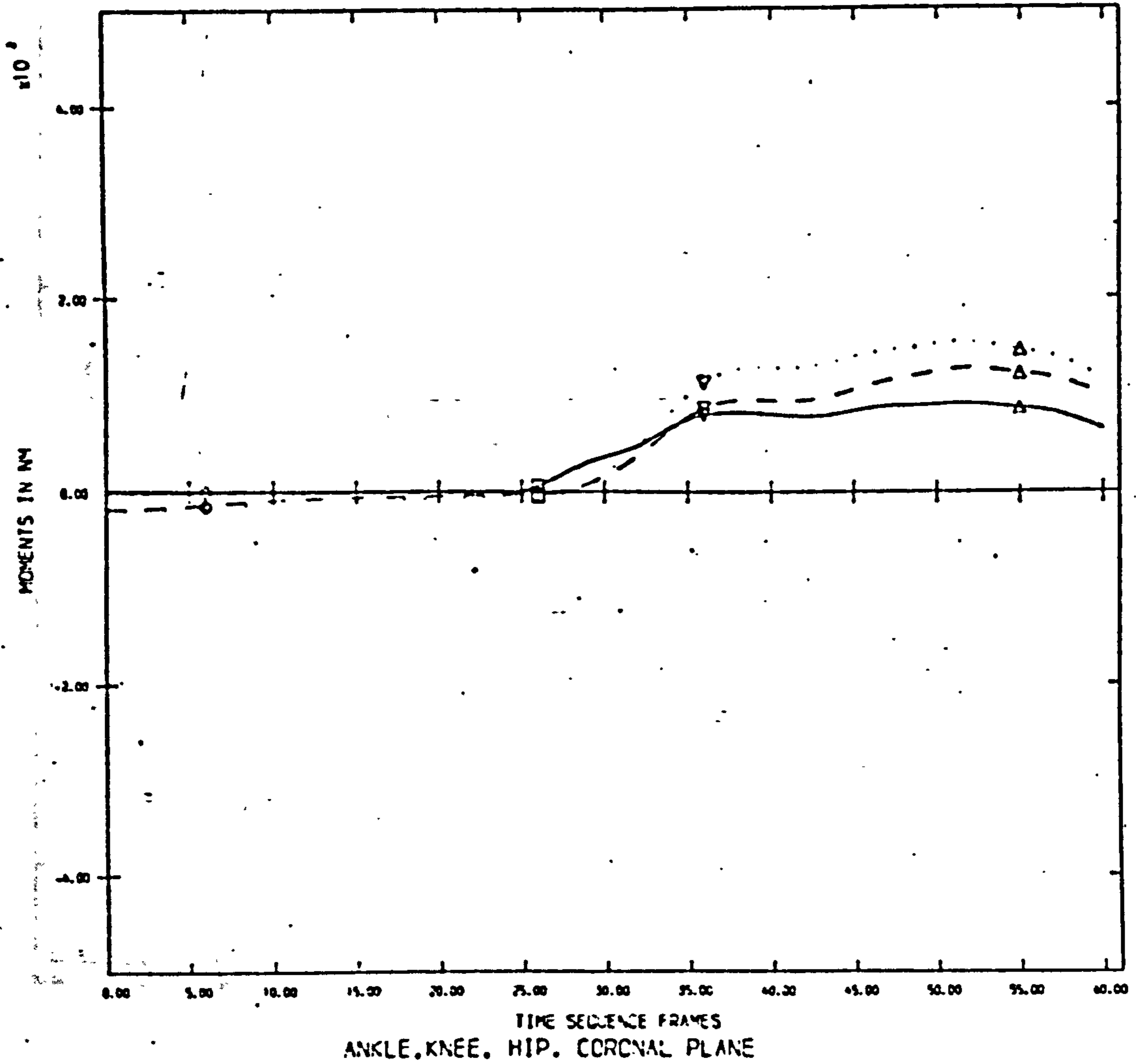
- |                   |   |            |       |
|-------------------|---|------------|-------|
| LEFT HEEL STRIKE  | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF      | ▼ | DASHED     | KNEE  |
| RIGHT HEEL STRIKE | ◻ | DOTTED     | HIP   |
| RIGHT TOE OFF     | ◊ |            |       |

S2/R/FUL0



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

S3/R/FULO



LEFT-HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

DASHED KNEE

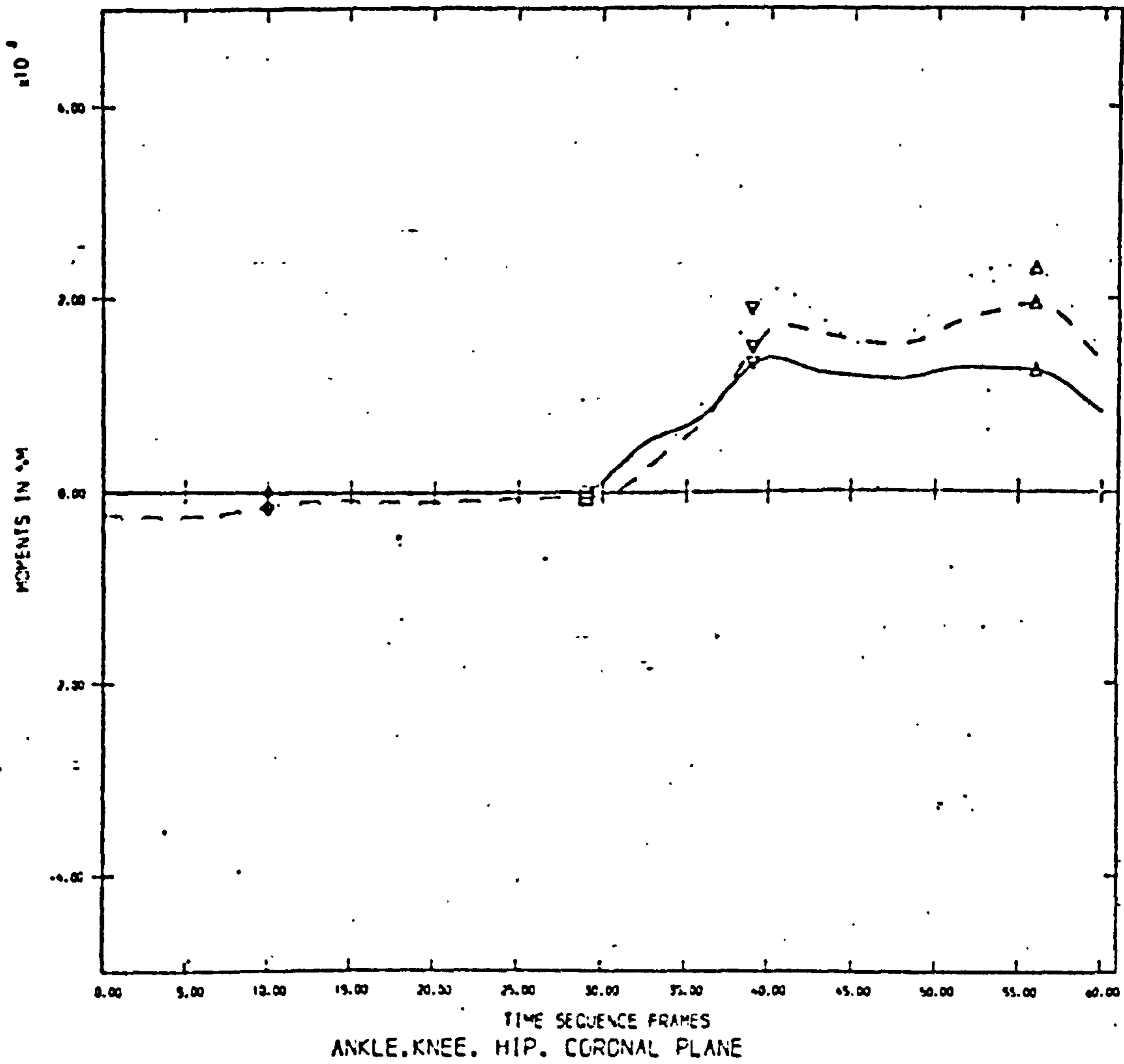
RIGHT HEELSTRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\circ$

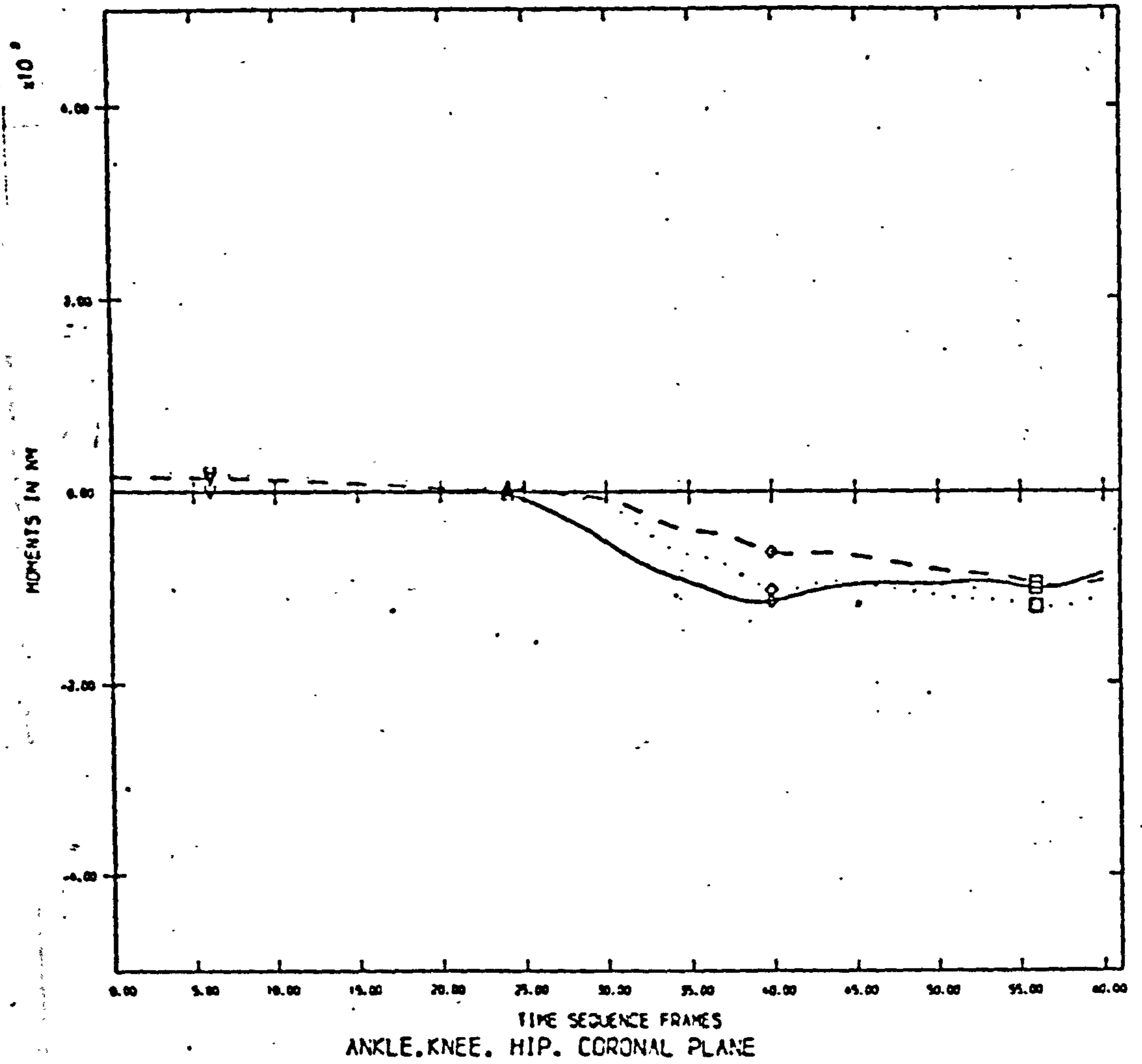


S5/R/FULO



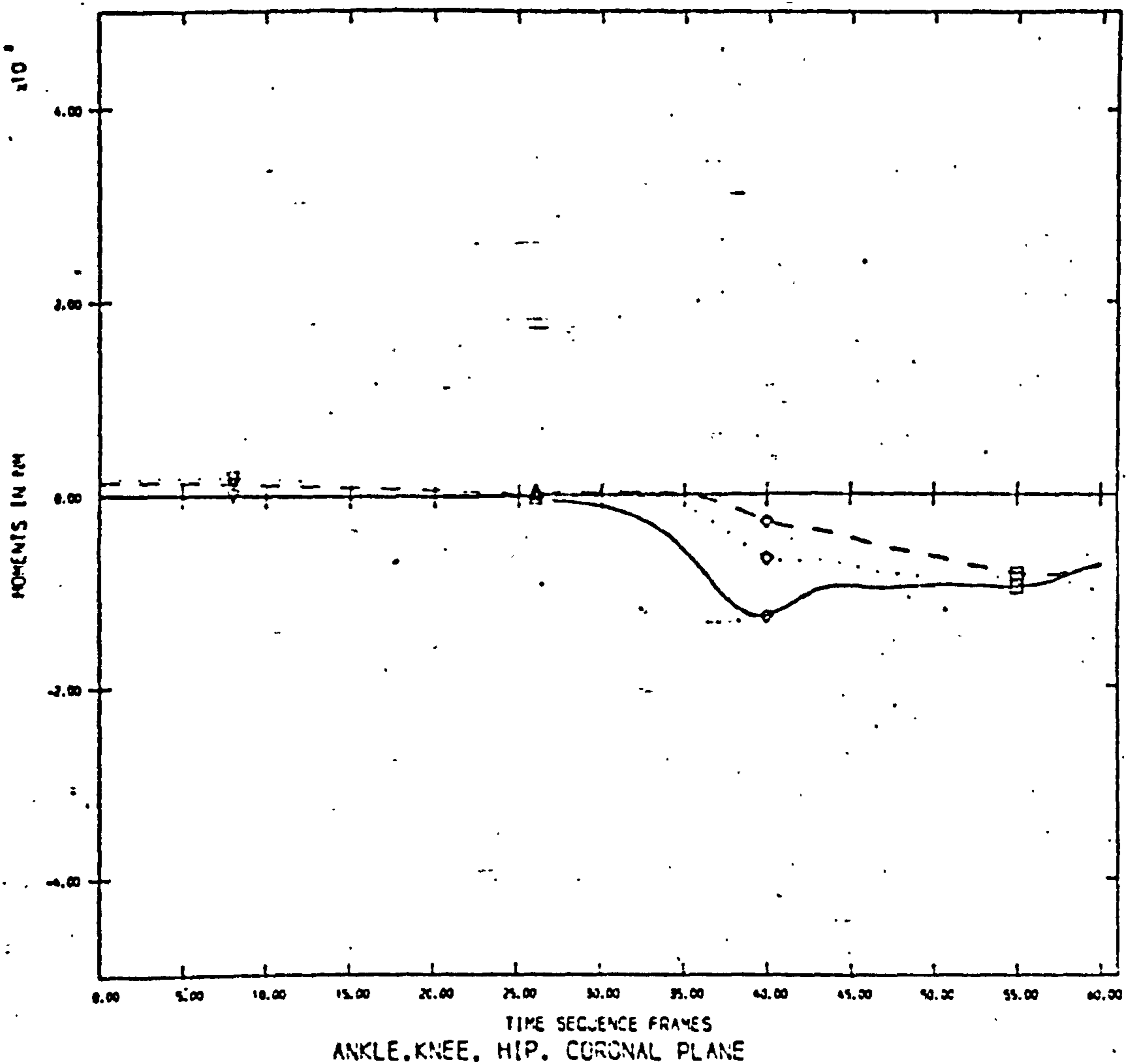
LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

SI/L/BDO



LEFT HEEL STRIKE ▲	CONTINUOUS	ANKLE
LEFT TOE OFF ▼	DASHED	KNEE
RIGHT HEELSTRIKE □	DOTTED	HIP
RIGHT TOE OFF ◇		

S2/L/BDTO



LEFT HEEL STRIKE  $\blacktriangle$

CONTINUOUS ANKLE

LEFT TOE OFF  $\blacktriangledown$

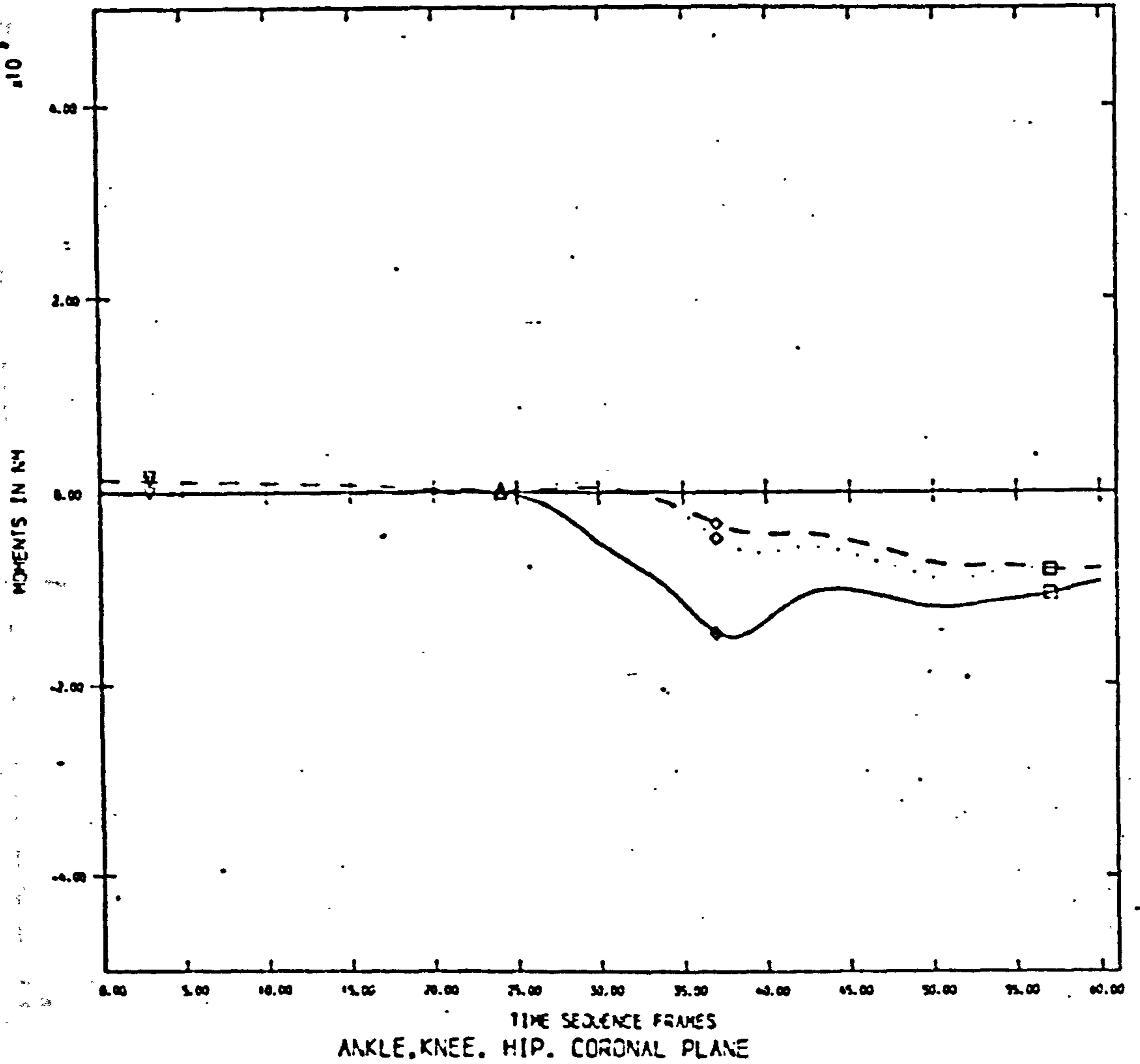
DASHED KNEE

RIGHT HEEL STRIKE  $\square$

DOTTED HIP

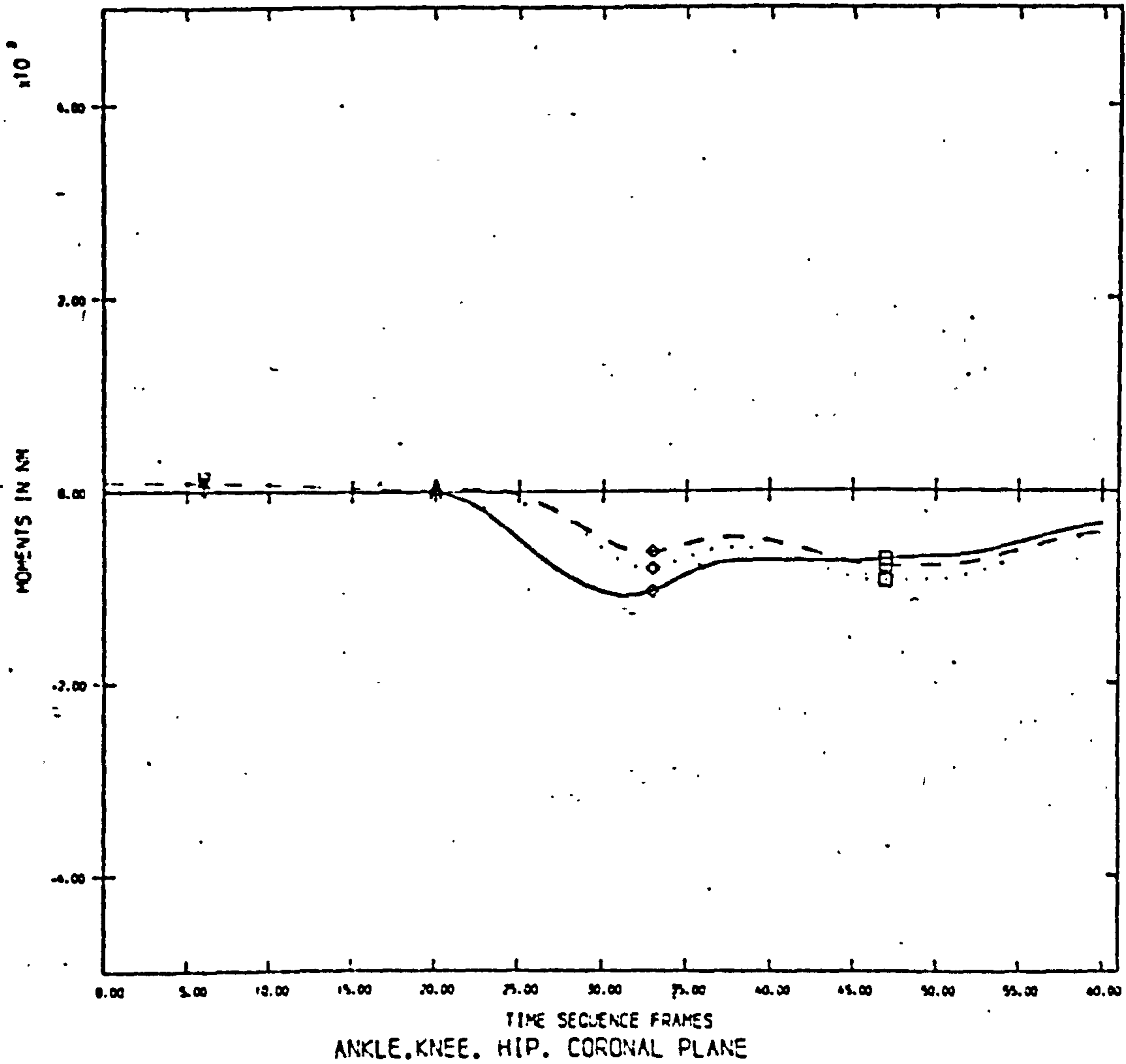
RIGHT TOE OFF  $\diamond$

S3/L/BOTO



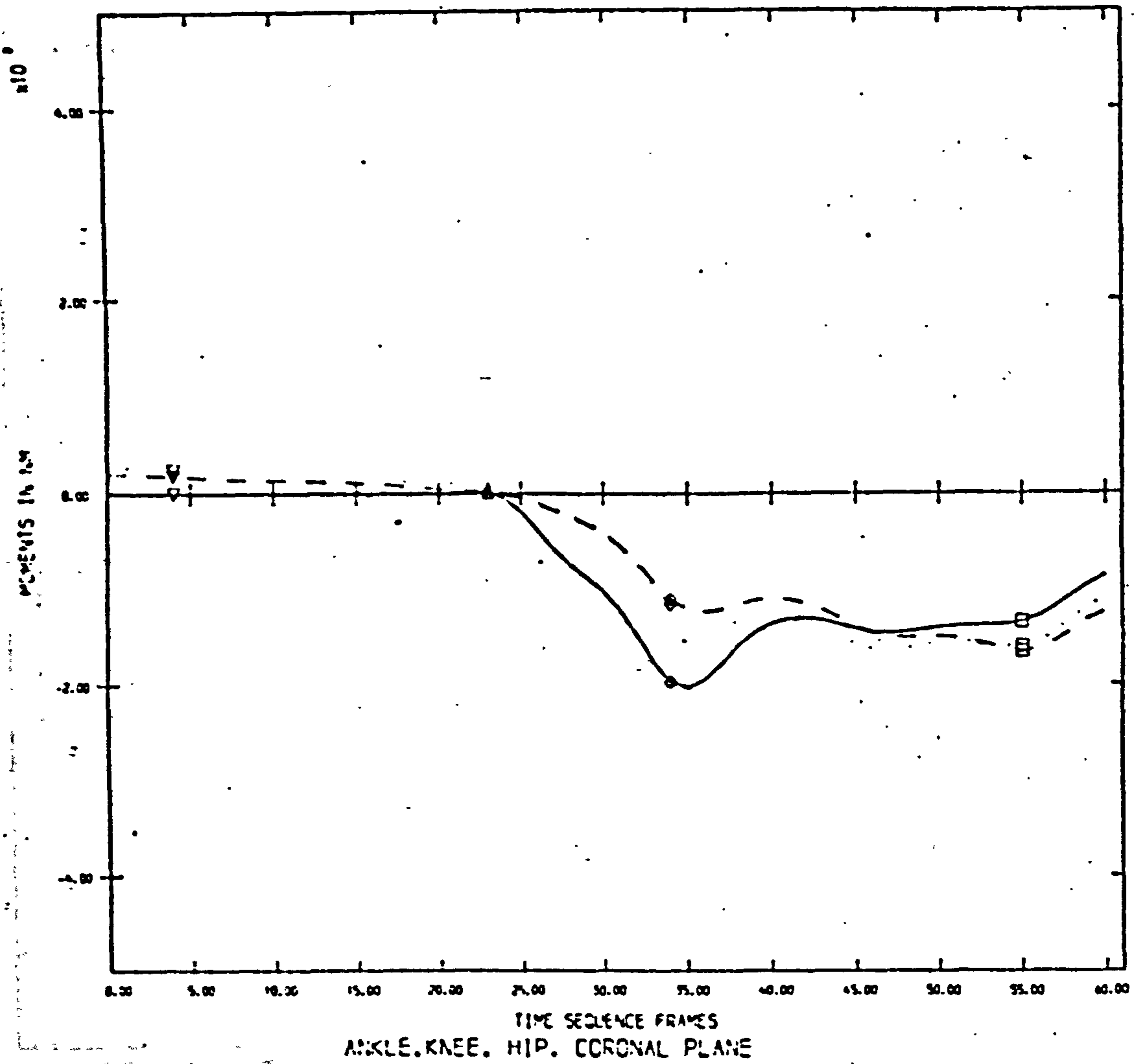
LEFT HEEL STRIKE $\Delta$	CONTINUOUS	ANKLE
LEFT TOE OFF $\nabla$	DASHED	KNEE
RIGHT HEELSTRIKE $\square$	DOTTED	HIP
RIGHT TOE OFF $\circ$		

S4/L/BOTO



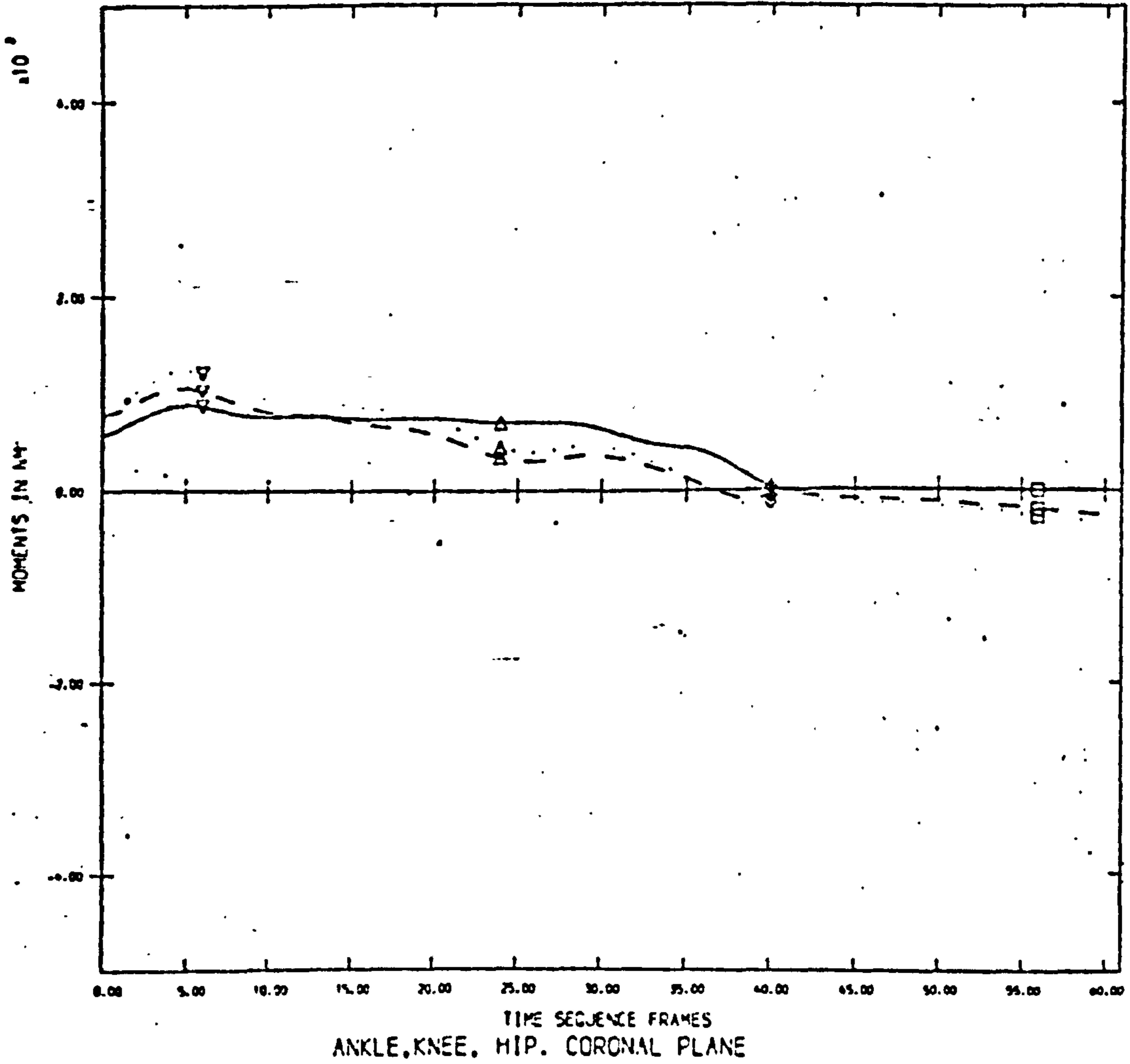
LEFT HEEL STRIKE $\Delta$	CONTINUOUS	ANKLE
LEFT TOE OFF $\nabla$	DASHED	KNEE
RIGHT HEELSTRIKE $\square$	DOTTED	HIP
RIGHT TOE OFF $\diamond$		

S5/L/BDT0



- LEFT HEEL STRIKE  $\Delta$  CONTINUOUS ANKLE
- LEFT TOE OFF  $\nabla$  DASHED KNEE
- RIGHT HEEL STRIKE  $\square$  DOTTED HIP
- RIGHT TOE OFF  $\diamond$

SI/R/BDTO



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

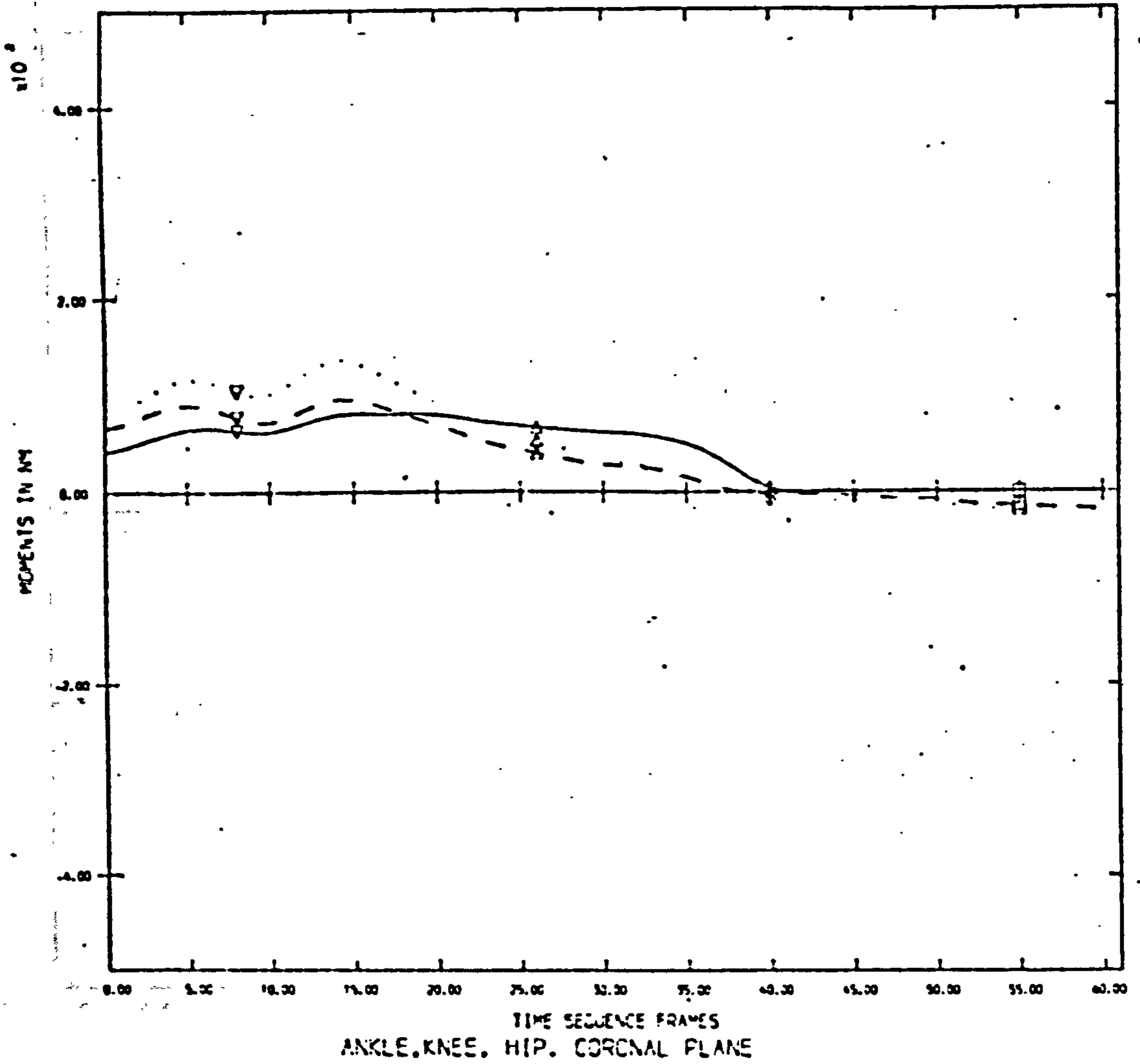
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\diamond$

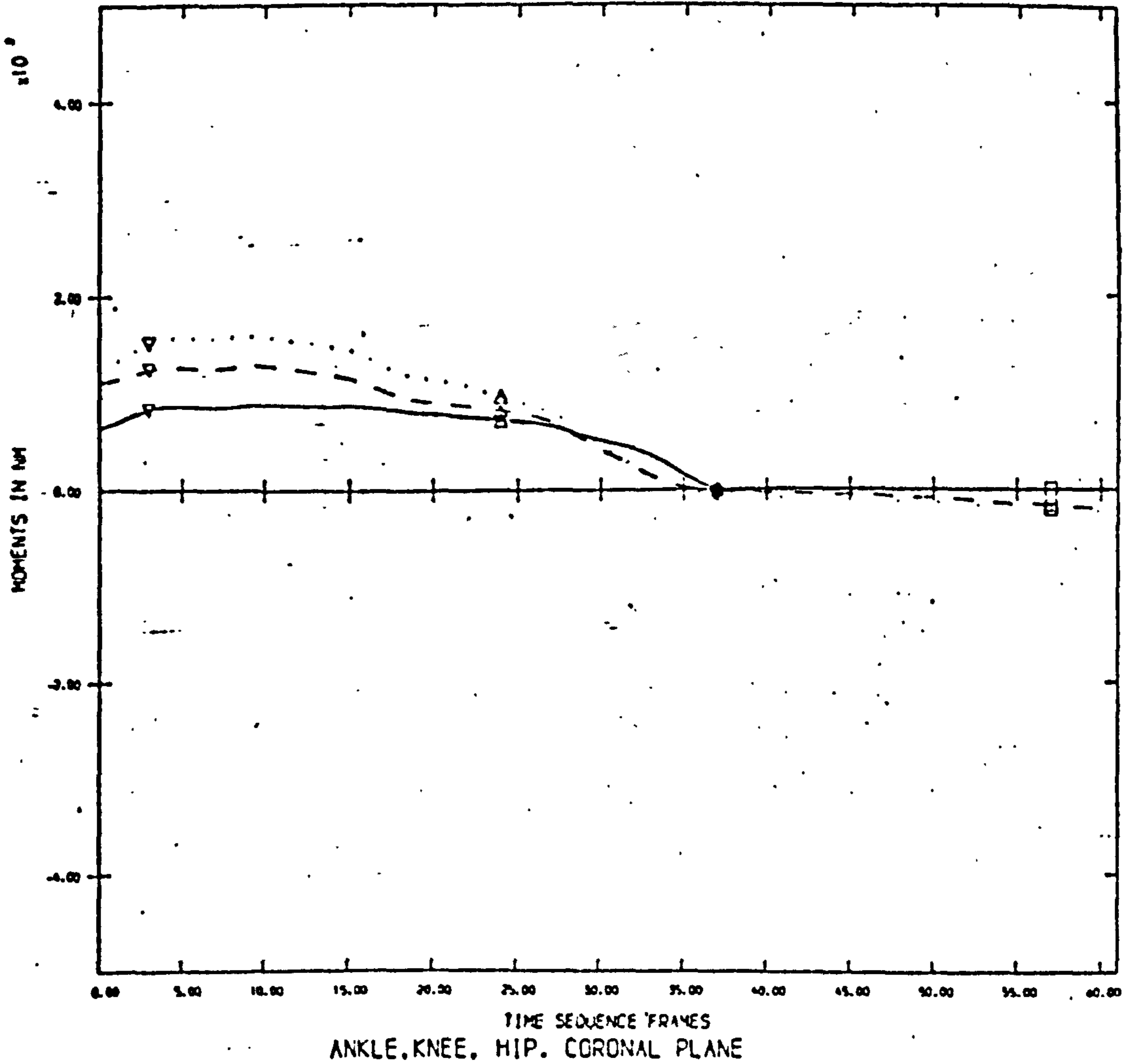
S2/R/BD10



LEFT HEEL STRIKE	Δ	CONTINUOUS	ANKLE
LEFT TOE OFF	▽	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	◇		



S3/R/BDT0



LEFT HEEL STRIKE ▲

CONTINUOUS ANKLE

LEFT TOE OFF ▼

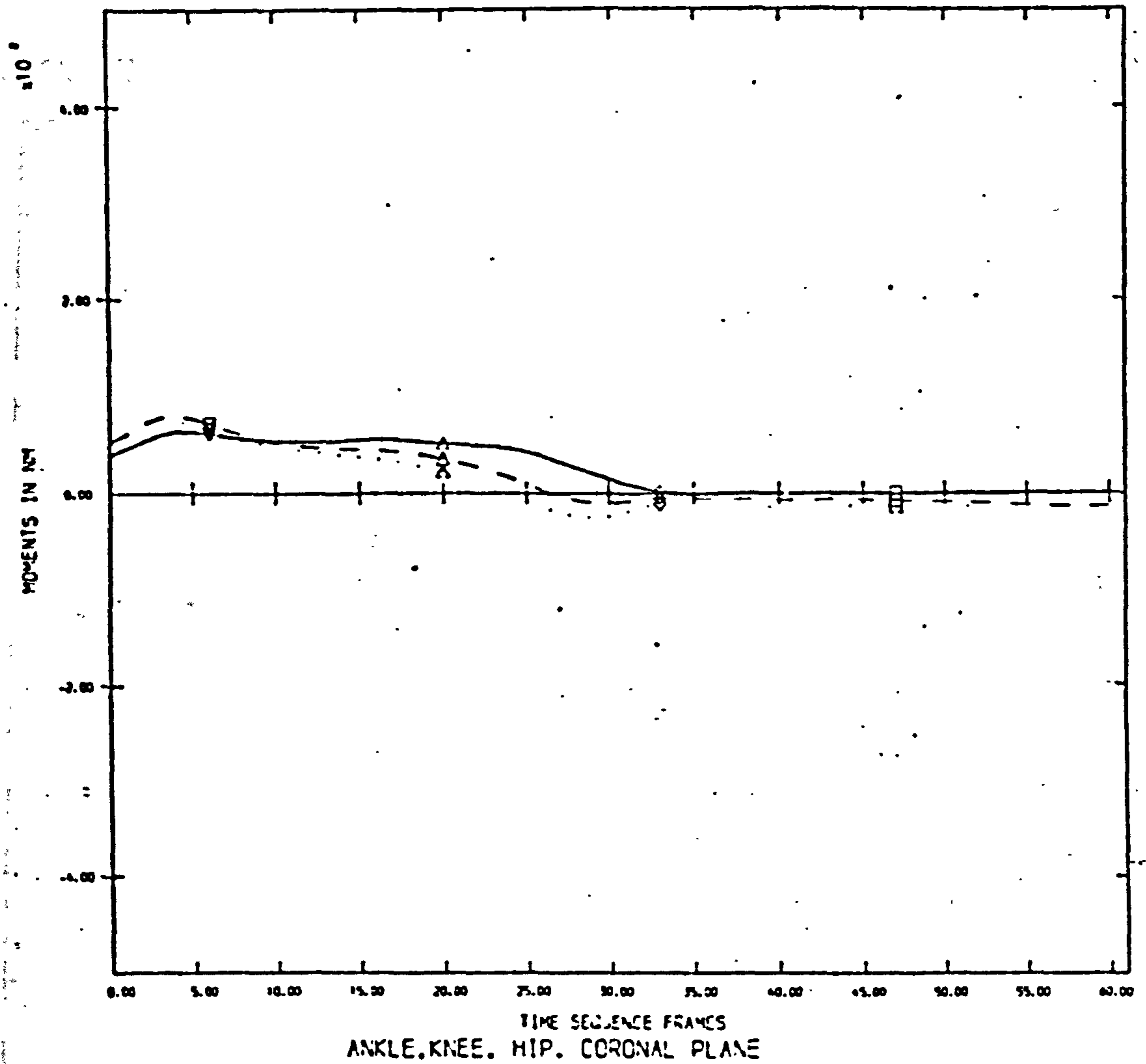
DASHED KNEE

RIGHT HEELSTRIKE □

DOTTED HIP

RIGHT TOE OFF ○

S4/R/BDT0



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

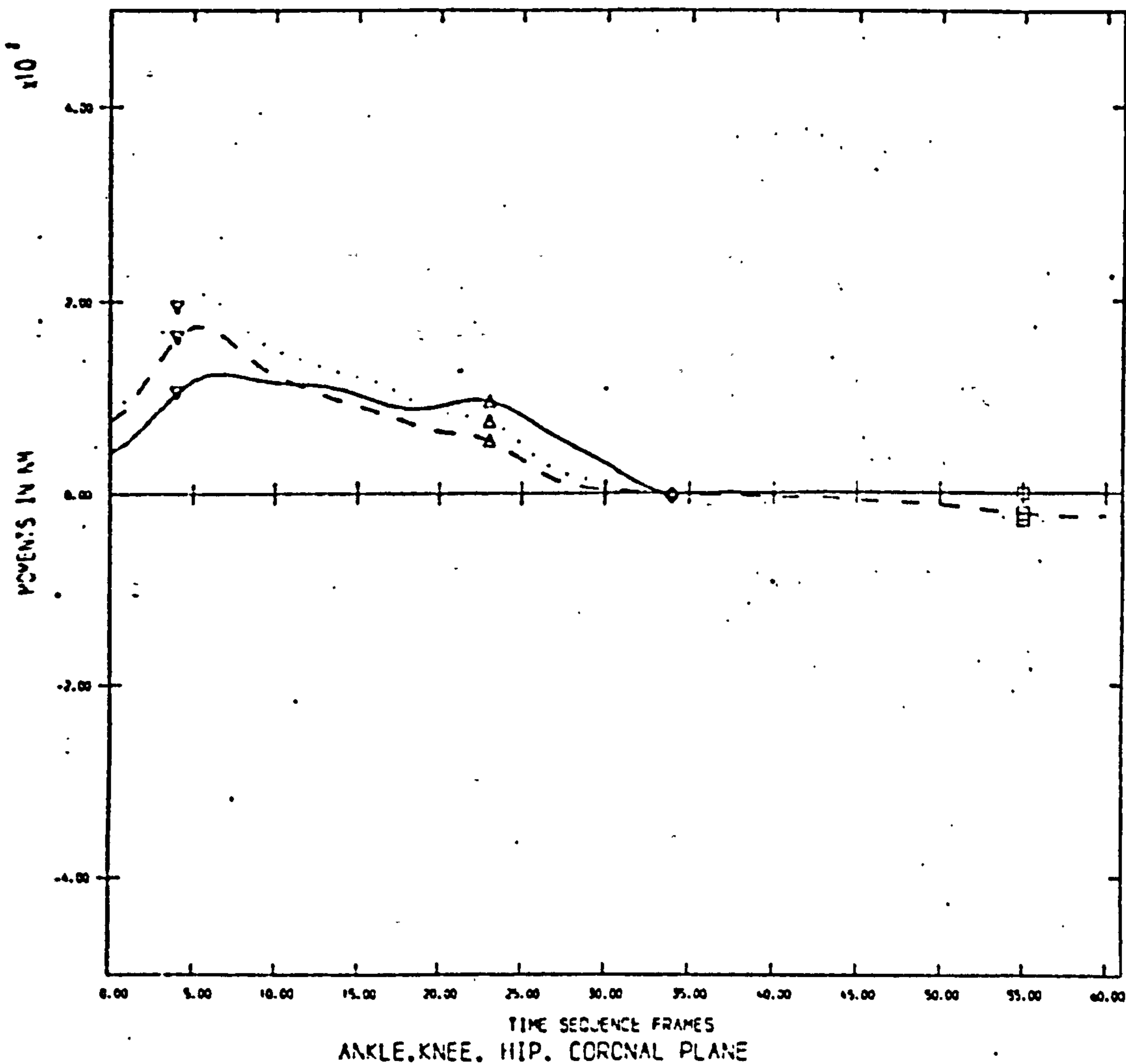
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

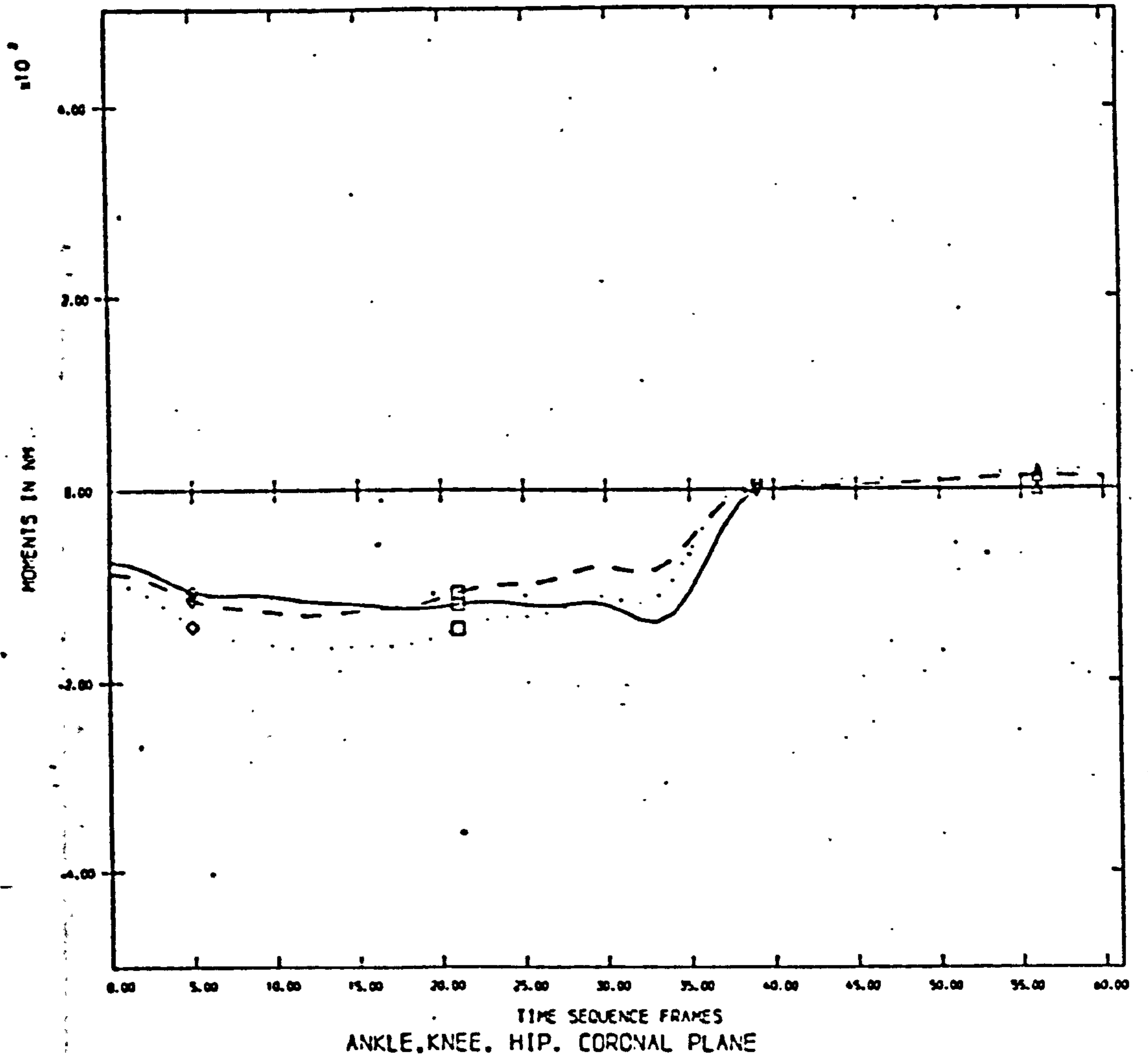
RIGHT TOE OFF  $\diamond$

S5/R/BOTO



- LEFT HEEL STRIKE  $\Delta$  CONTINUOUS ANKLE
- LEFT TOE OFF  $\nabla$  DASHED KNEE
- RIGHT HEELSTRIKE  $\square$  DOTTED HIP
- RIGHT TOE OFF  $\diamond$

SI/L/FUL1



LEFT HEEL STRIKE  $\Delta$

LEFT TOE OFF  $\nabla$

RIGHT HEELSTRIKE  $\square$

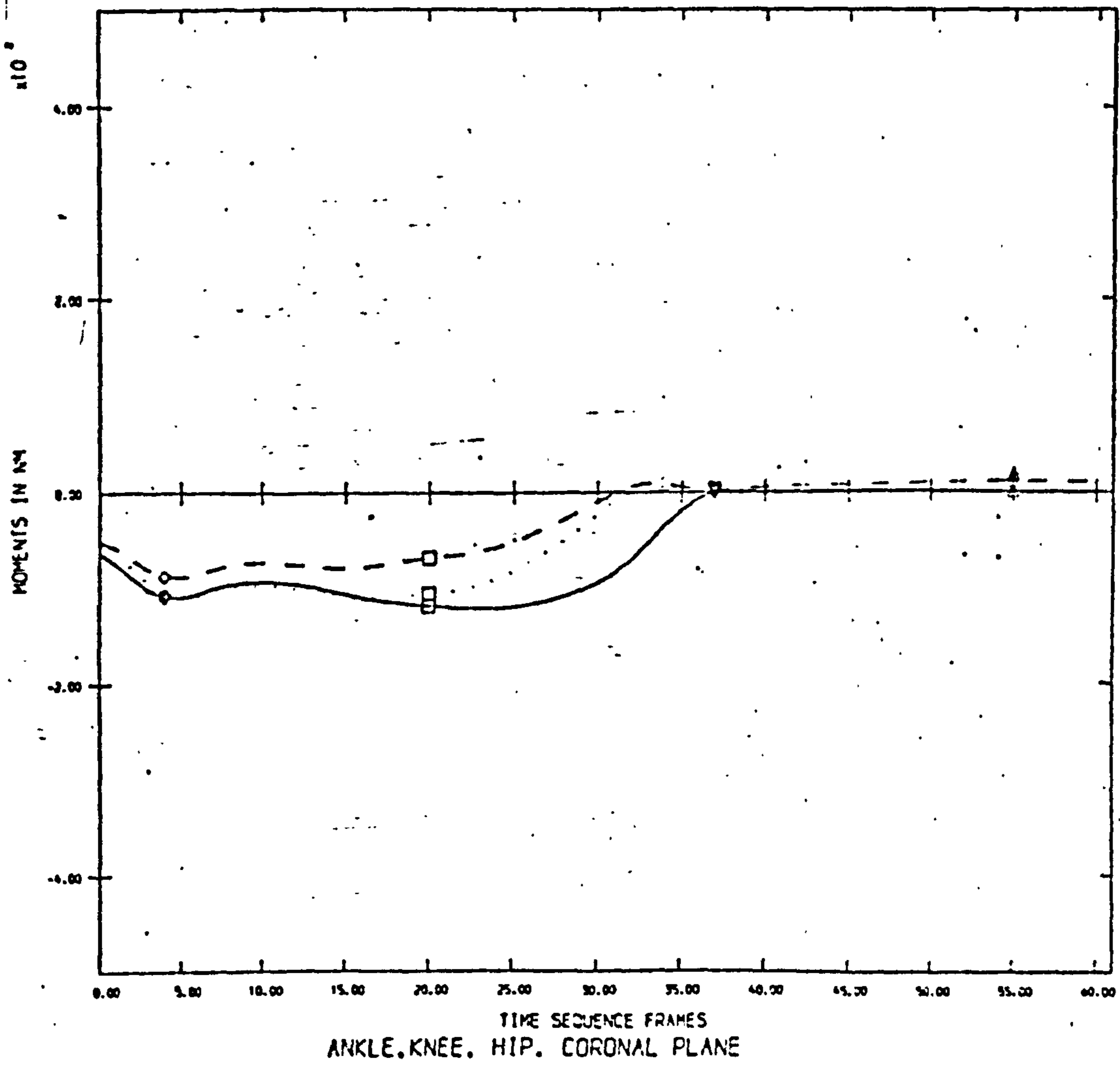
RIGHT TOE OFF  $\diamond$

CONTINUOUS ANKLE

DASHED KNEE

DOTTED HIP

S2/L/FUL1



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

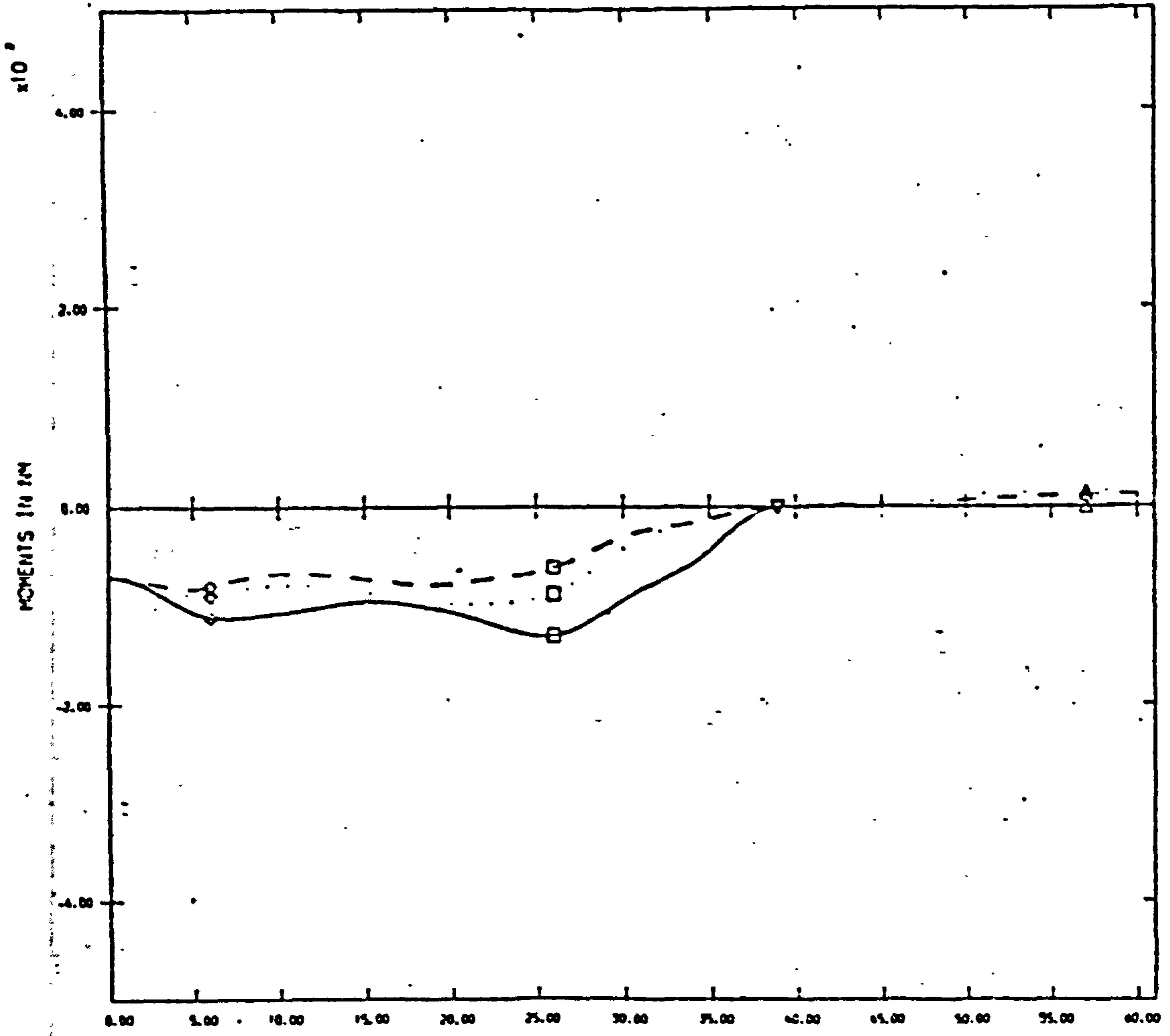
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\diamond$

S3/L/FUL1



TIME SEQUENCE FRAMES  
ANKLE, KNEE, HIP, CORONAL PLANE

LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

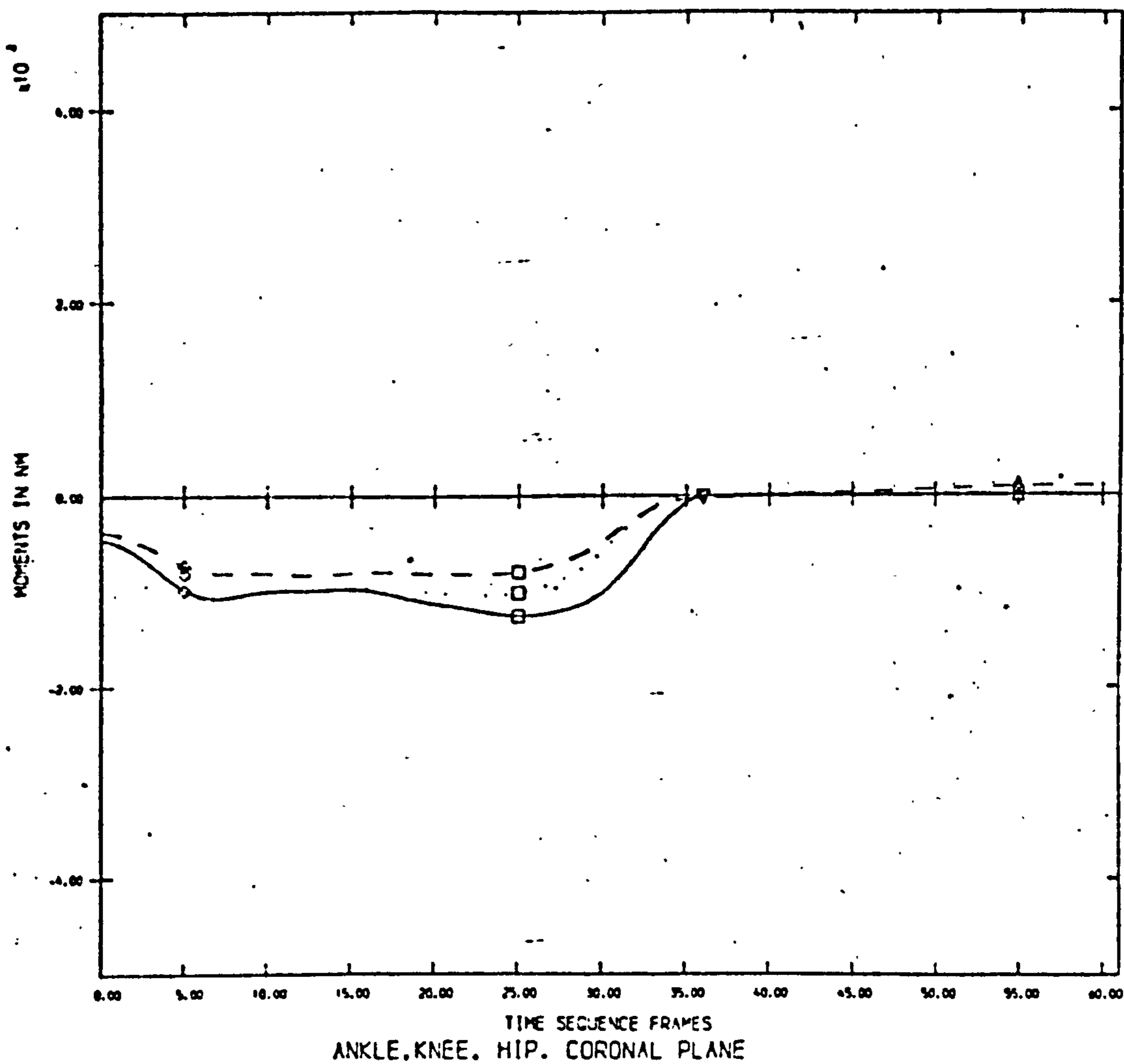
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

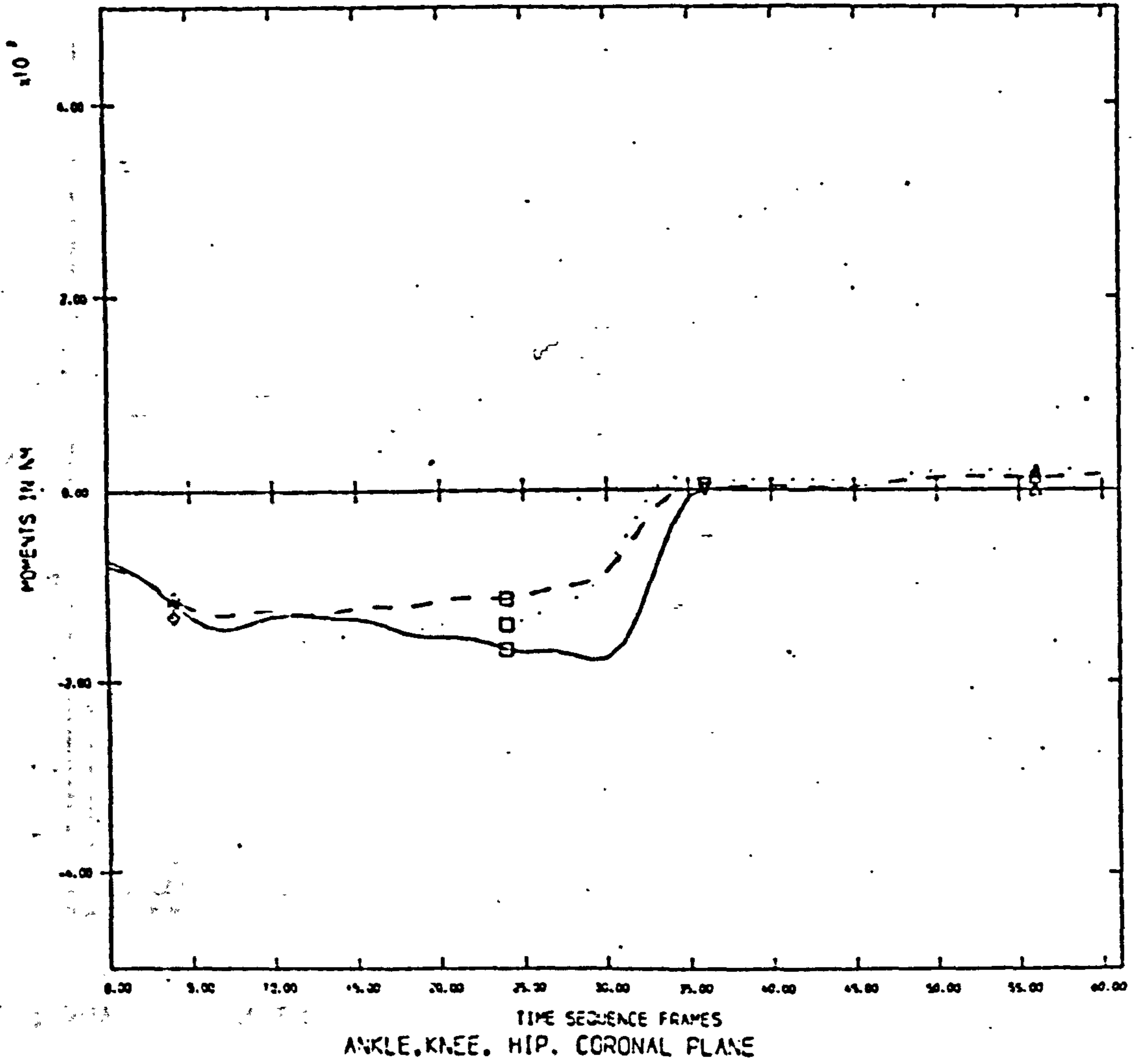
RIGHT TOE OFF  $\diamond$

S4/L/FUL1



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	▢	DOTTED	HIP
RIGHT TOE OFF	◇		

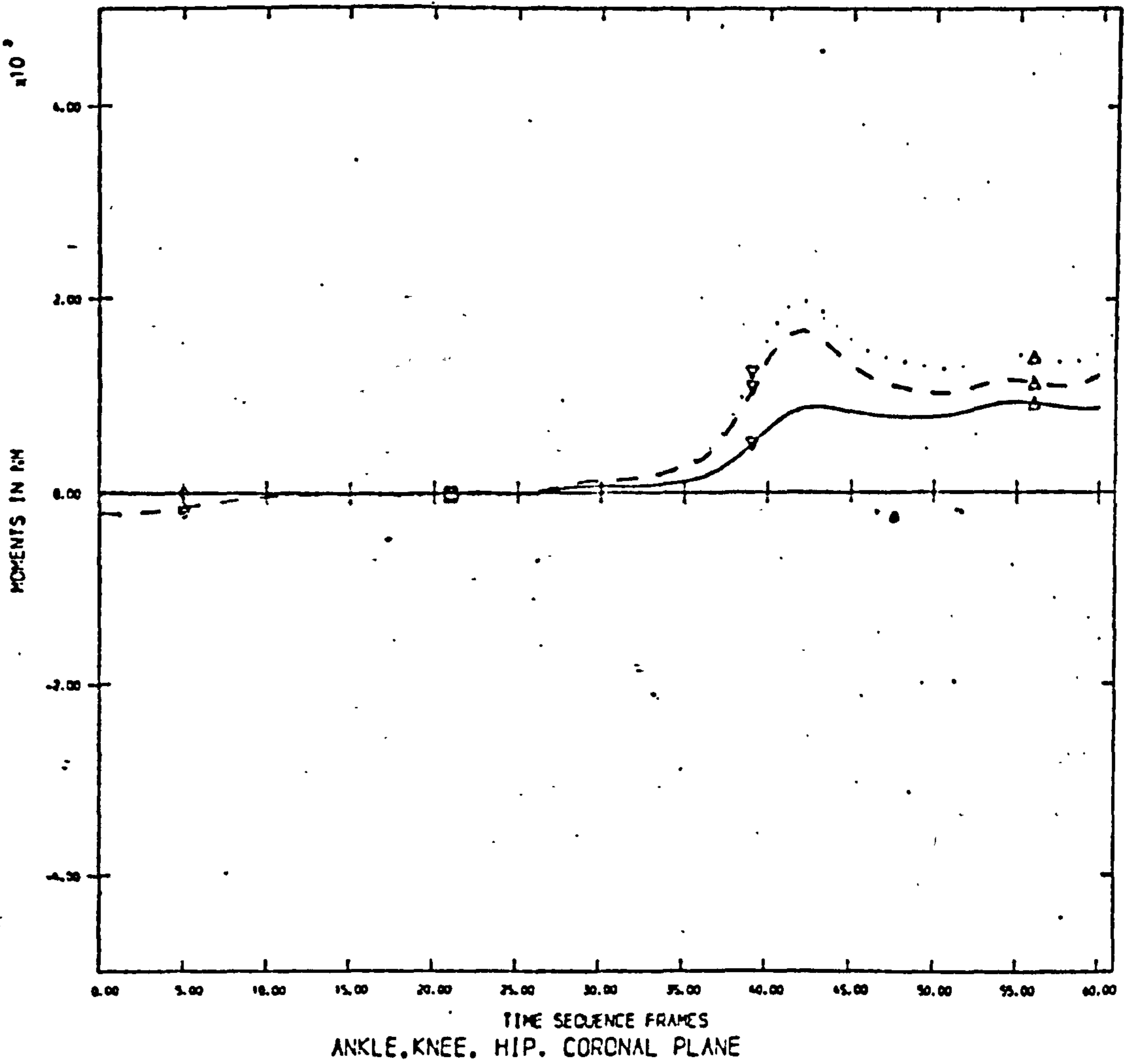
SS/L/FUL1



▲ LEFT HEEL STRIKE	CONTINUOUS	ANKLE
▼ LEFT TOE OFF	DASHED	KNEE
□ RIGHT HEEL STRIKE	DOTTED	HIP
◇ RIGHT TOE OFF		



S1/R/FUL1



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

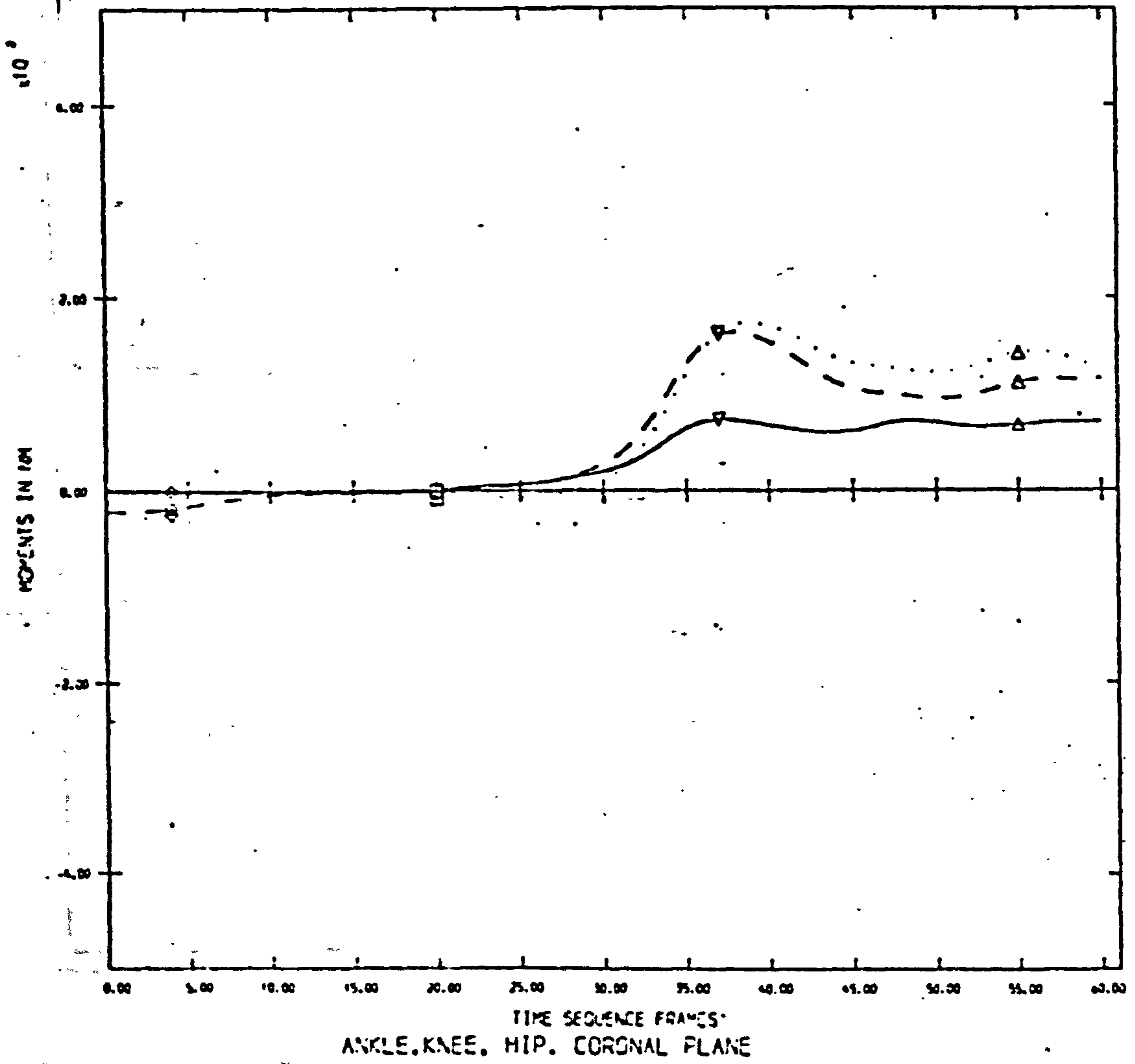
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\diamond$

S2/R/FUL1



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

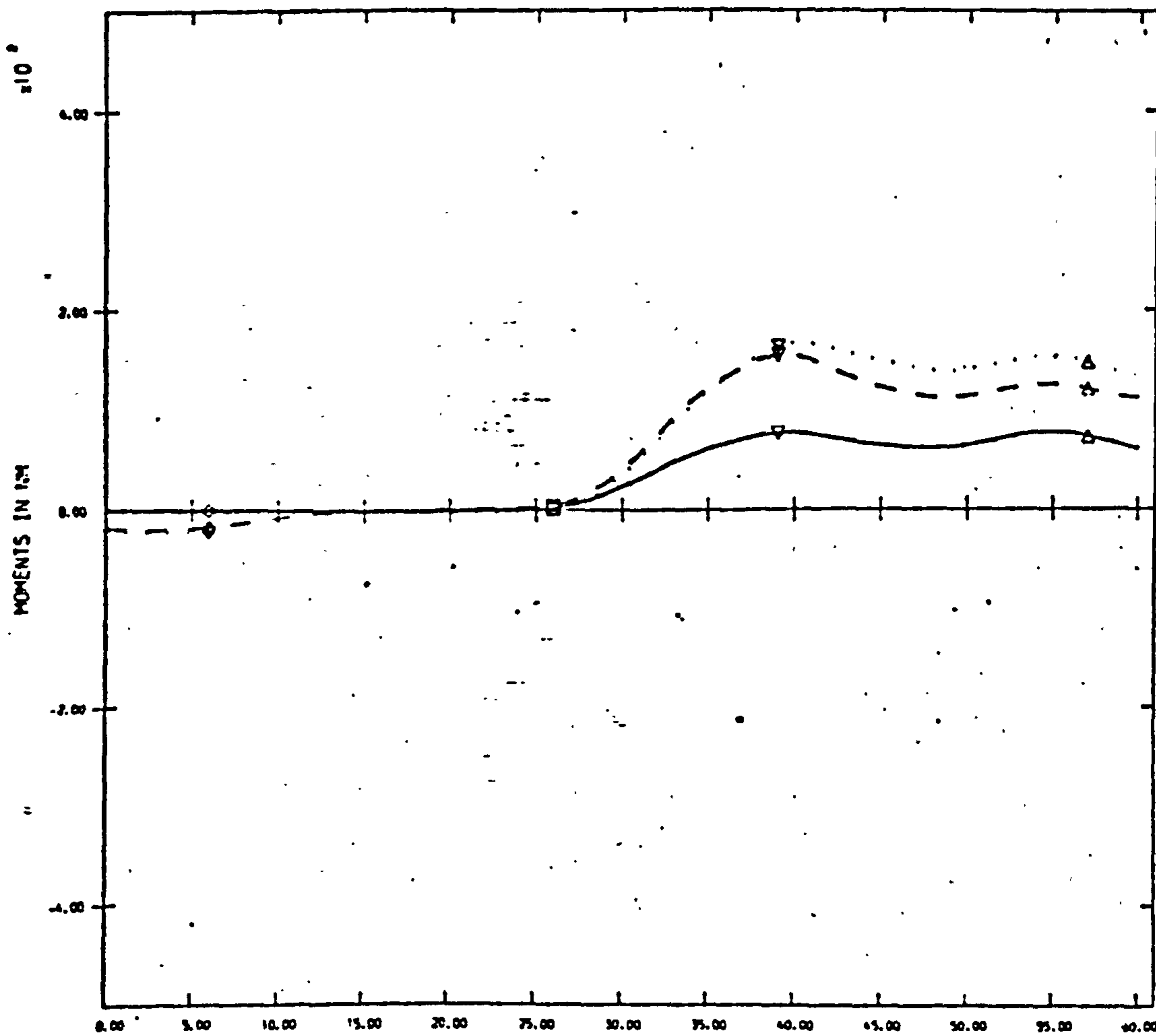
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

RIGHT TOE OFF  $\circ$

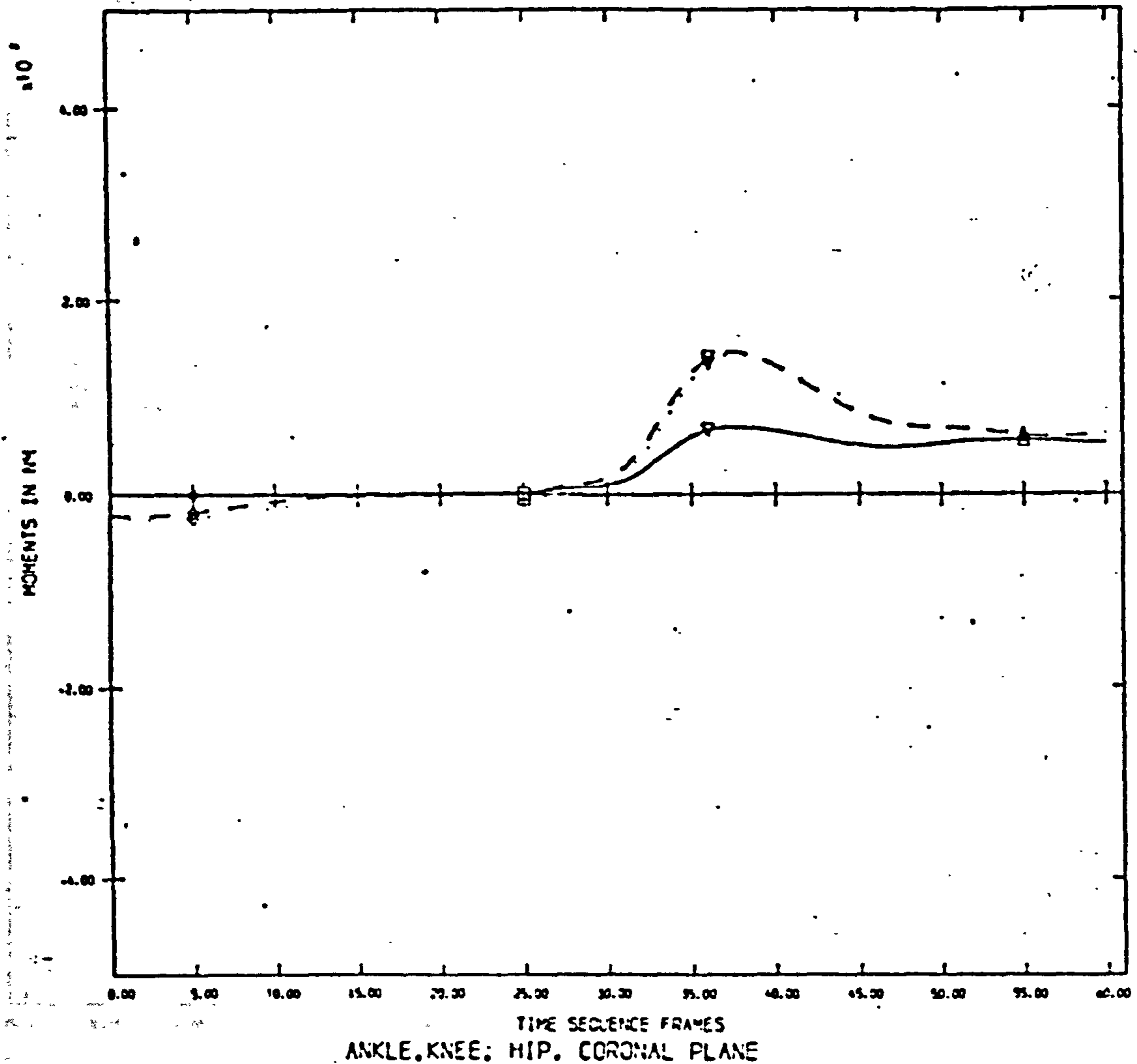
S3/R/FUL1



TIME SEQUENCE FRAMES  
ANKLE, KNEE, HIP, CORONAL PLANE

LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	□	DOTTED	HIP
RIGHT TOE OFF	◇		

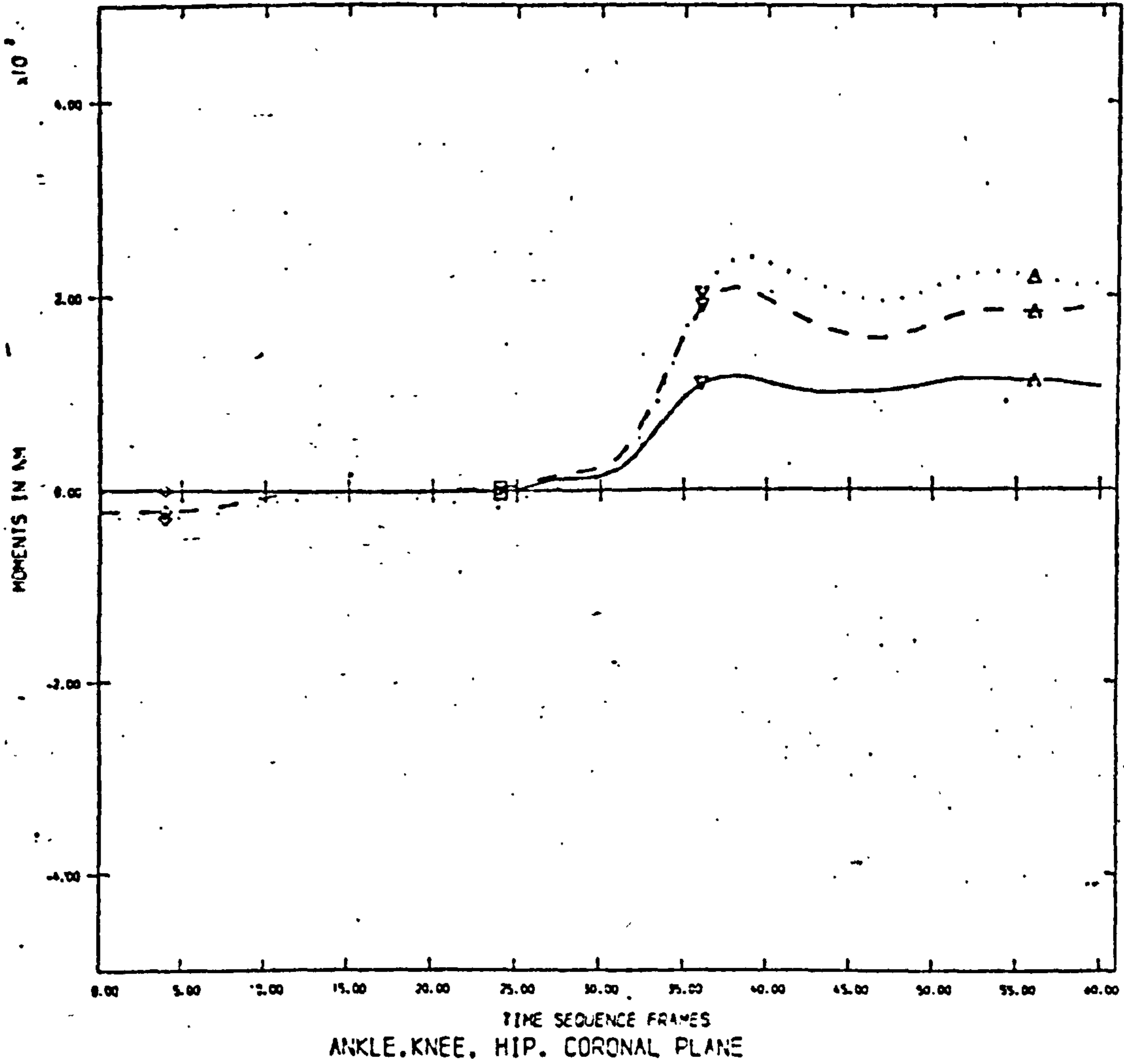
S4/R/FUL1



ANKLE, KNEE; HIP, CORONAL PLANE

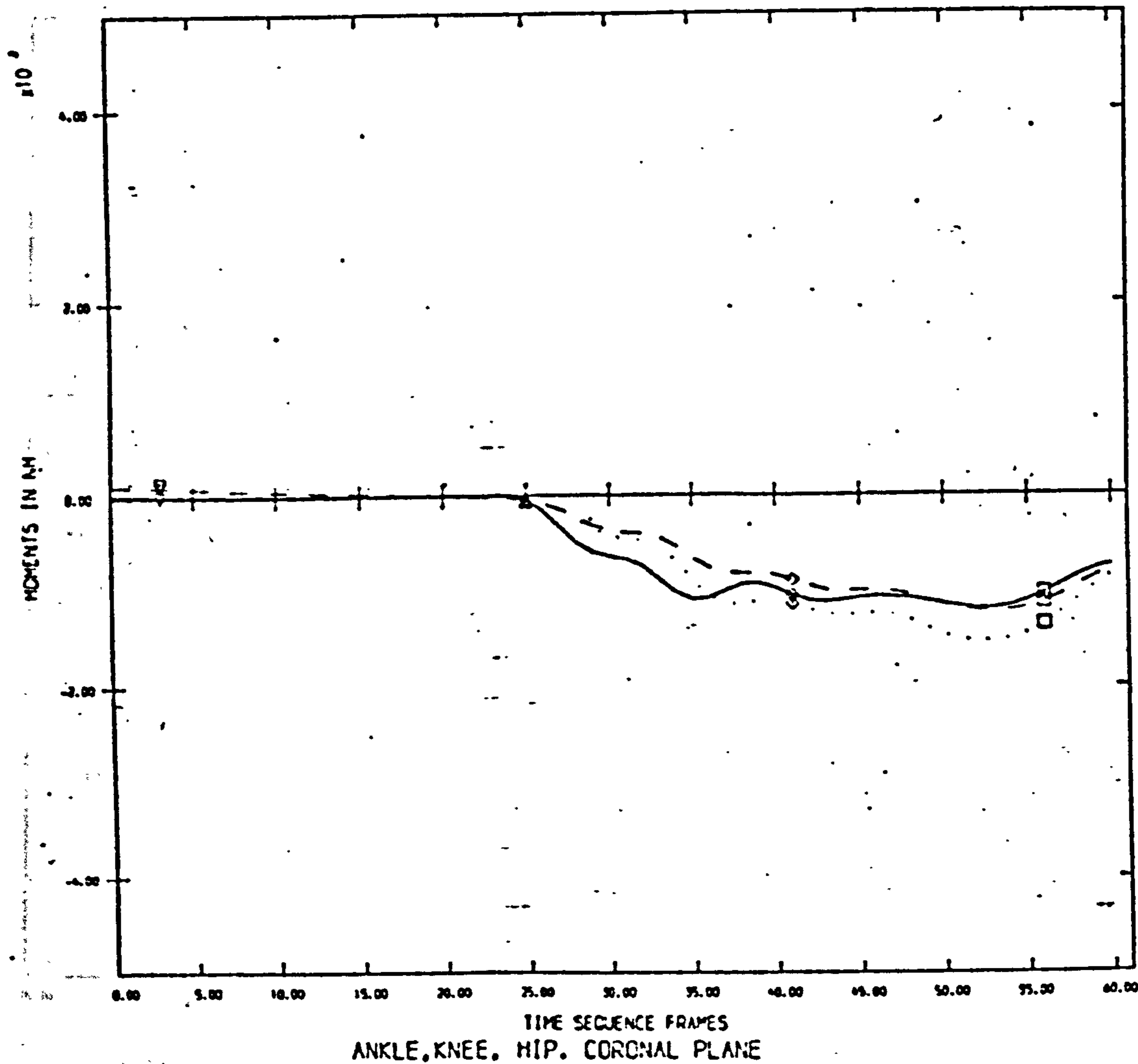
- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▼ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | ◻ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ◊ |            |       |

S5/R/FUL1



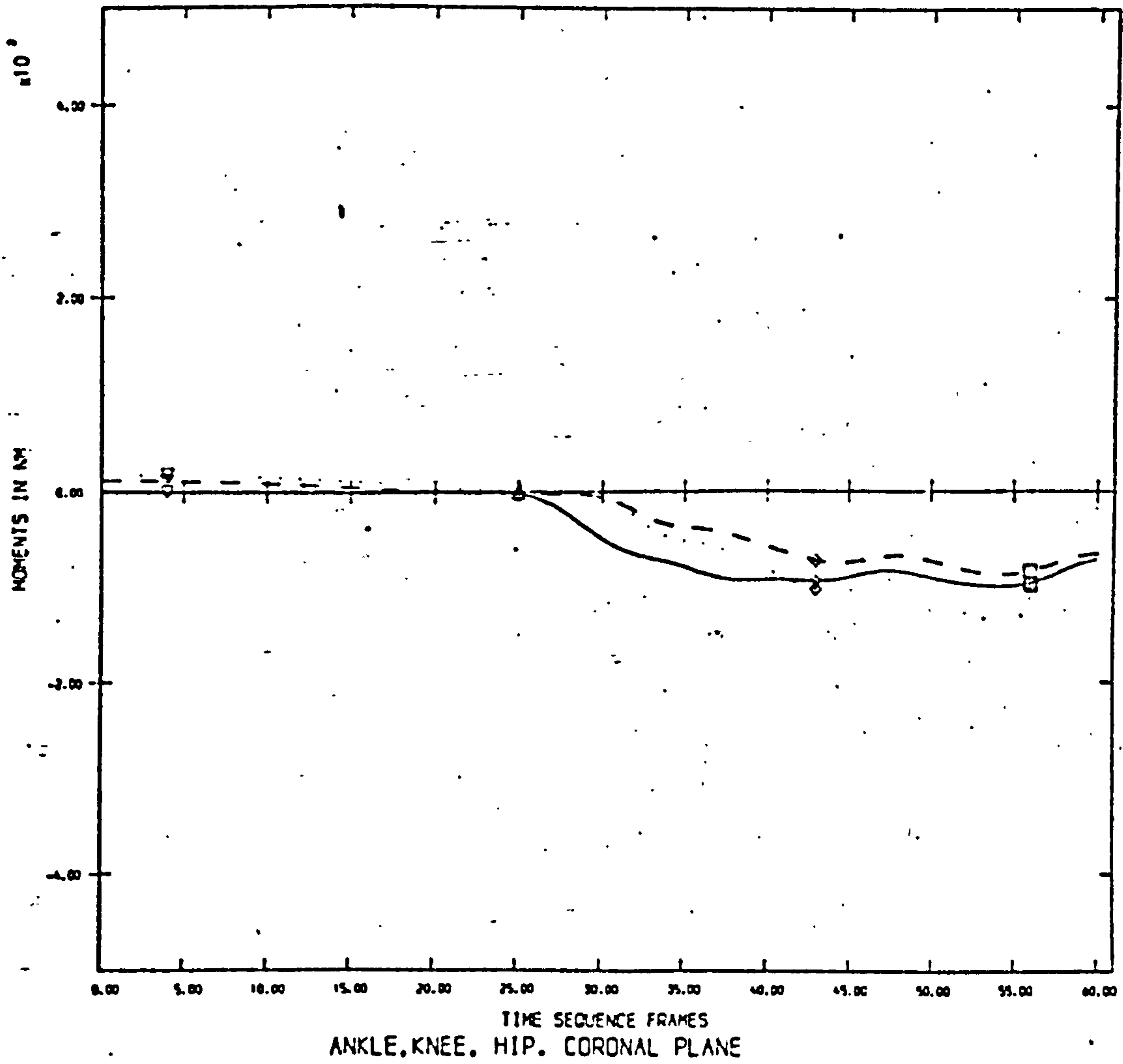
LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

S1/L/BOT1

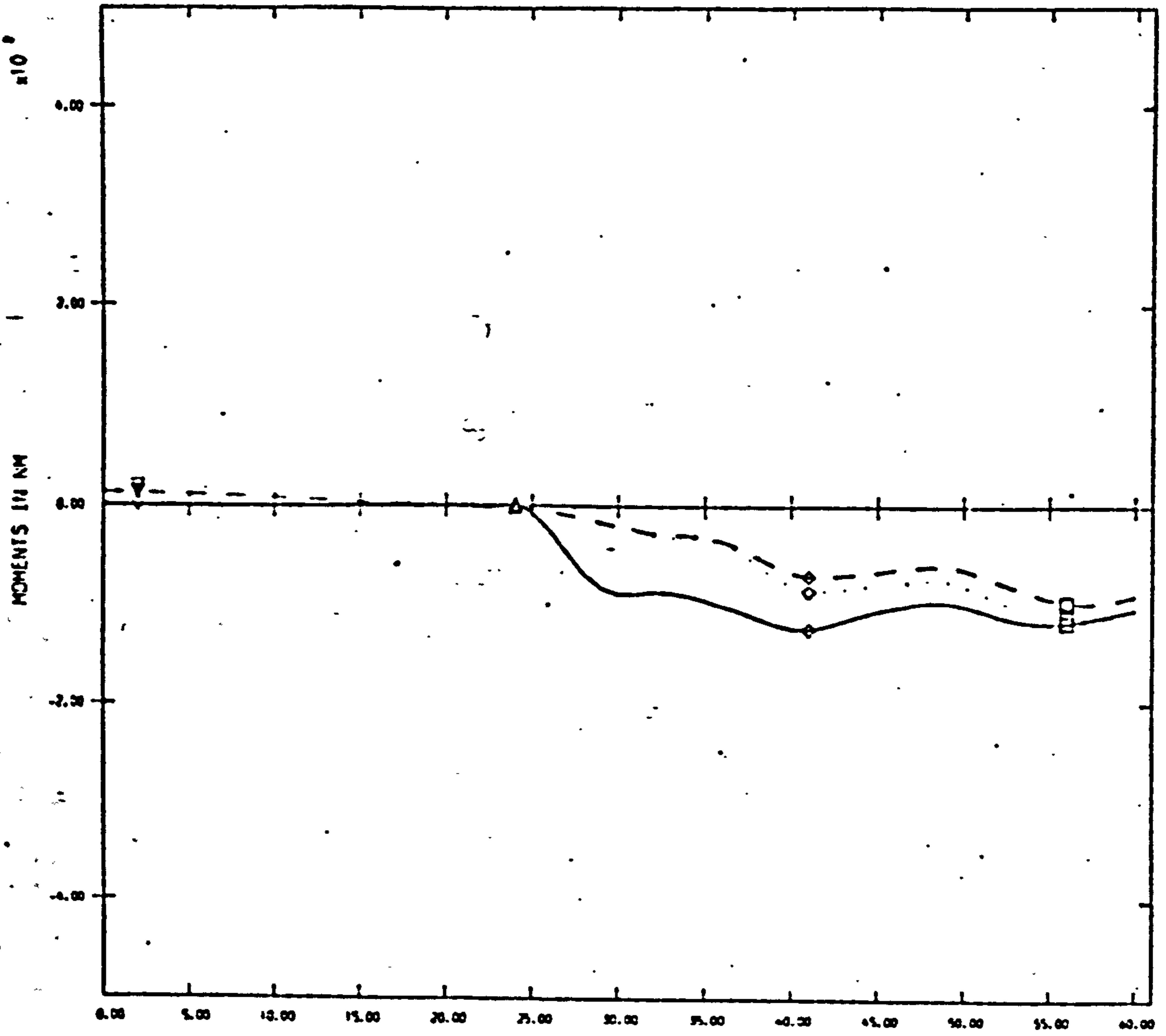


- LEFT HEEL STRIKE  $\Delta$  CONTINUOUS ANKLE
- LEFT TOE OFF  $\nabla$  DASHED KNEE
- RIGHT HEELSTRIKE  $\square$  DOTTED HIP
- RIGHT TOE OFF  $\diamond$

S2/L/BDT1



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

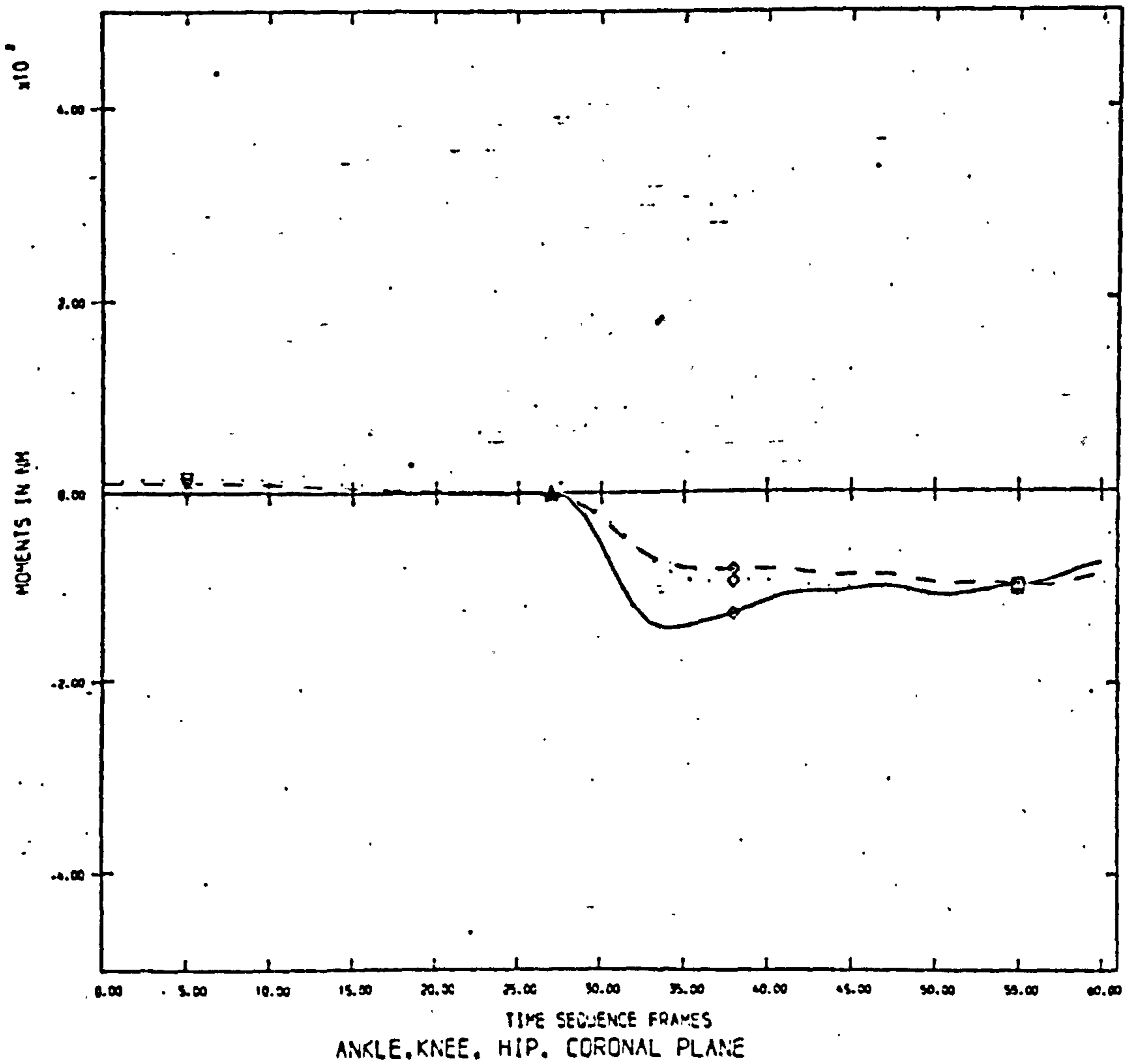


TIME SEQUENCE FRAMES  
ANKLE, KNEE, HIP, CORONAL PLANE

- |                  |   |            |       |
|------------------|---|------------|-------|
| LEFT HEEL STRIKE | ▲ | CONTINUOUS | ANKLE |
| LEFT TOE OFF     | ▼ | DASHED     | KNEE  |
| RIGHT HEELSTRIKE | □ | DOTTED     | HIP   |
| RIGHT TOE OFF    | ◊ |            |       |

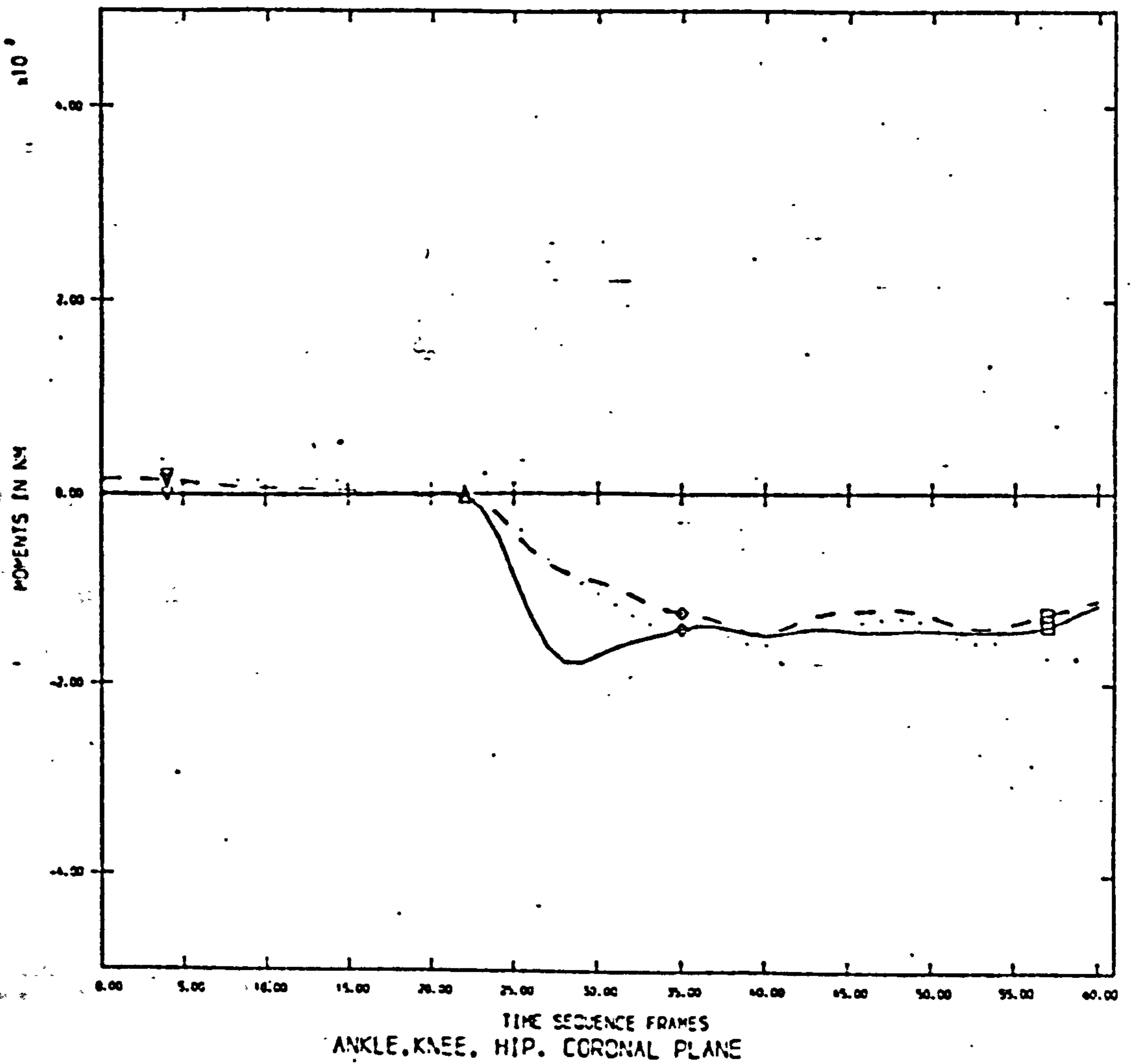


S4/L/BOT1



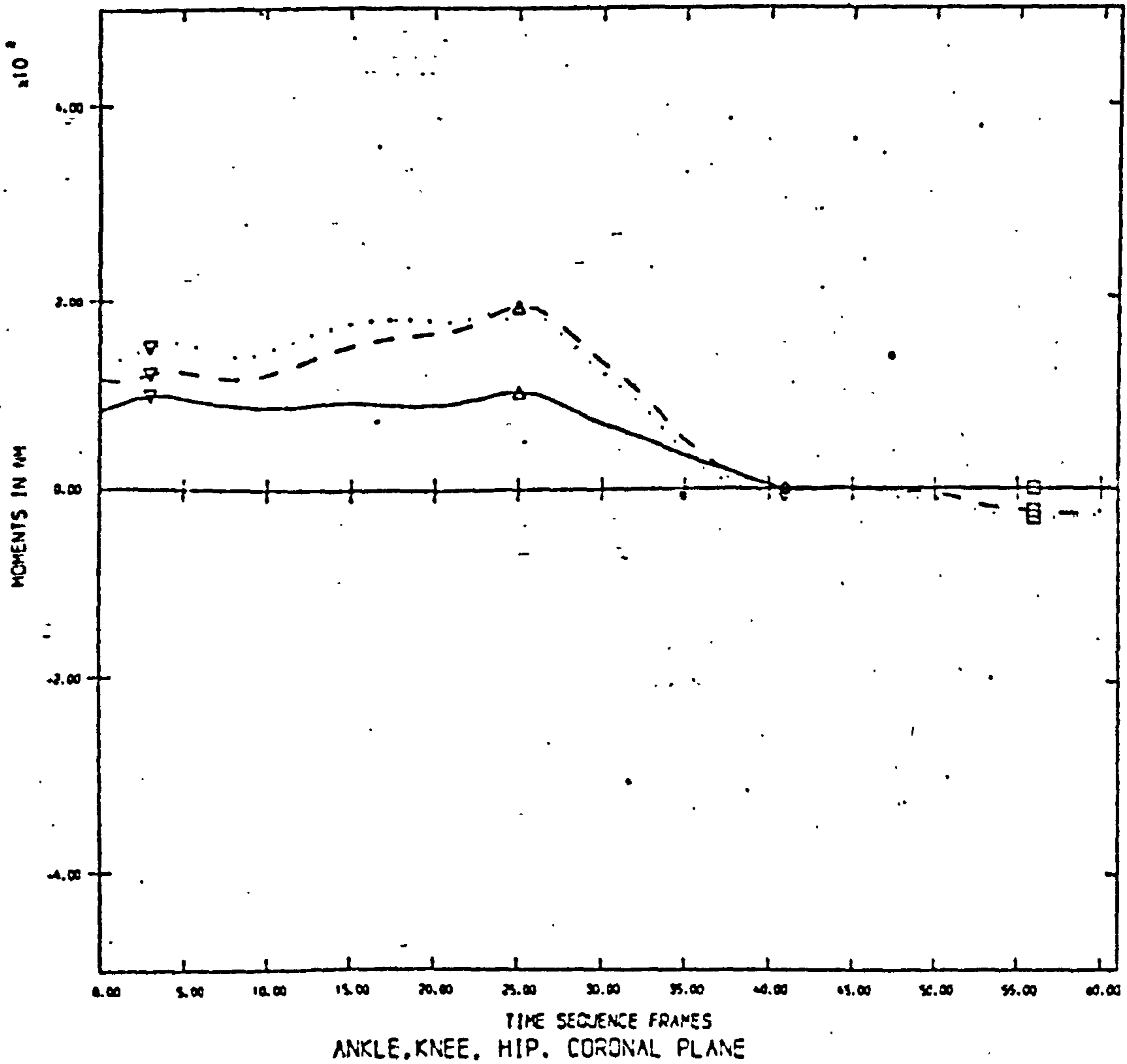
LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

S5/L/80T1



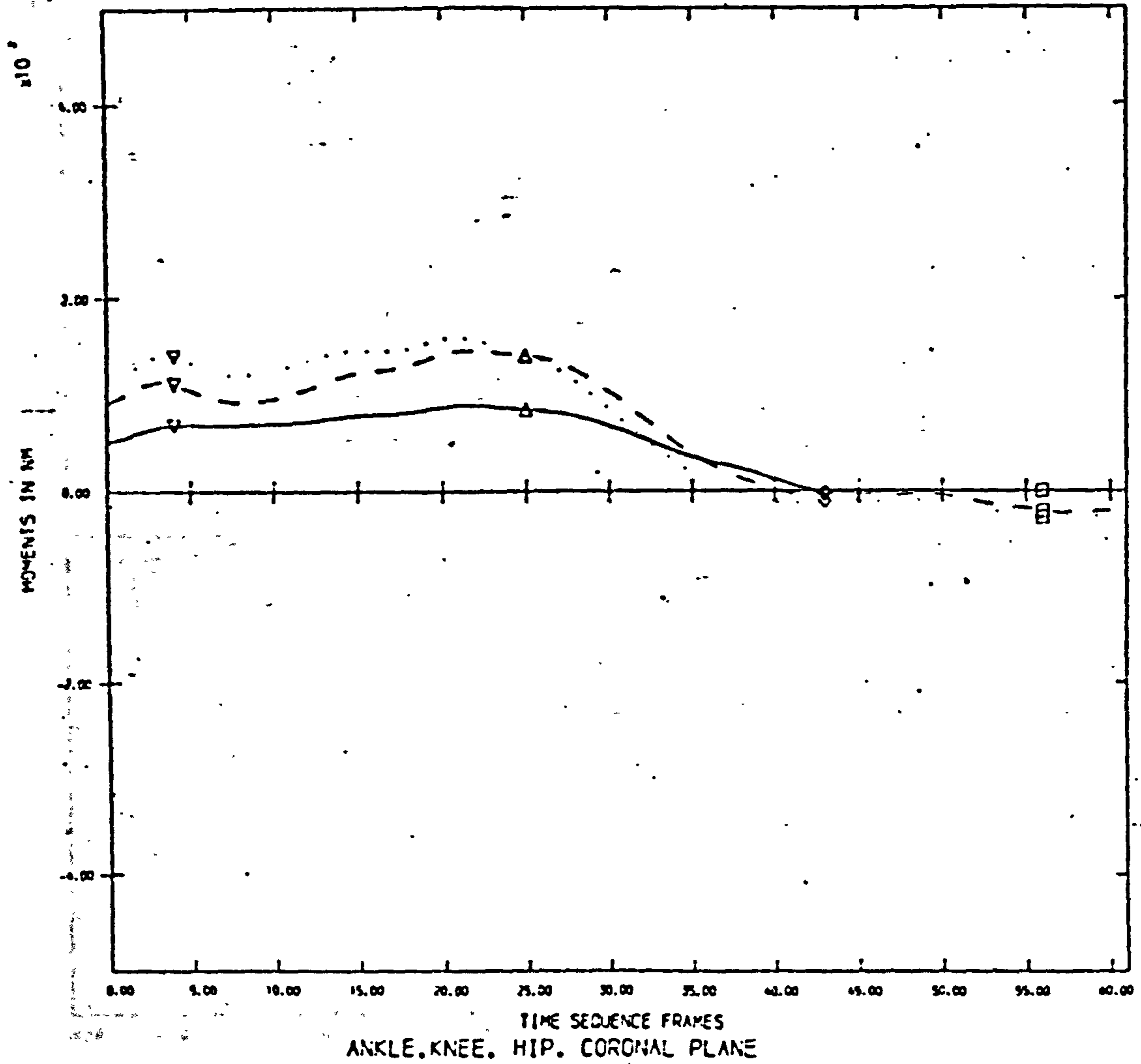
LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEEL STRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

S1/R/BDT1



- LEFT HEEL STRIKE  $\Delta$  CONTINUOUS ANKLE
- LEFT TOE OFF  $\nabla$  DASHED KNEE
- RIGHT HEELSTRIKE  $\square$  DOTTED HIP
- RIGHT TOE OFF  $\diamond$

S2/R/BOT1



LEFT HEEL STRIKE  $\Delta$

CONTINUOUS ANKLE

LEFT TOE OFF  $\nabla$

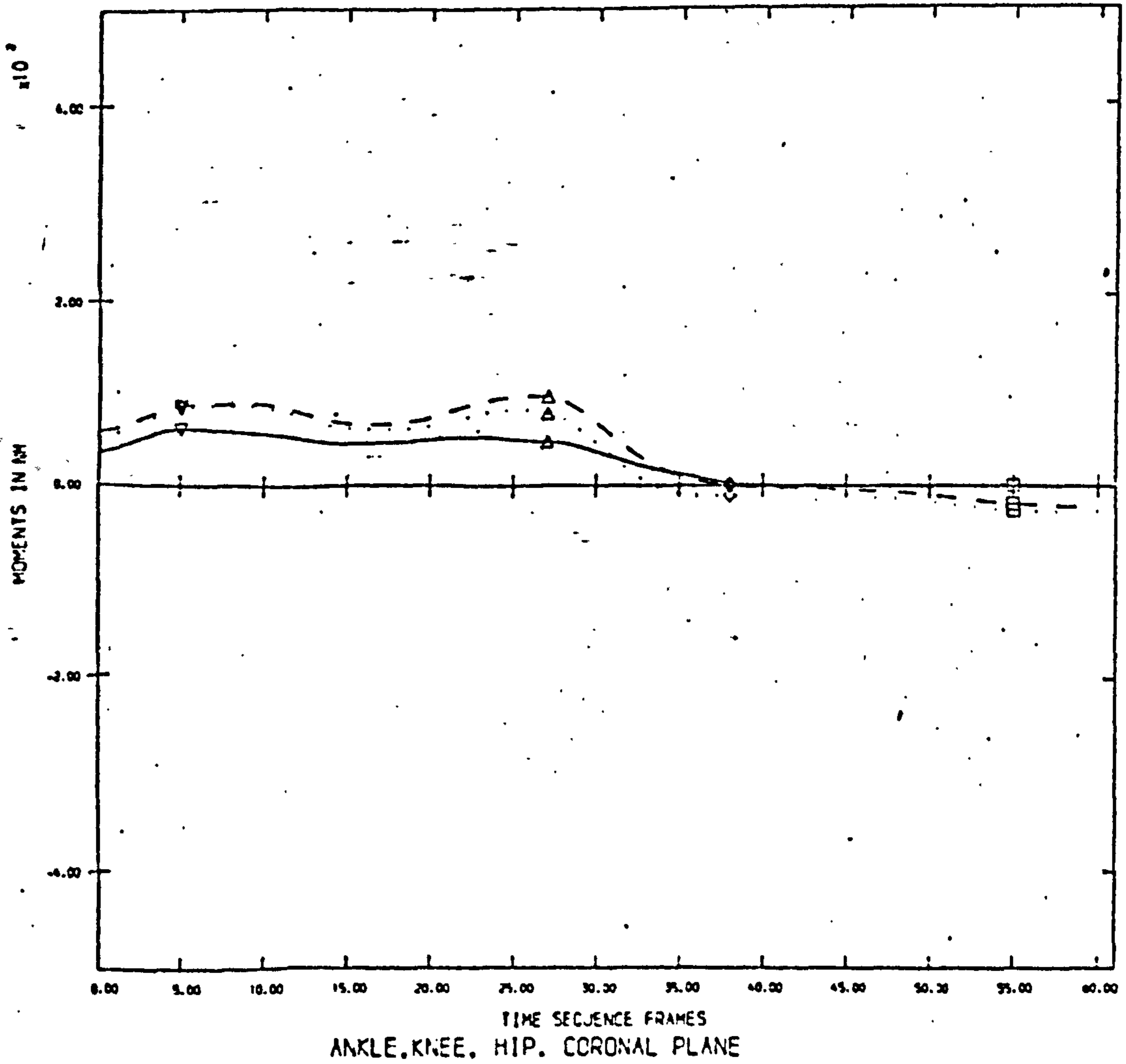
DASHED KNEE

RIGHT HEELSTRIKE  $\square$

DOTTED HIP

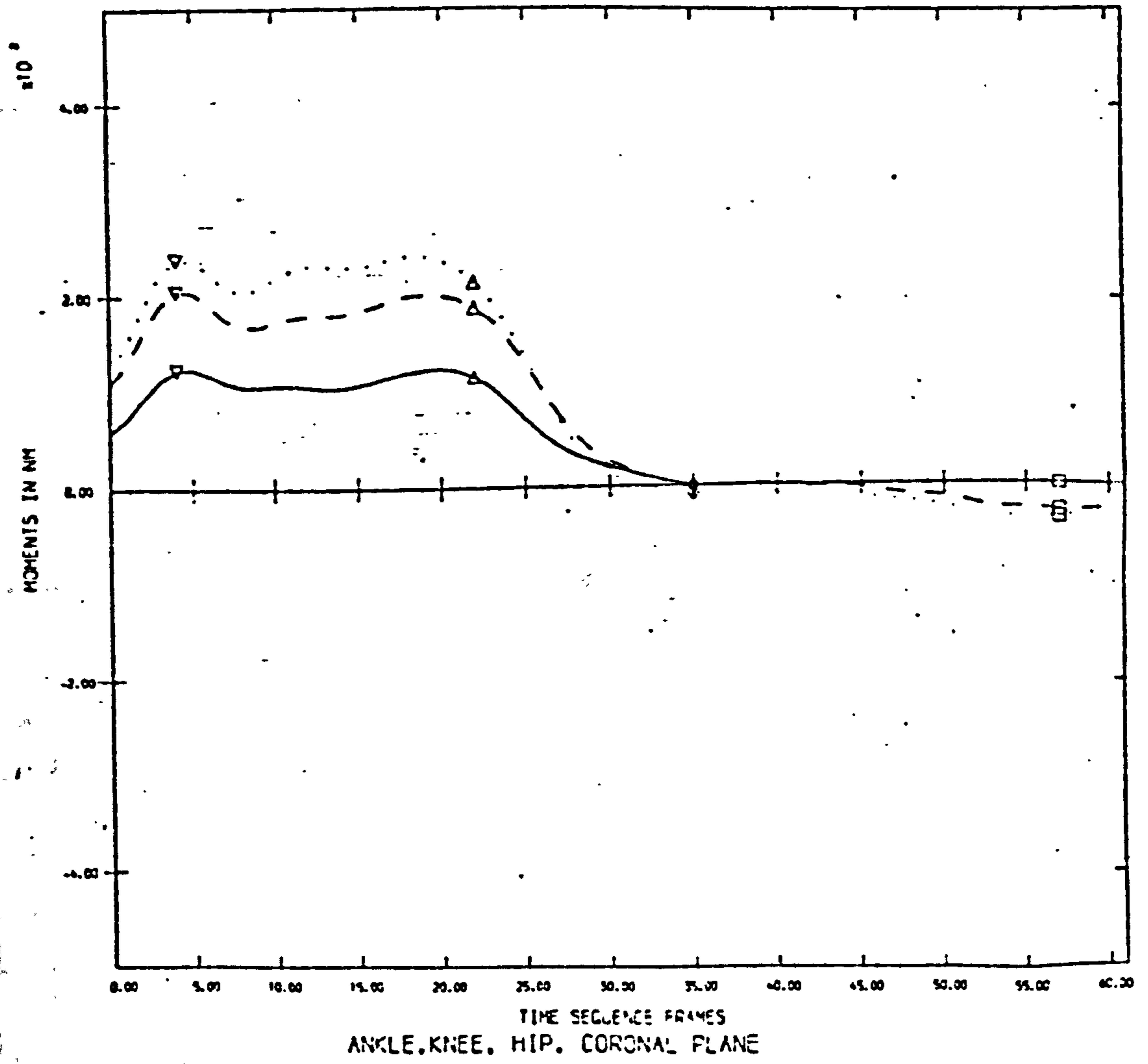
RIGHT TOE OFF  $\diamond$

S4/R/BDT1



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		

SS/R/BOT 1



LEFT HEEL STRIKE	▲	CONTINUOUS	ANKLE
LEFT TOE OFF	▼	DASHED	KNEE
RIGHT HEELSTRIKE	◻	DOTTED	HIP
RIGHT TOE OFF	◊		